

# **FRET Live-Cell Imaging and Quantitation Summer Workshop, 2015**

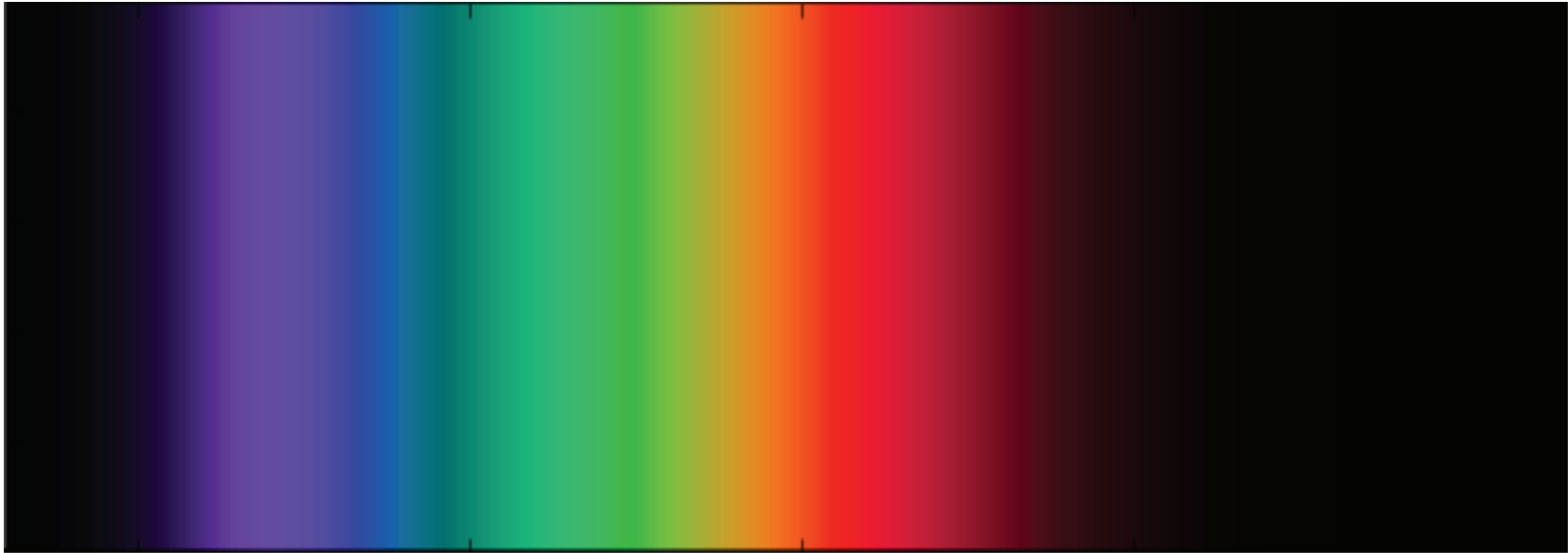
Fluorescence Microscopy : Fundamentals

Philbert S. Tsai

# The Visible Spectrum of Light

Higher Energy

Lower Energy



400

500

600

700

800

Shorter Wavelength

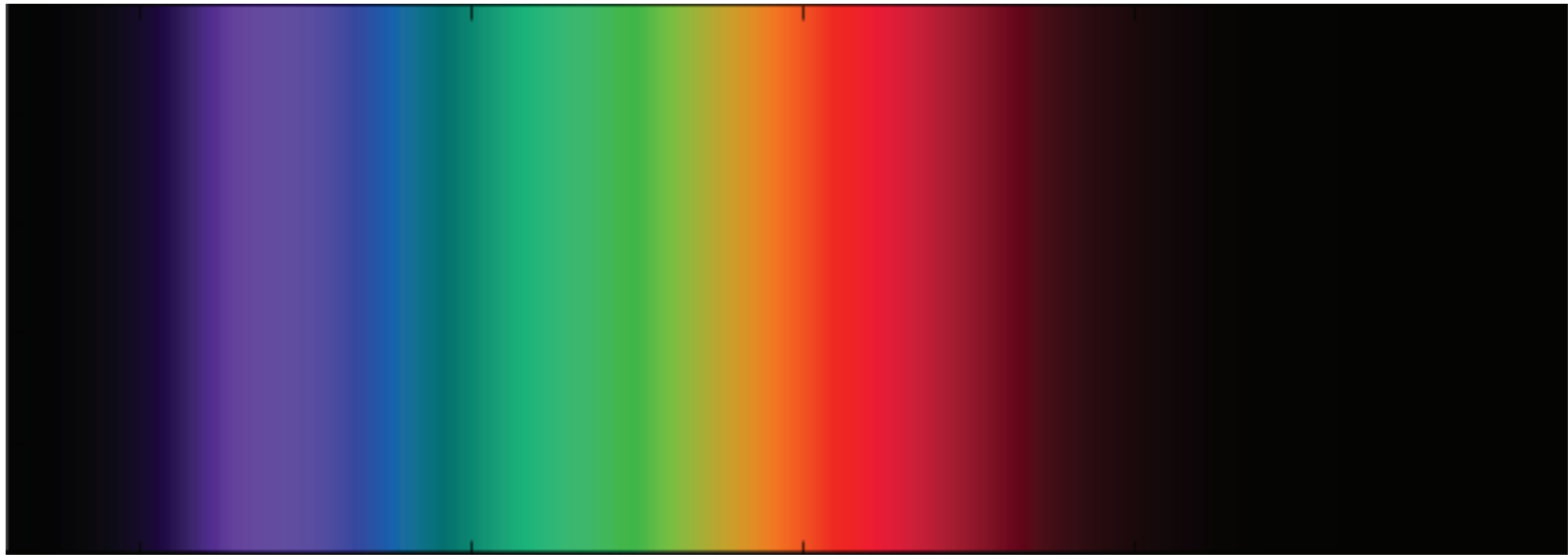
Wavelength (nm)

Longer Wavelength

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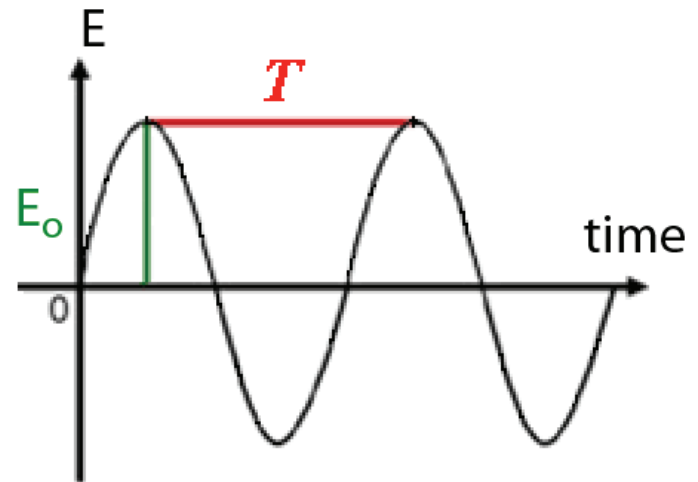
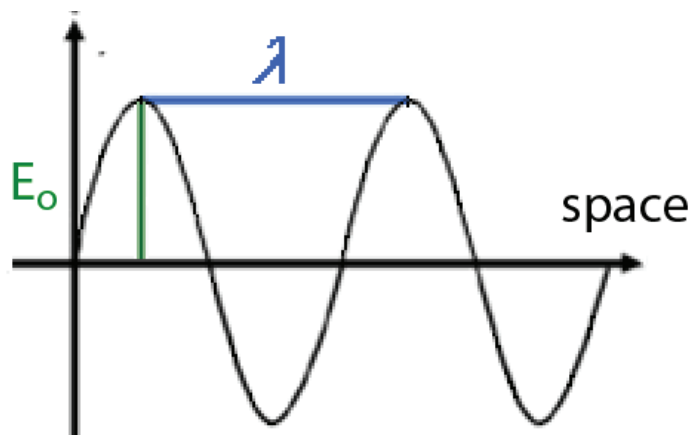
700

800

Shorter Wavelength

Wavelength (nm)

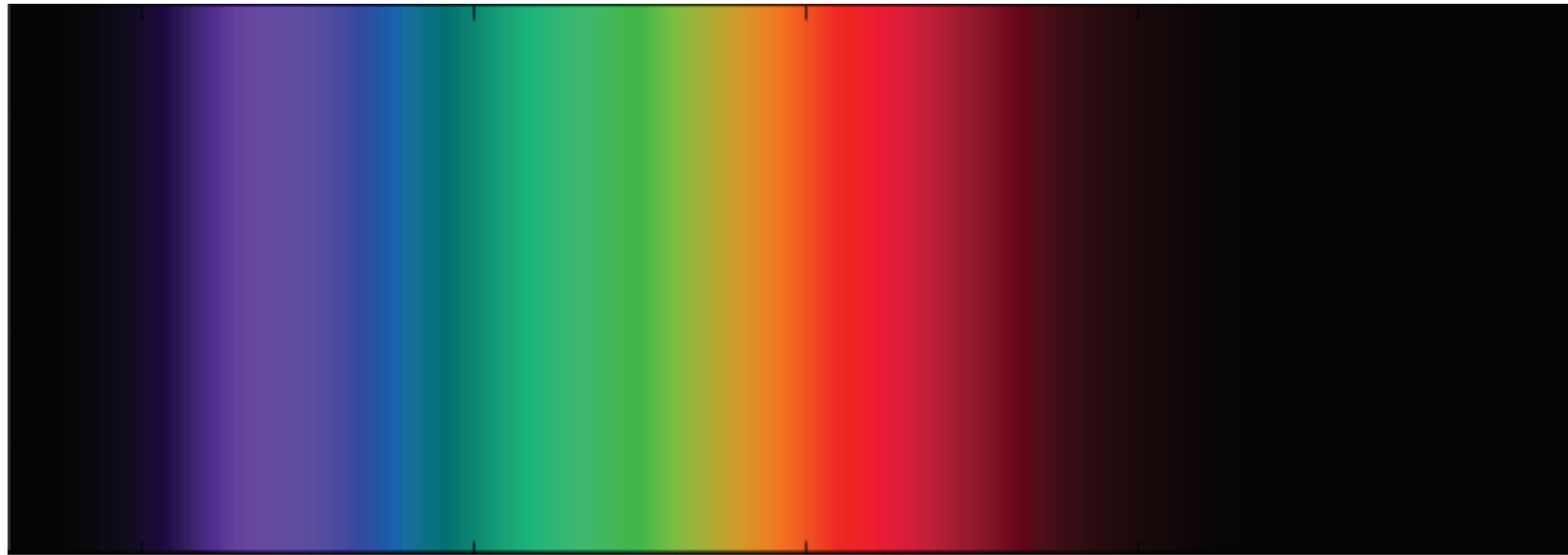
Longer Wavelength



# The Visible Spectrum of Light

Higher Energy

Lower Energy



Shorter Wavelength

Wavelength (nm)

Longer Wavelength

$$E = h * f \quad (\text{Photon Energy} = \text{Planck's Constant} * \text{Frequency})$$

$$E = h * c / \lambda$$

$$h = \text{Planck's Constant} = 6.626 * 10^{-34} \text{ J*s}$$

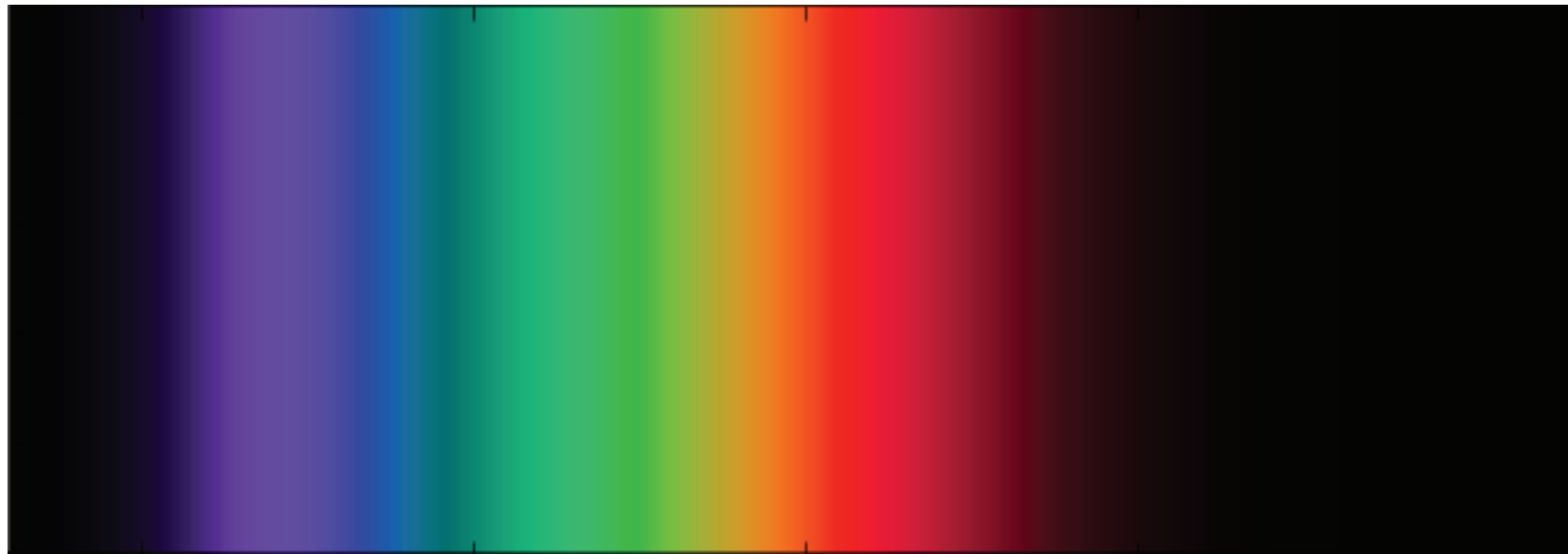
$$c = \text{speed of light} = 3 * 10^8 \text{ m/s}$$

$$\lambda = \text{wavelength}$$

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1 photon @ 546 nm

$$E = 3.64 * 10^{-19} \text{ J*s}$$

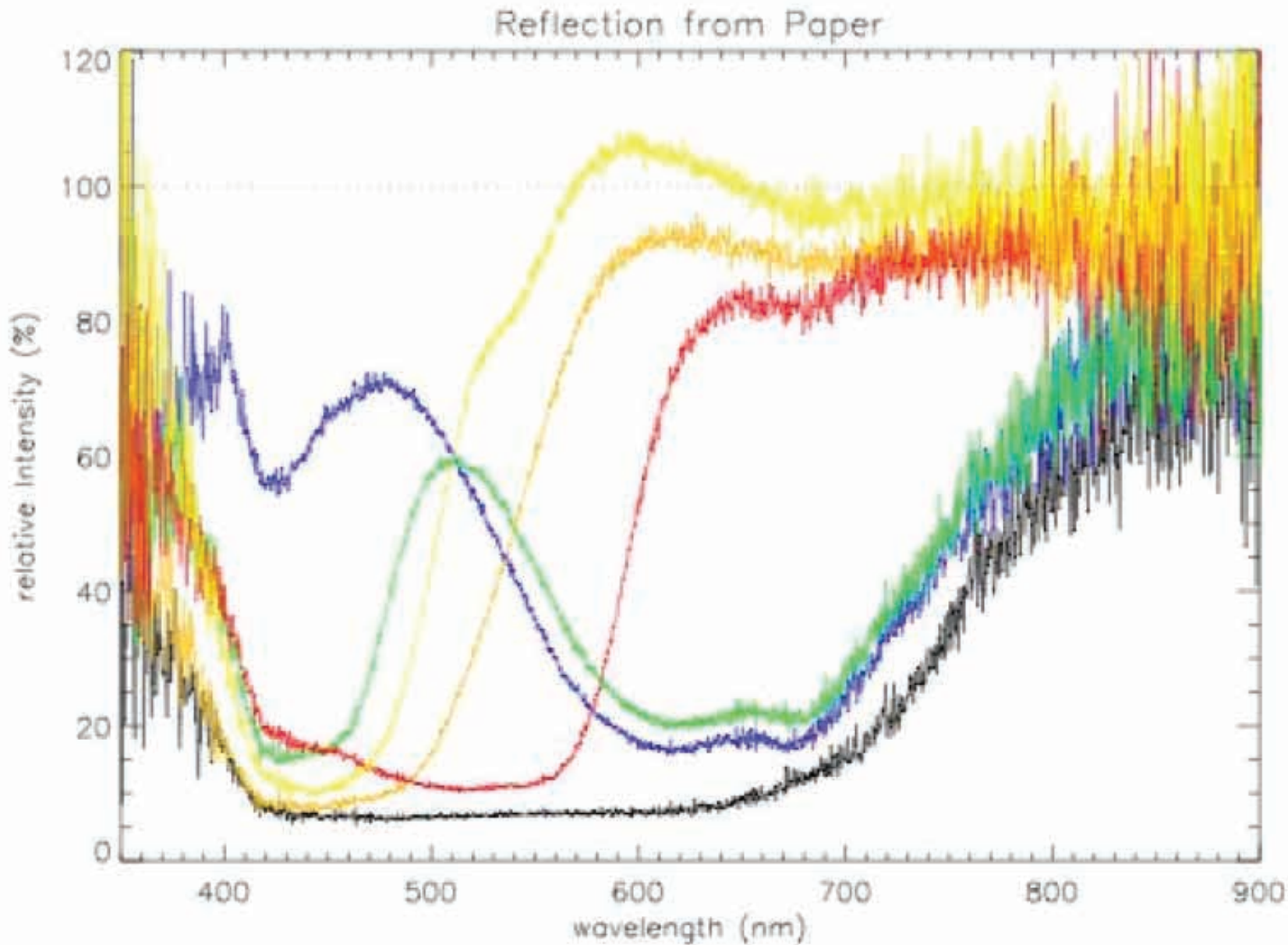
so:

1 Watt = 1 Joule/sec

$$= 2.7 * 10^{18} \text{ photons / s}$$



# Reflectance spectra from colored paper

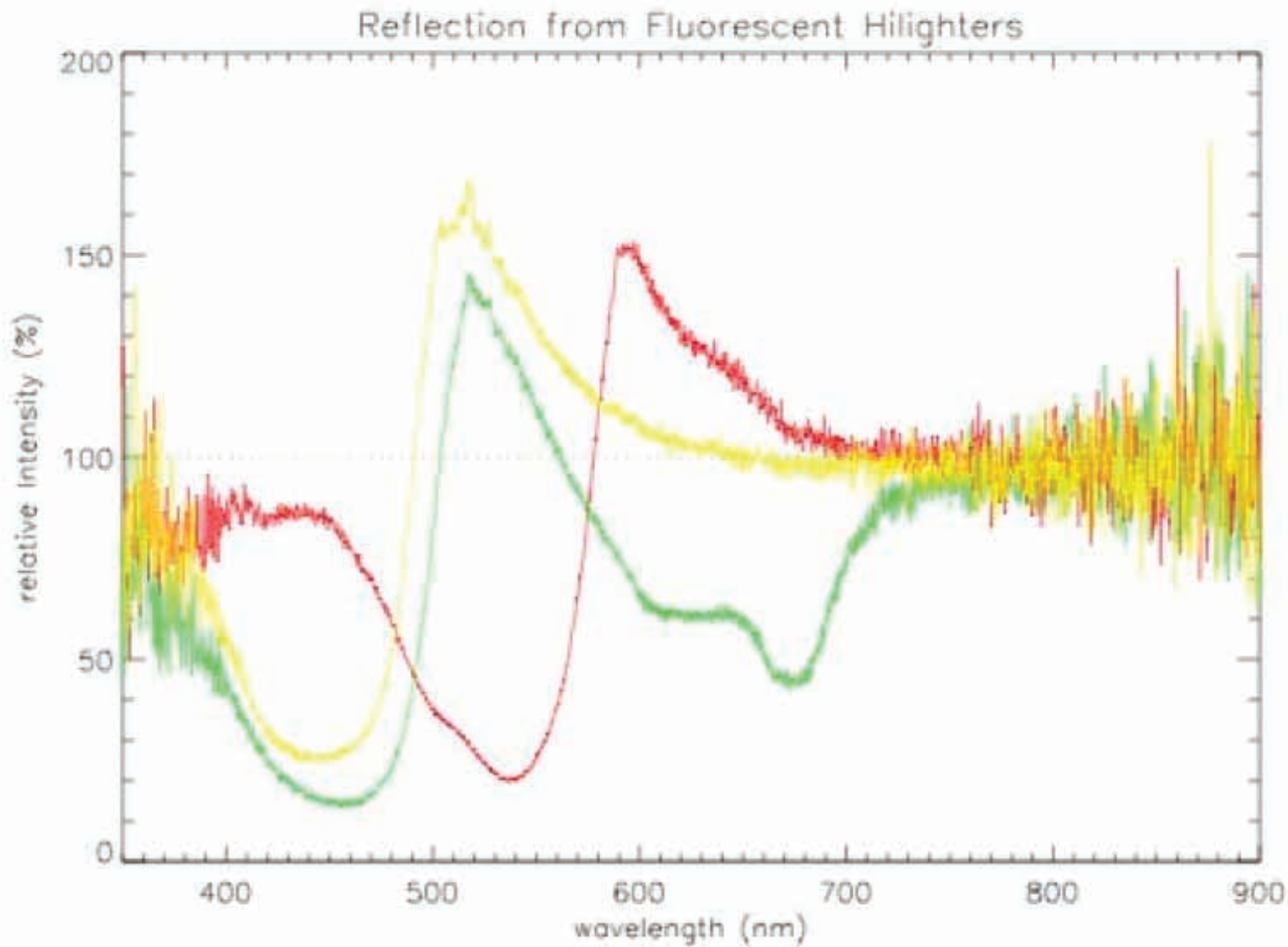


Spectra of sunlight reflecting off of color papers appearing :

- blue
- green
- yellow
- orange
- red
- black

aside from slight fluorescence in the yellow paper, colors operating by reflectance only never peak above 100%

# Emission spectra for fluorescent markers (highlighter pens)



Fluorescent markers convert light from lower wavelengths to higher wavelengths.

green highlighter  
yellow highlighter  
pink highlighter

All three highlighters have emissions that exceed the 100% that would be possible from reflection alone.



# Fluorescence

Luminescence that is caused by the absorption of radiation at one wavelength followed by nearly immediate re-radiation usually at a longer wavelength.

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# Microscopy

*An unfortunate series of compromises*  
that we are forced to make to look at very small objects.

# Fluorescence

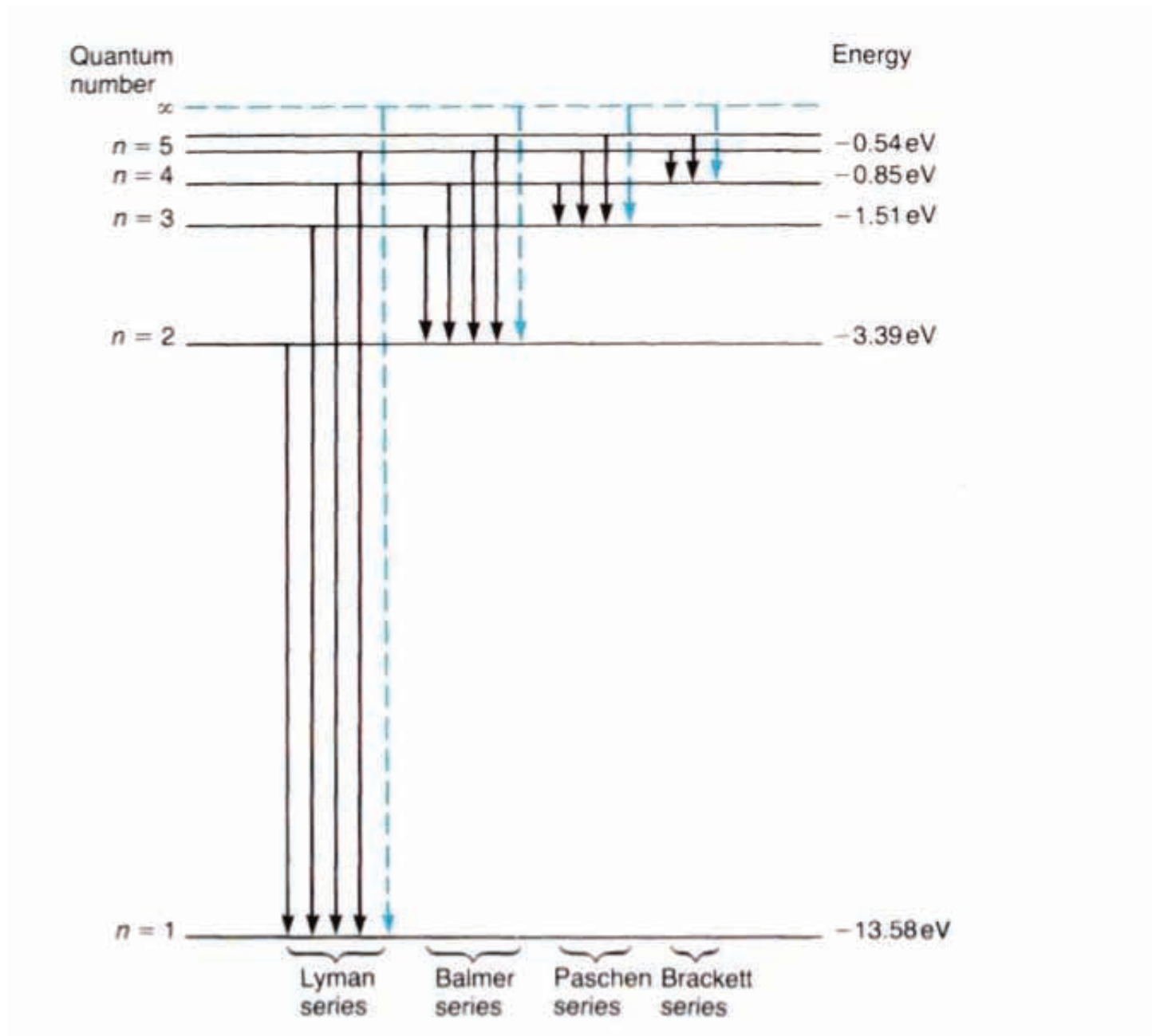
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# Microscopy

**An unfortunate series of compromises**  
that we are forced to make to look at very small objects.

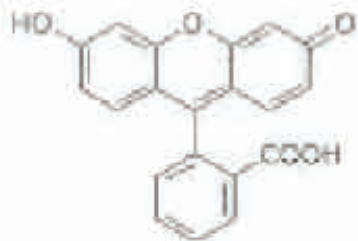
- Resolution
- Specificity
- Signal to Noise
- Speed
- Uniformity
- Phototoxicity
- \$\$\$\$

# Energy levels for atomic spectra of hydrogen

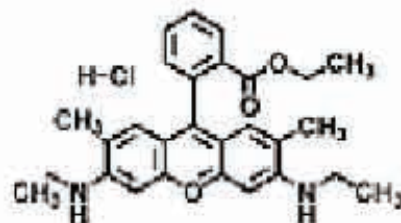


# Absorption & emission spectra of fluorescent organic dyes

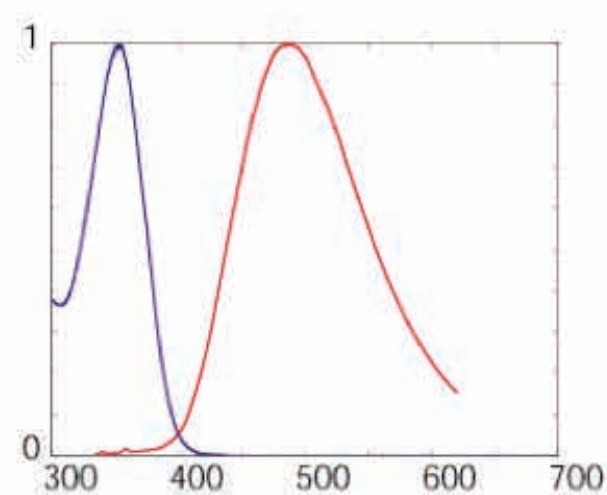
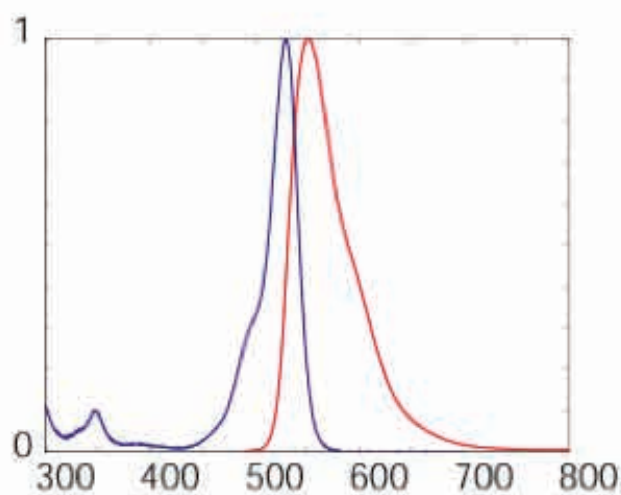
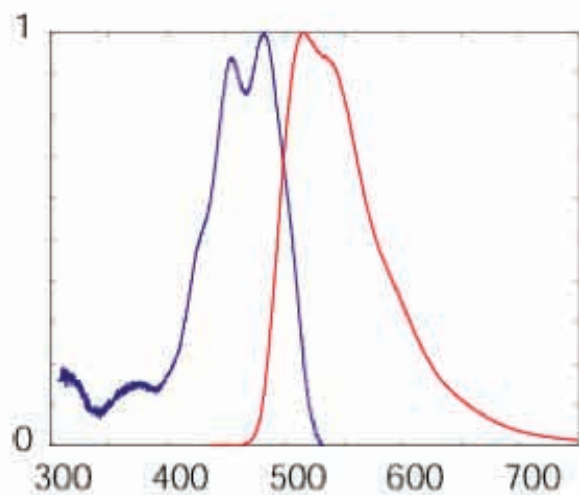
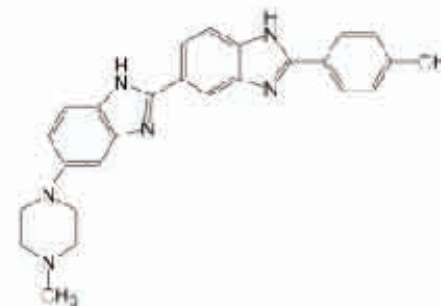
Fluorescein



Rhodamine 6G



Hoechst 33258

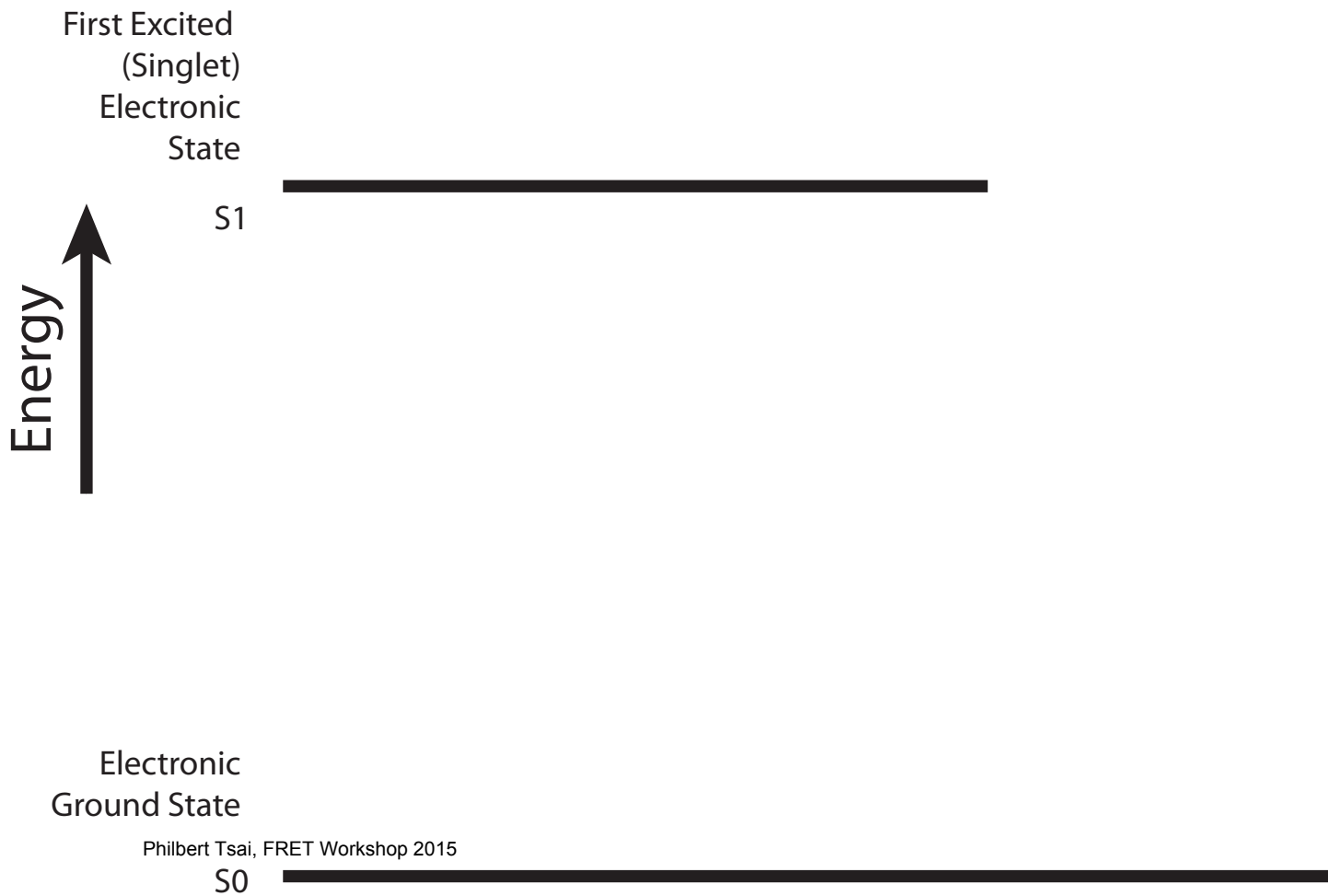


Wavelength (nm)

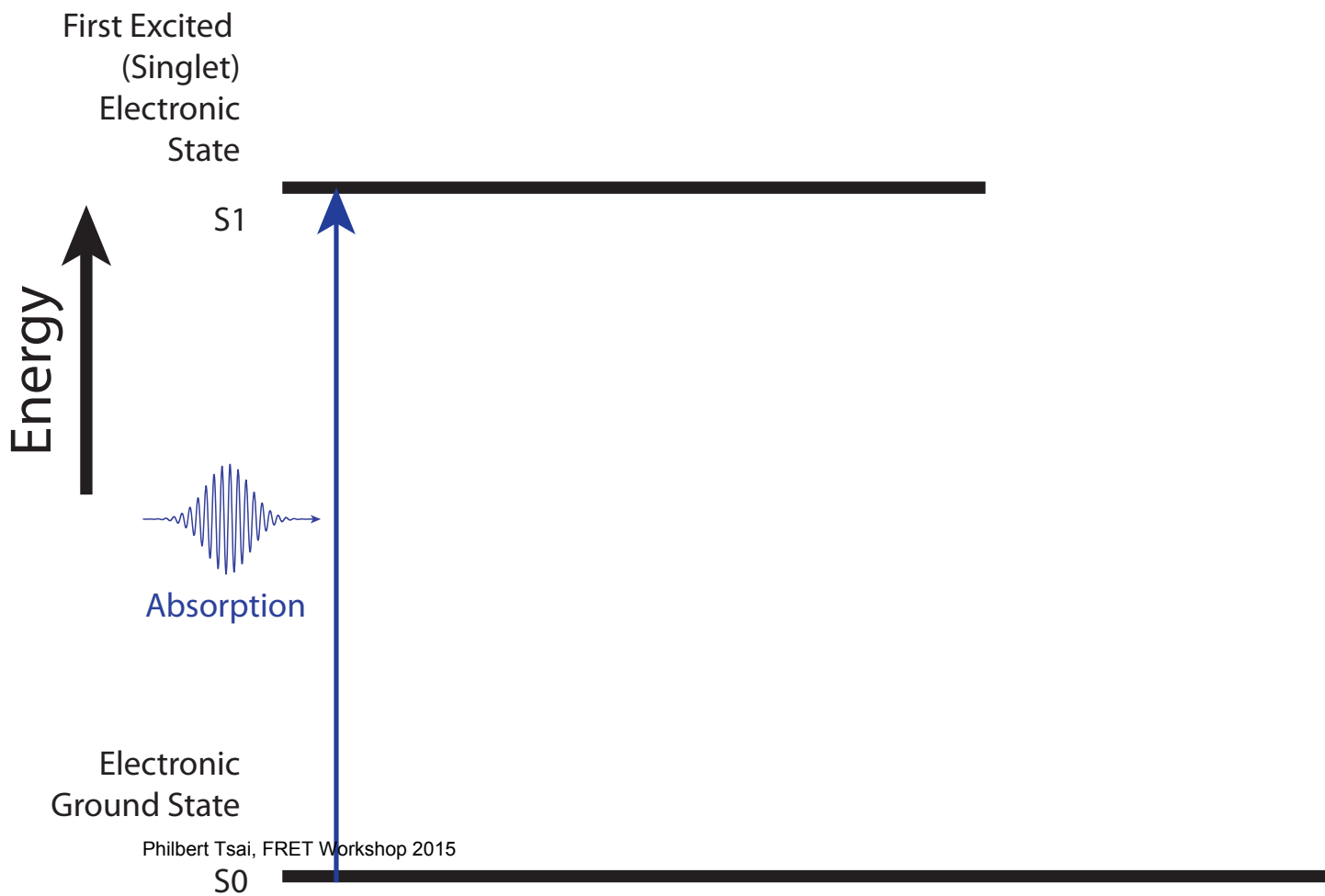
— Normalized Absorption Spectrum

— Normalized Fluorescence Emission Spectrum

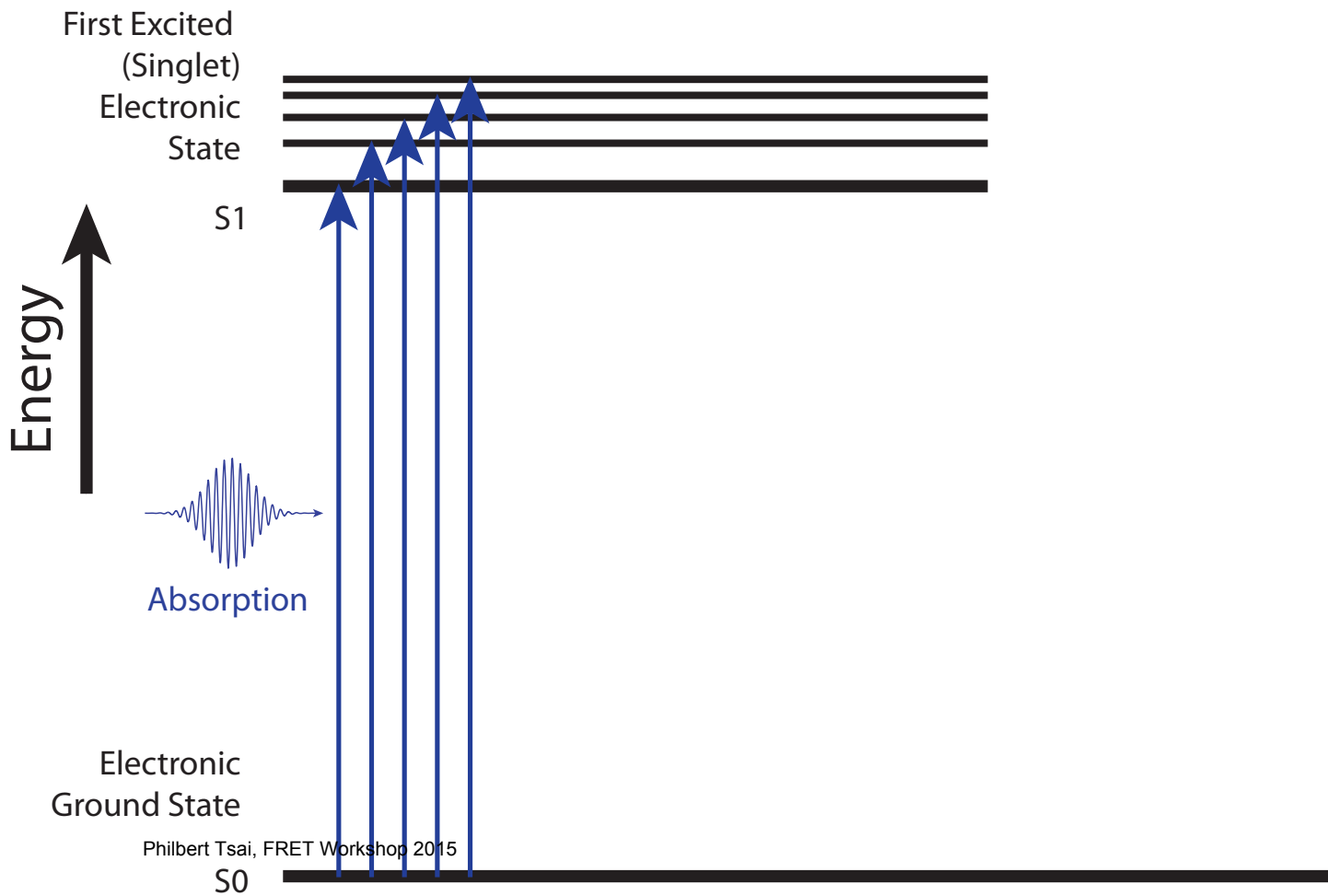
# Jablonski Energy Diagram



# Jablonski Energy Diagram

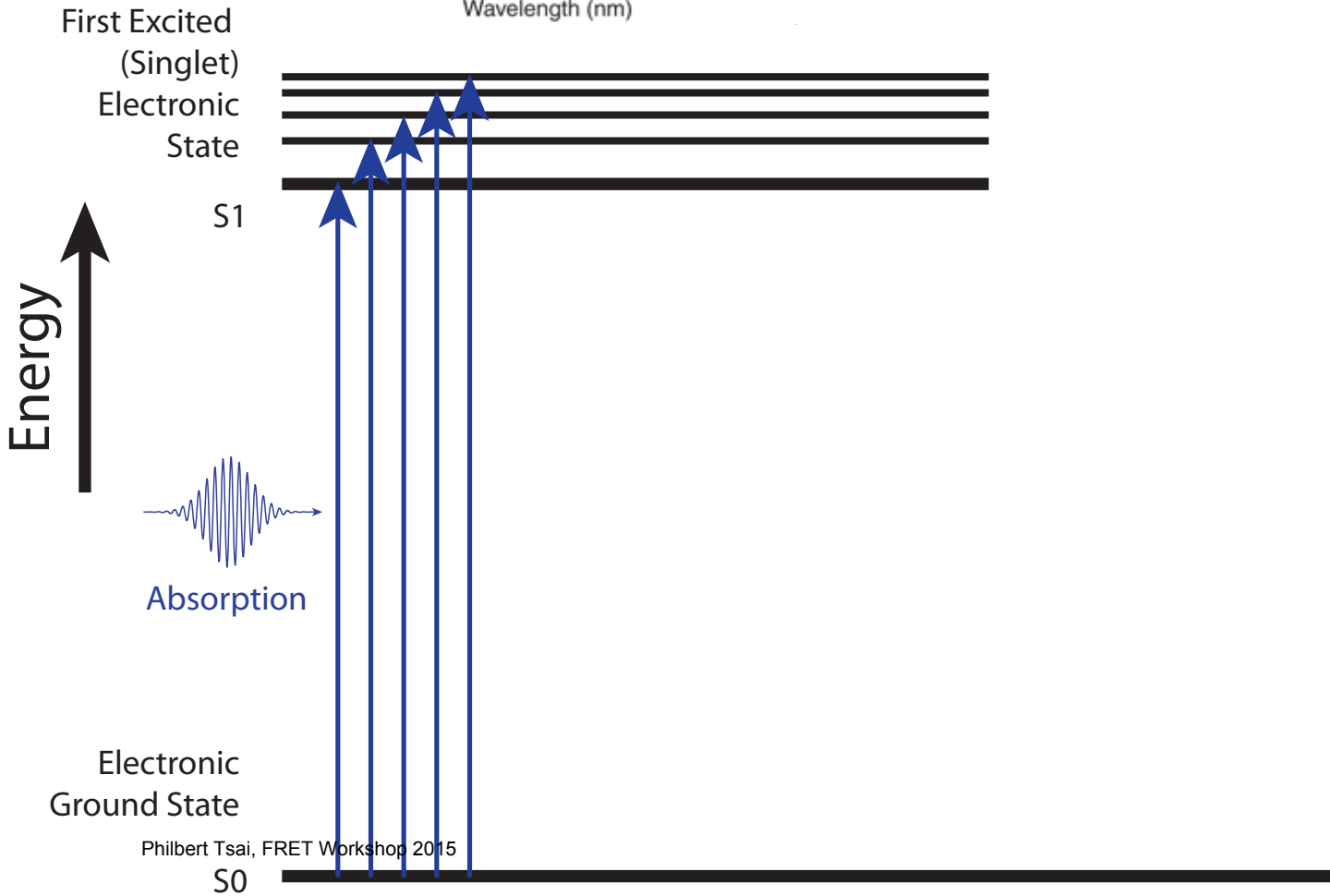
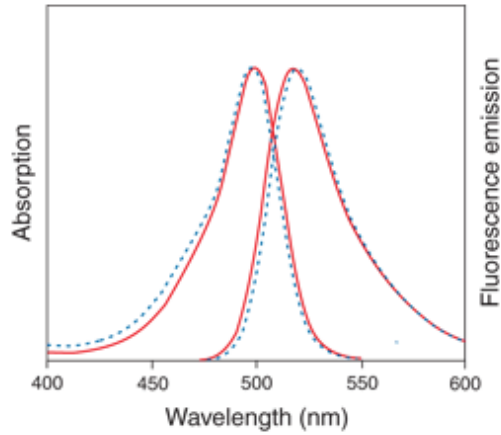


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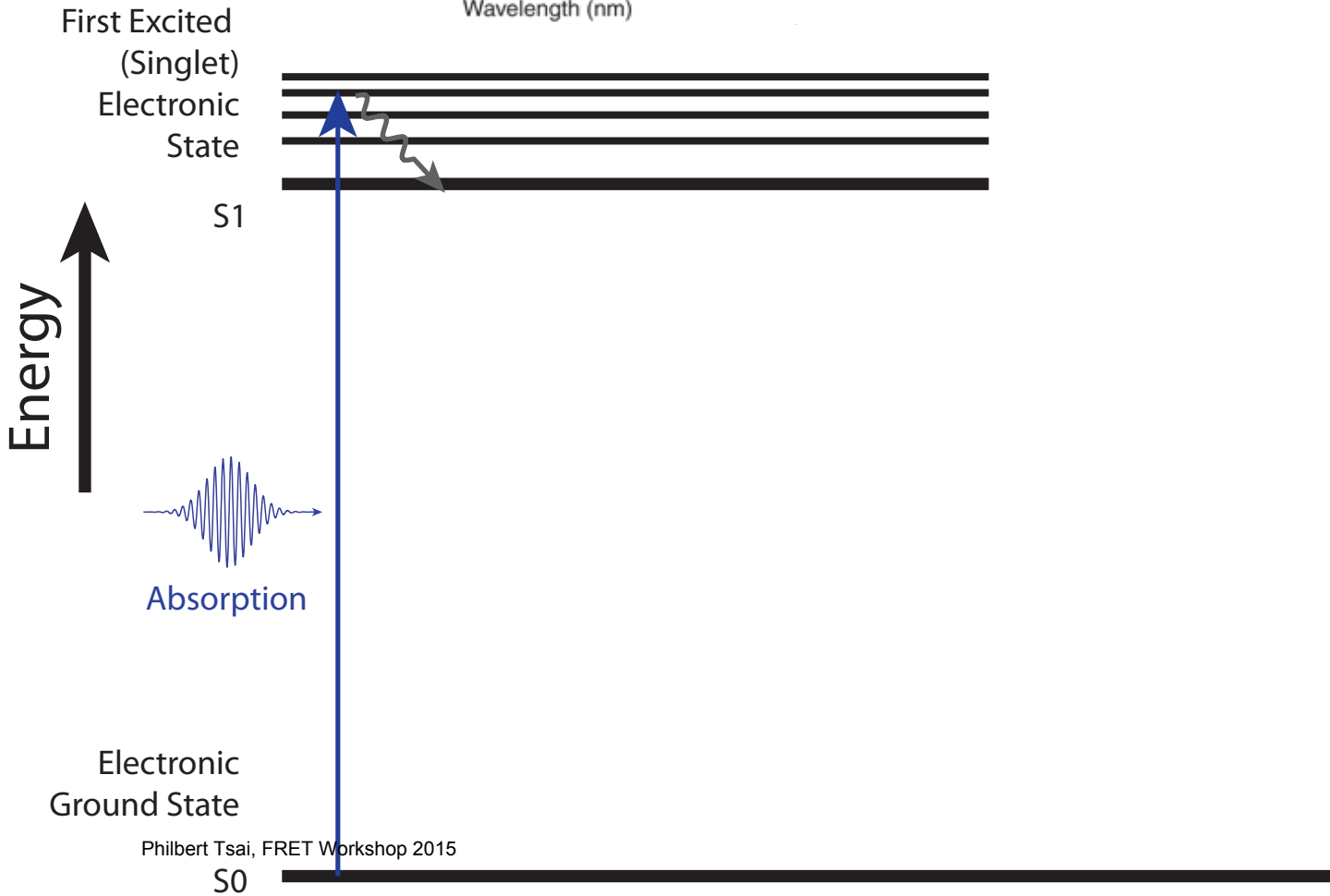
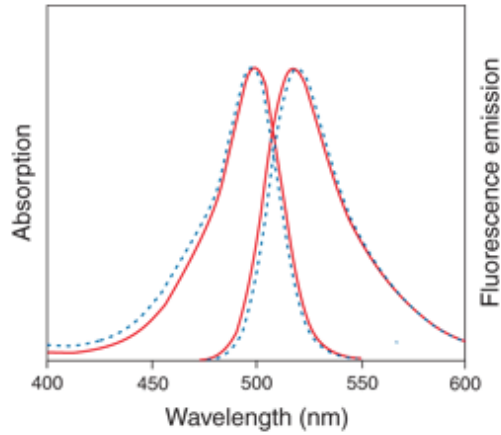




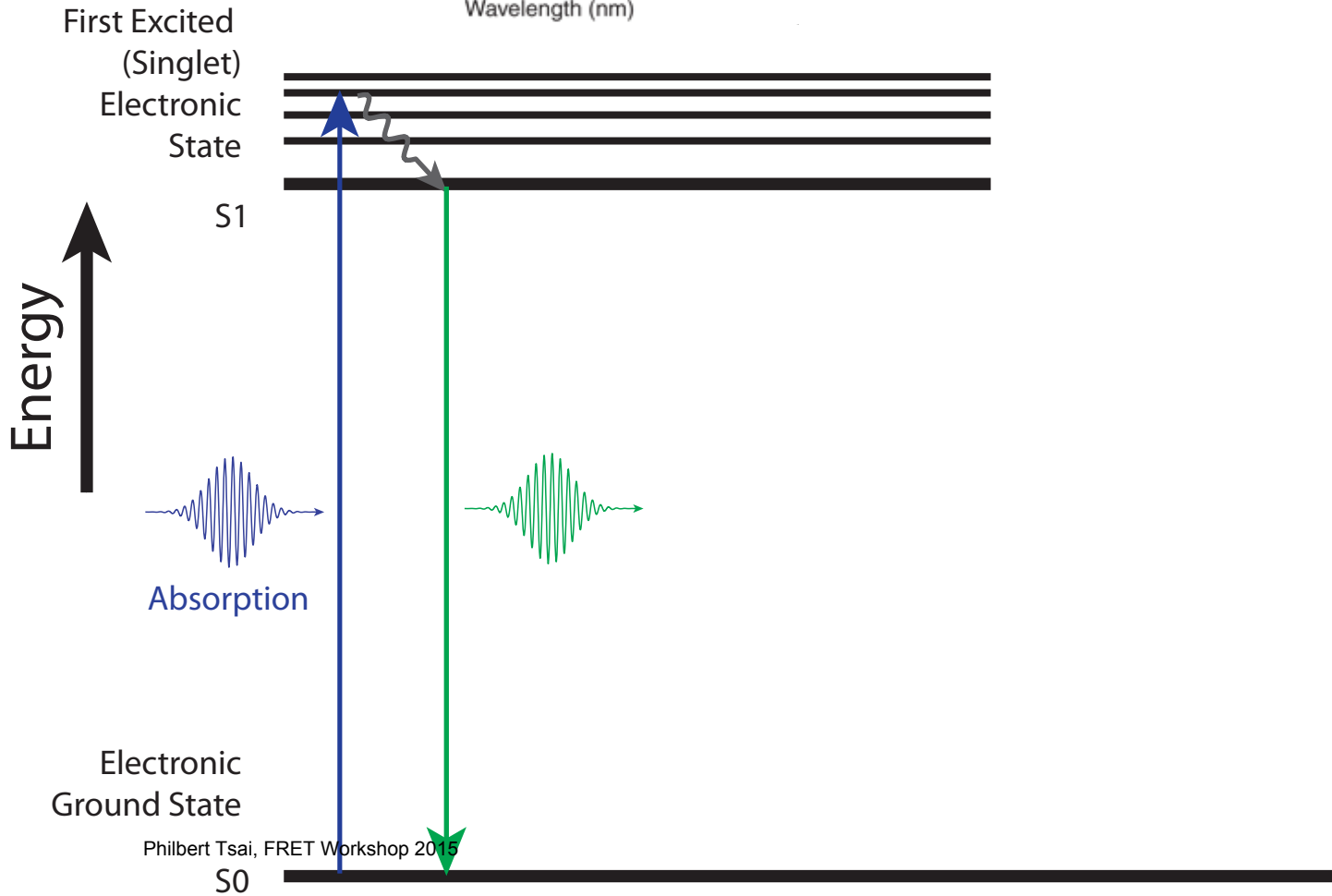
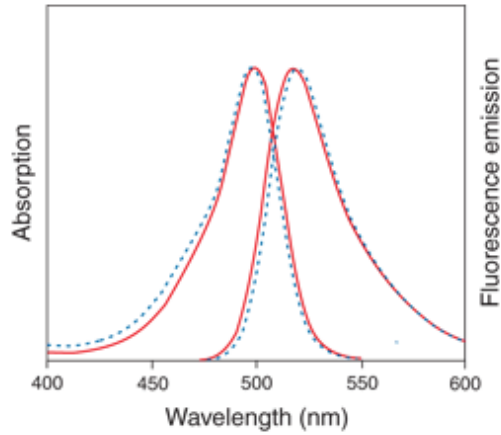
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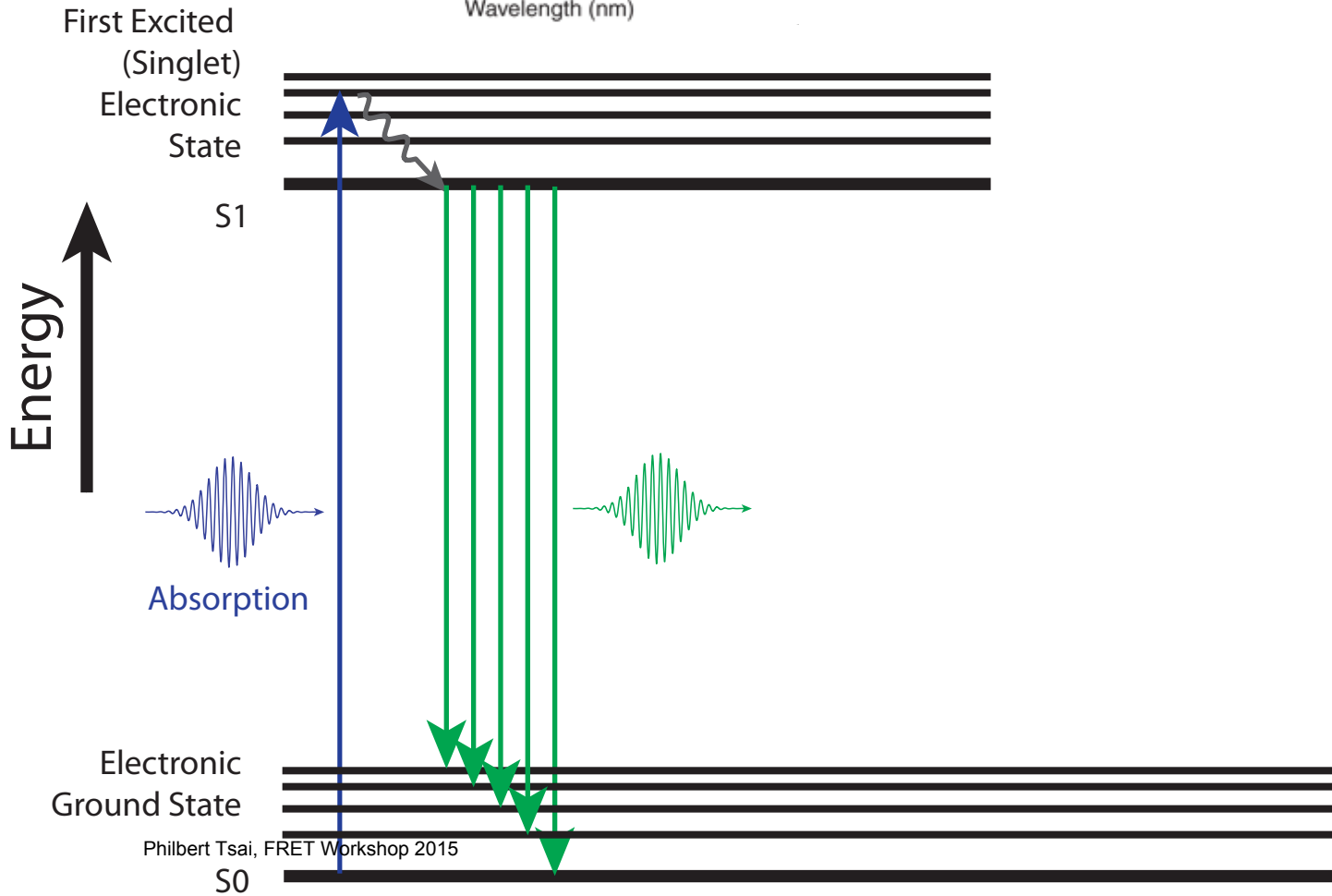
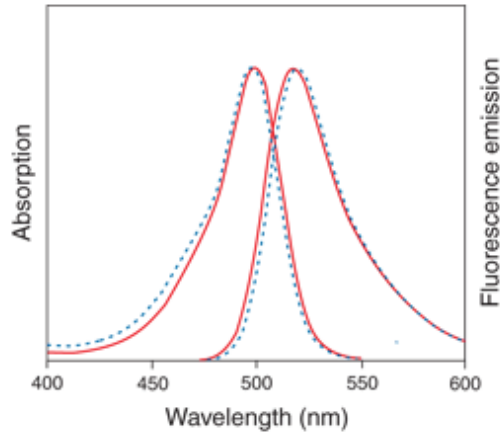
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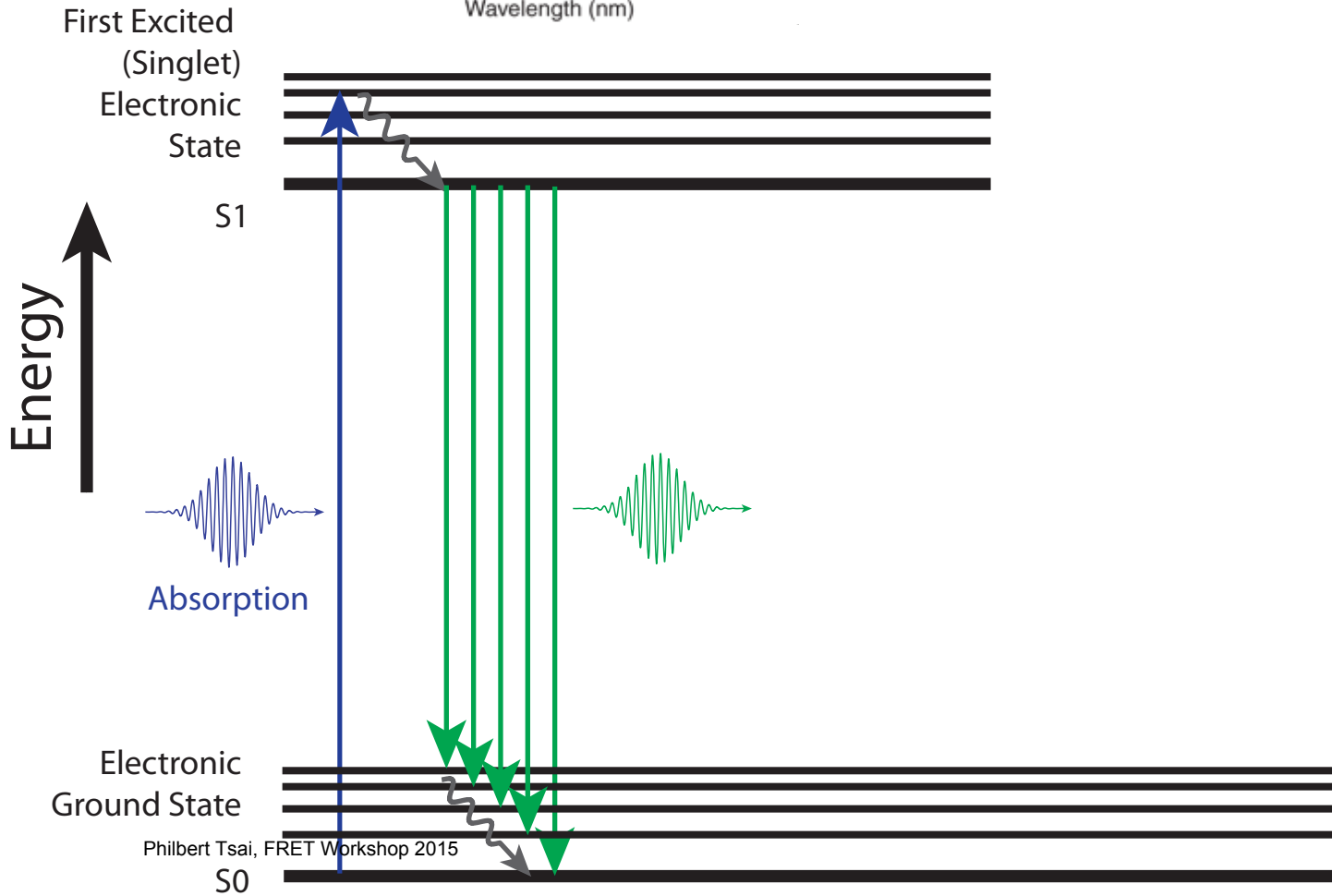
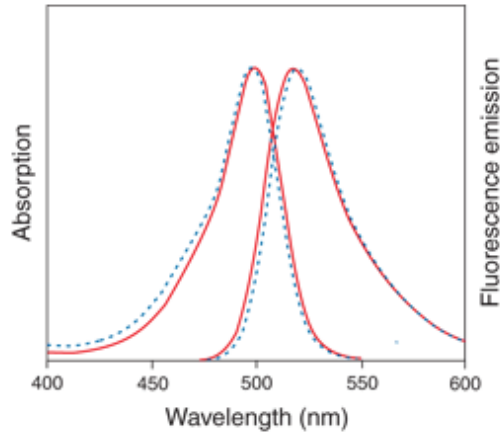
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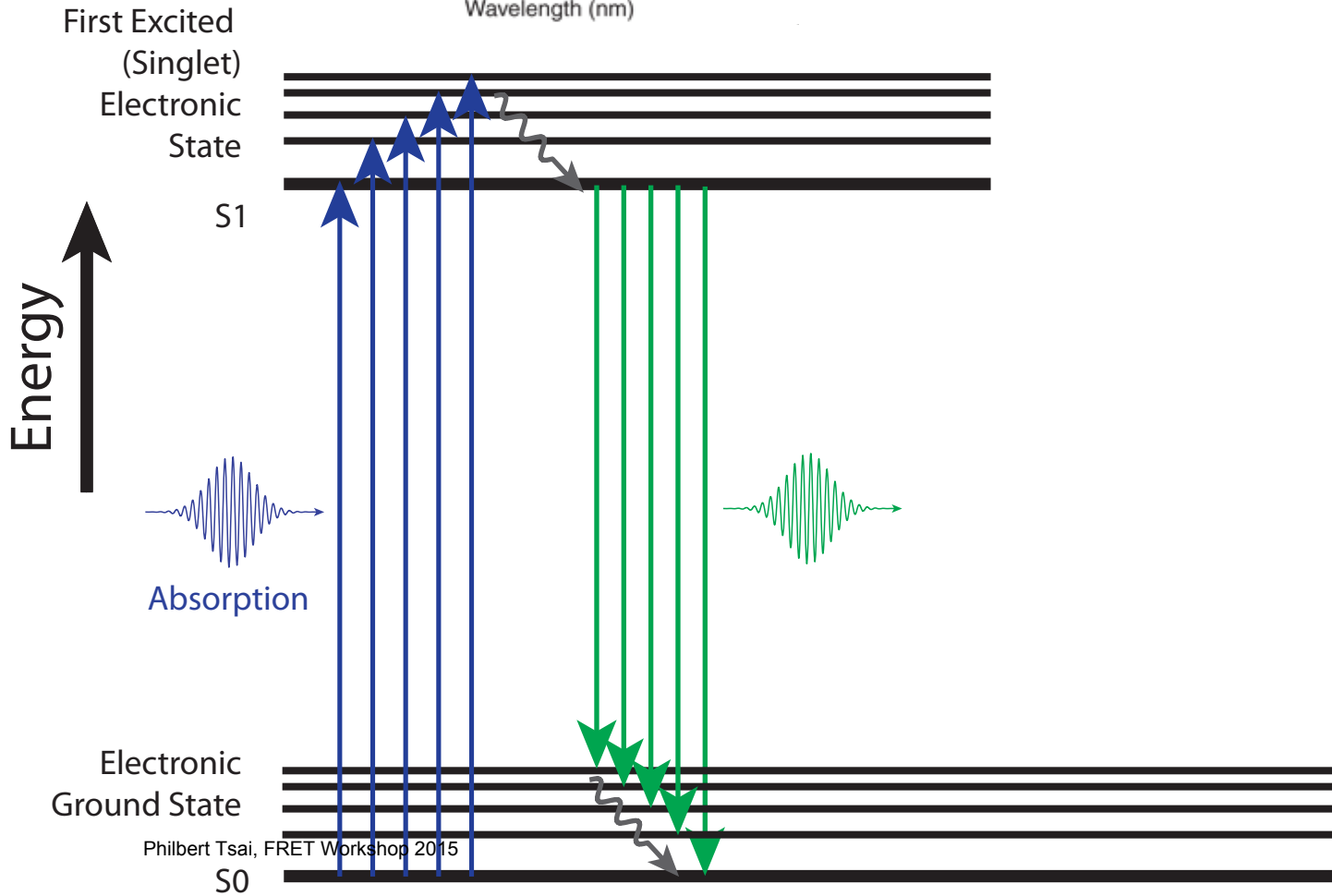
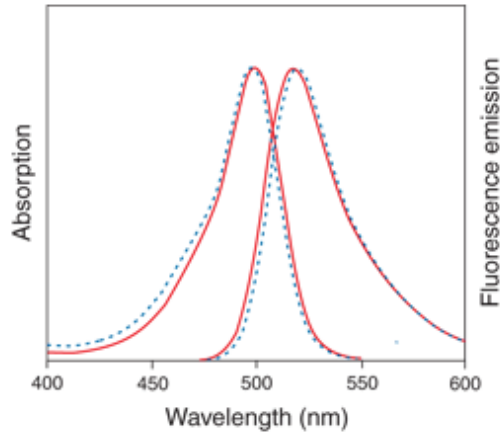
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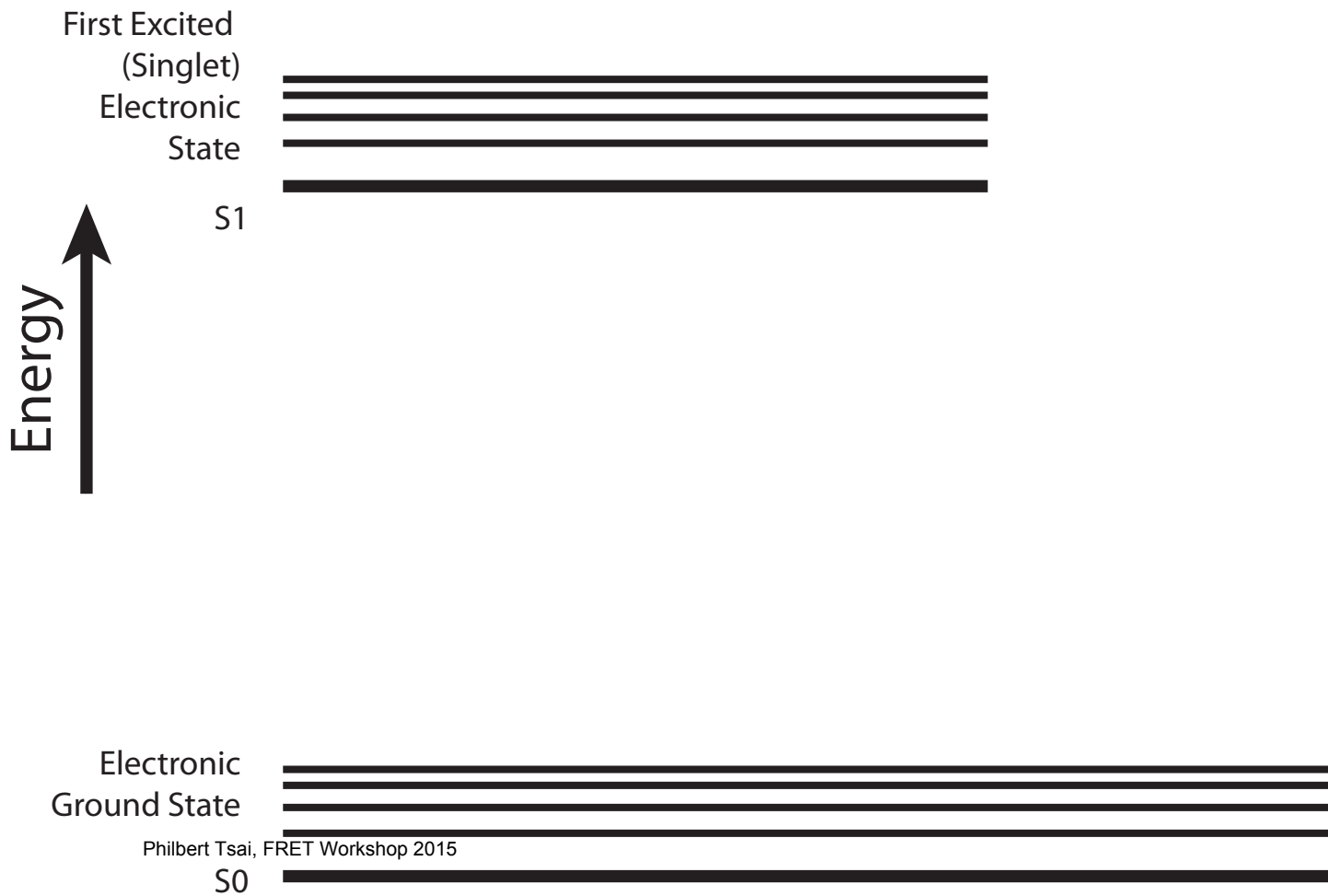
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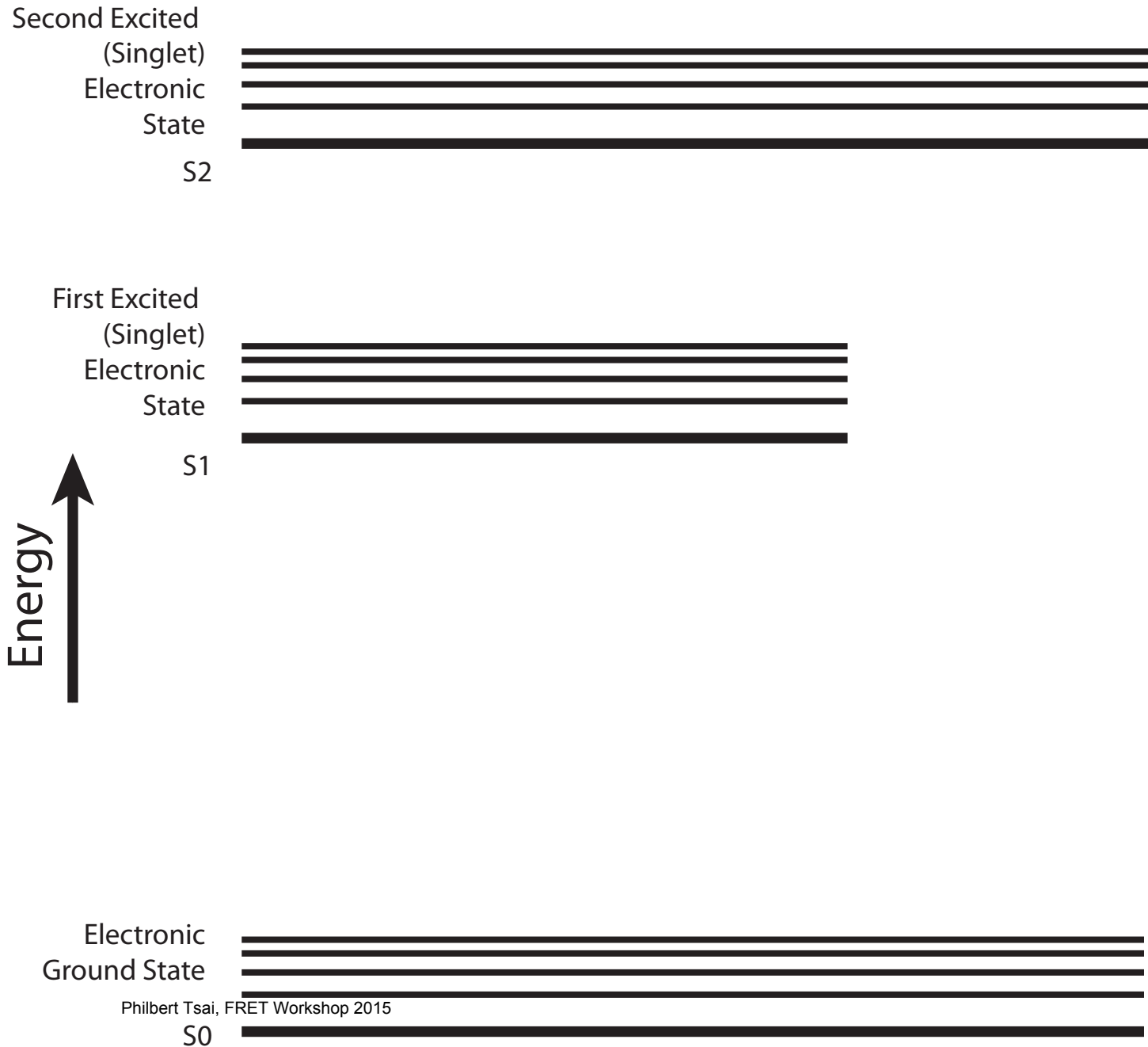
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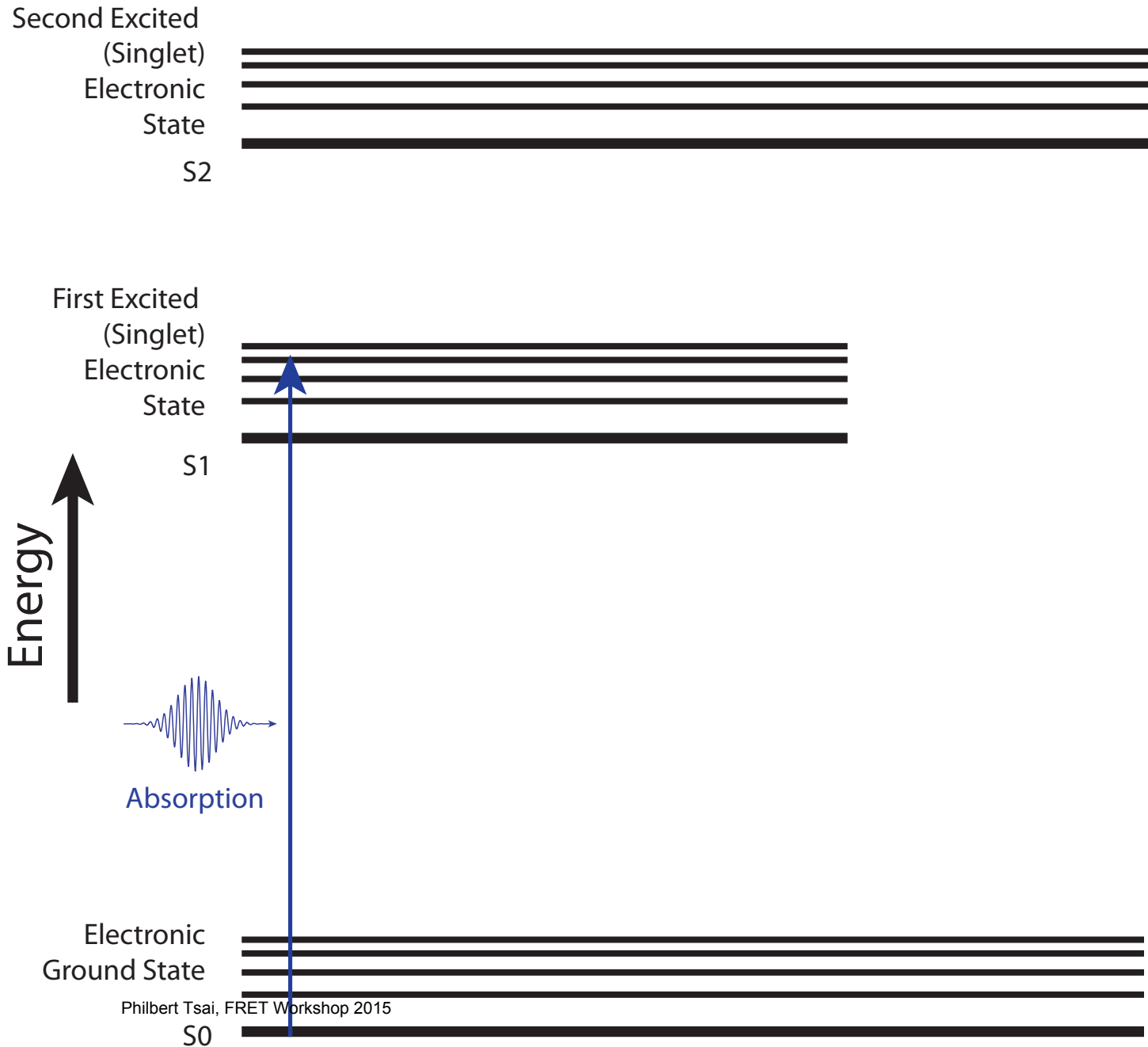


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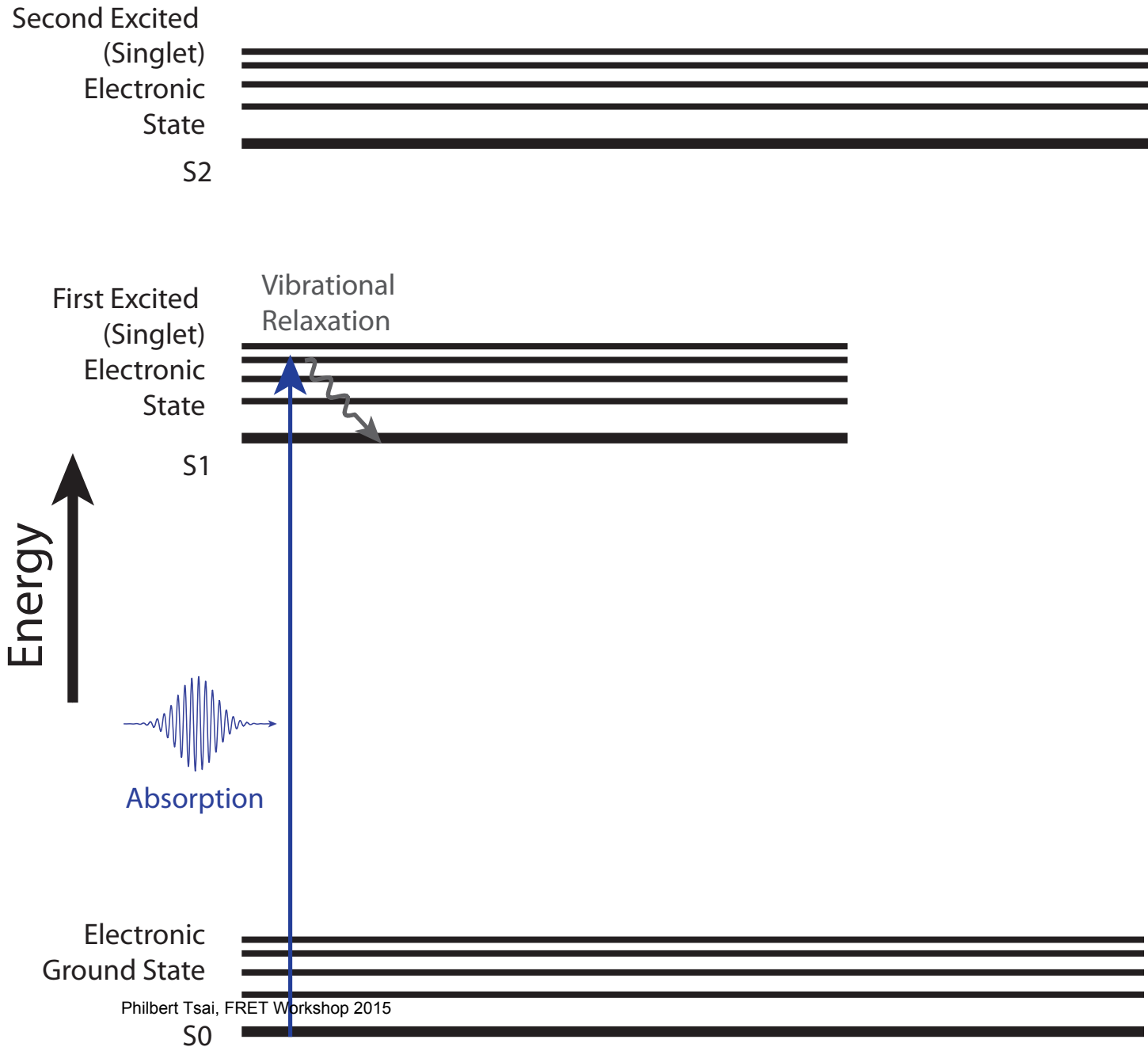




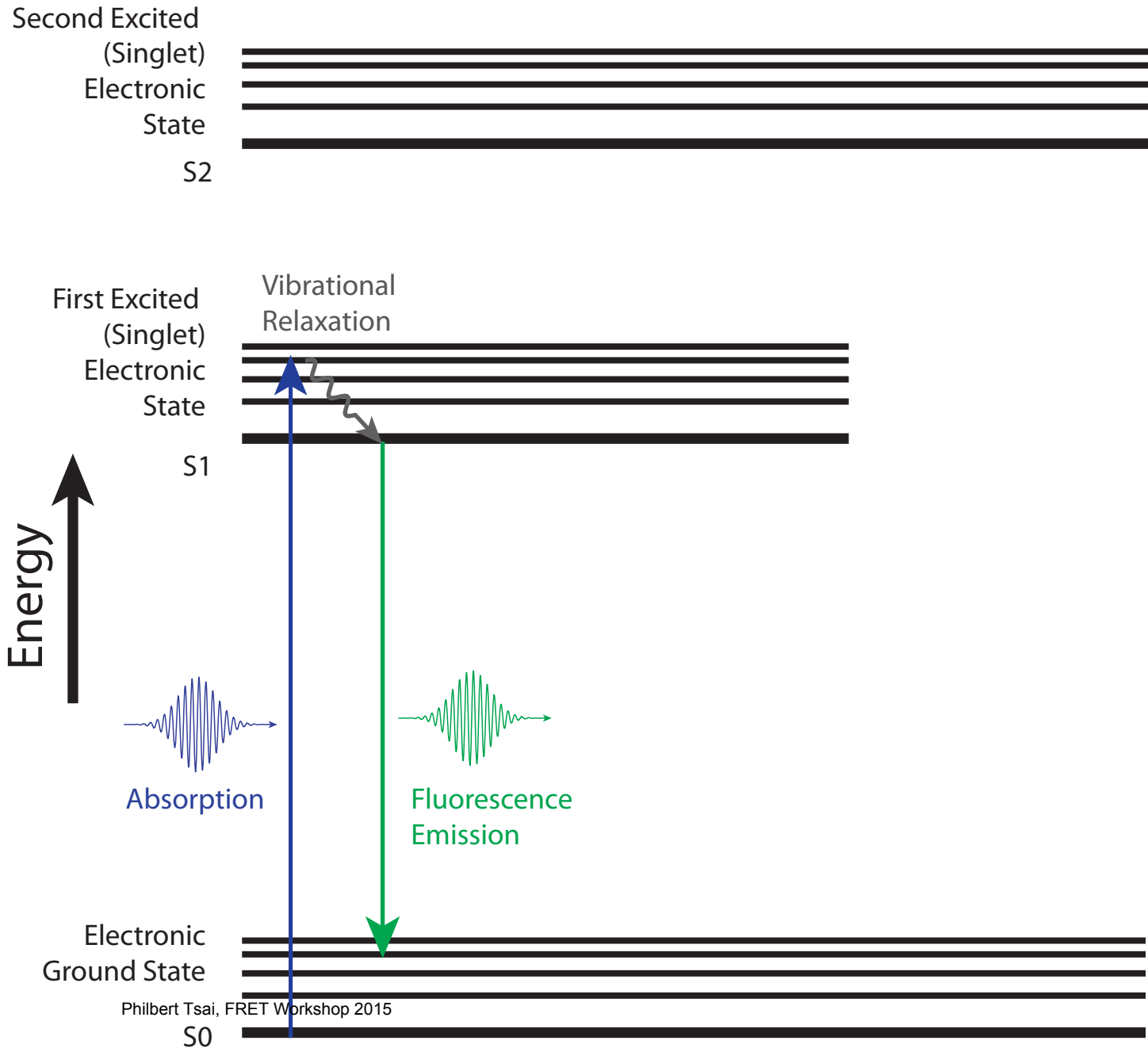
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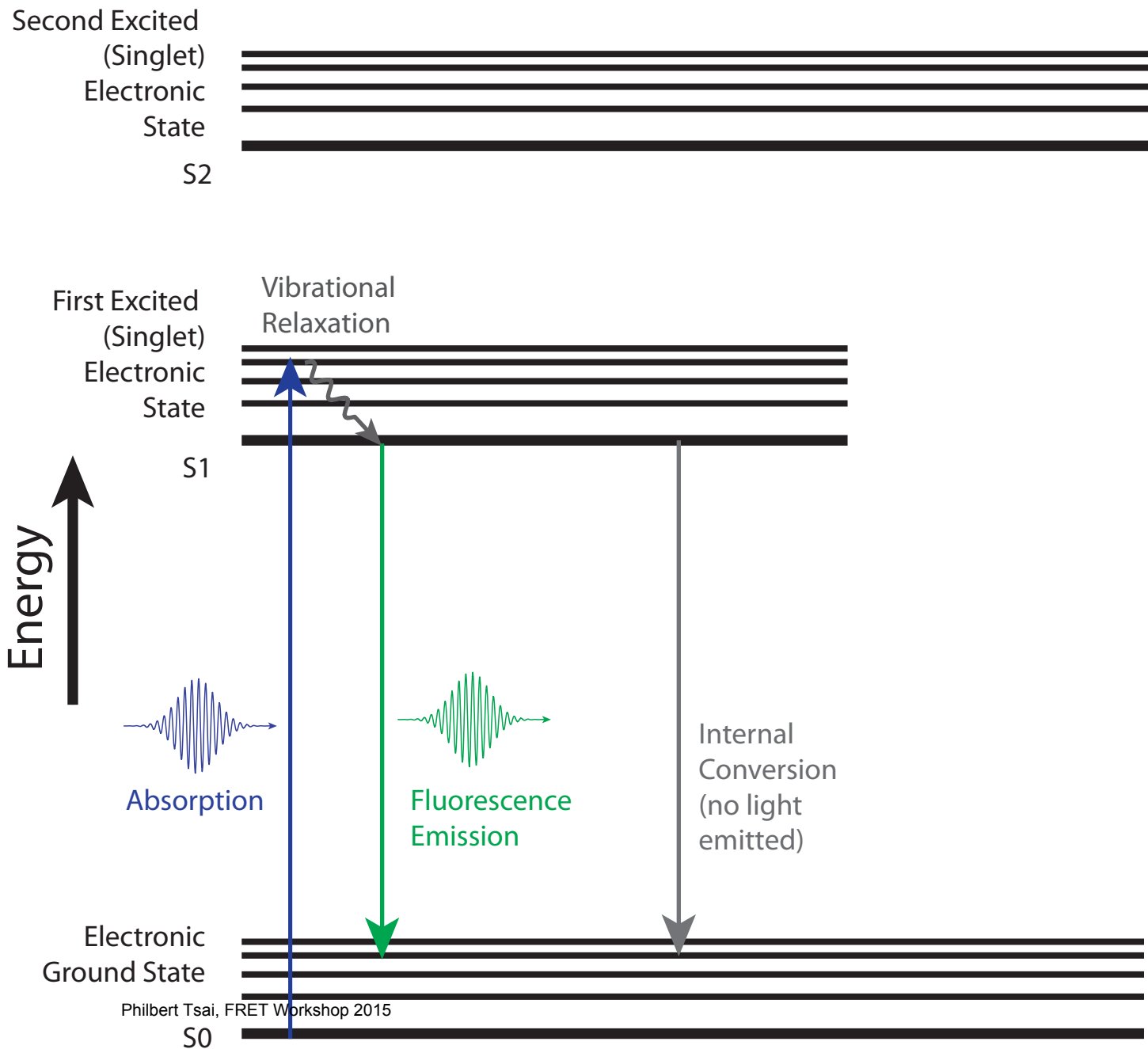
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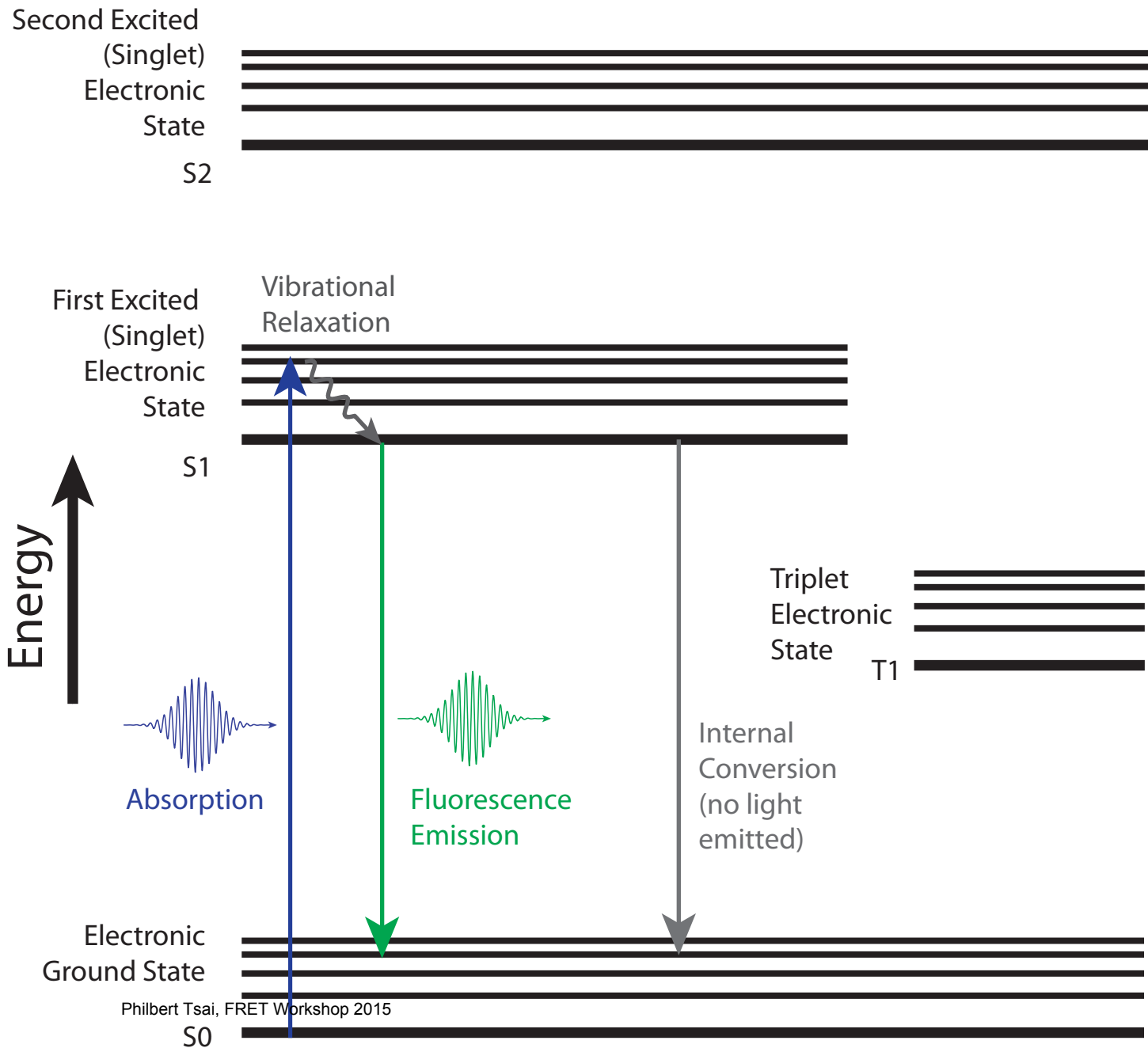
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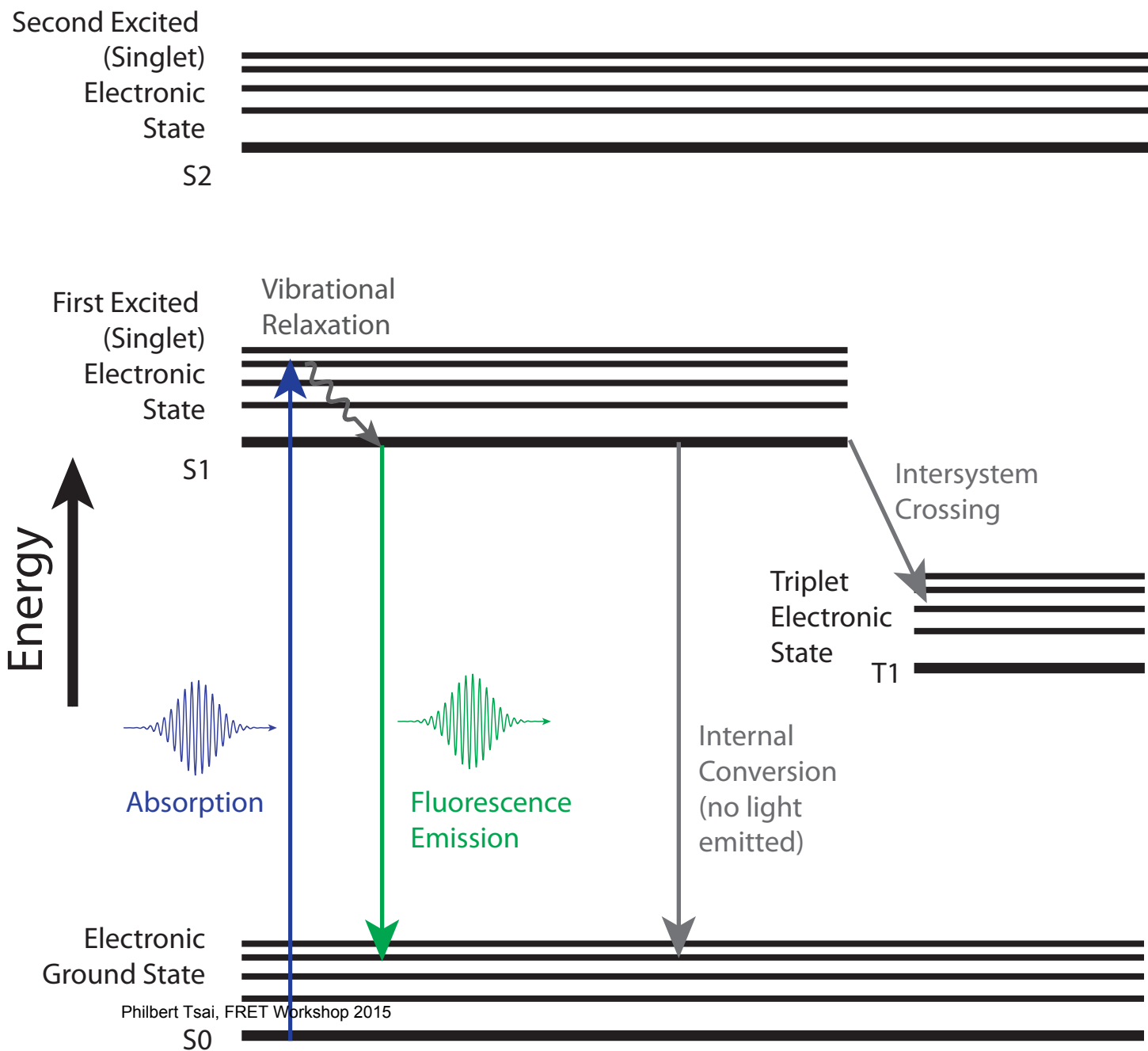
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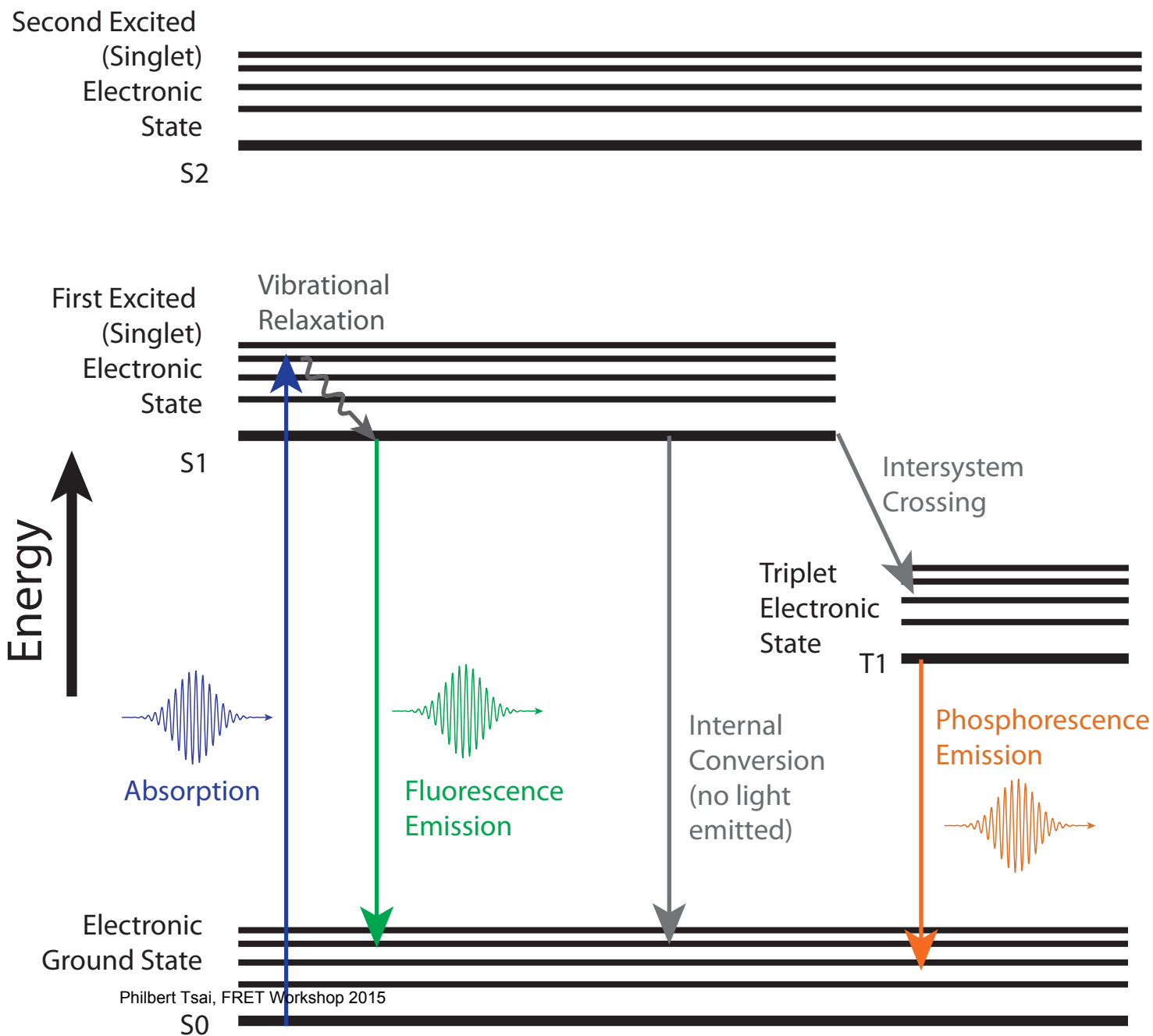
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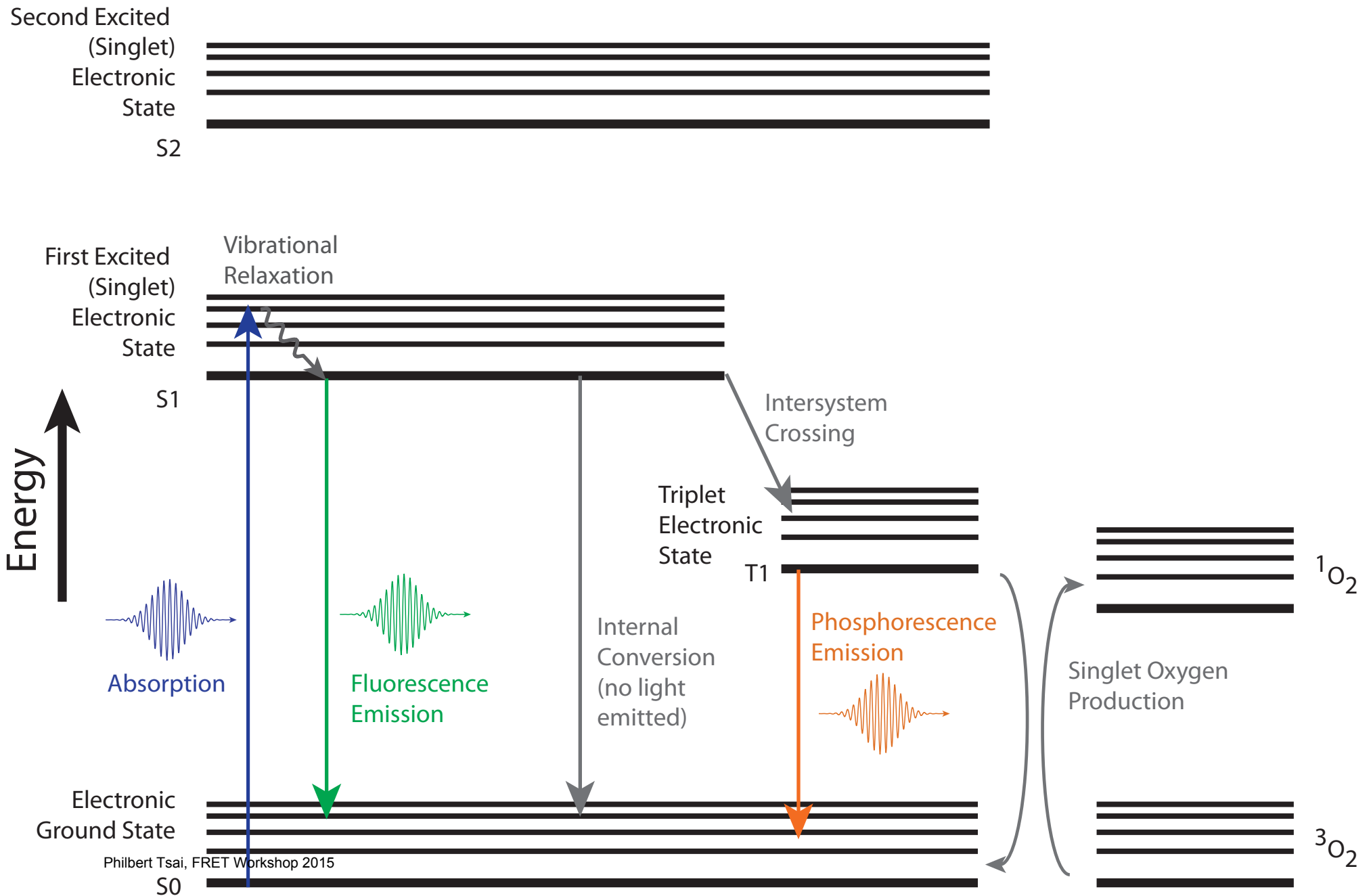
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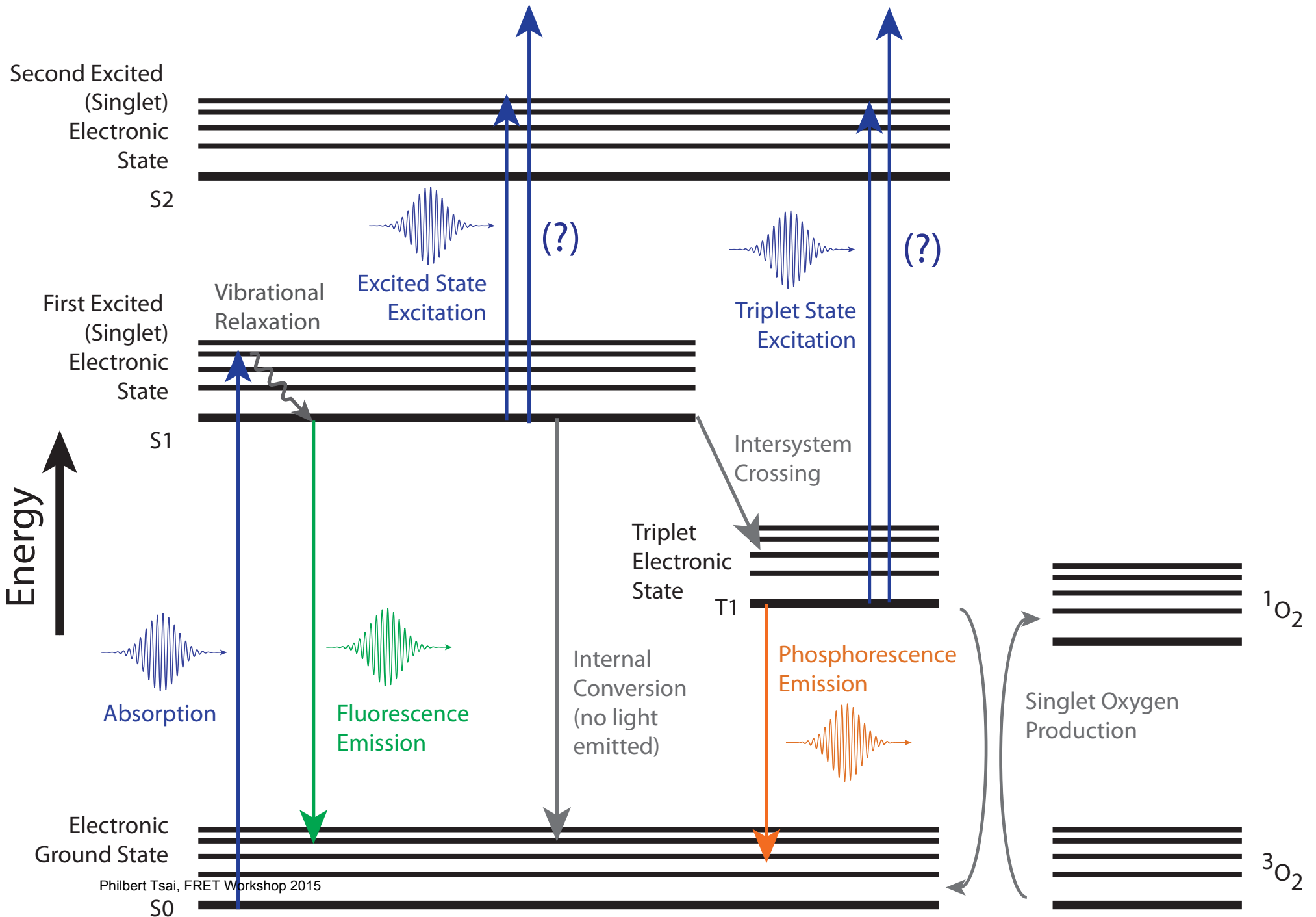


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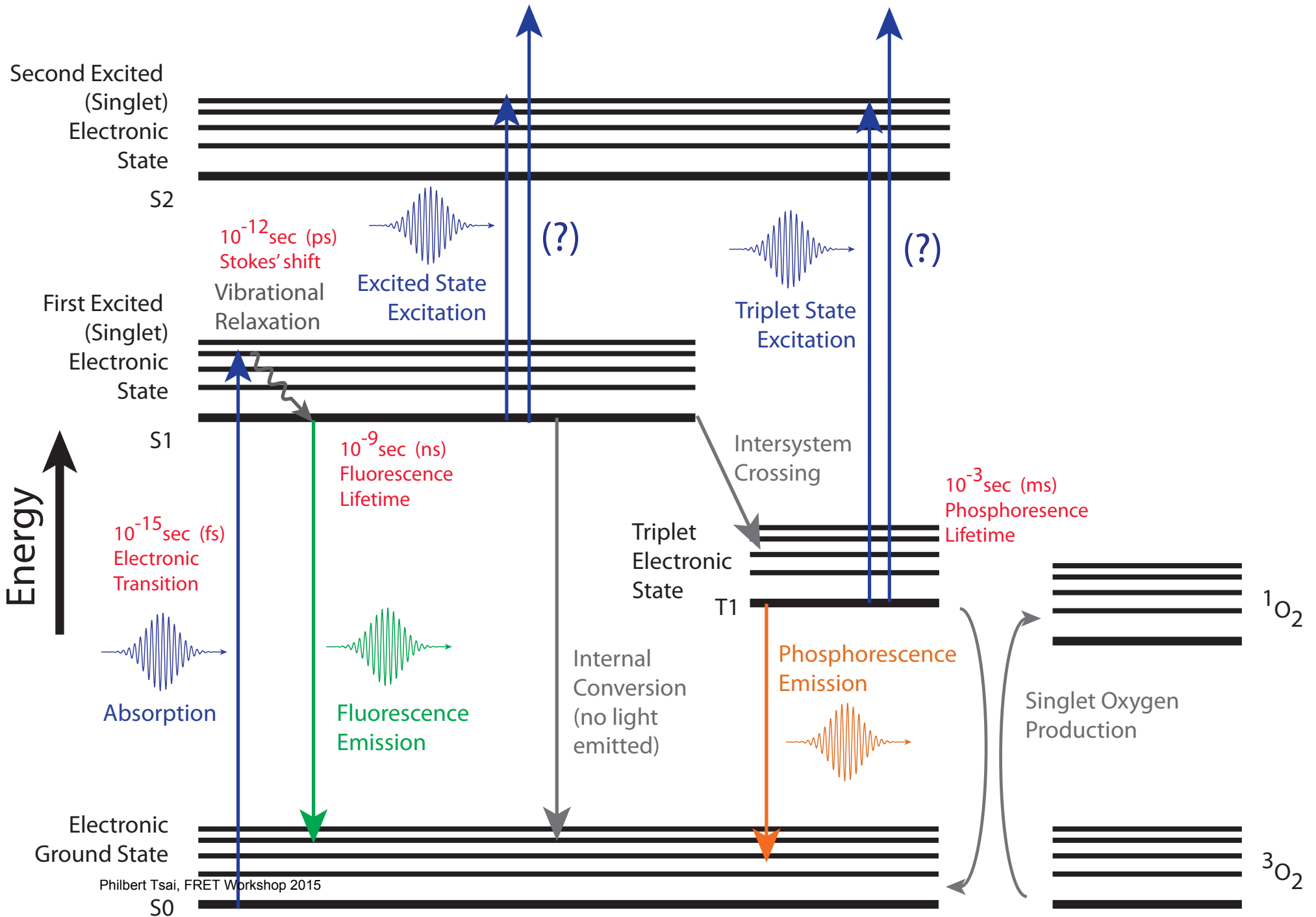




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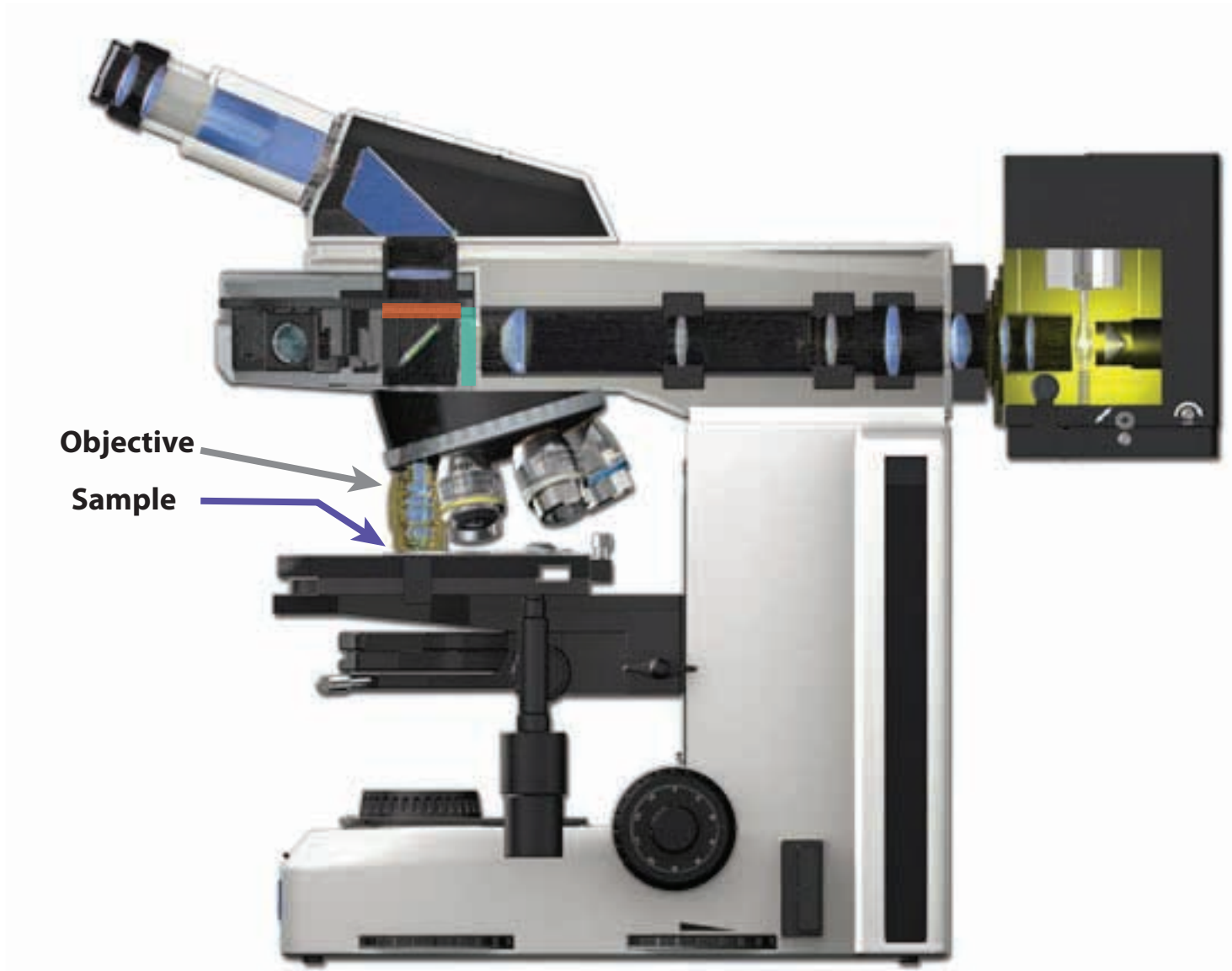




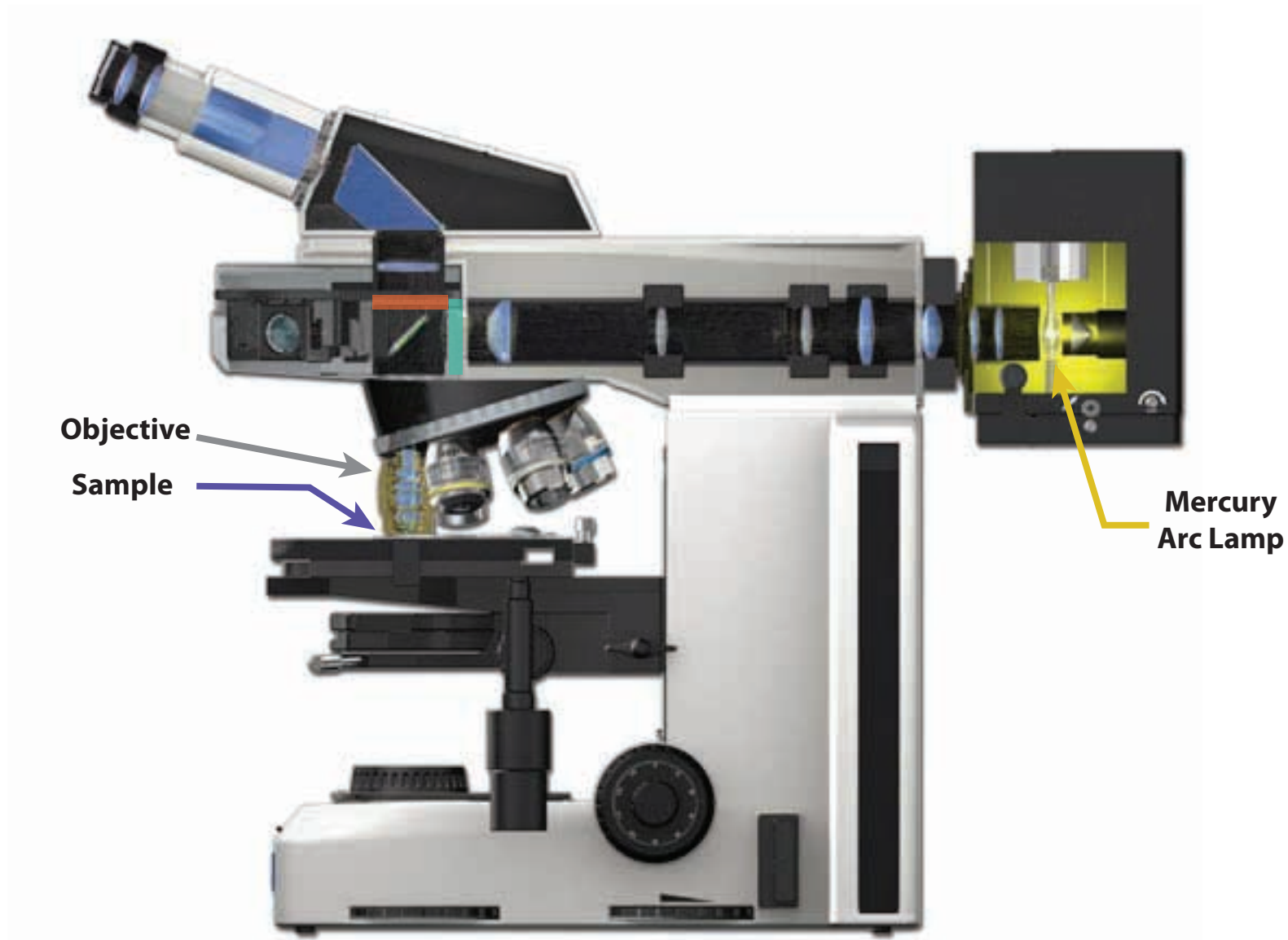
# Upright Microscope : Epifluorescence Light Path



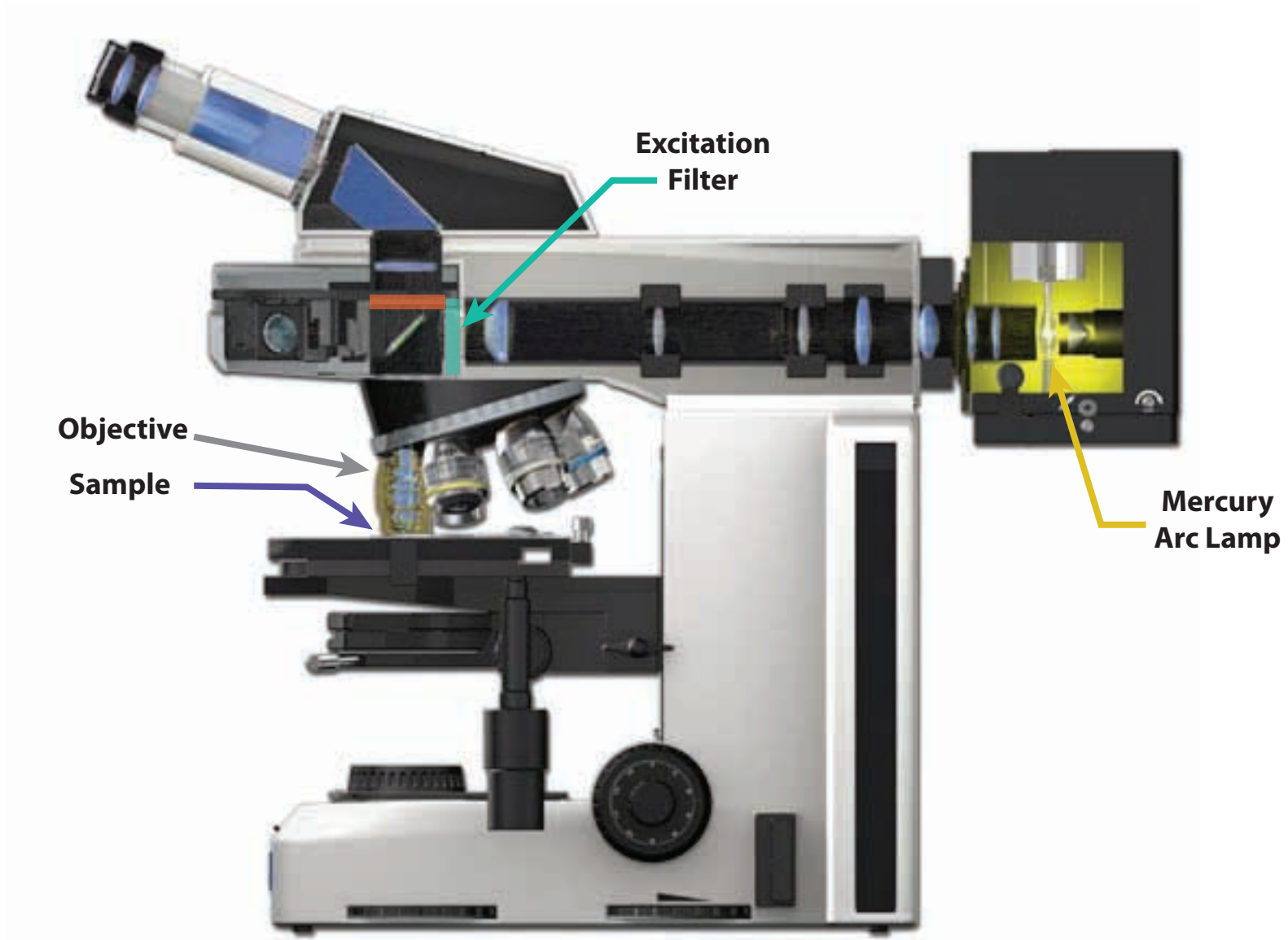
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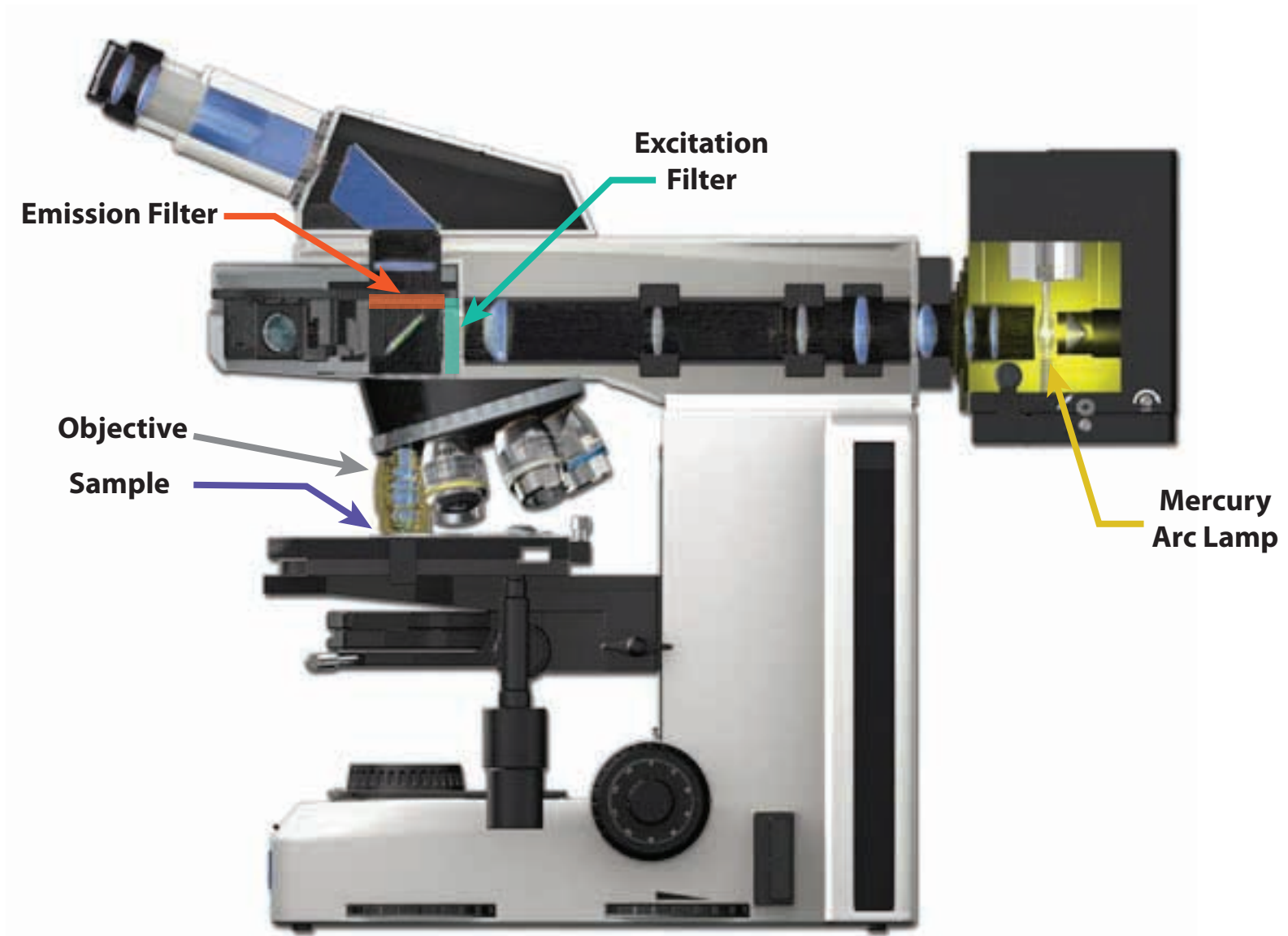
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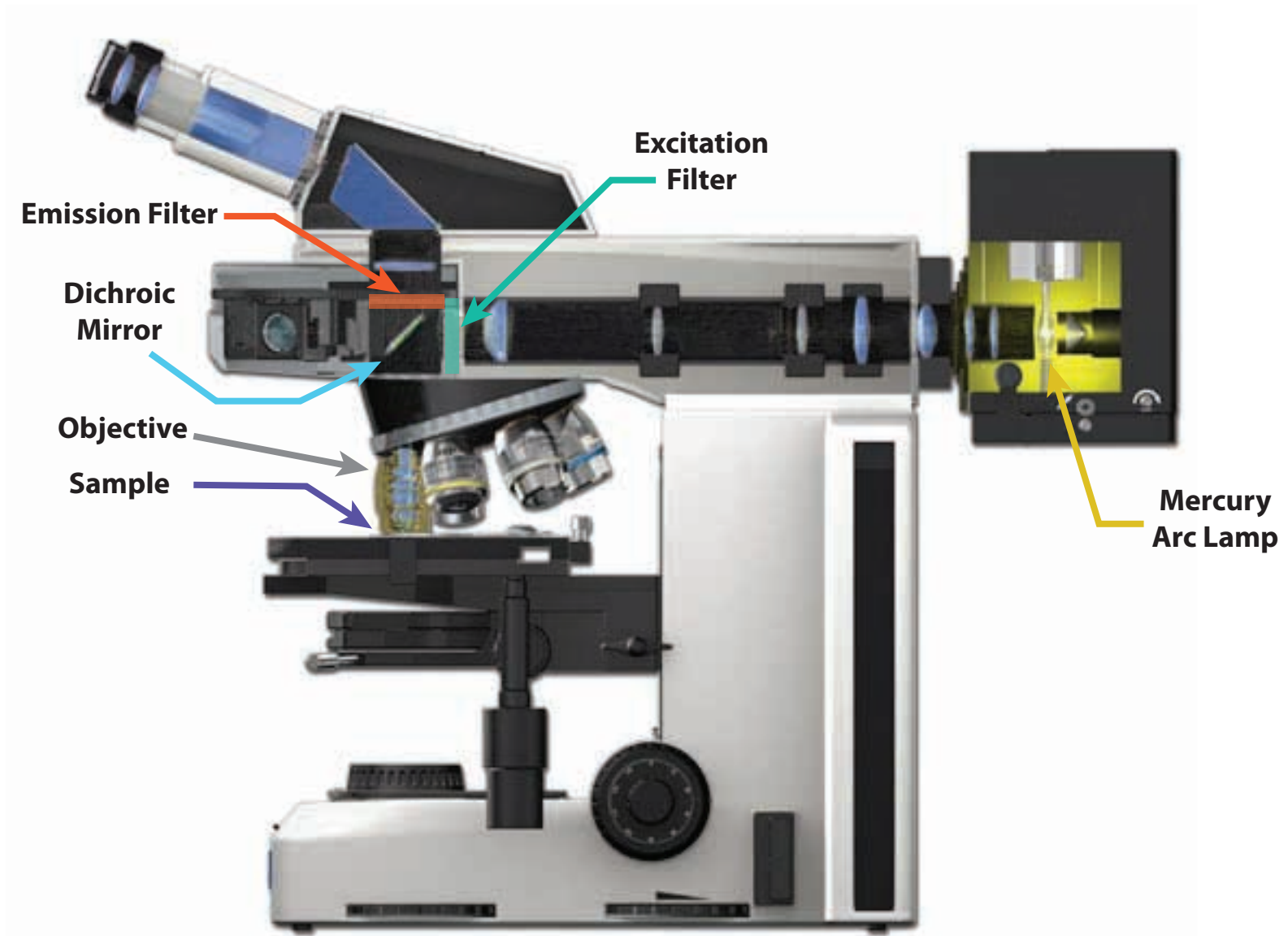


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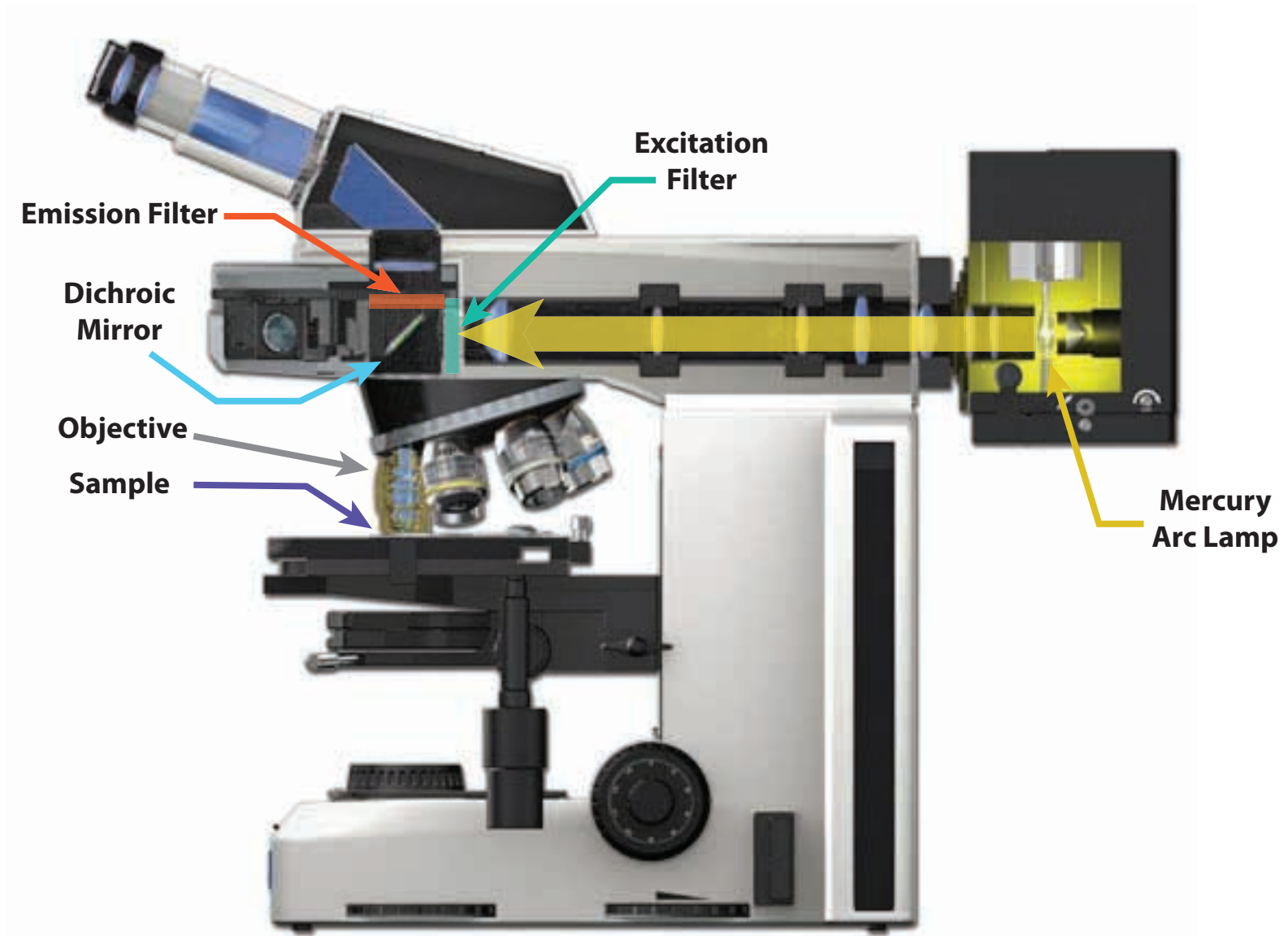




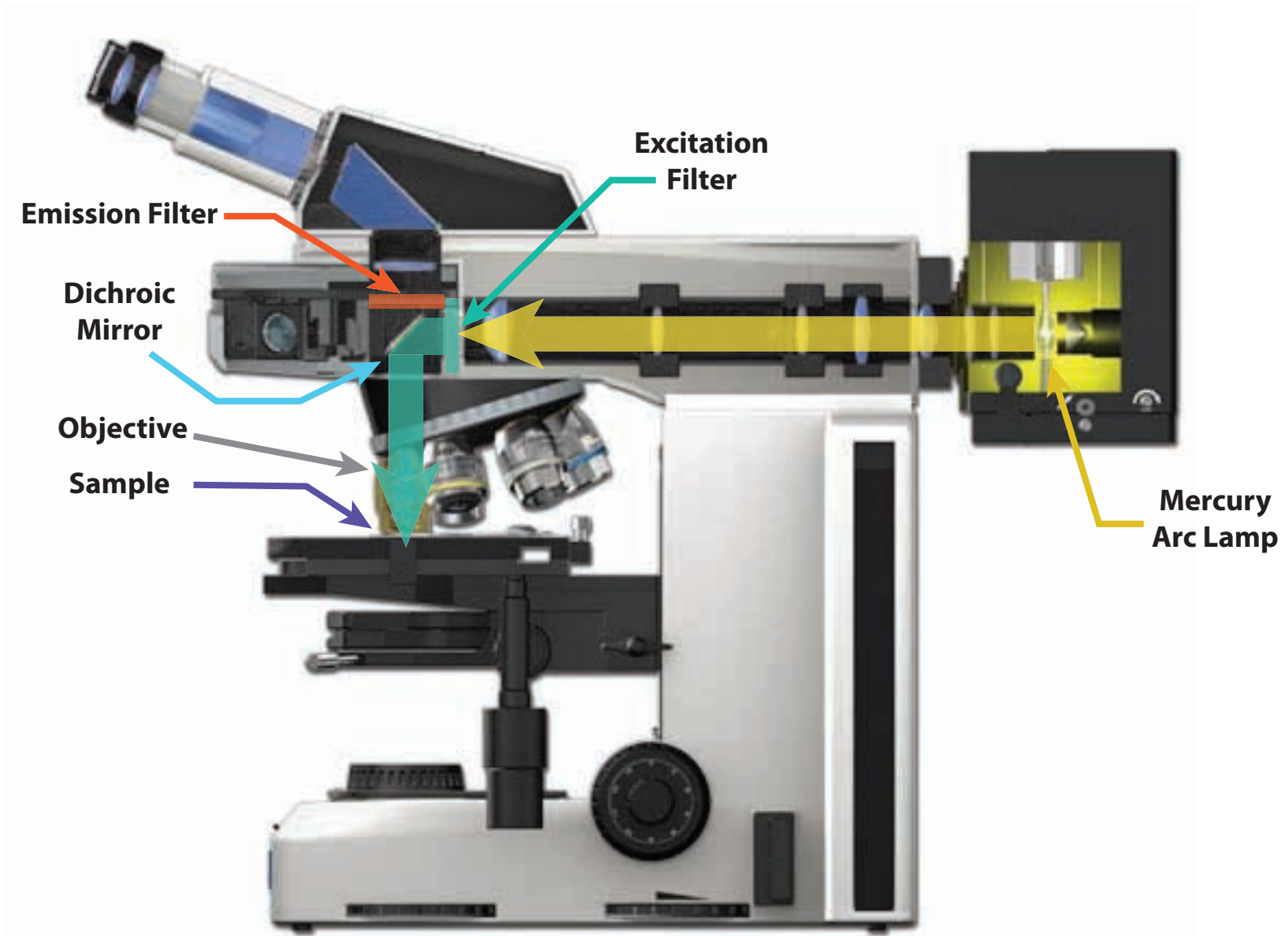
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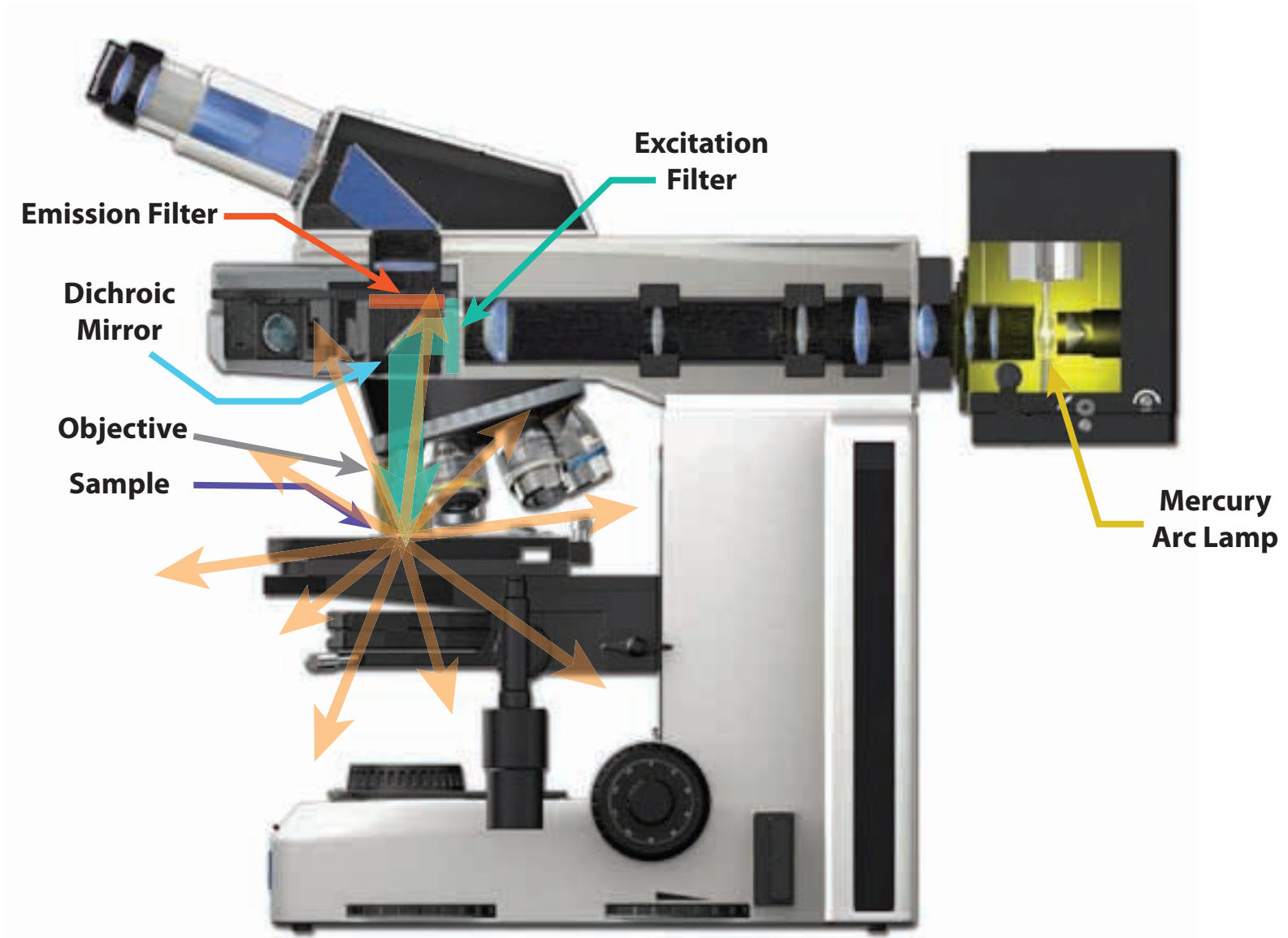
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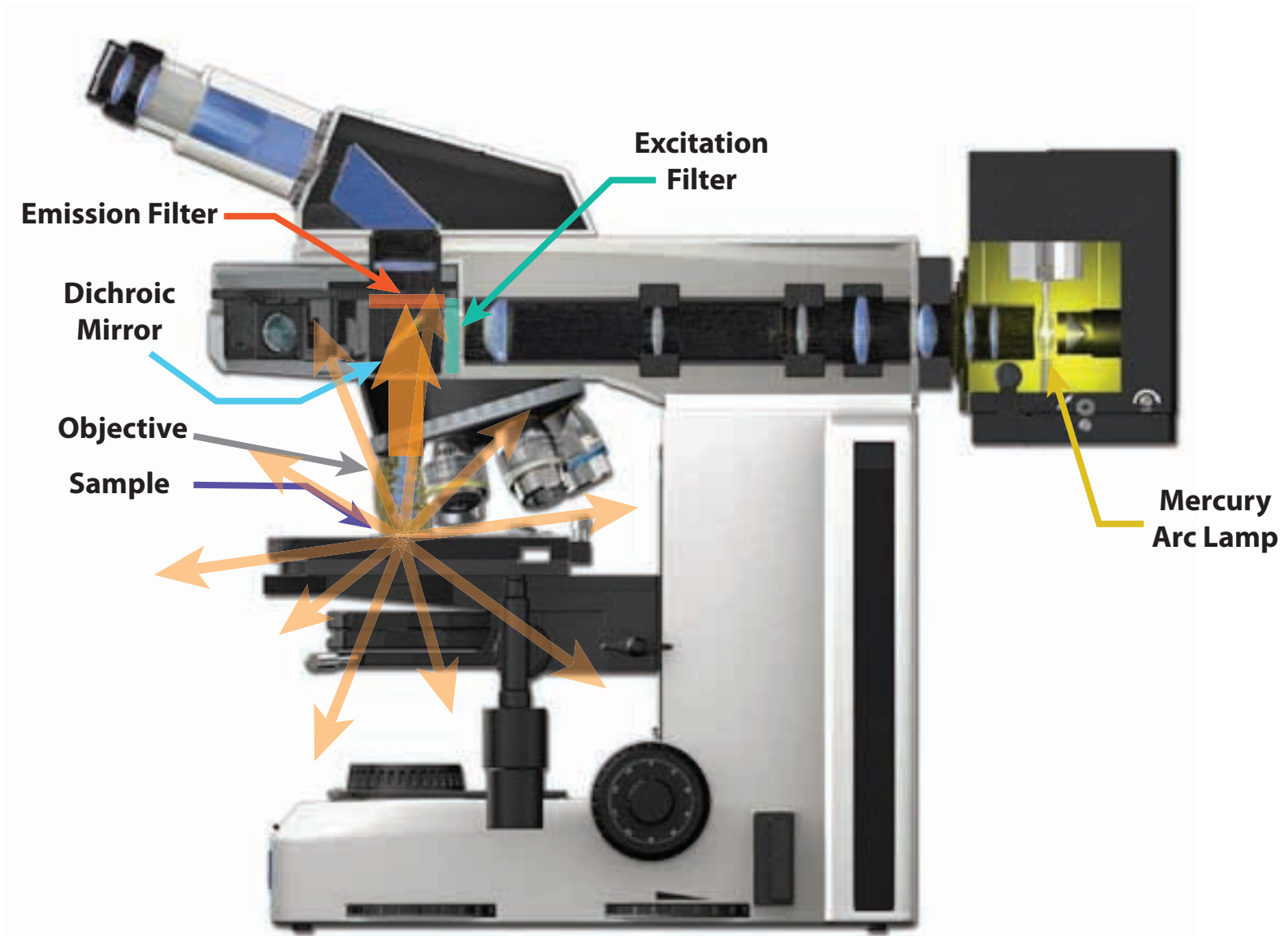
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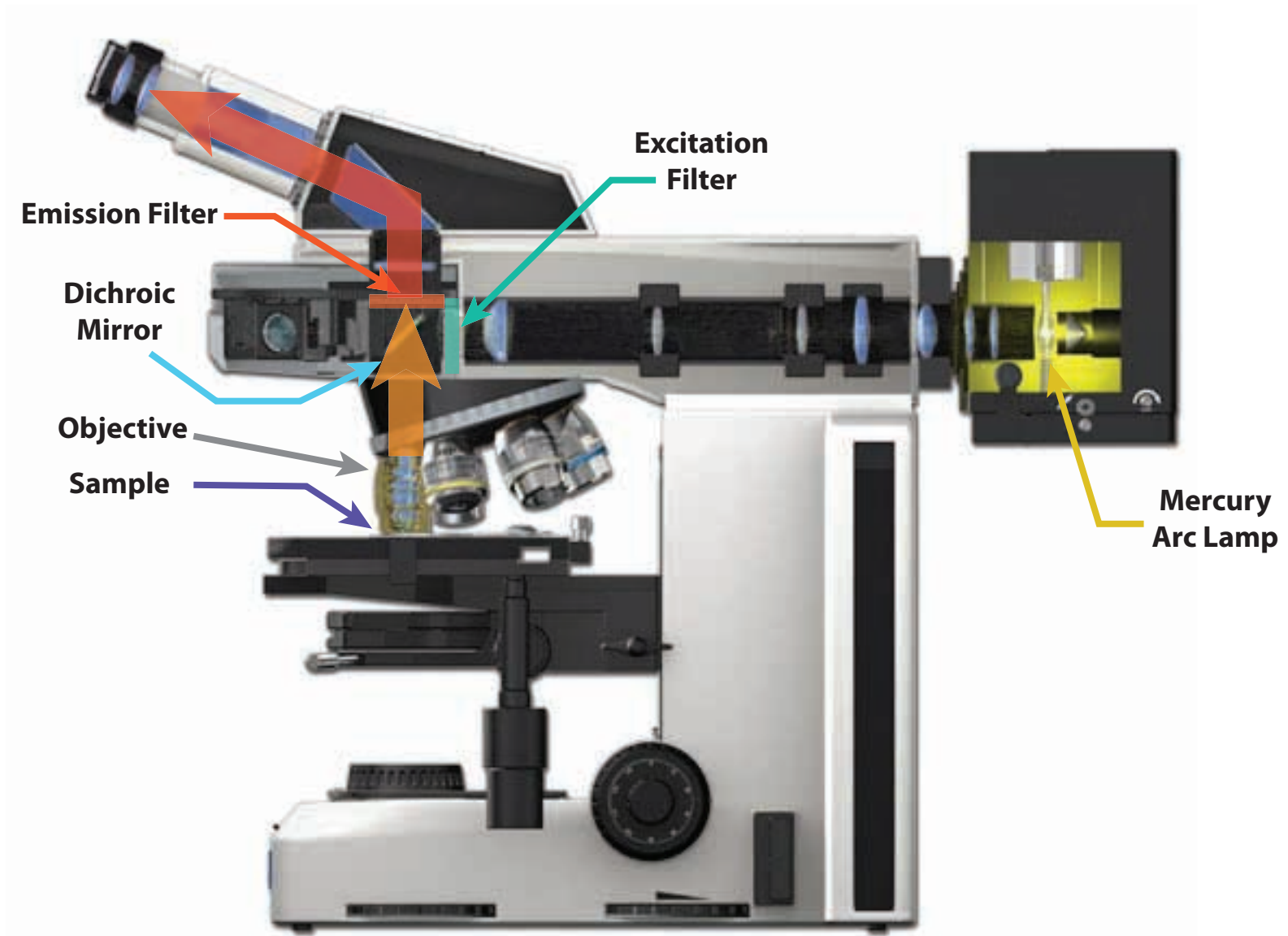
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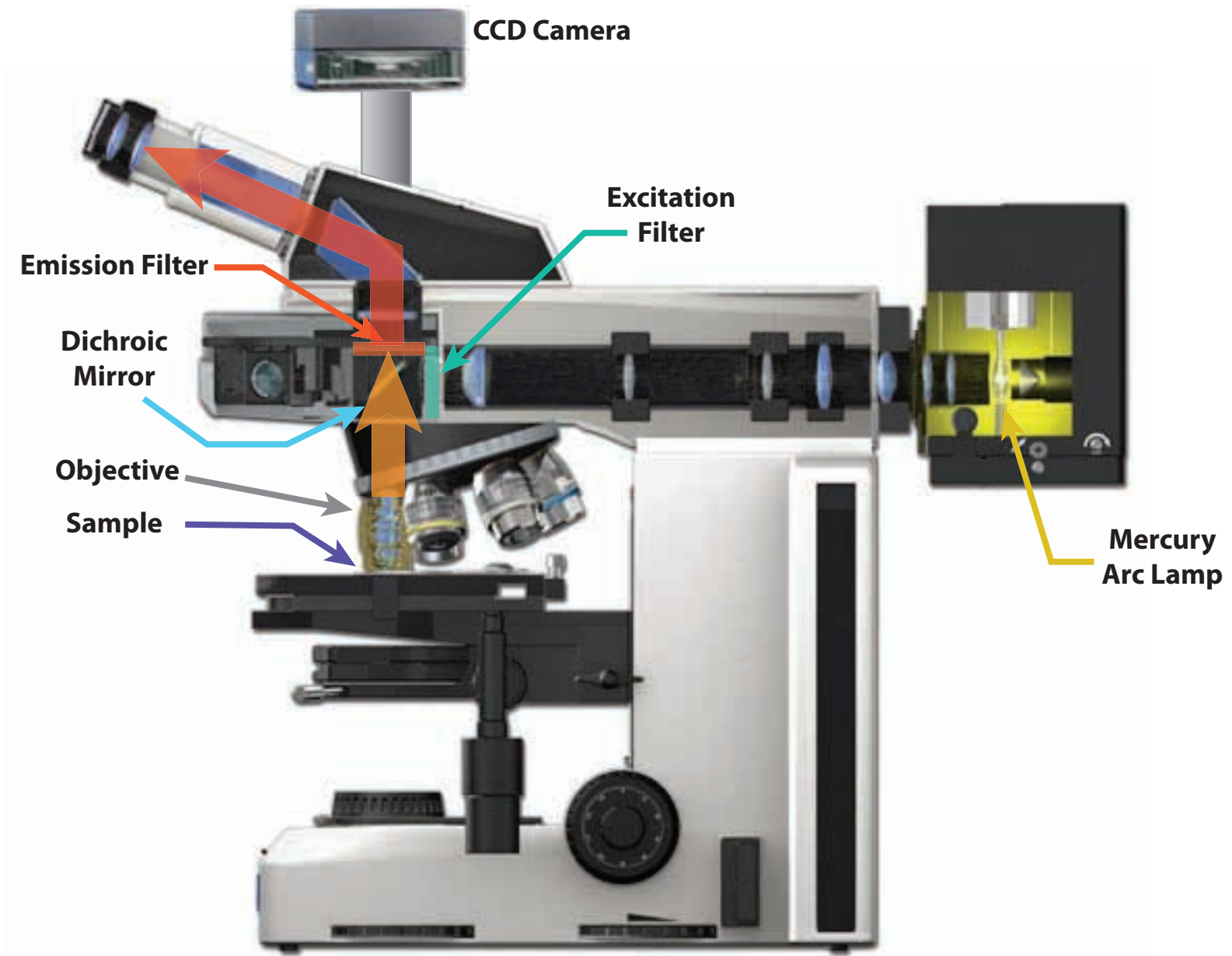
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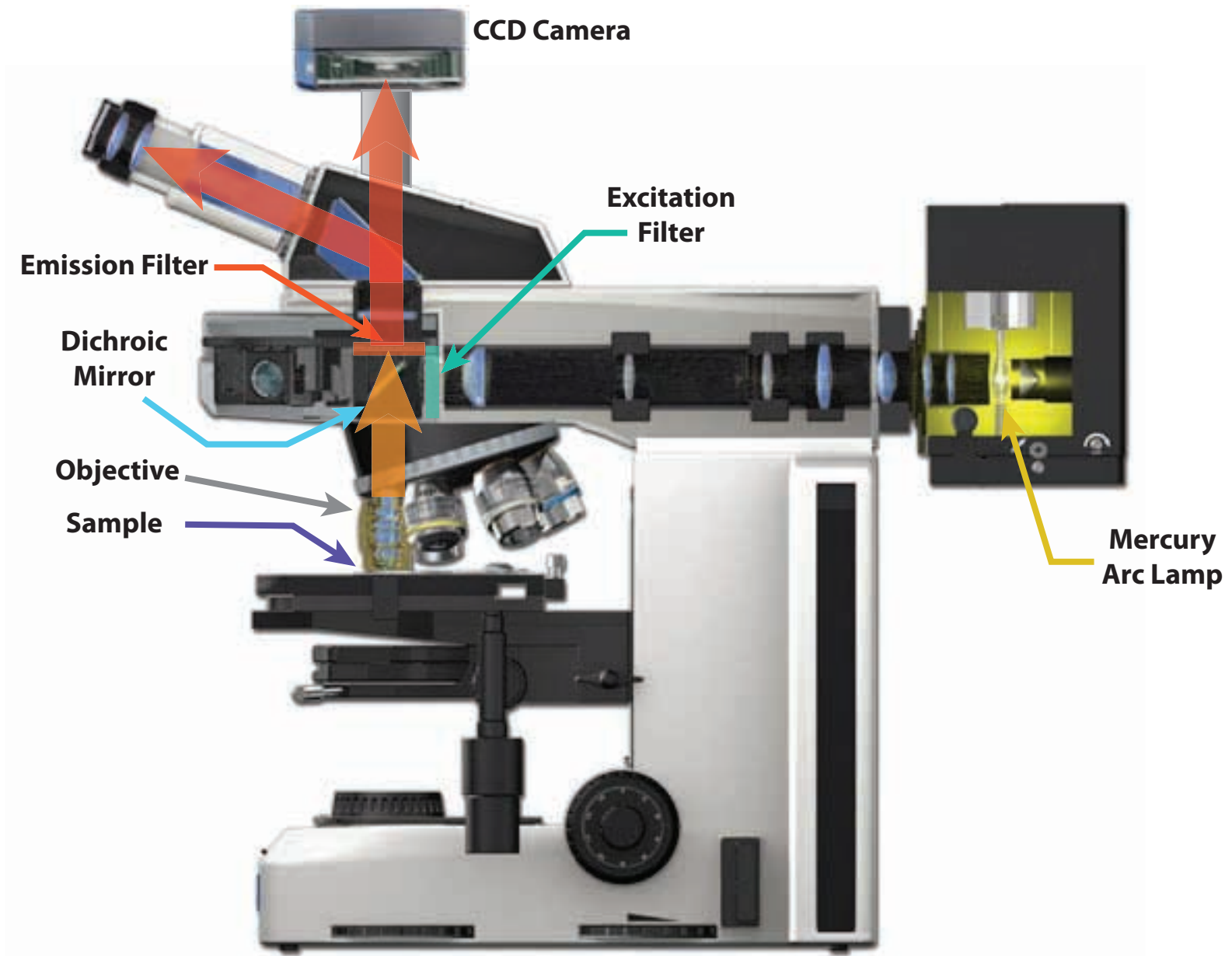
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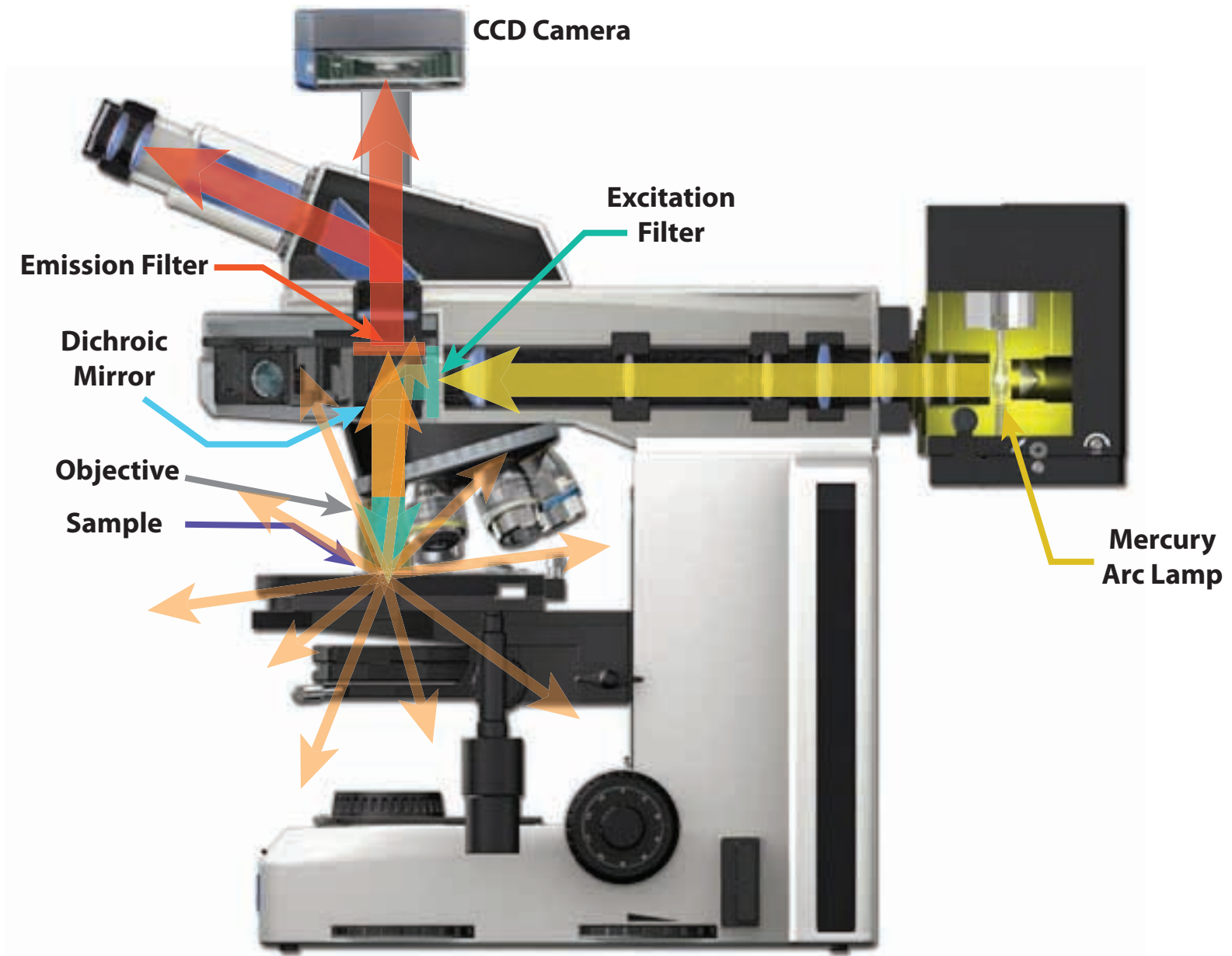


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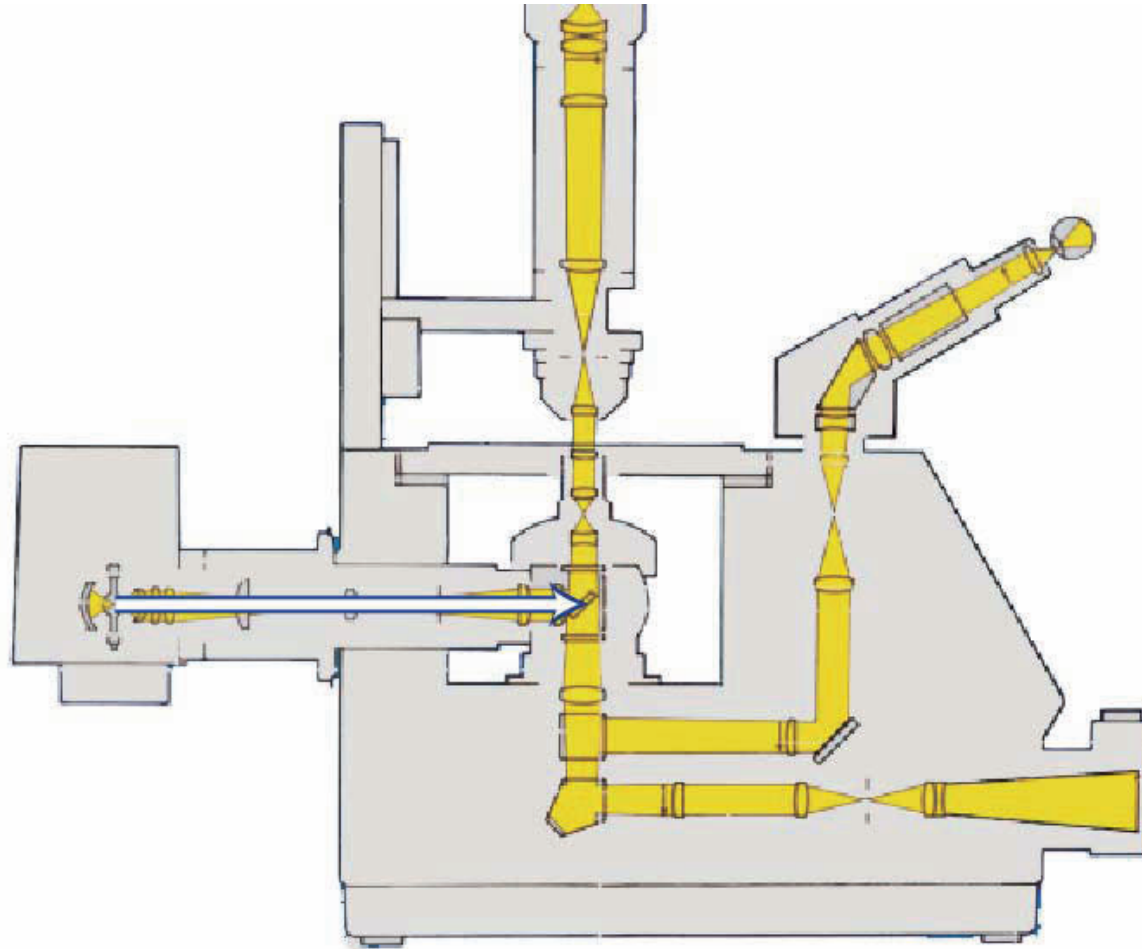




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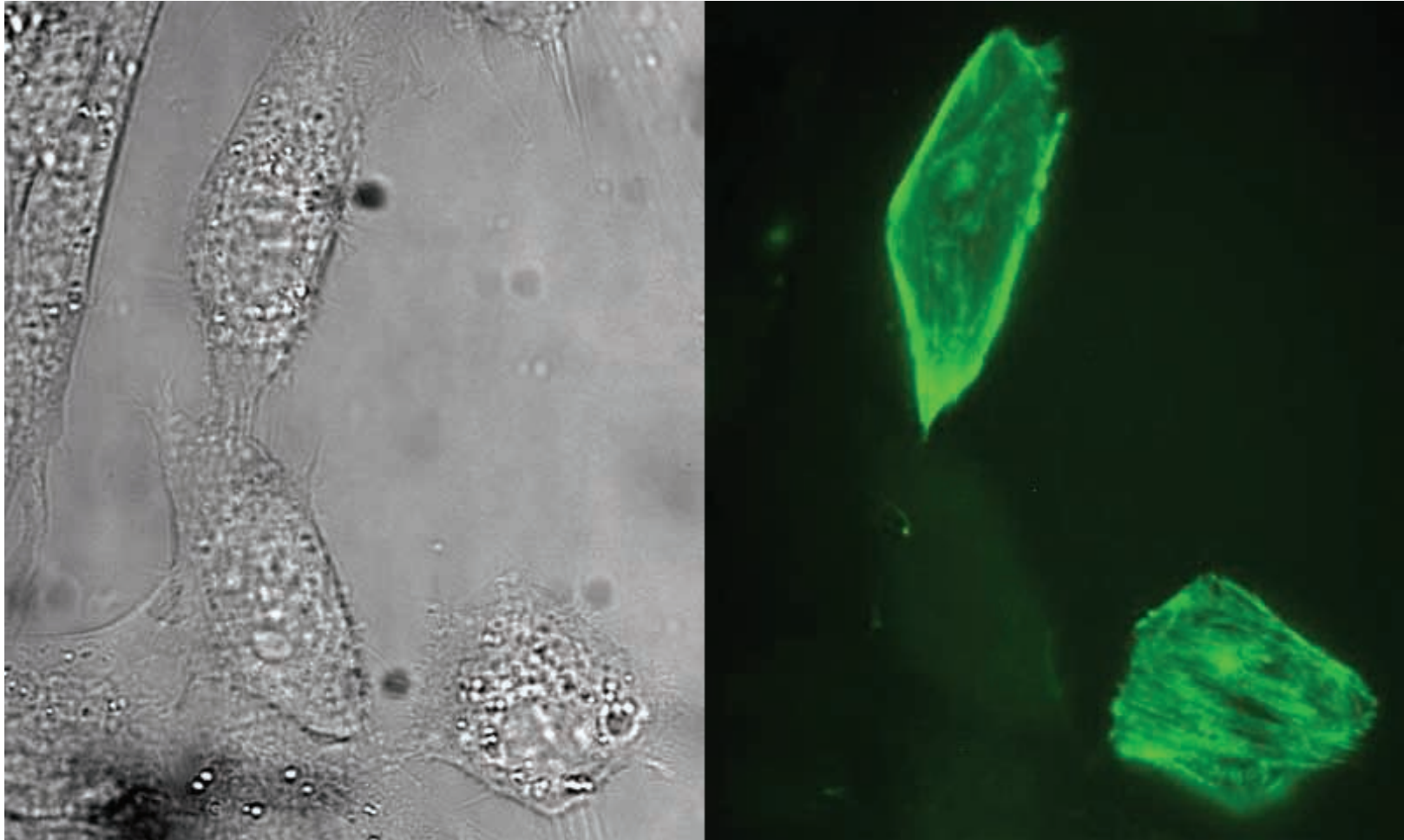
# Optical schematic of an inverted epifluorescence microscope



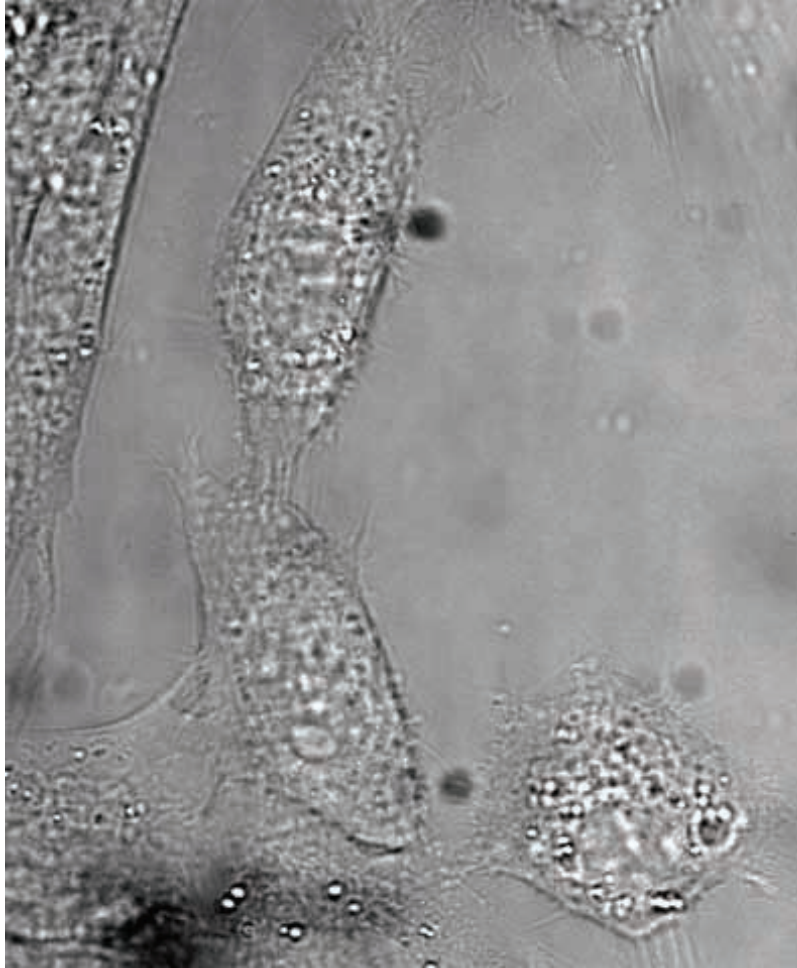
Philbert S. Tsai, July 28, 2010



# Brightfield vs. Fluorescence Microscopy

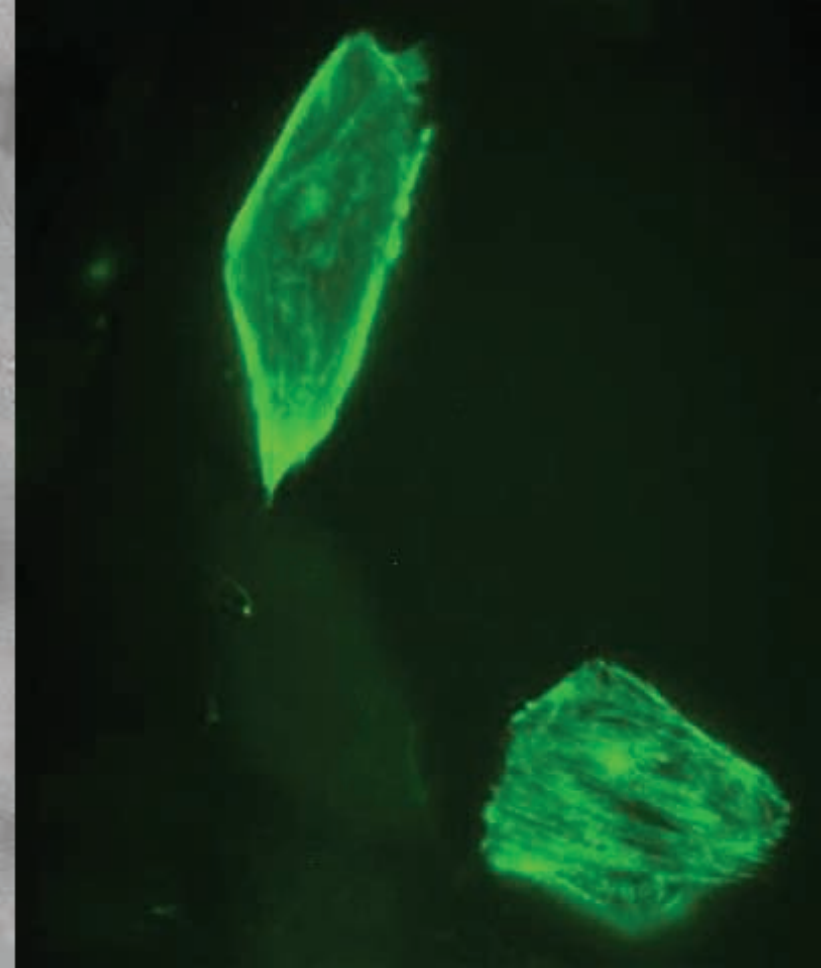


# Brightfield vs. Fluorescence Microscopy



Ambiguous Signal

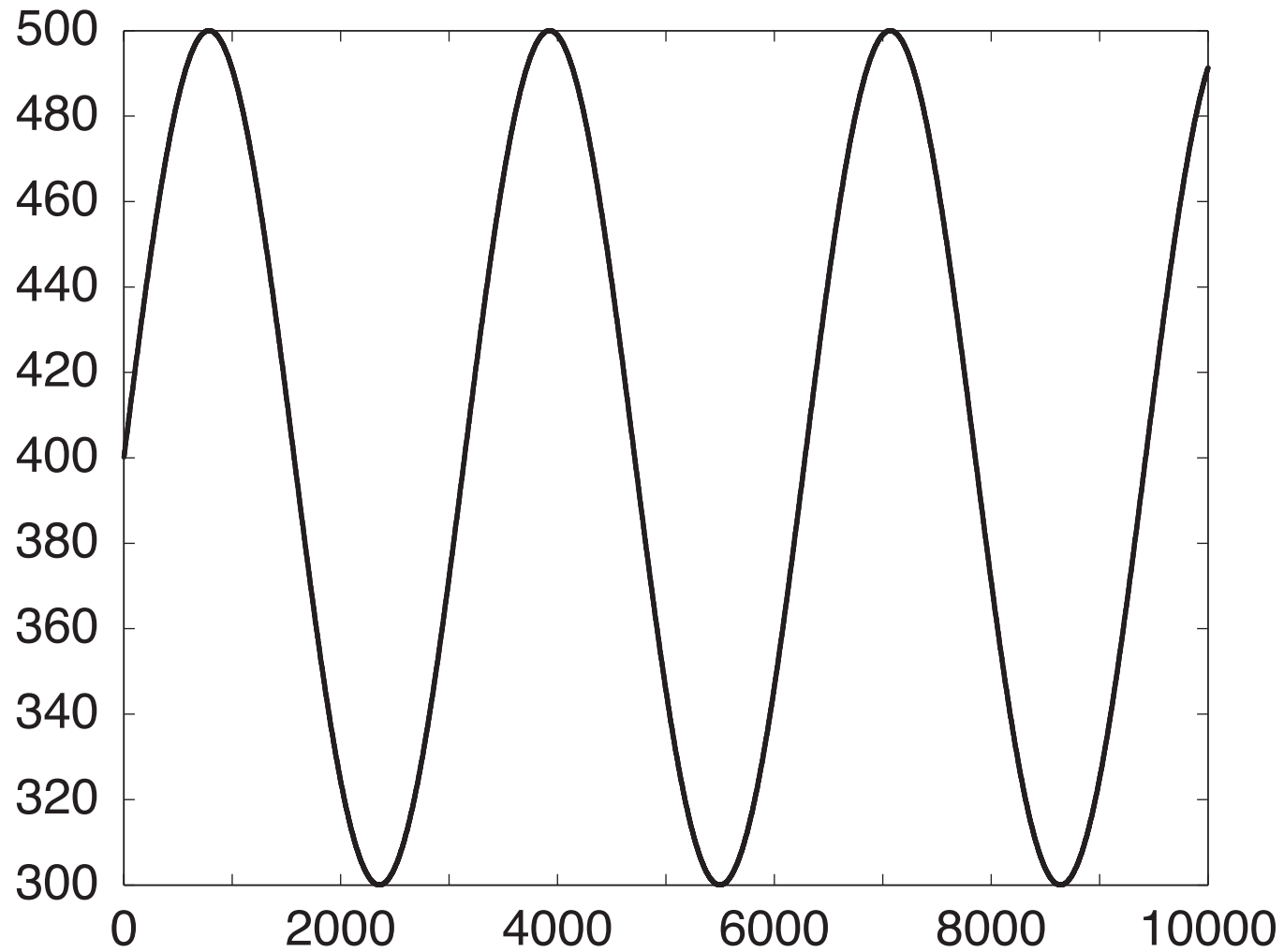
Small changes on a bright background



**Cell-specific or subcellular-specific labeling**

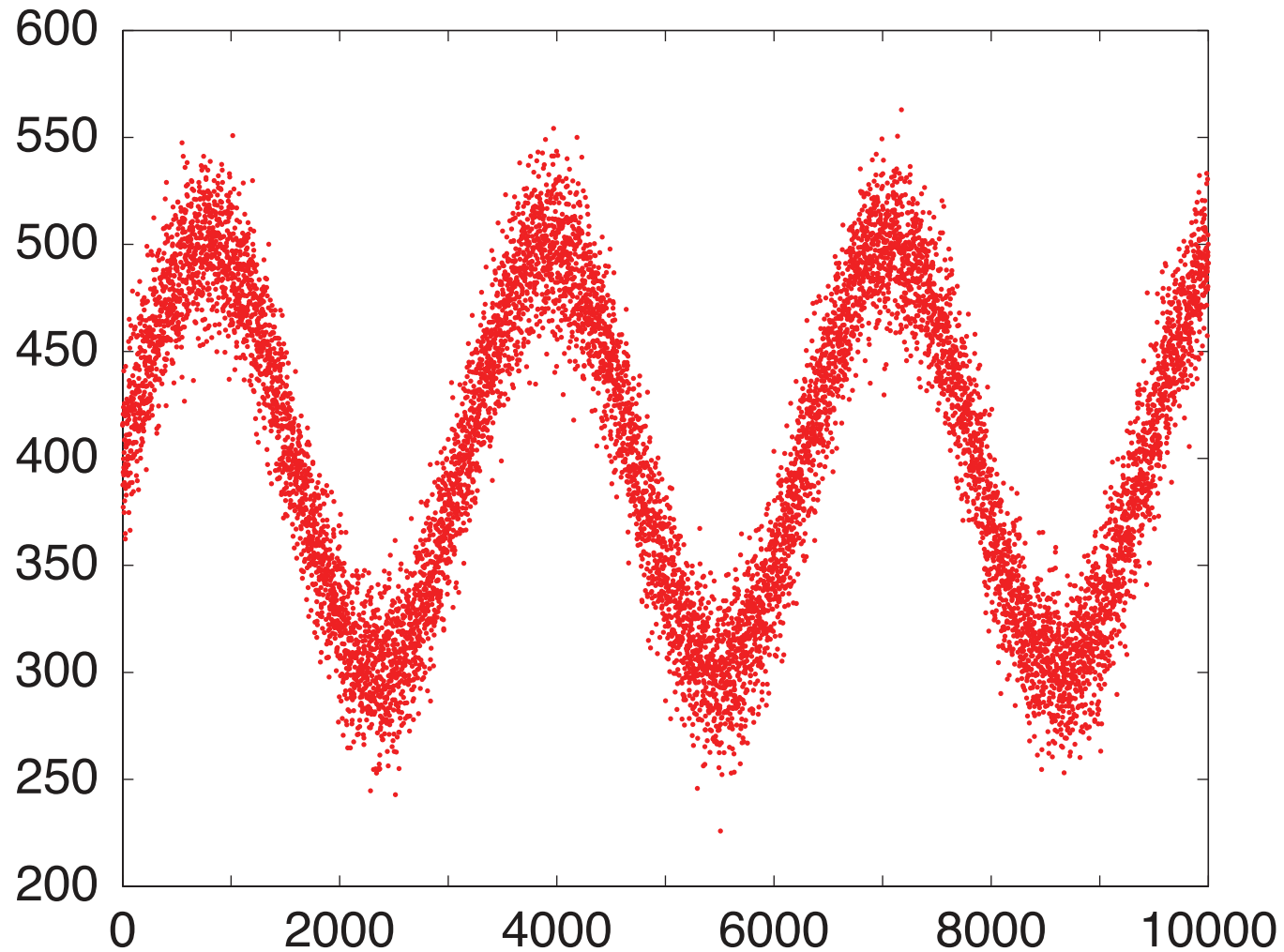
**Bright signal on dark background**

# The Fluorescence Advantage : Signal on a Dark Background



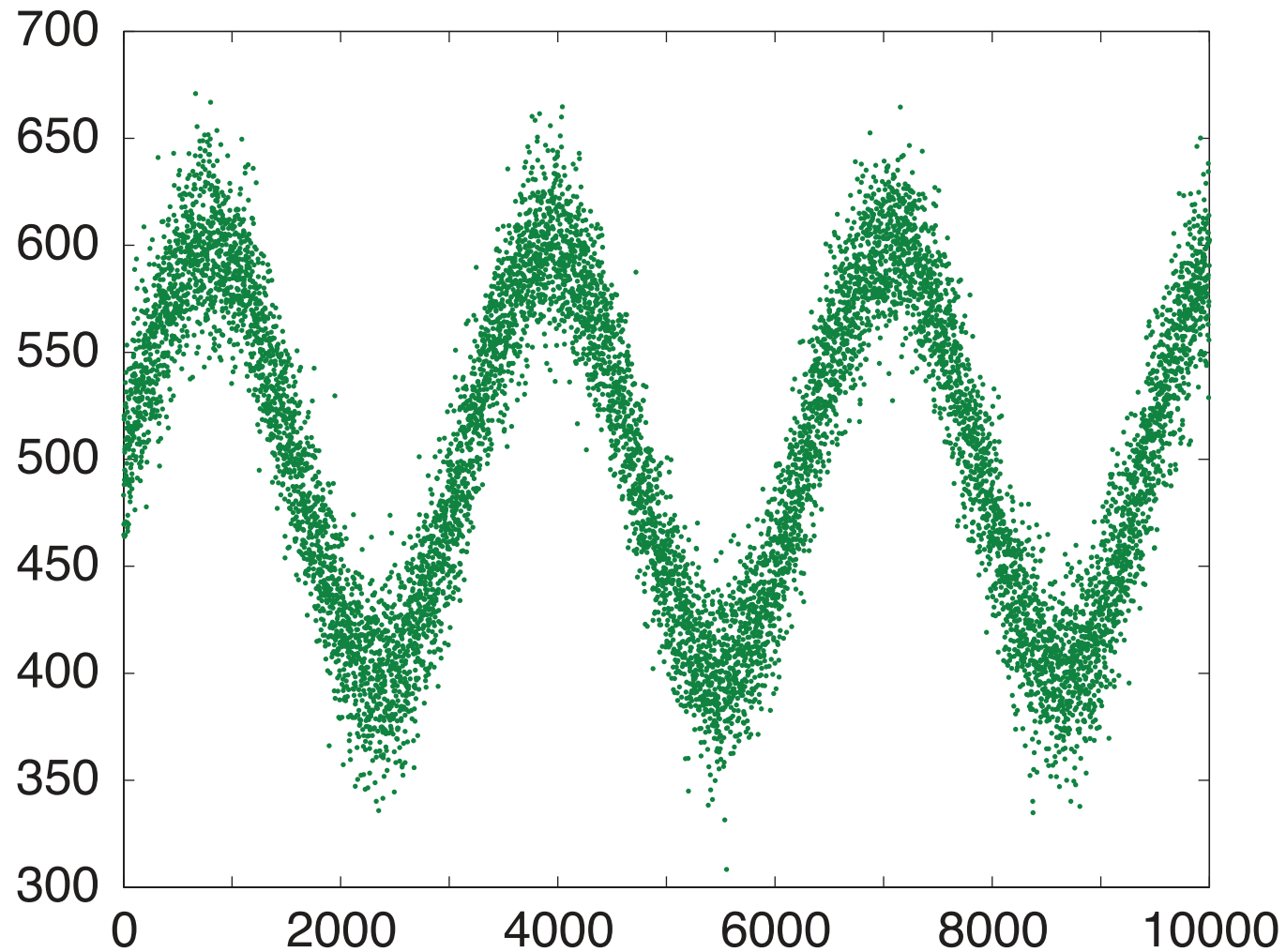
A noise-free, low-background signal

# The Fluorescence Advantage : Signal on a Dark Background



**A shot-noise-limited signal with low-background**

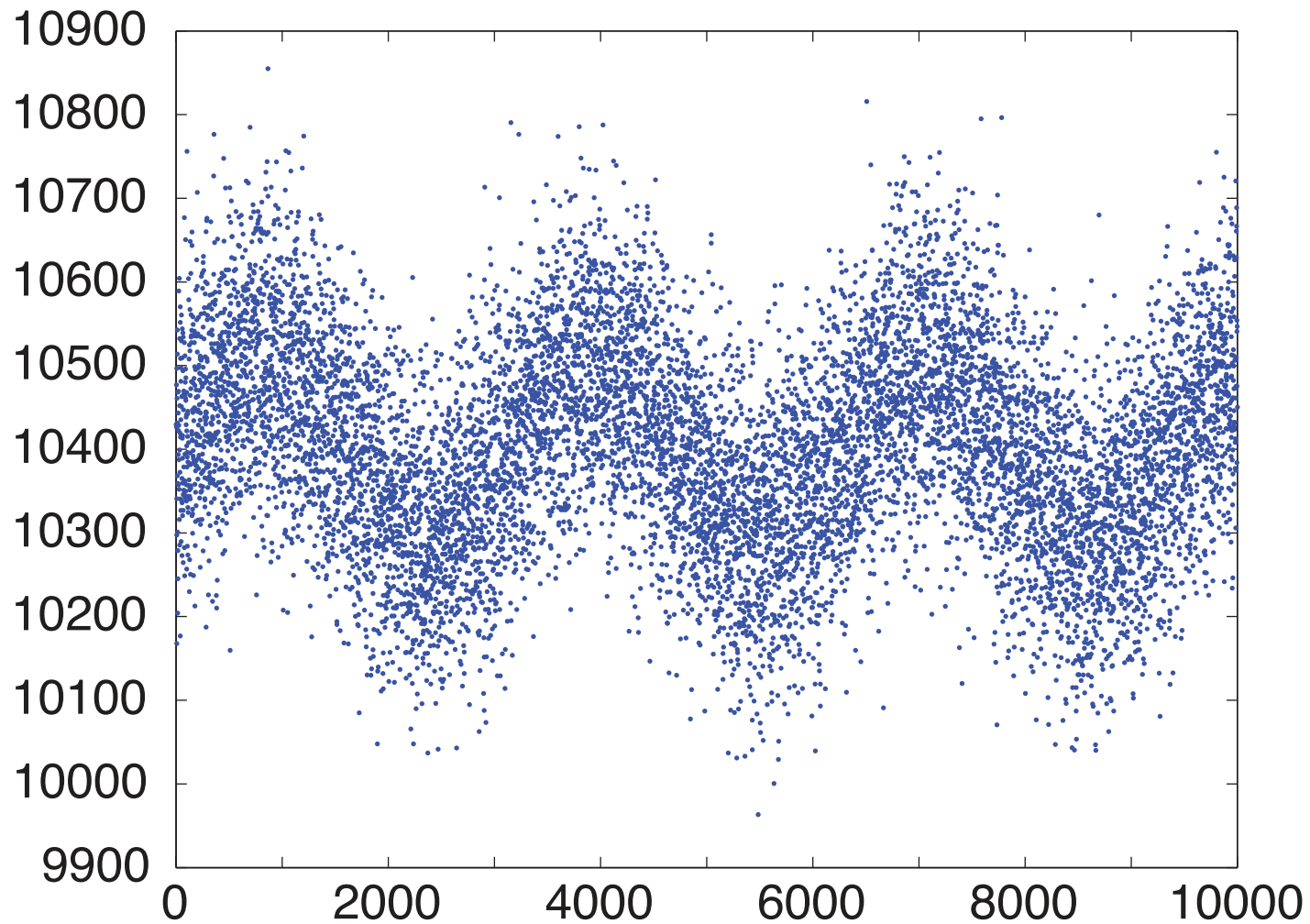
# The Fluorescence Advantage : Signal on a Dark Background



A shot-noise-limited signal with slightly higher background

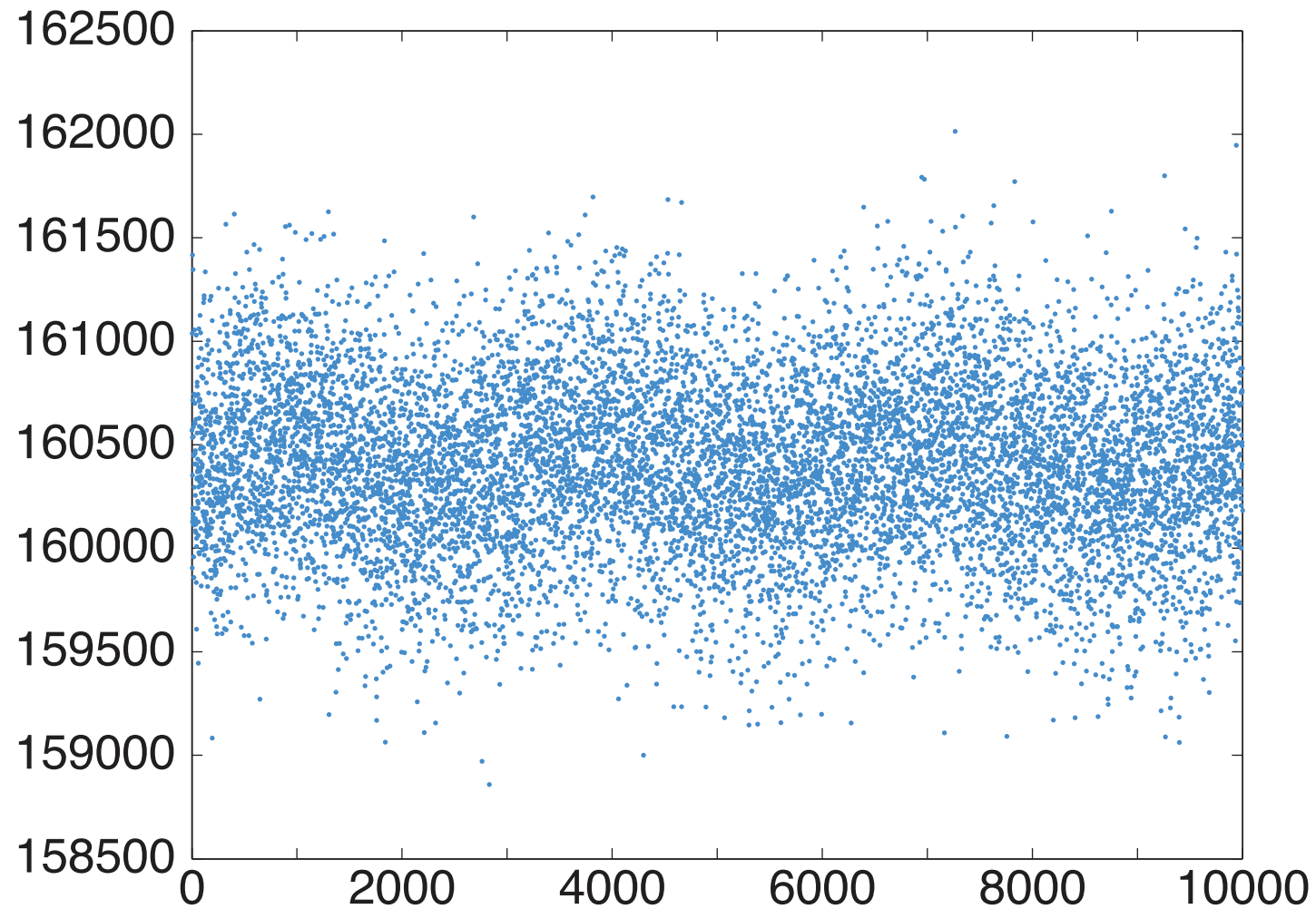


# The Fluorescence Advantage : Signal on a Dark Background



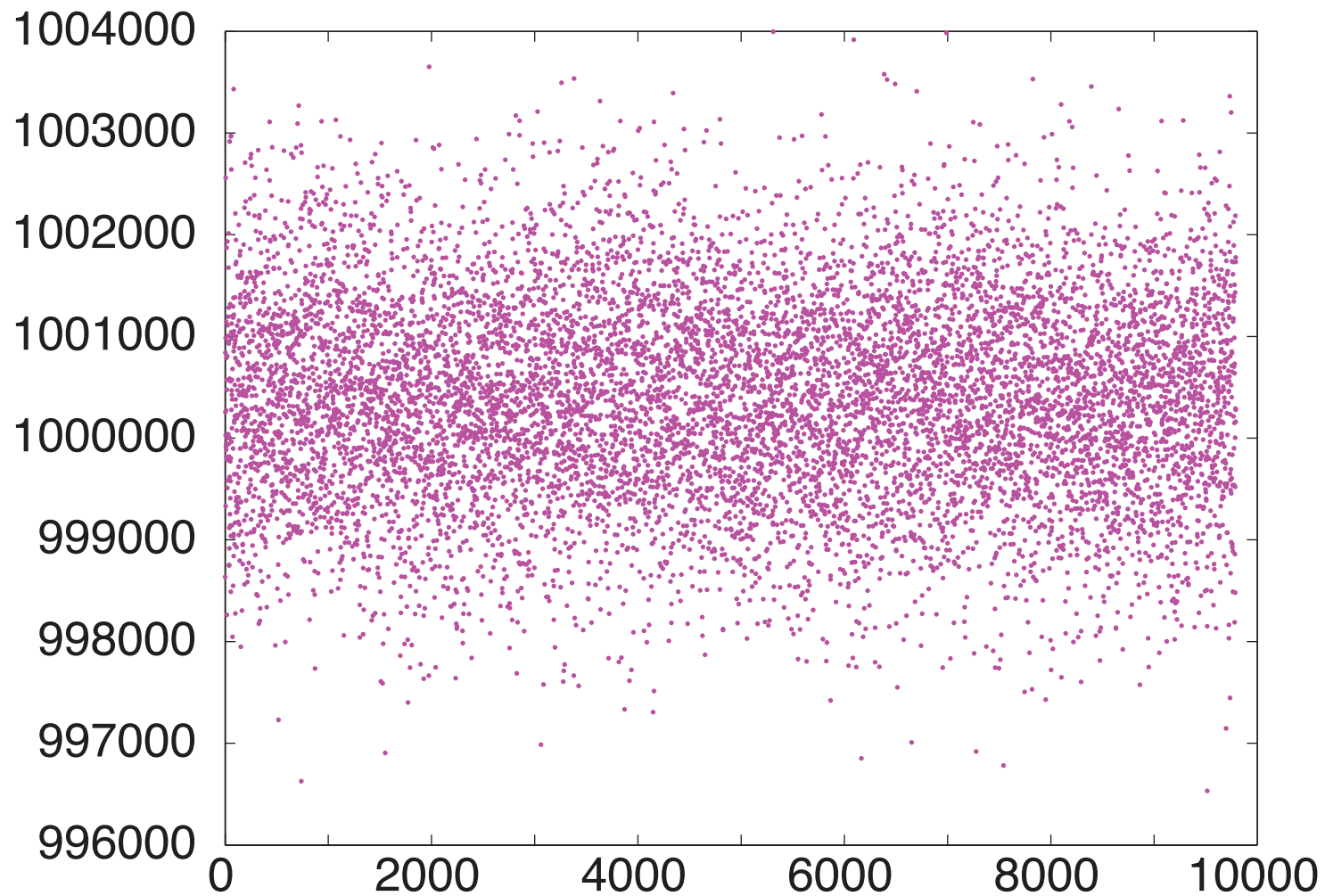
A shot-noise-limited signal with high background

# The Fluorescence Advantage : Signal on a Dark Background

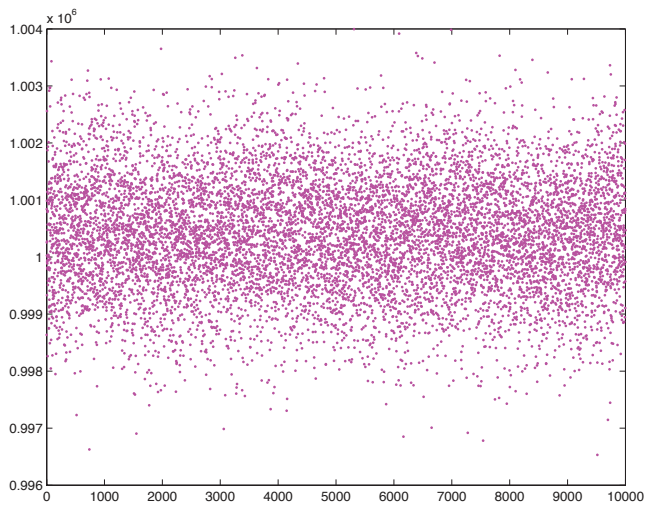
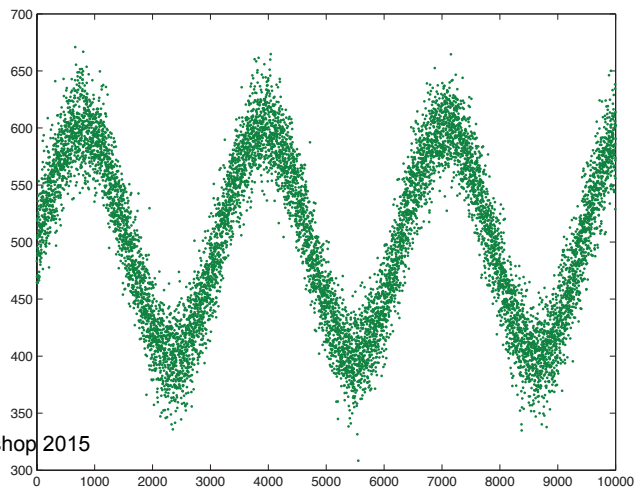
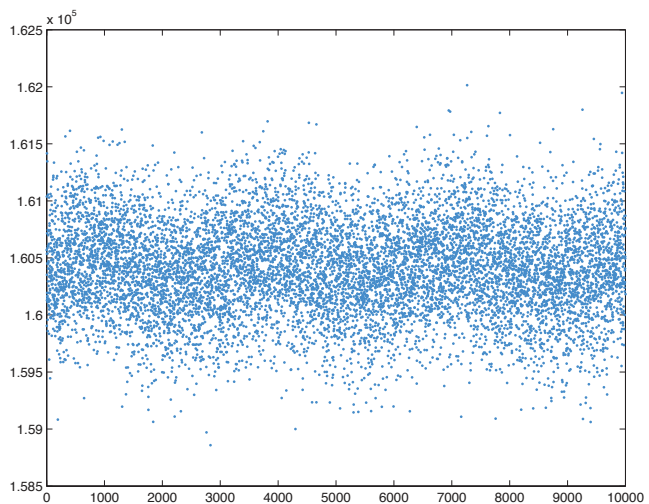
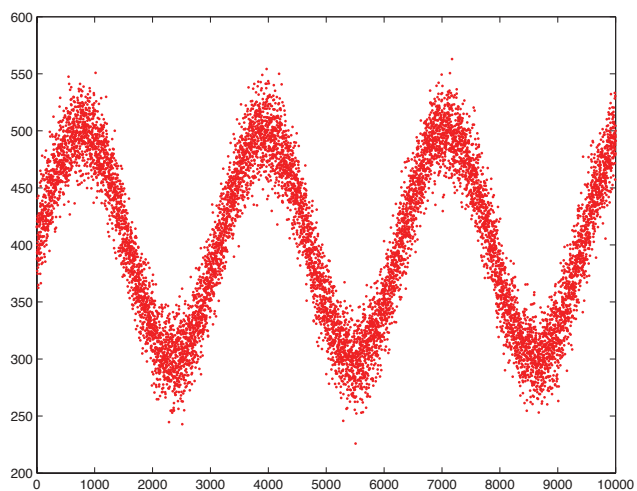
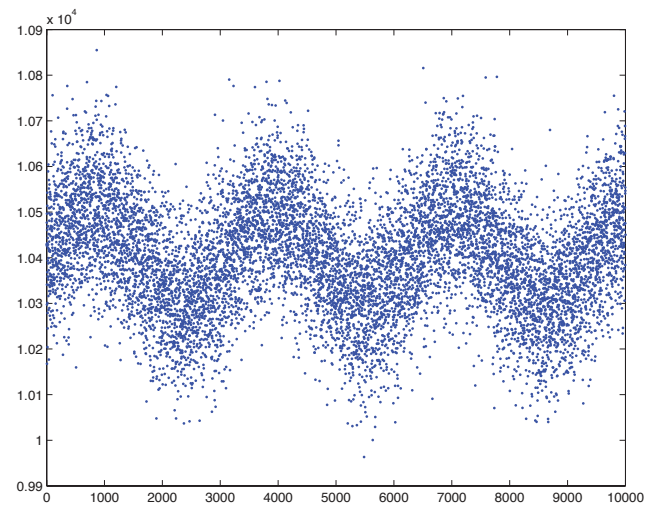
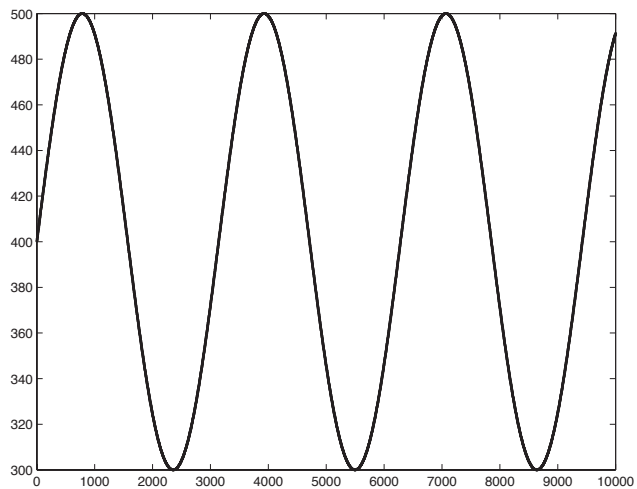


A shot-noise-limited signal with very high background

# The Fluorescence Advantage : Signal on a Dark Background



A shot-noise-limited signal with extremely high background





# Modern Microscope Components

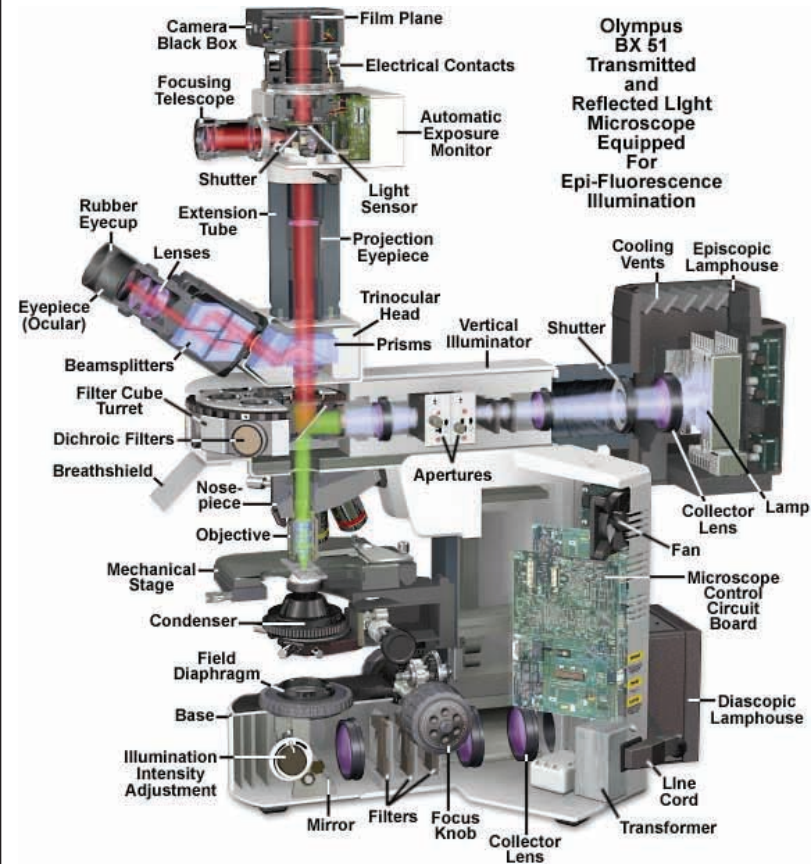


Image from Molecular Expressions webpage

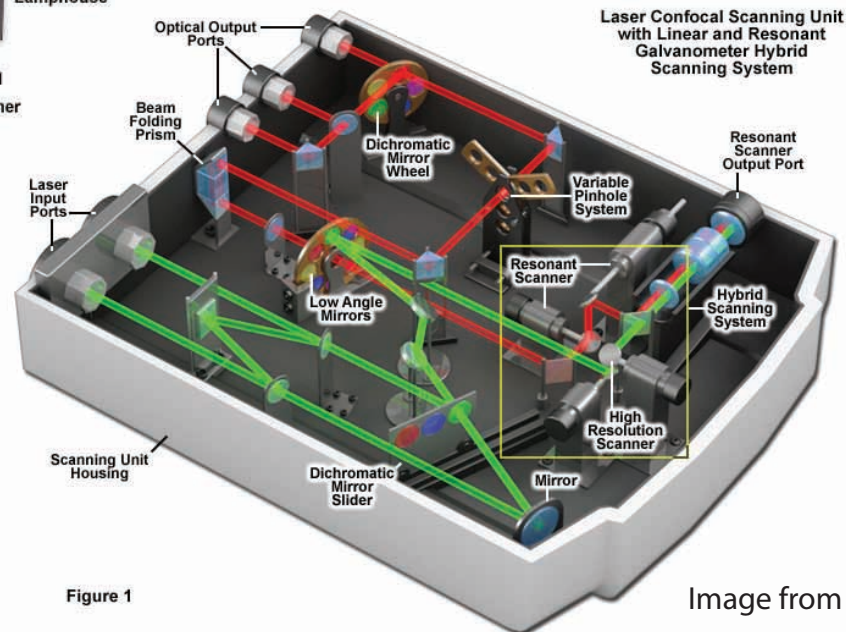
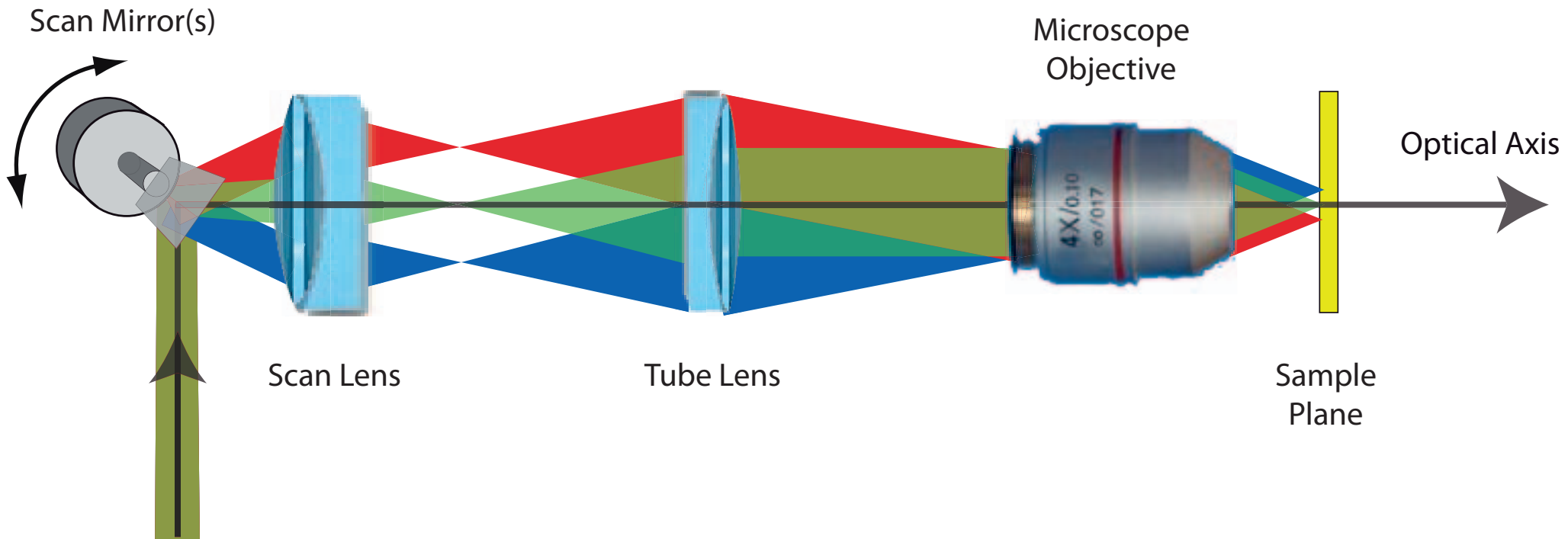


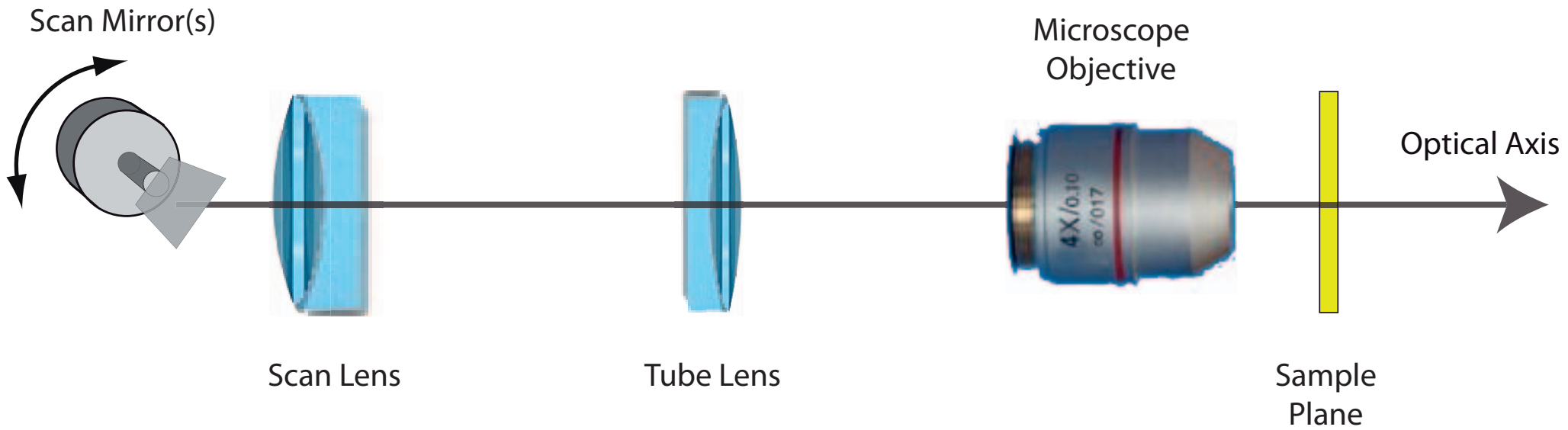
Image from MicroscopyU webpage

Figure 1

# Laser Scanning Microscopy

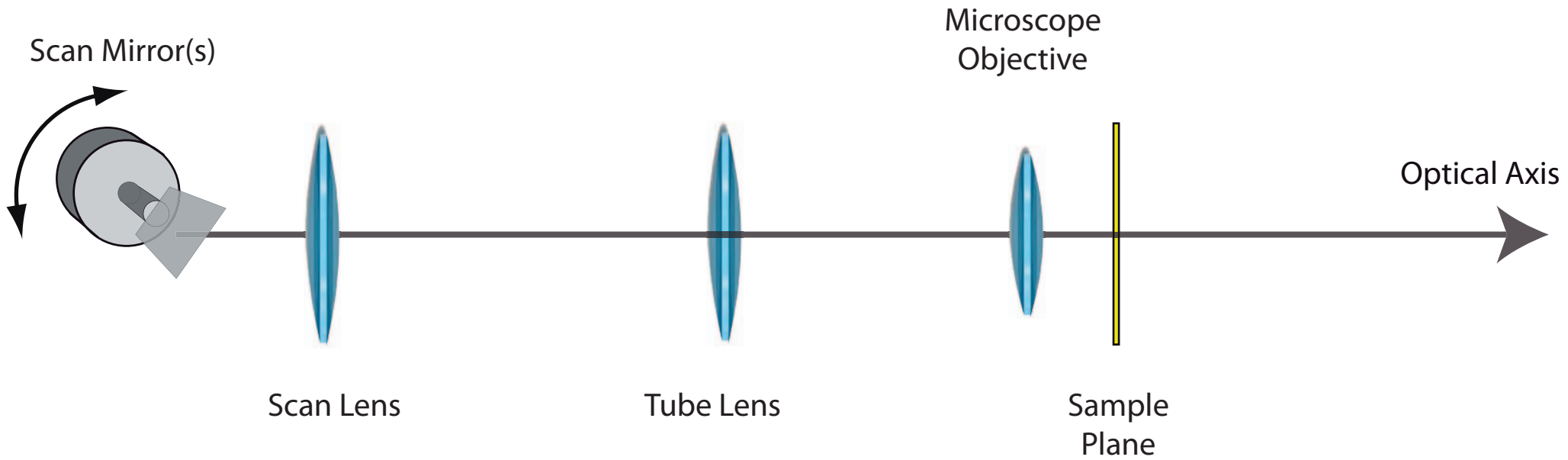


# Laser Scanning Microscopy

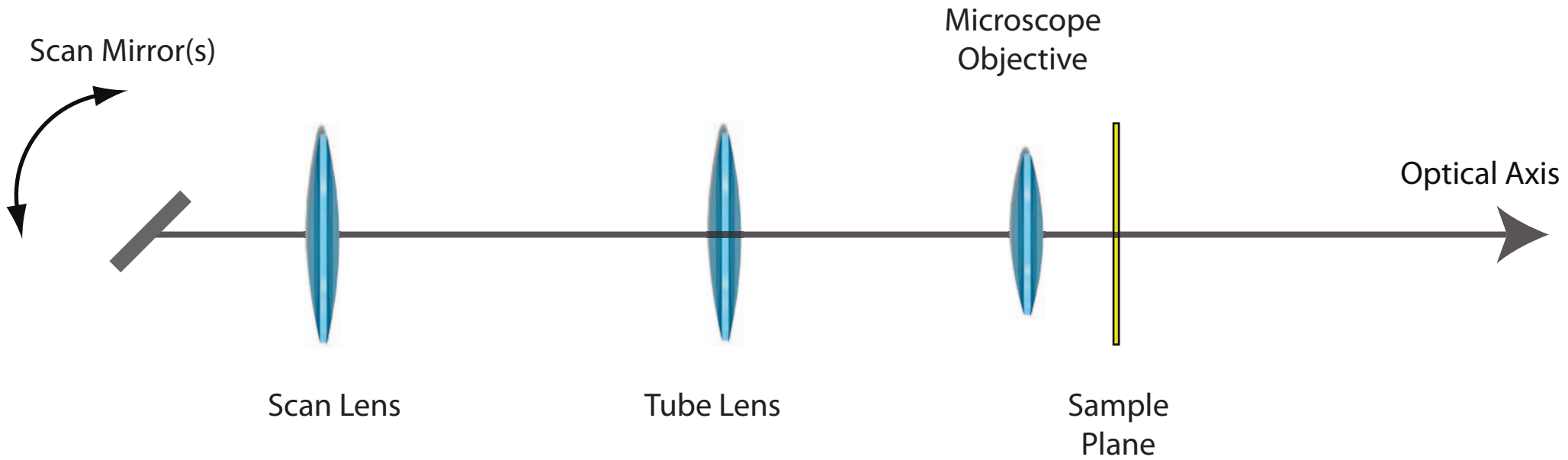




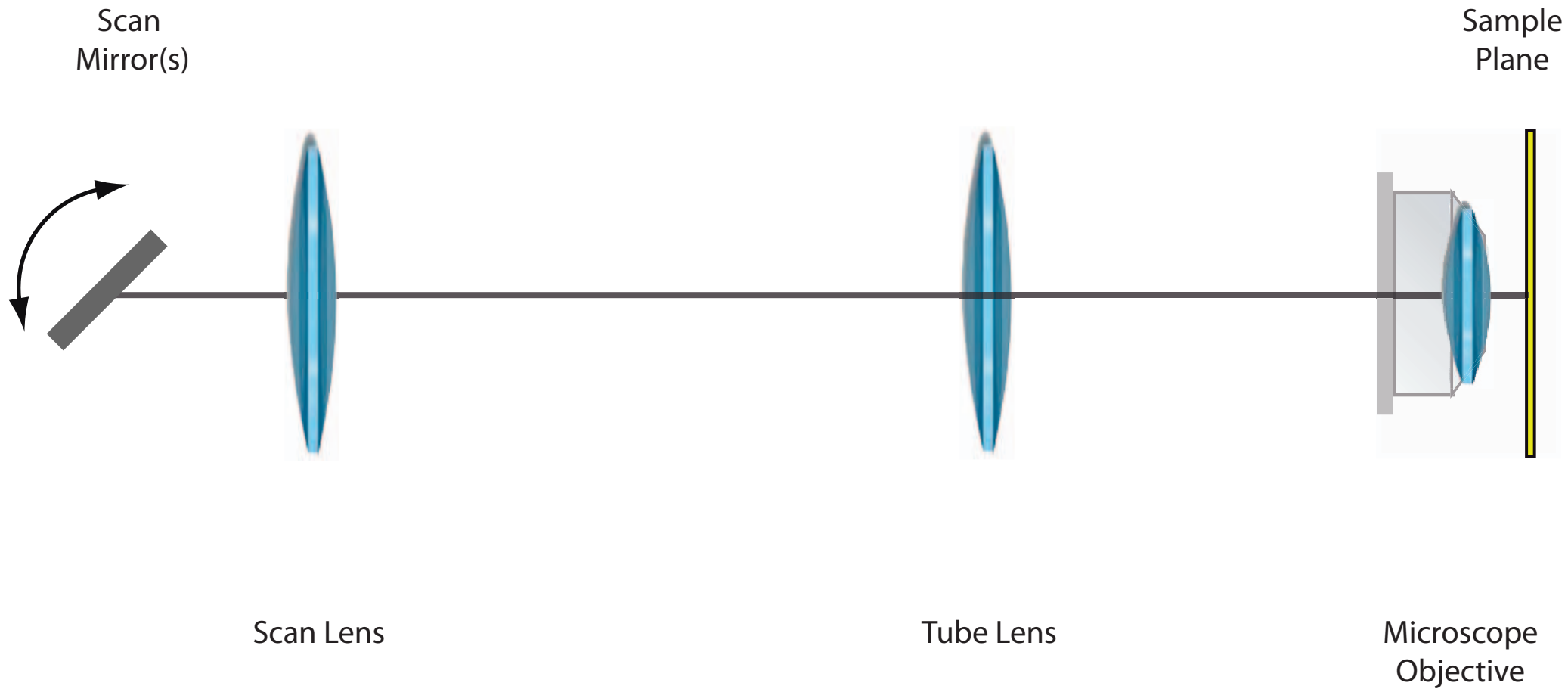
# Laser Scanning Microscopy



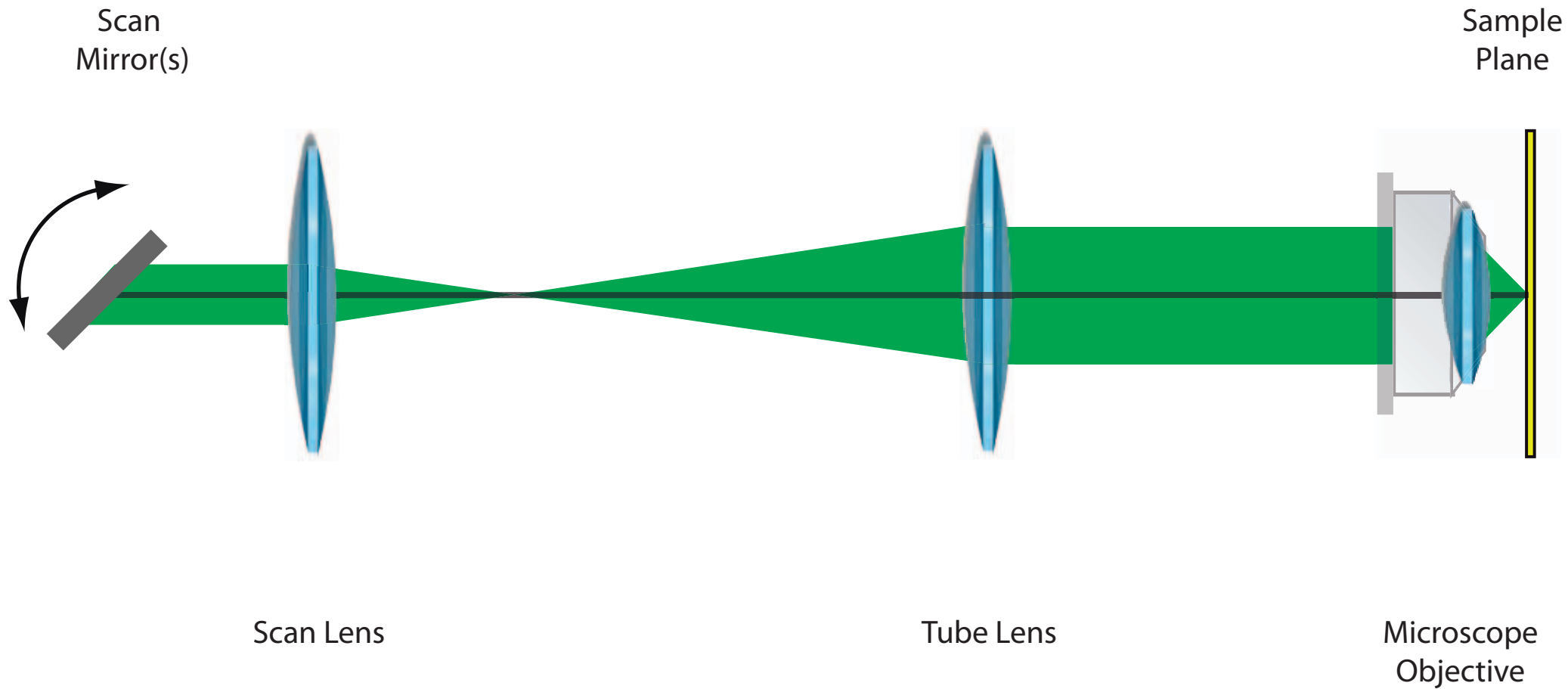
# Laser Scanning Microscopy



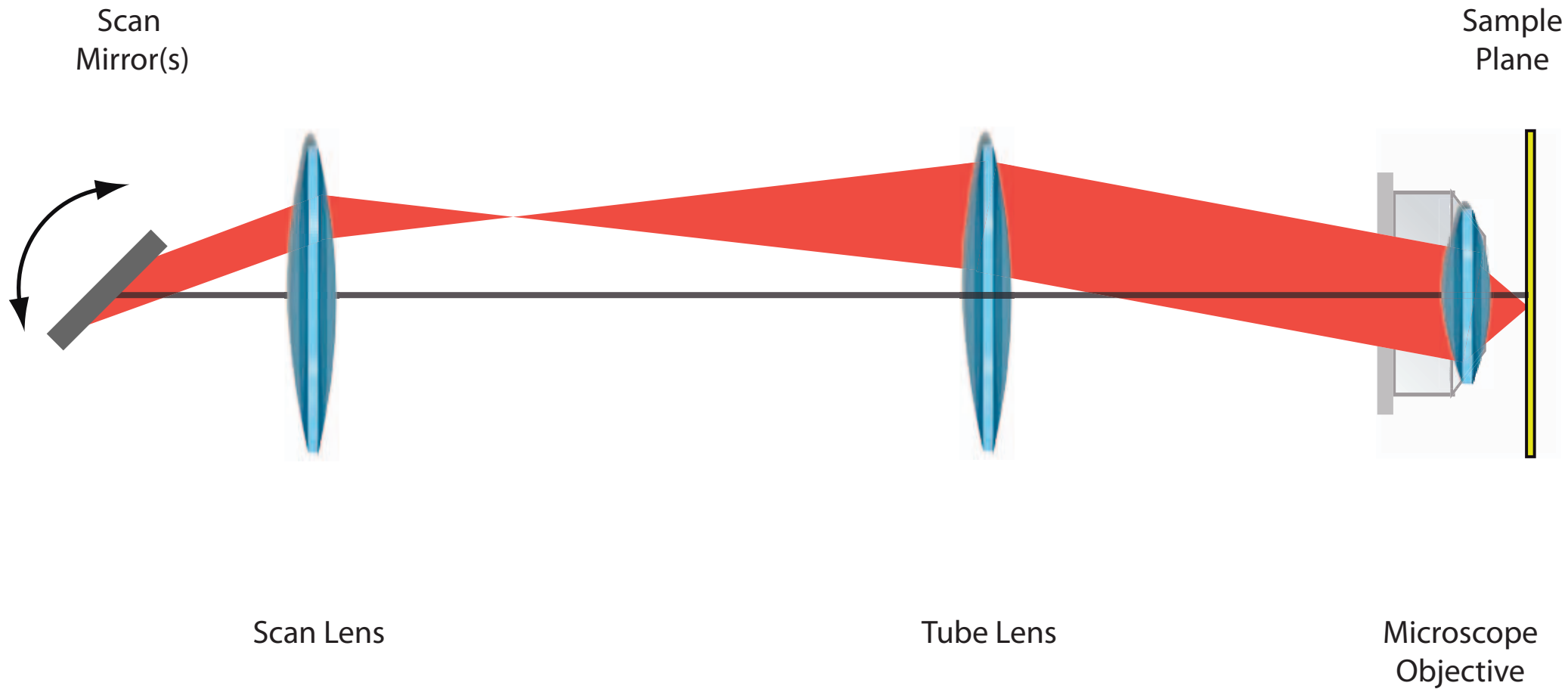
# Laser Scanning Microscopy



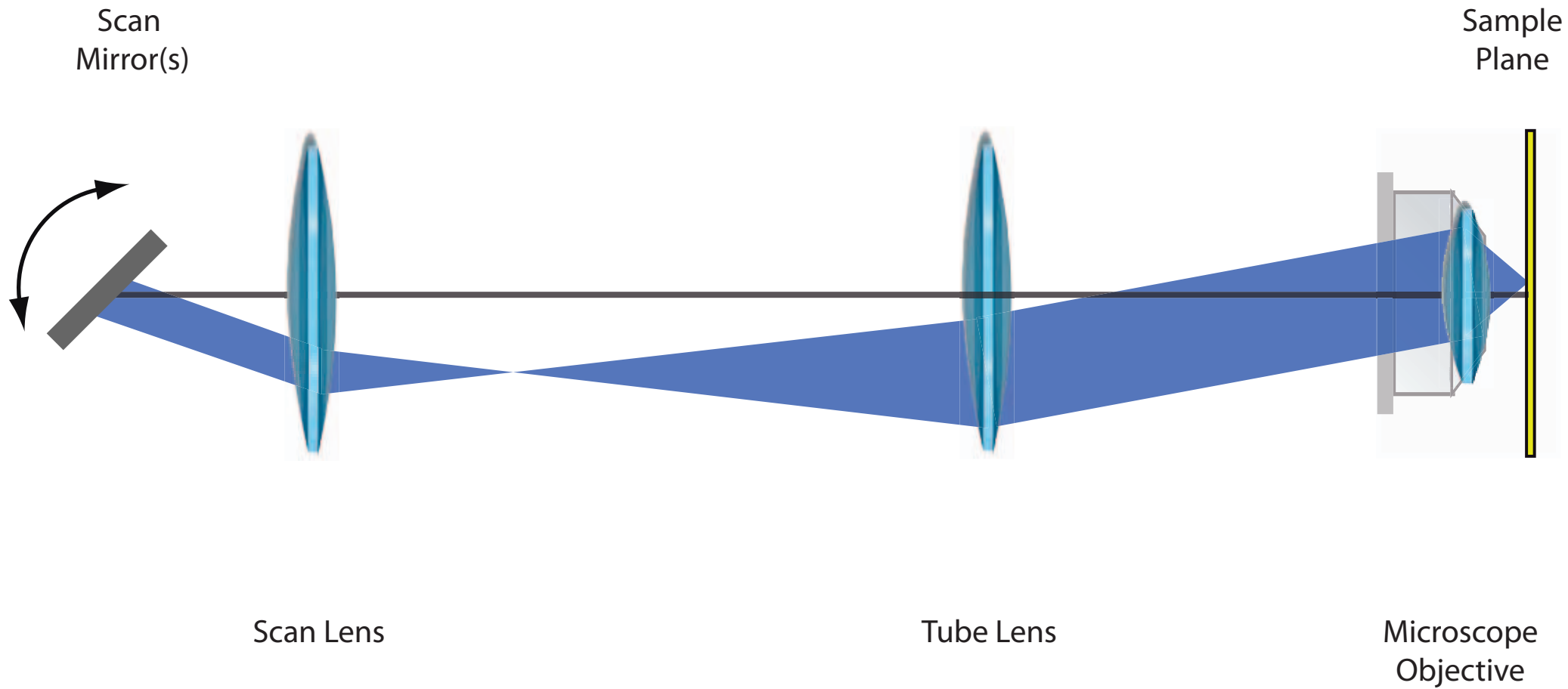
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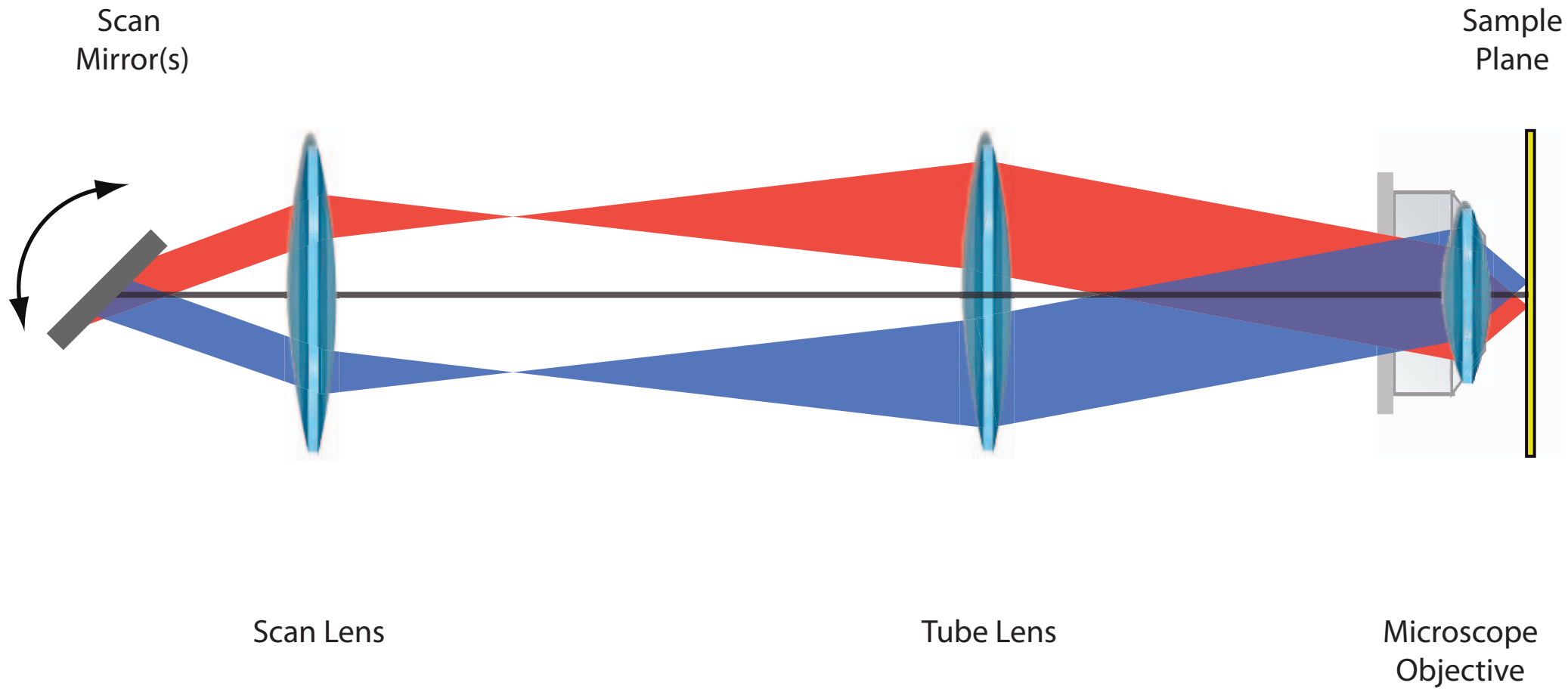
# Laser Scanning Microscopy



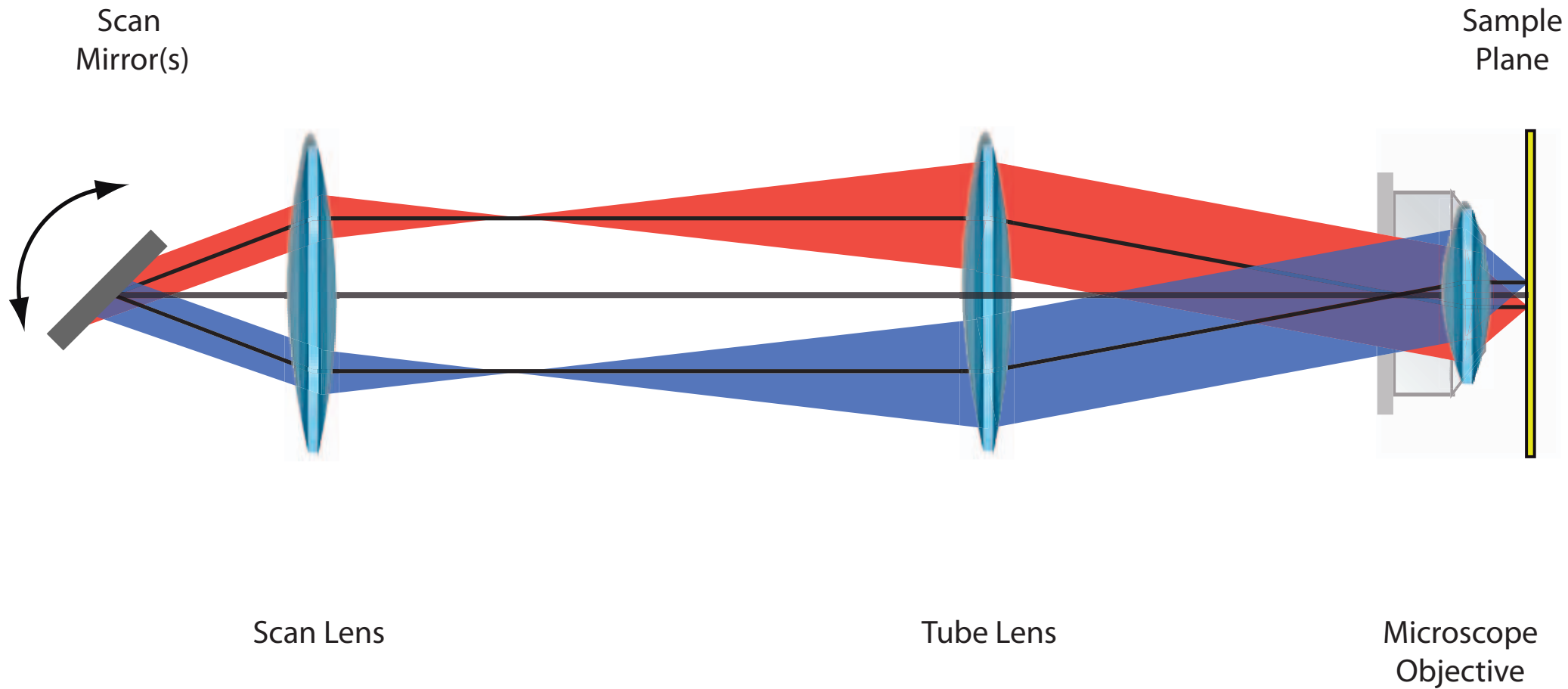
# Laser Scanning Microscopy



# Laser Scanning Microscopy

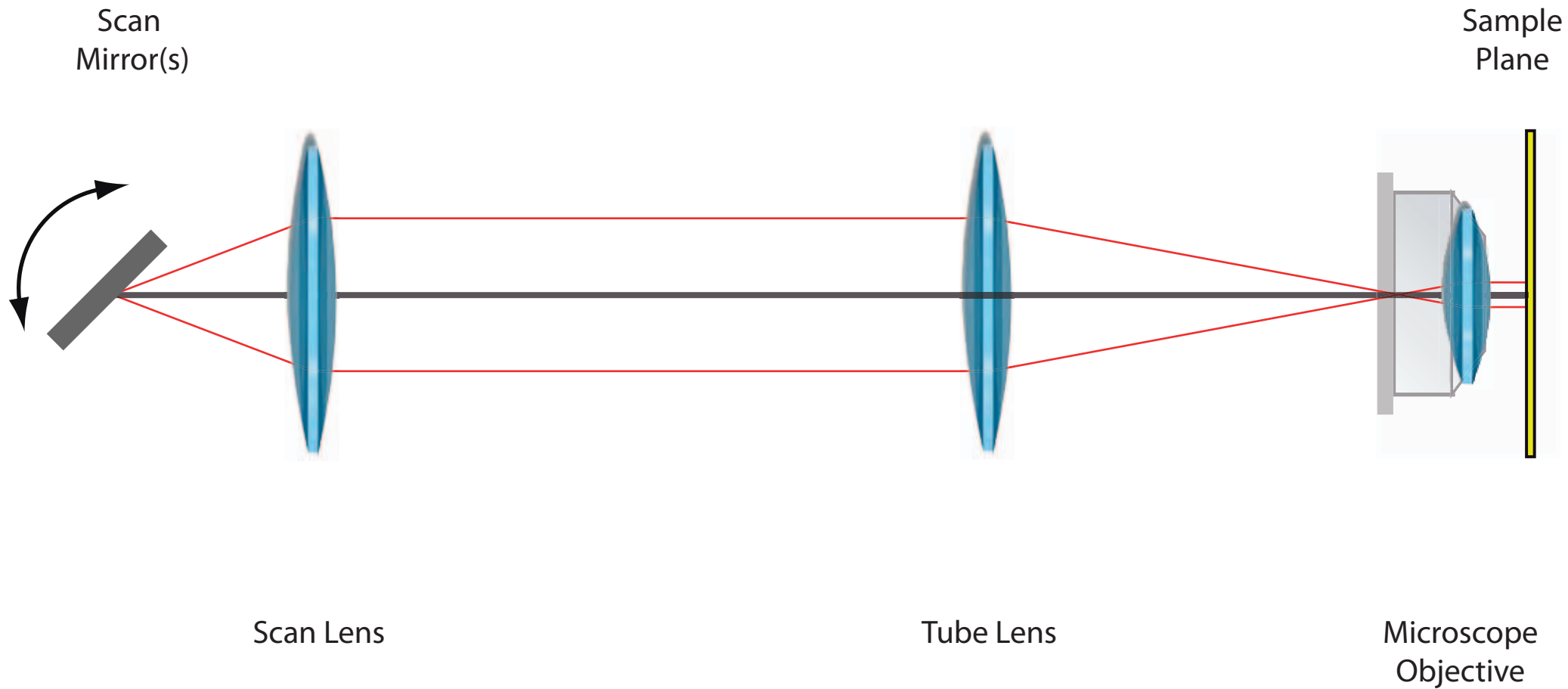


# Laser Scanning Microscopy



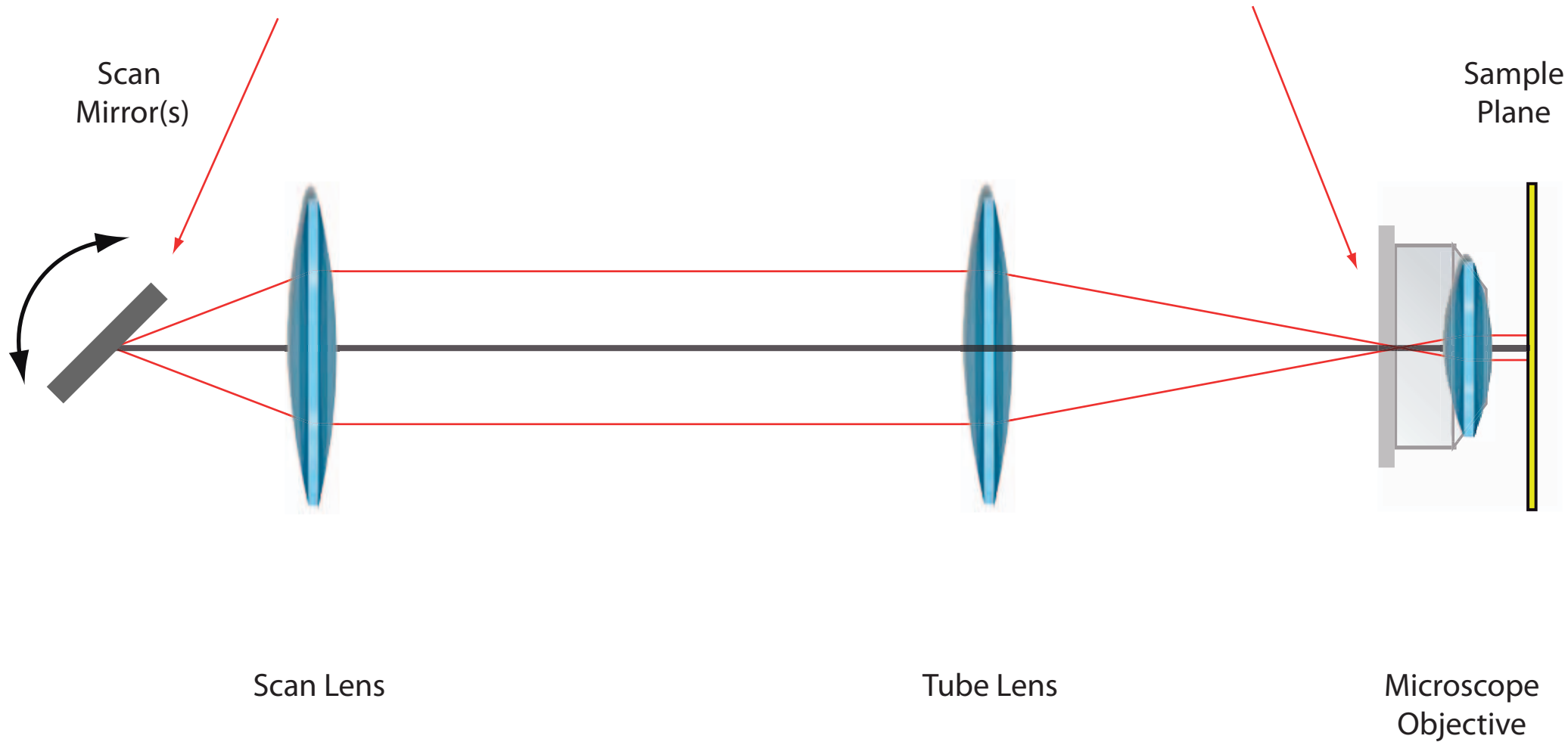


# Laser Scanning Microscopy

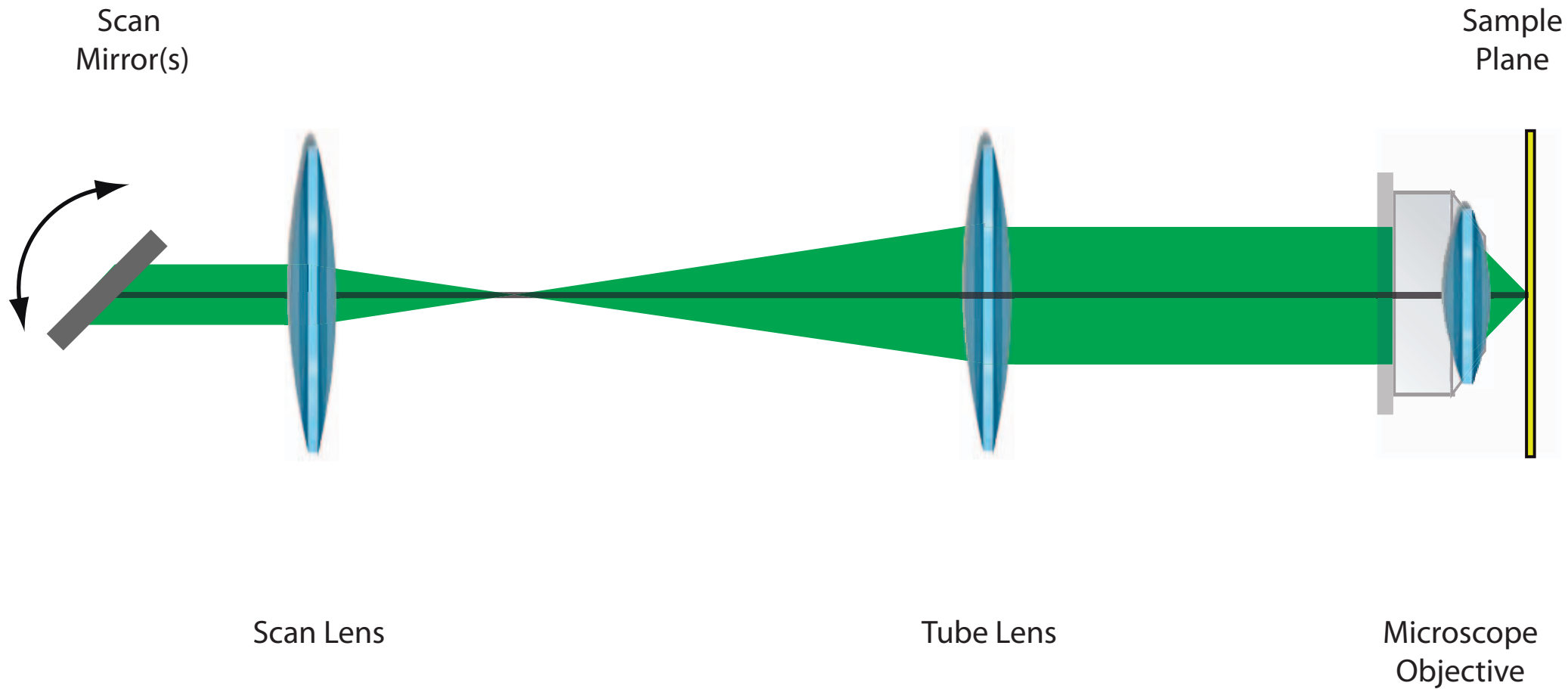


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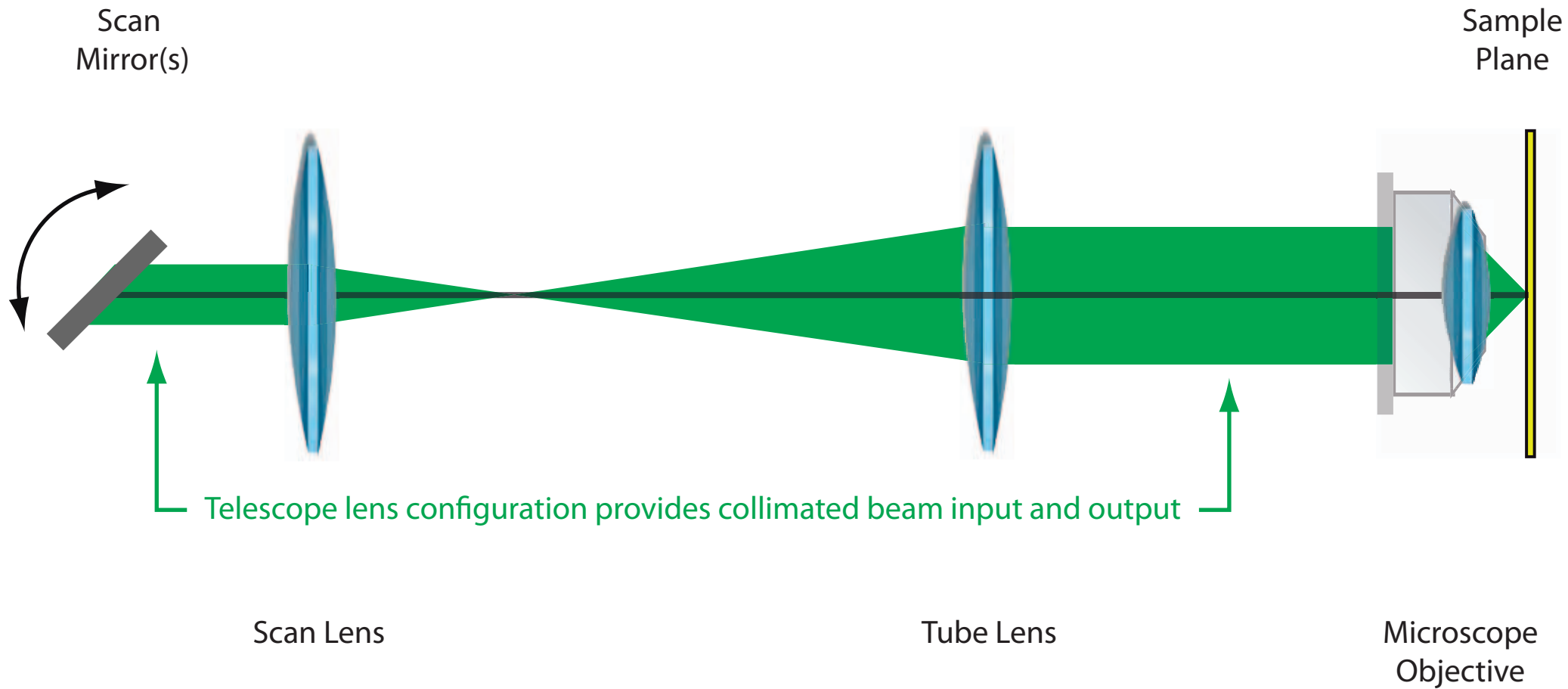
Imaging condition between scan mirror and back aperture of microscope objective



# Laser Scanning Microscopy

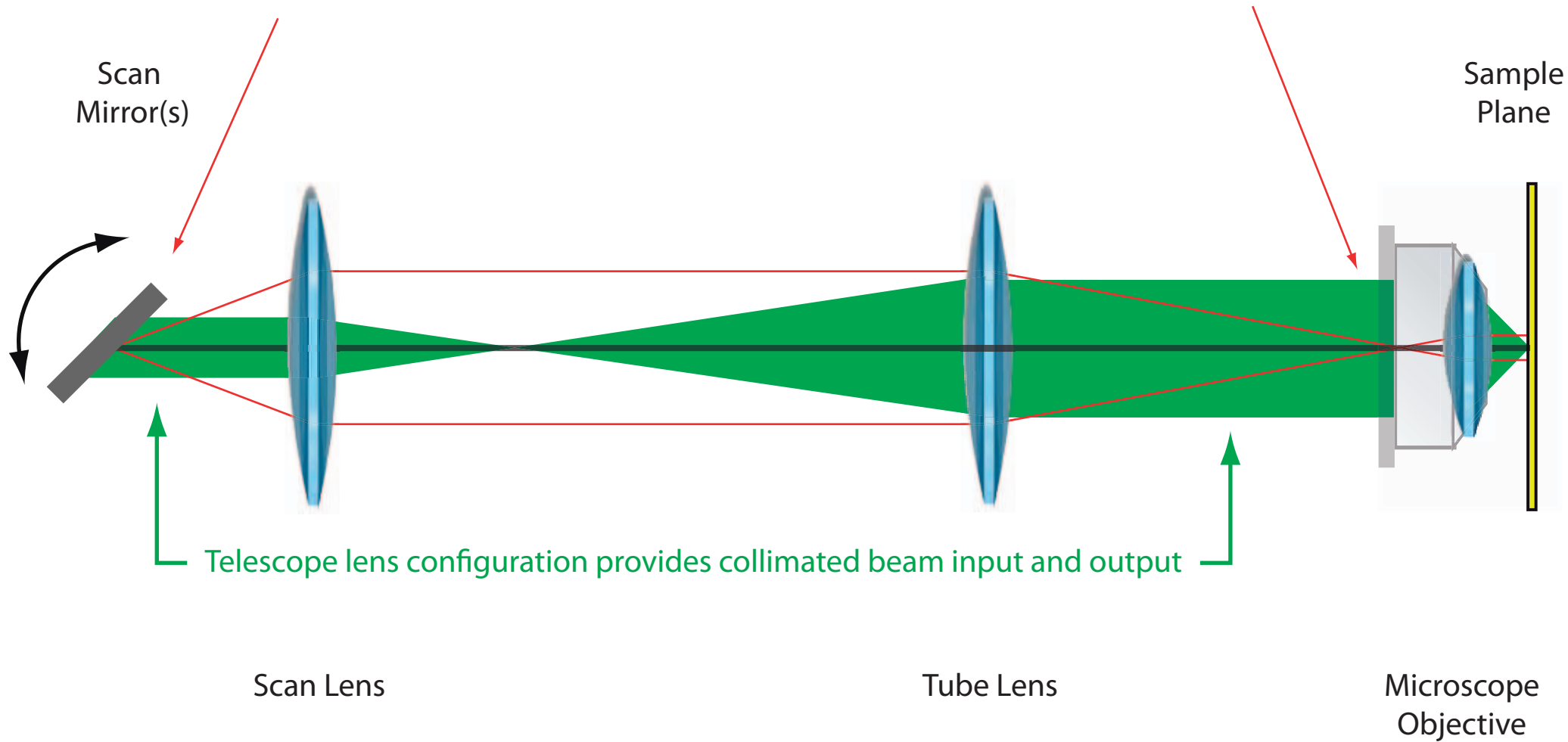


# Laser Scanning Microscopy



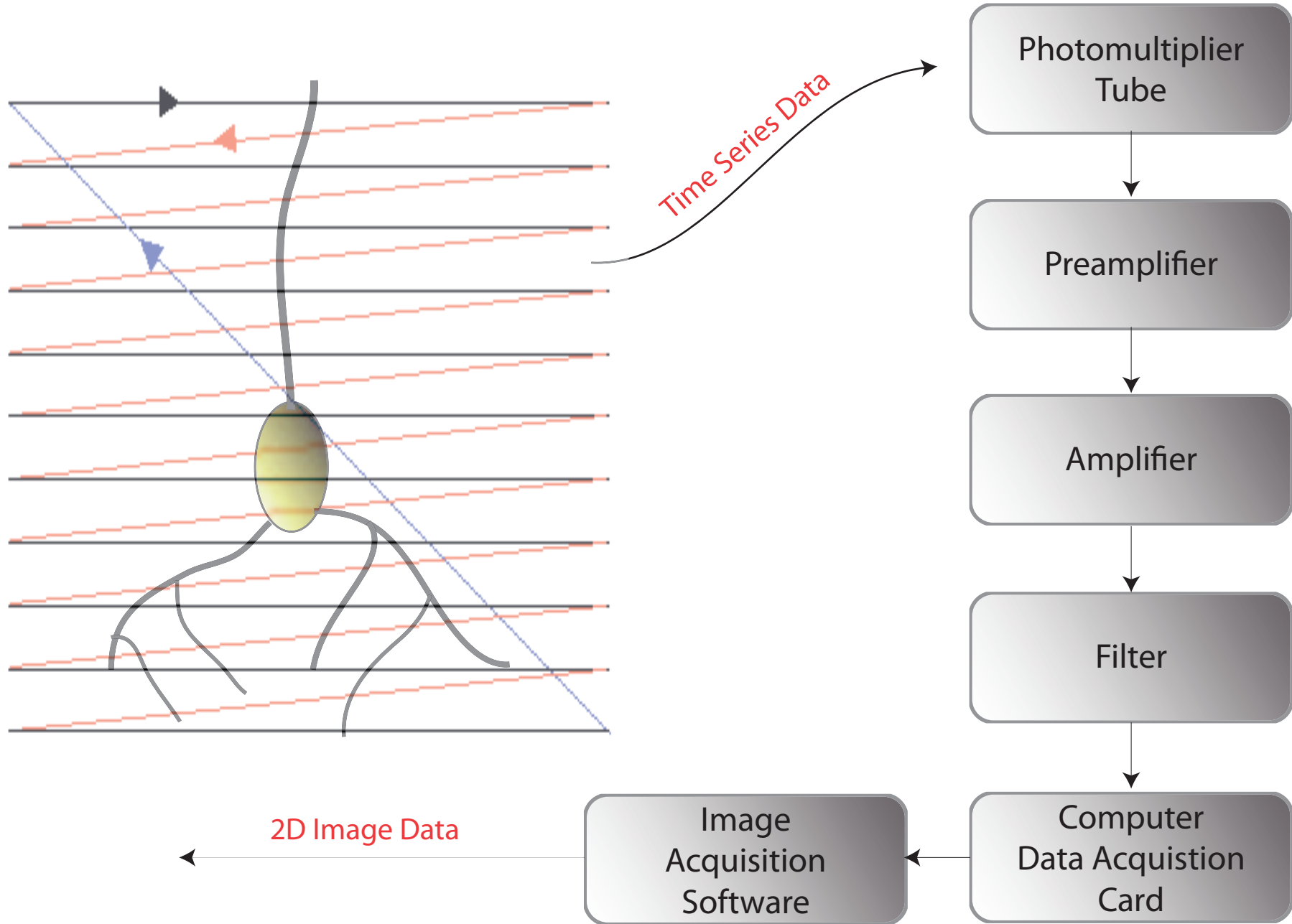
# Laser Scanning Microscopy

Imaging condition between scan mirror and back aperture of microscope objective



# Data Acquisition

## Raster Scan Imaging





# Some Relevant Parameters

## Extinction Coefficient

$\epsilon = 5,000 - 200,000 \text{ M}^{-1} \text{ cm}^{-1}$  for most fluorophores  
refers to the absorption at a single wavelength (typically the maximum)

## Quantum Yield

$Q = 0.05 - 1$  for most fluorophores  
refers to the integrated photon emission over the entire emission spectrum

Below saturation, total fluorescence intensity  $\sim Q * \epsilon$

## Lifetime

$\tau = 1 - 10 \text{ ns}$  for most fluorophores



# A quick & dirty calculation of saturation

Absorption cross-section,  $\sigma$

$$\varepsilon = 80,000 \text{ M}^{-1} \text{ cm}^{-1}$$

$$\sigma = \varepsilon \cdot \ln(10) / 6.023 \cdot 10^{23}$$

$$\sigma(\text{fluorescein}) = 3 \cdot 10^{-16} \text{ cm}^2 \cdot \text{molecule}^{-1} \cdot \text{photon}^{-1}$$

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Assume 1 mW of green light (around 488 nm) at the sample:

$$1 \text{ mW} = 1 \cdot 10^{-3} \text{ J/s}$$

$$1 \text{ photon (488nm)} \leftrightarrow 2.5 \text{ eV} = 4 \cdot 10^{-19} \text{ J}$$

$$1 \text{ mW (488nm)} = 2.5 \cdot 10^{15} \text{ photons/s}$$

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Epifluorescence : Illuminate 500 x 500 um area  $\sim 2 \cdot 10^{-3} \text{ cm}^{-2}$

$$\text{Intensity} = \text{Power} / \text{Area} \sim 1.25 \cdot 10^{18} \cdot \text{photons} \cdot \text{cm}^{-2} \cdot \text{s}^{-1}$$

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Point Scanning : Illuminate 0.5 x 0.5 um area  $\sim 2 \cdot 10^{-9} \text{ cm}^{-2}$

$$\text{Intensity} = \text{Power} / \text{Area} \sim 1.25 \cdot 10^{24} \cdot \text{photons} \cdot \text{cm}^{-2} \cdot \text{s}^{-1}$$

# A quick & dirty calculation of saturation

## Absorption and Fluorescence Rates

$$k_a = \sigma \cdot I$$

$$k_f = 1/\tau$$

Let  $x$  = fraction of fluorophores in the excited state

$$k_a \cdot (1-x) = k_f \cdot x \quad \leftarrow \text{in steady state}$$

$$\mathbf{x = k_a / (k_a + k_f)}$$

# A quick & dirty calculation of saturation

## Epifluorescence :

$$I = \text{Power} / \text{Area} \sim 1.25 \cdot 10^{18} \cdot \text{photons} \cdot \text{cm}^{-2} \cdot \text{s}^{-1}$$

$$\sigma(\text{fluorescein}) = 3 \cdot 10^{-16} \text{ cm}^2 \cdot \text{molecule}^{-1} \cdot \text{photon}^{-1}$$

$$k_f = 1/\tau = 1 / 4.5 \text{ ns} = 2.2 \cdot 10^8 \text{ s}^{-1}$$

$$k_a = \sigma \cdot I = 375 \text{ s}^{-1}$$

$$x = k_a / (k_a + k_f) = 1.7 \cdot 10^{-6}$$

**Only ~ 2 out of every billion fluorophores is in the excited state**

# A quick & dirty calculation of saturation

## Point Scanning :

$$I = \text{Power} / \text{Area} \sim 1.25 \cdot 10^{24} \cdot \text{photons} \cdot \text{cm}^{-2} \cdot \text{s}^{-1}$$

$$\sigma(\text{fluorescein}) = 3 \cdot 10^{-16} \text{ cm}^2 \cdot \text{molecule}^{-1} \cdot \text{photon}^{-1}$$

$$k_f = 1/\tau = 1 / 4.5 \text{ ns} = 2.2 \cdot 10^8 \text{ s}^{-1}$$

$$k_a = \sigma \cdot I = 3.75 \cdot 10^8 \text{ s}^{-1}$$

$$x = k_a / (k_a + k_f) = 0.63$$

**63% of the fluorophores is in the excited state!**



# Why is saturation bad?

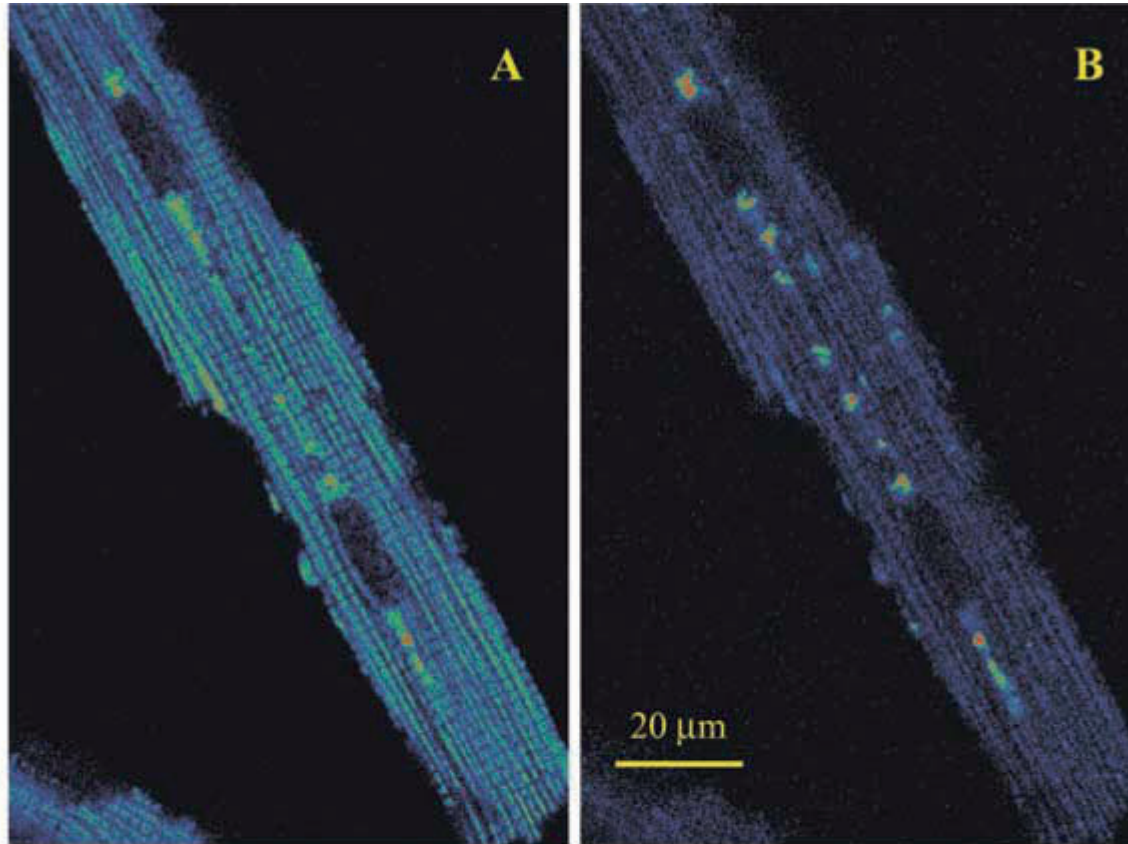
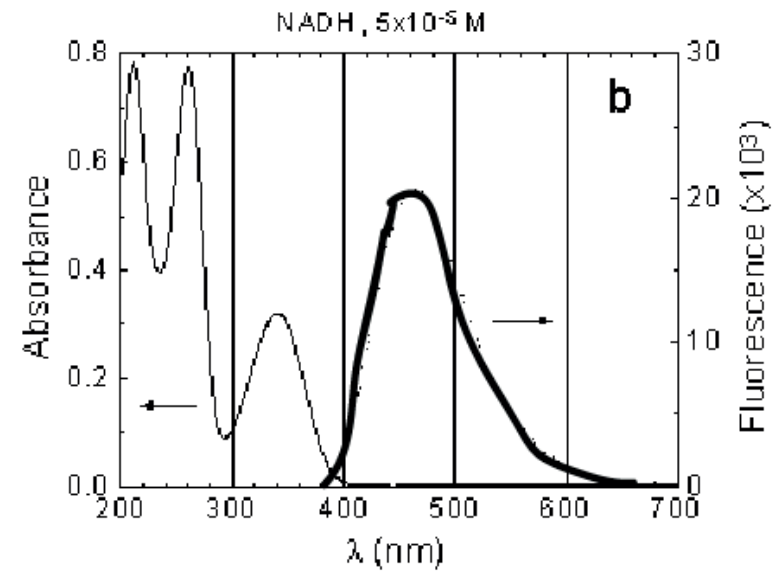
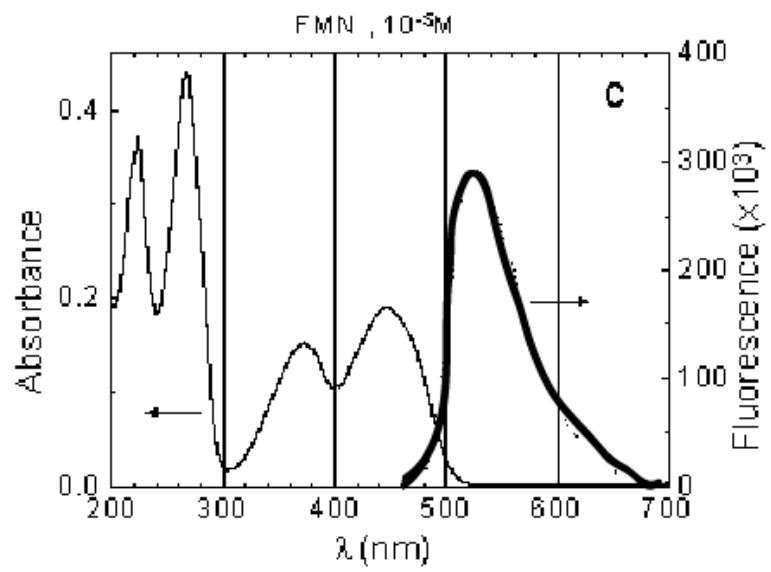


FIGURE 3 At 750 nm excitation, the autofluorescence emission of isolated cardiomyocyte is divided between PMT1 (~410–490 nm) and PMT2 (~510–650 nm), which are set up for maximal detection of the NAD(P)H and FP fluorescence, respectively. The 2P-autofluorescence image obtained at PMT1 (*A*) is much brighter than that at PMT2 (*B*), indicating a predominant NAD(P)H signal. Images shown are the average of five consecutive scans.

Taken from Huang, et. al., Biophysical Journal., 2002



web source : [http://www.photobiology.com/photobiology2000/V5itas/ps\\_abs\\_sp\\_resd.htm](http://www.photobiology.com/photobiology2000/V5itas/ps_abs_sp_resd.htm)

# Molar Extinction Coefficients

Alexa Fluor 555 : 150000 cm<sup>-1</sup> M<sup>-1</sup>

Fluorescein : 70000 cm<sup>-1</sup> M<sup>-1</sup>

eGFP : 55000 cm<sup>-1</sup> M<sup>-1</sup>

NADH : 6220 cm<sup>-1</sup> M<sup>-1</sup>

# Time averaging to recover S/N

# Photobleaching

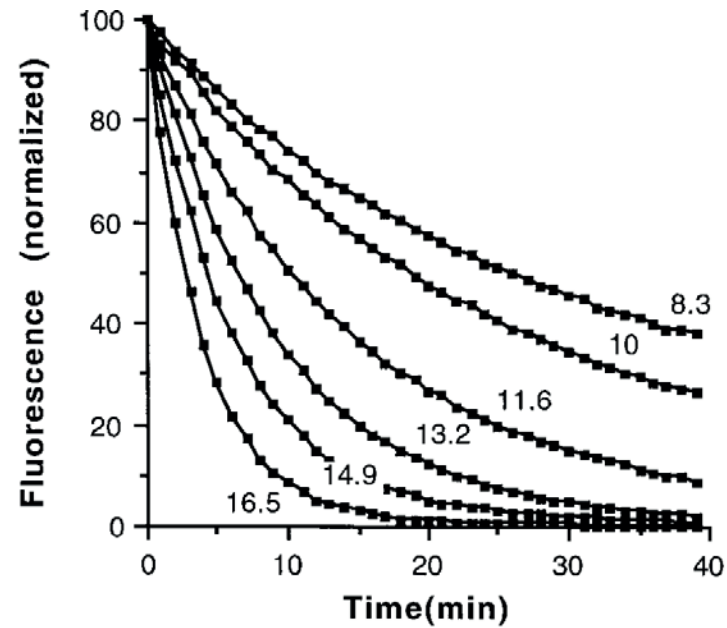
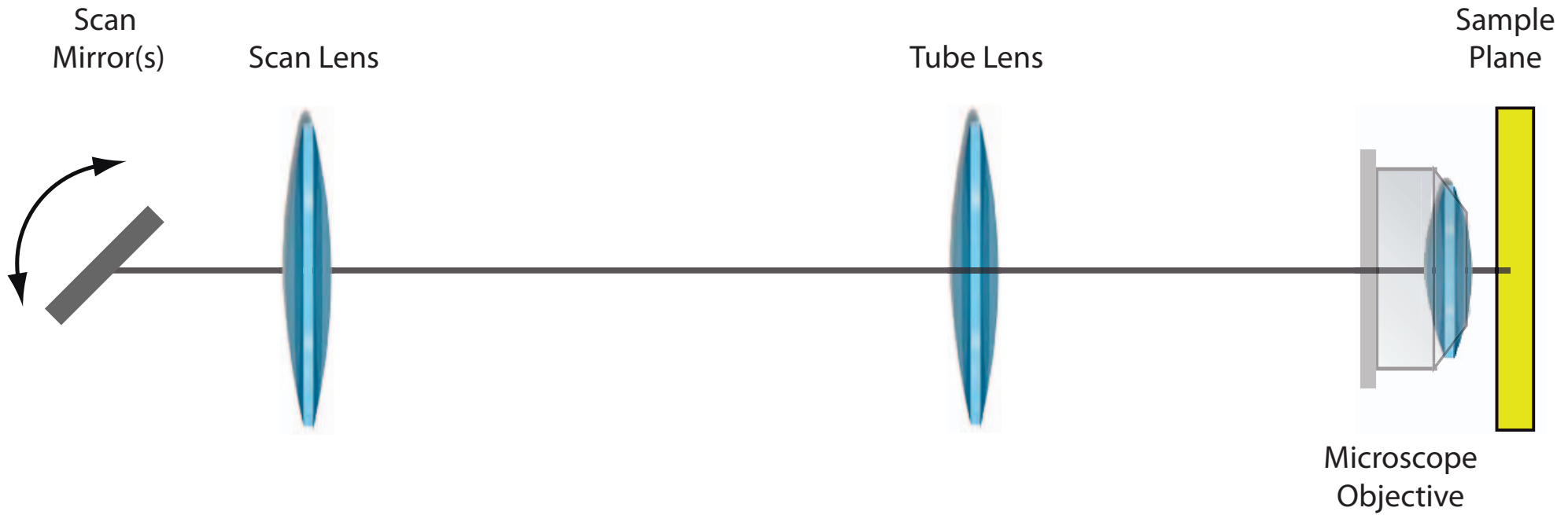


FIGURE 1 Fluorescein dextran ( $10 \mu\text{M}$  in pH 7.3) was suspended in  $\sim 1\text{-}\mu\text{m}$ -thick microdroplets and continuously irradiated with 710 nm mode-locked laser light at six different power levels (in mW units) while collecting images at 1-min time points.

Taken from Patterson & Piston, 2000, Biophysical Journal

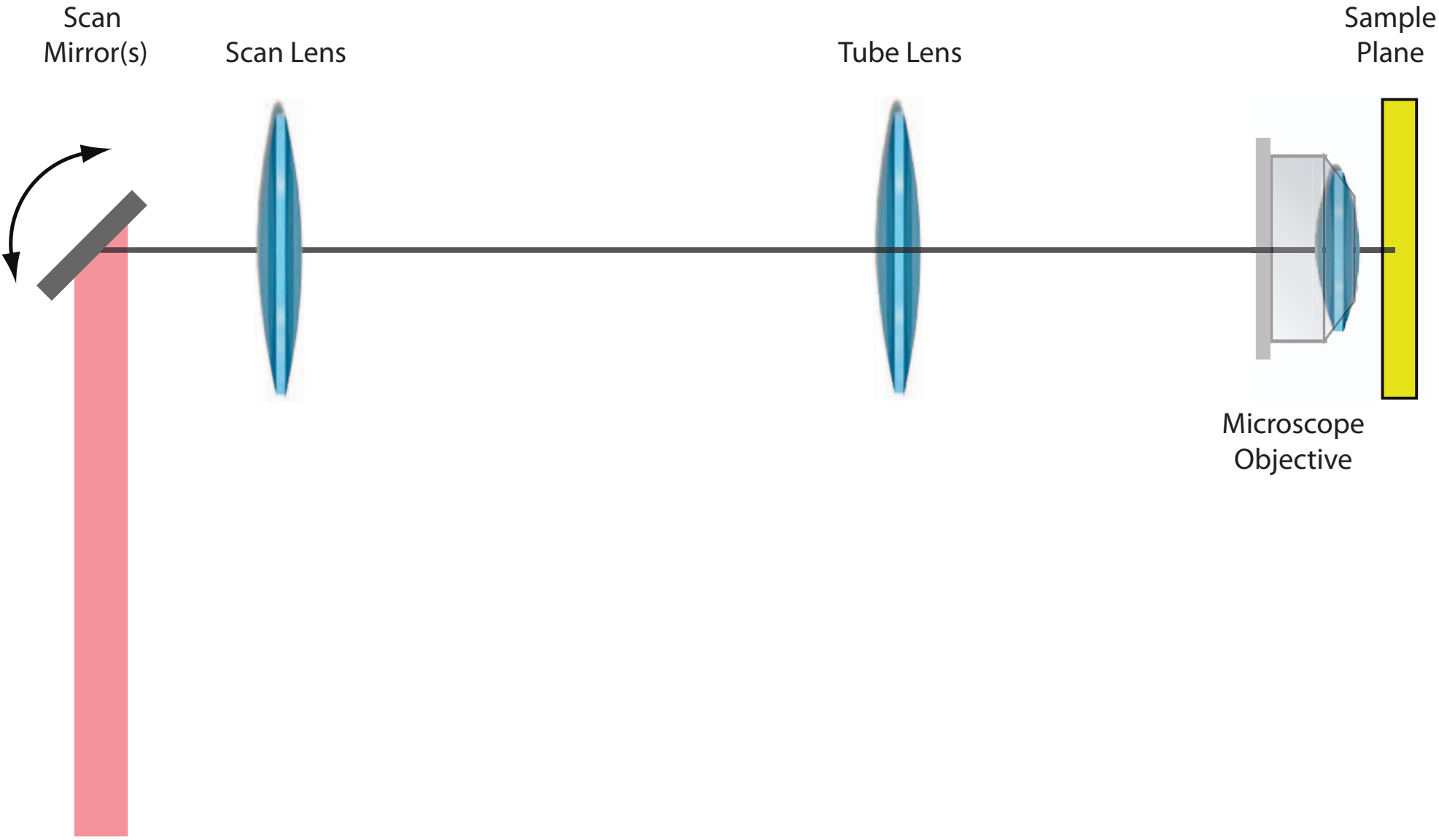


# Confocal Laser Scanning Microscopy

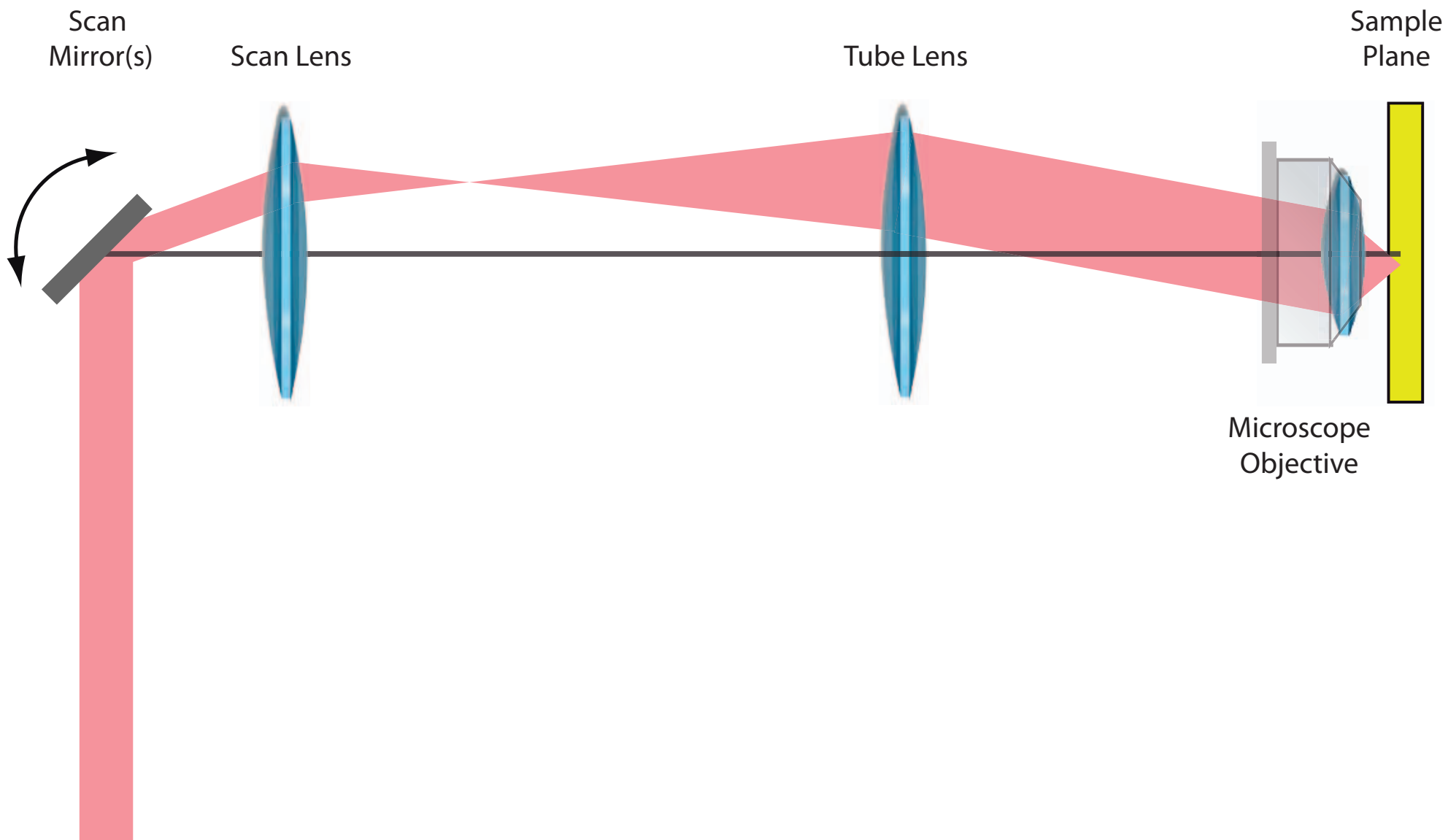




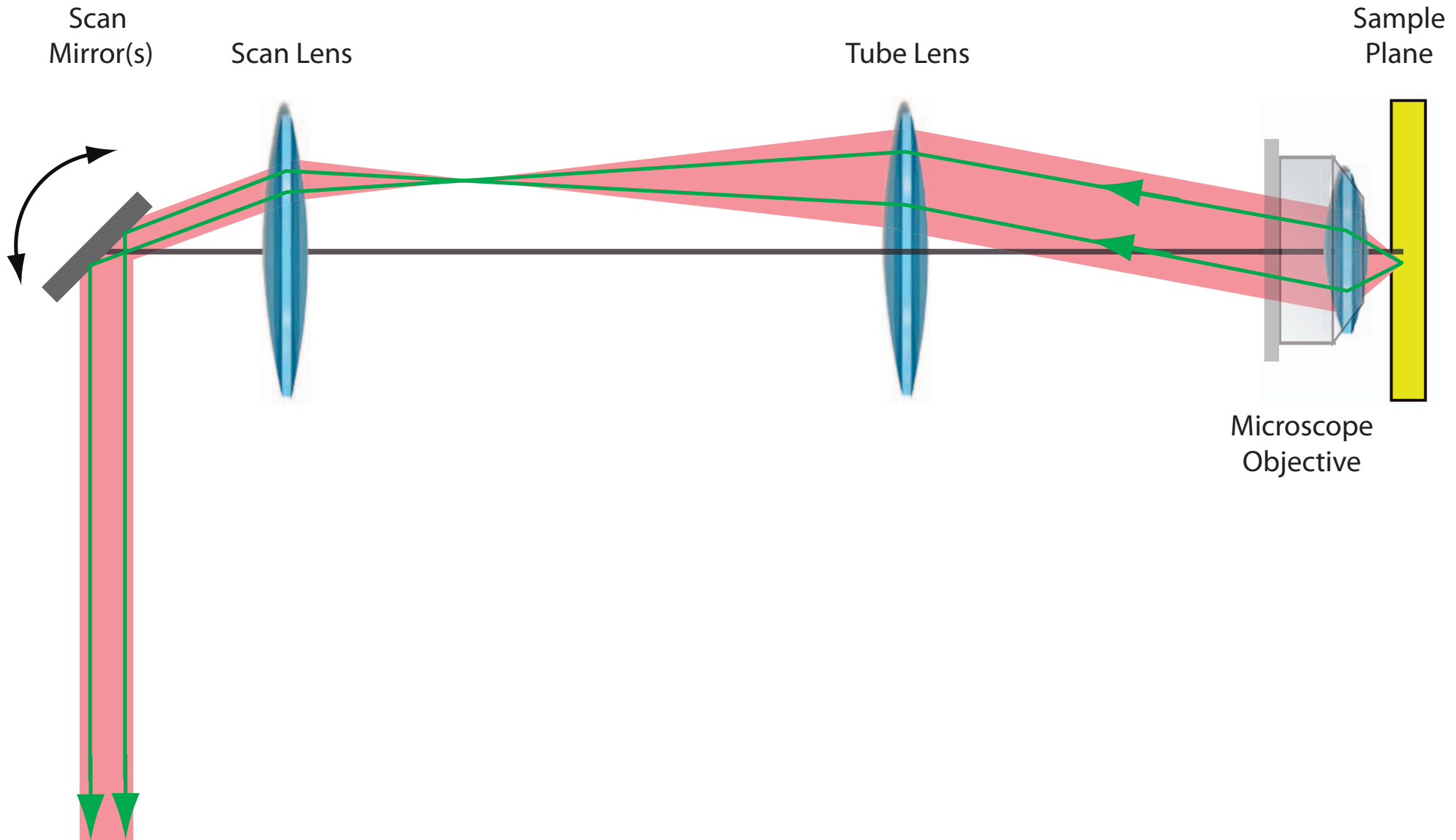
# Confocal Laser Scanning Microscopy



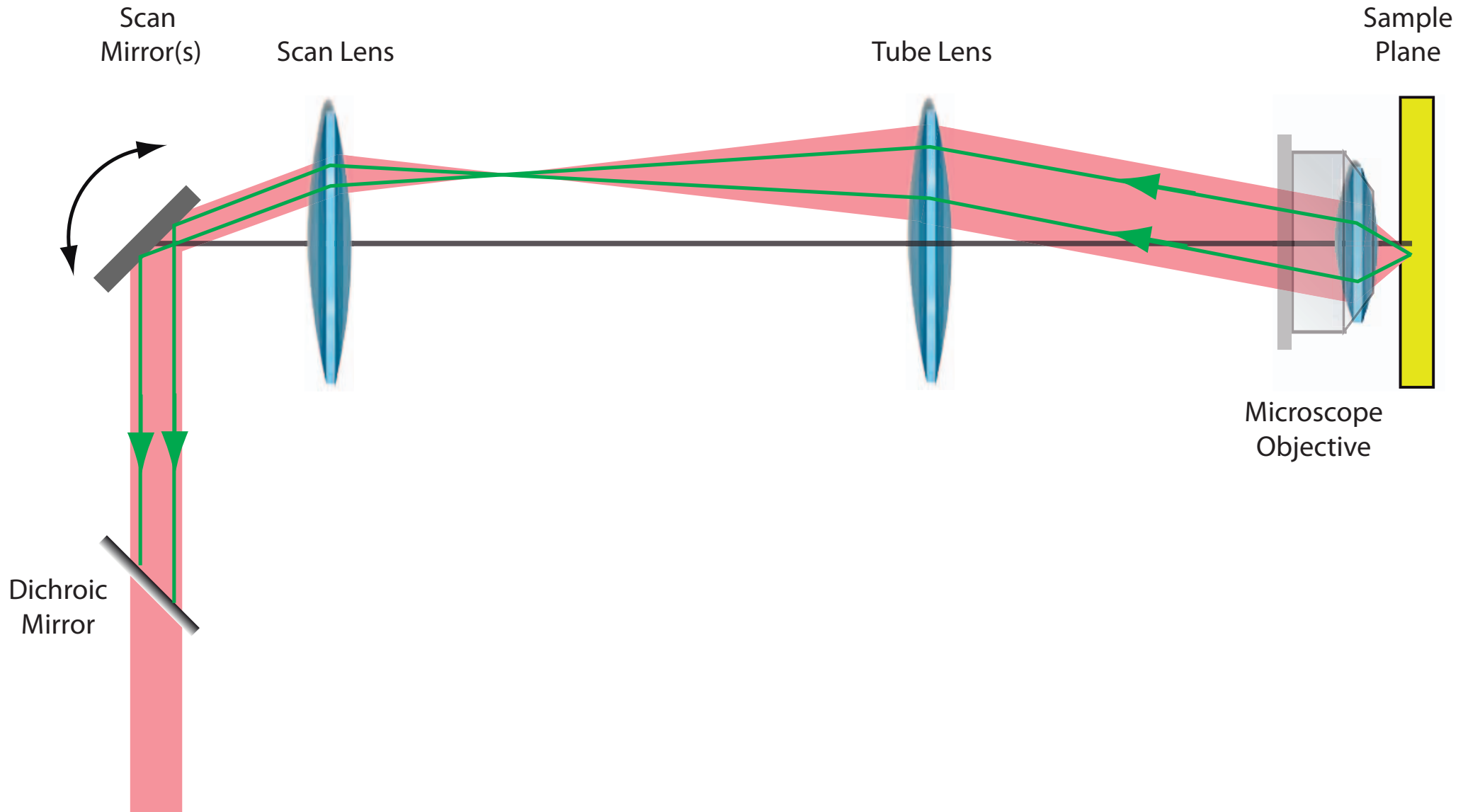
# Confocal Laser Scanning Microscopy



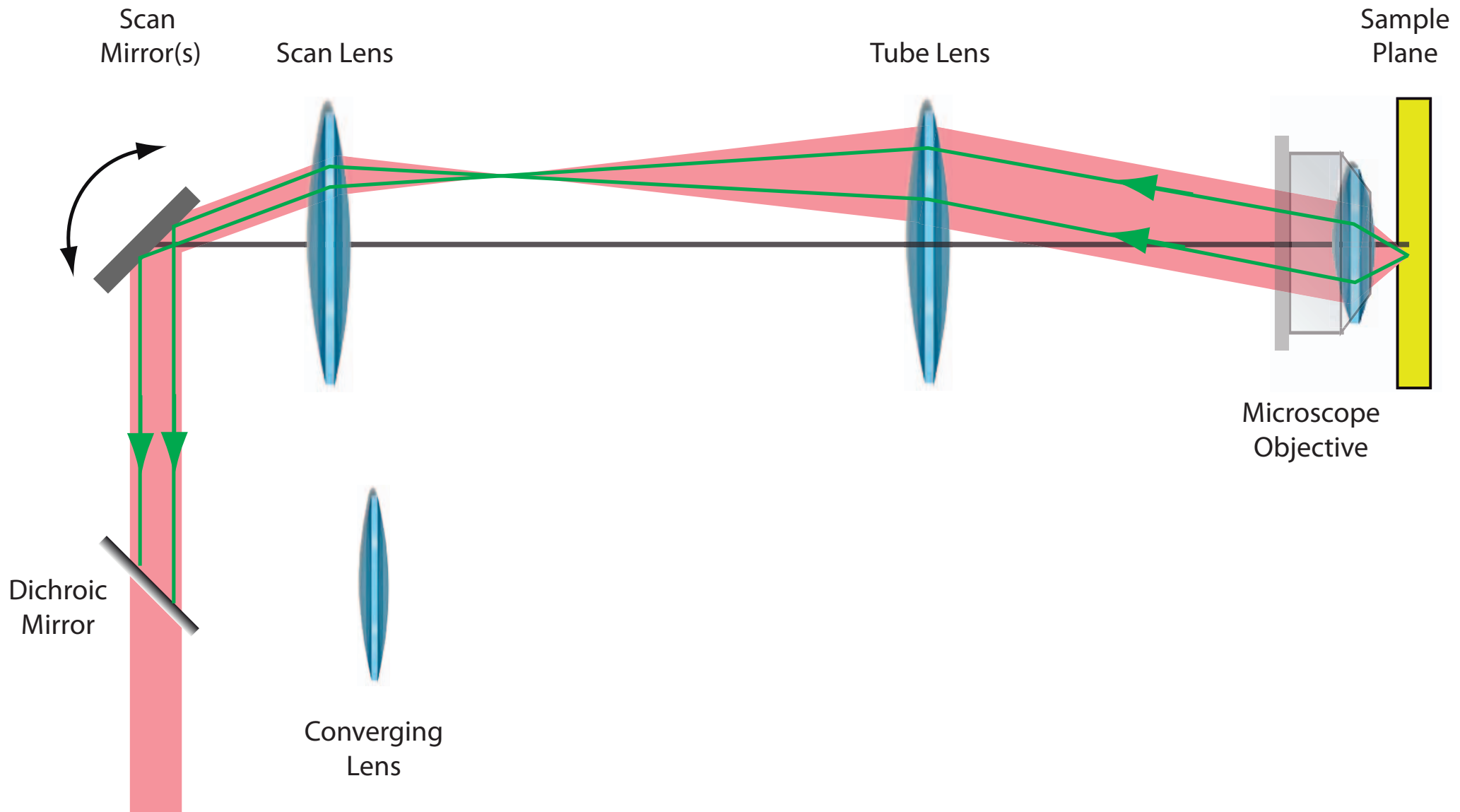
# Confocal Laser Scanning Microscopy



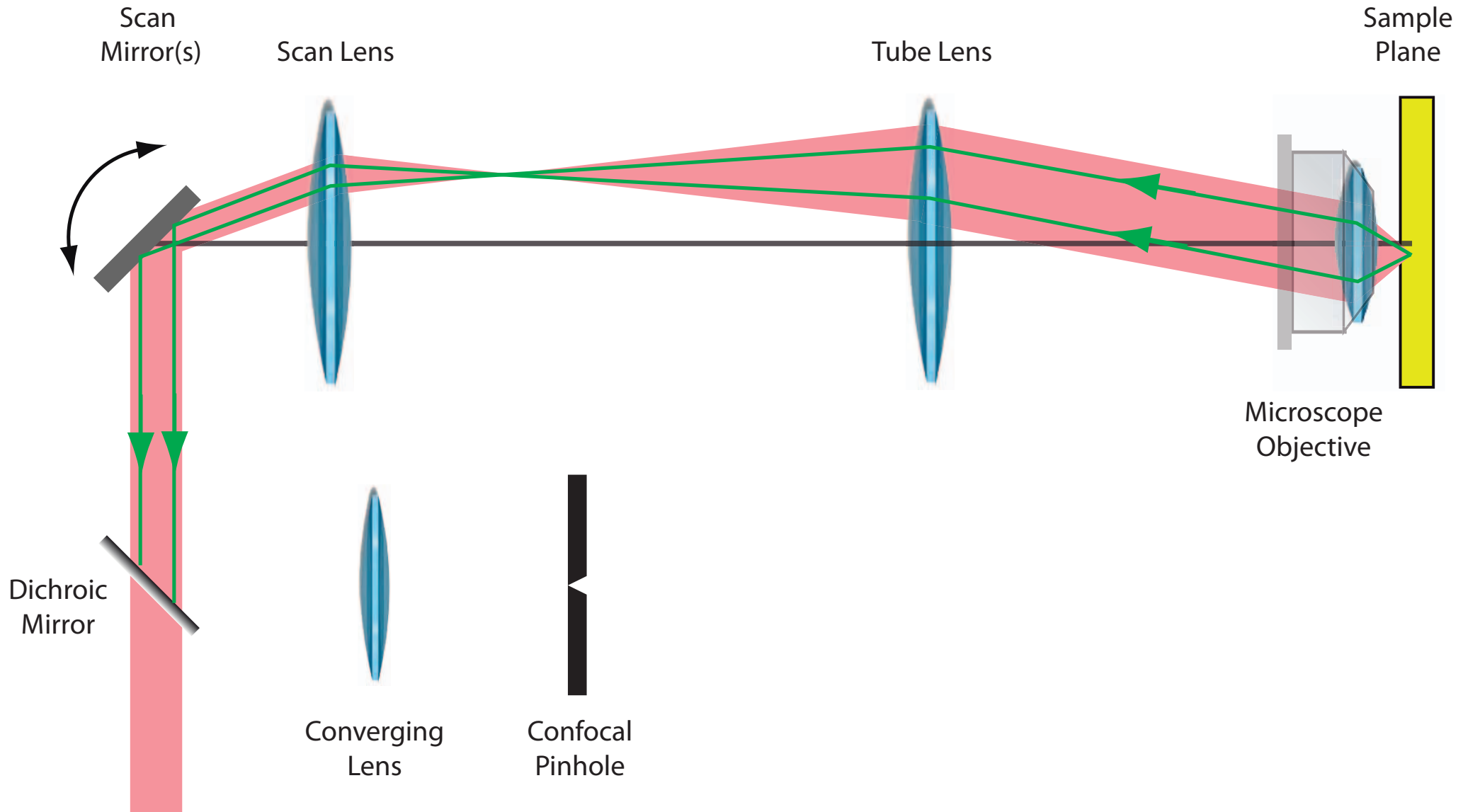
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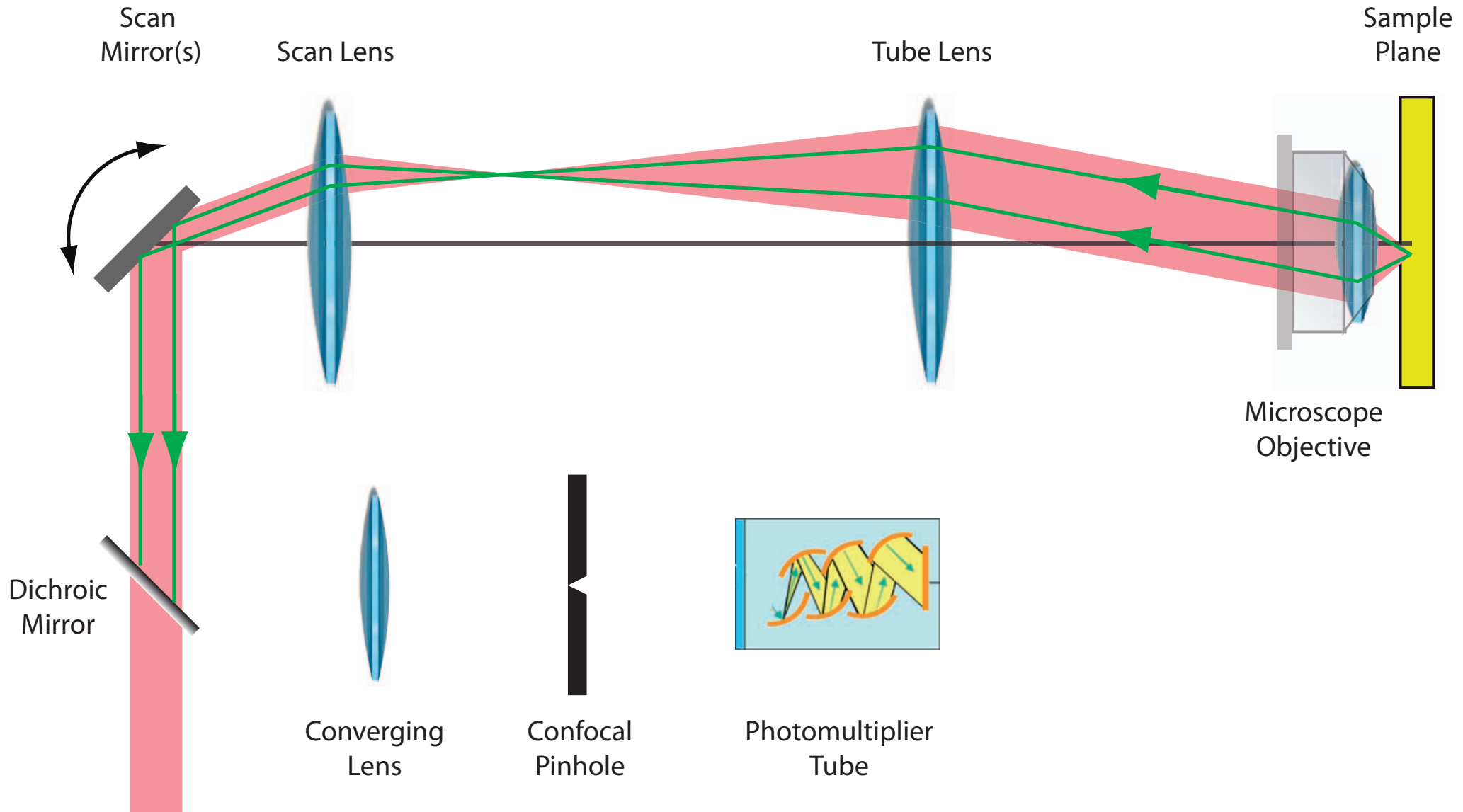
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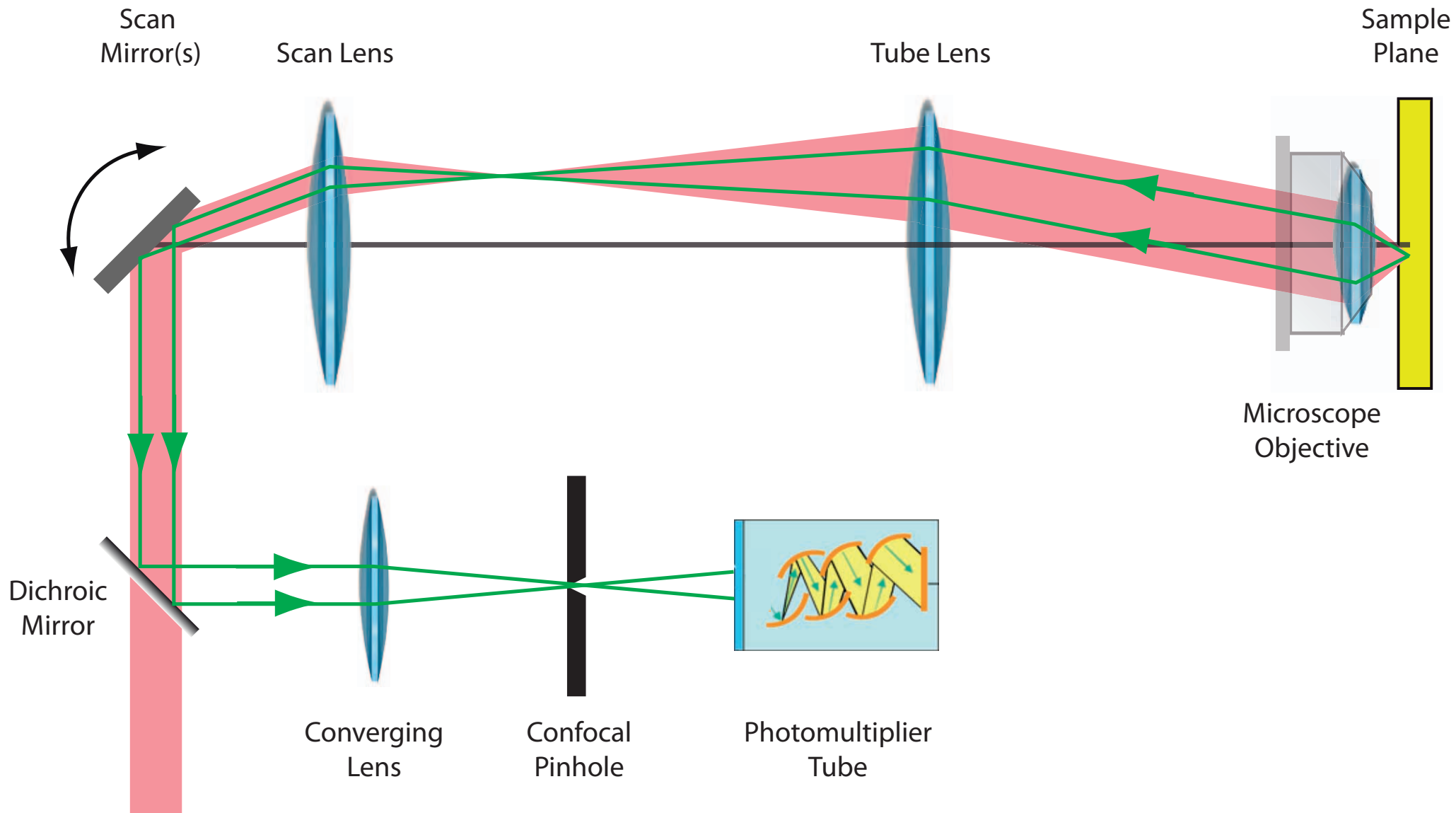
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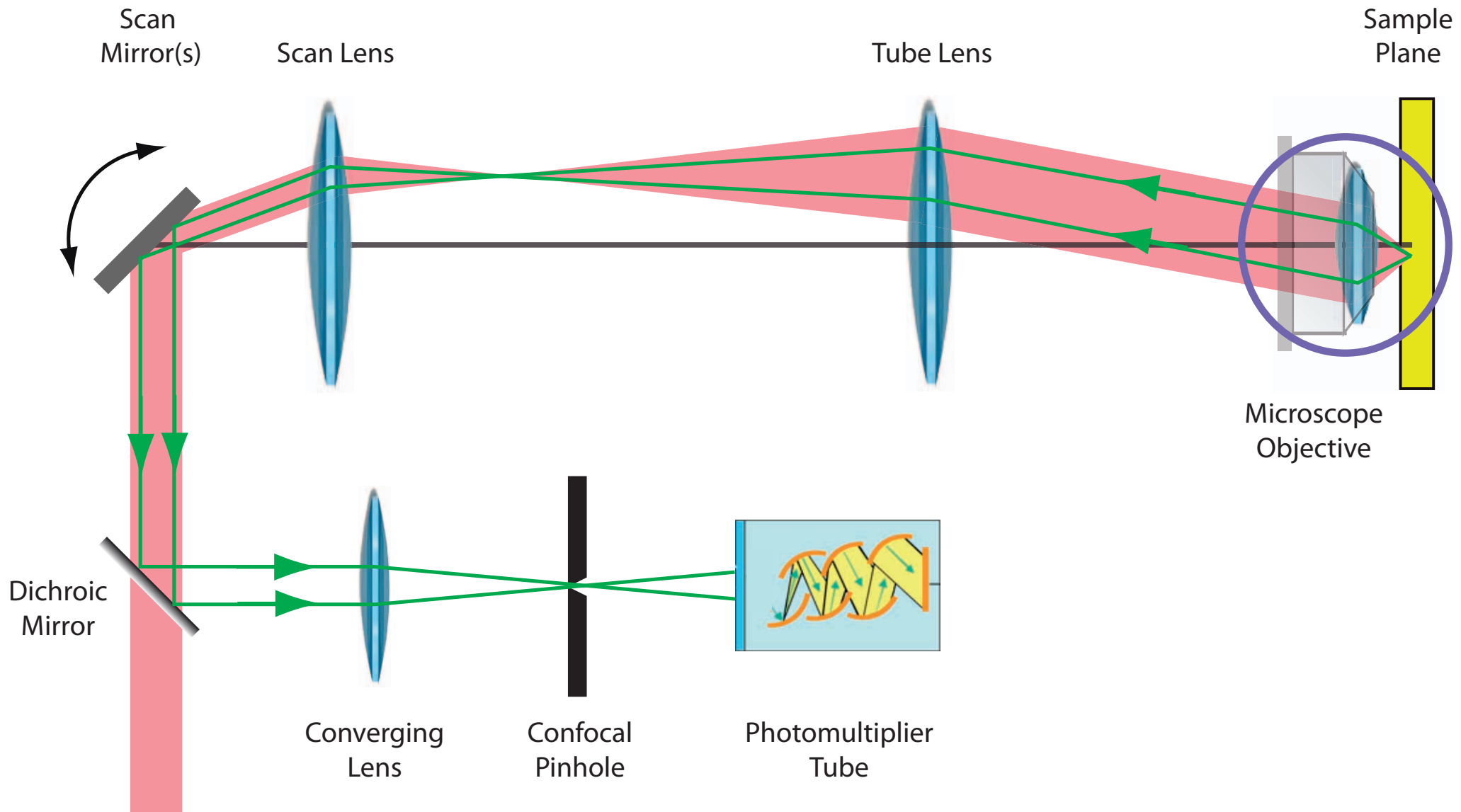


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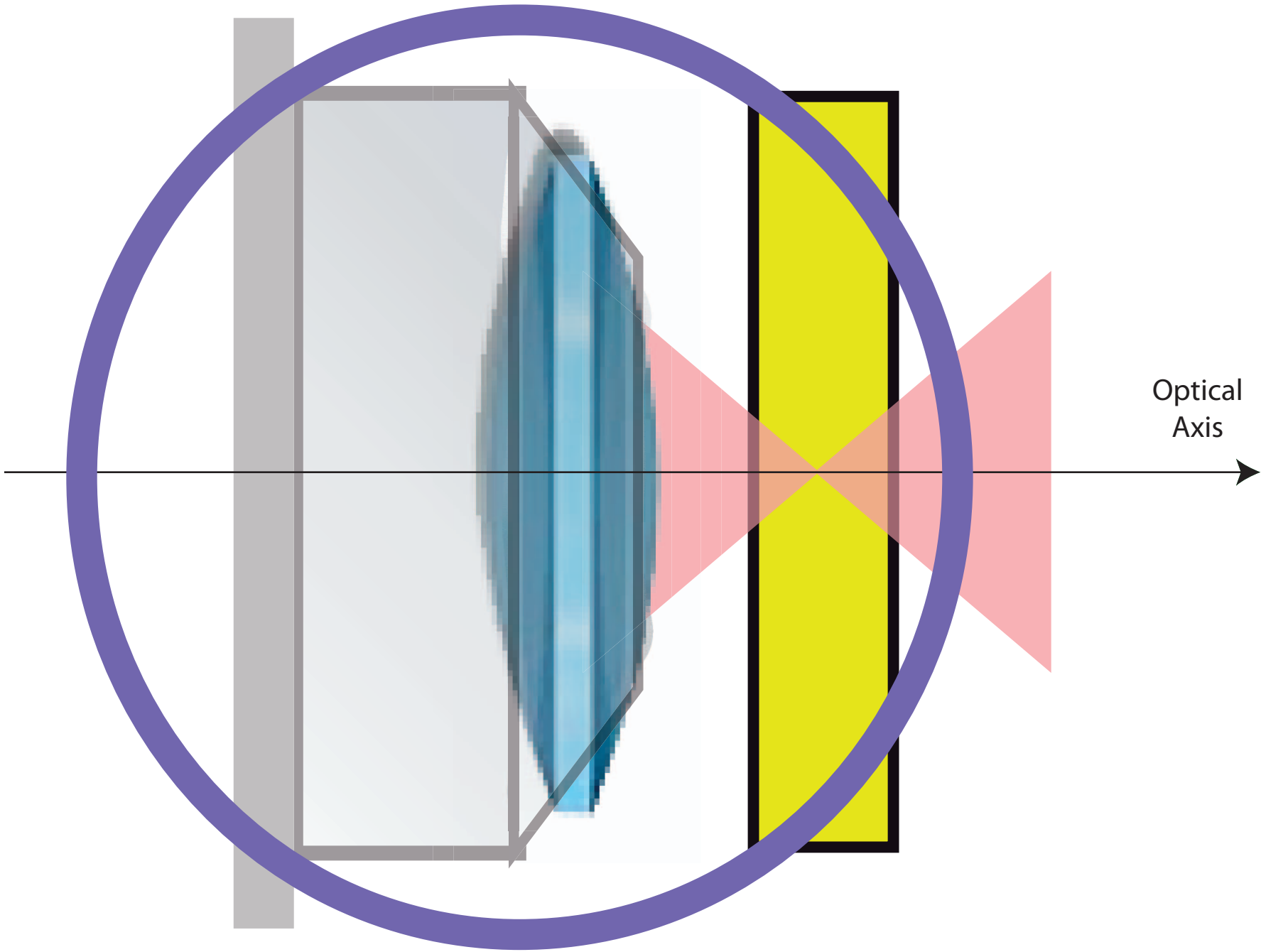




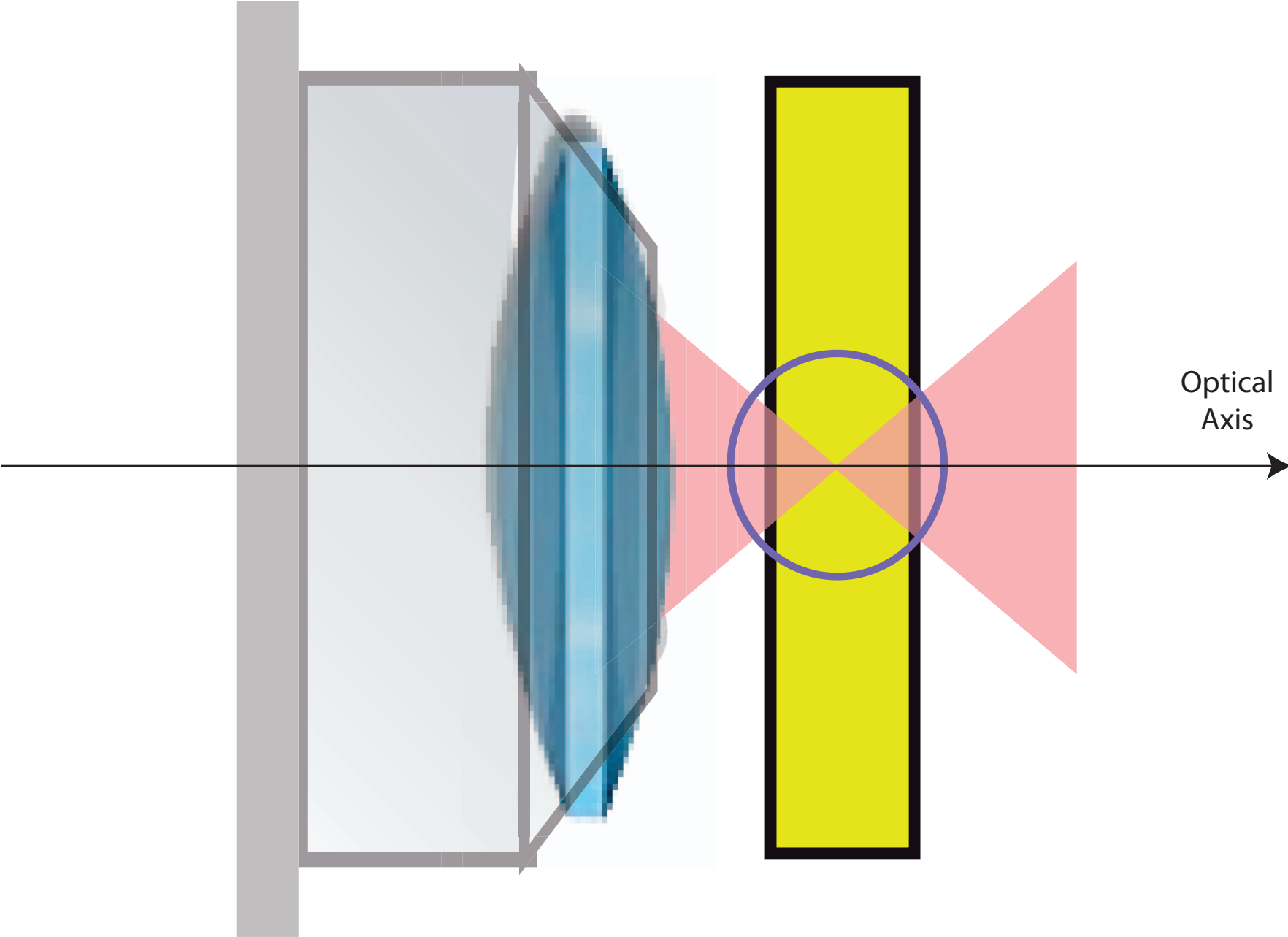
# Confocal Laser Scanning Microscopy



# Confocal Laser Scanning Microscopy

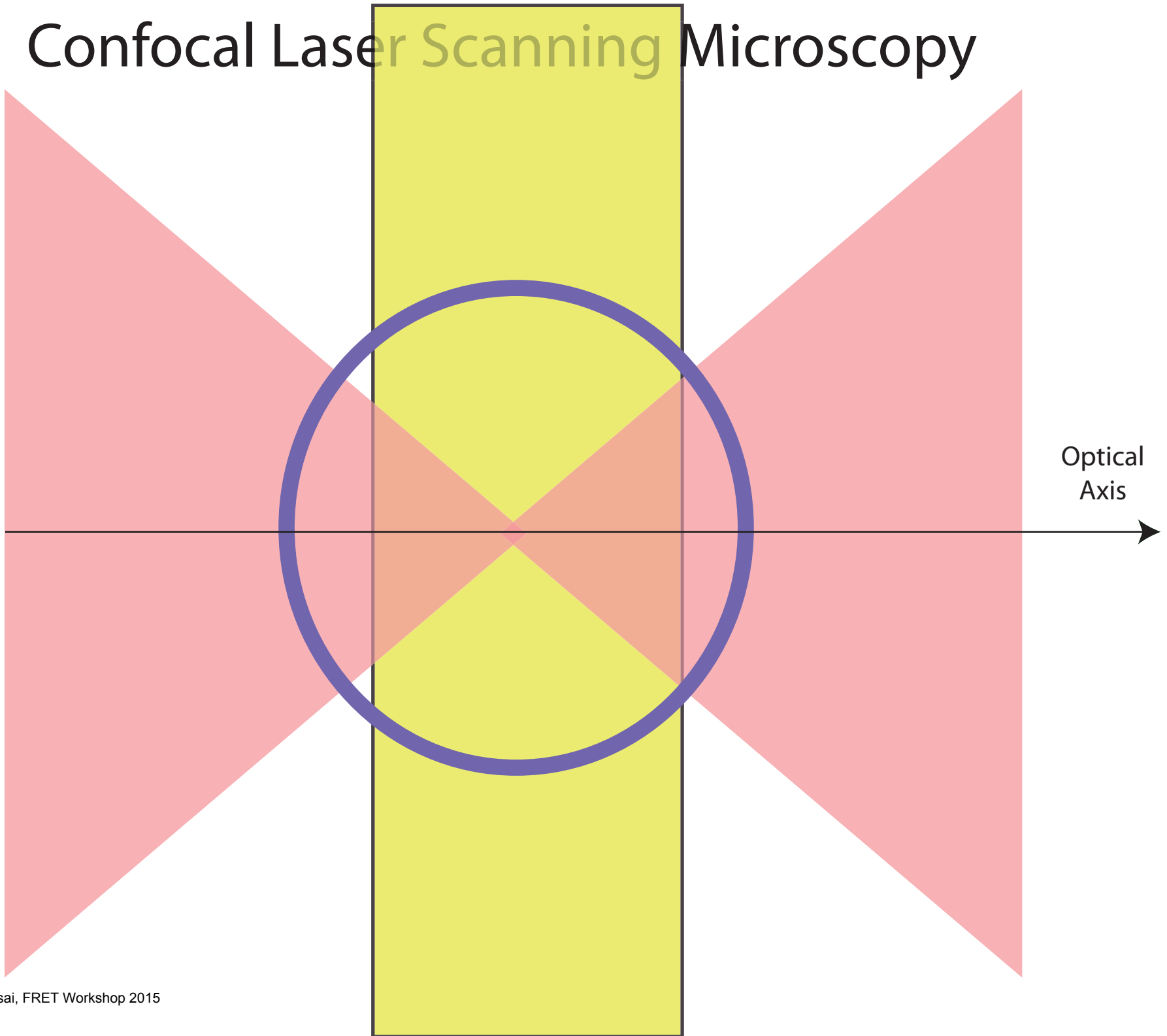


# Confocal Laser Scanning Microscopy

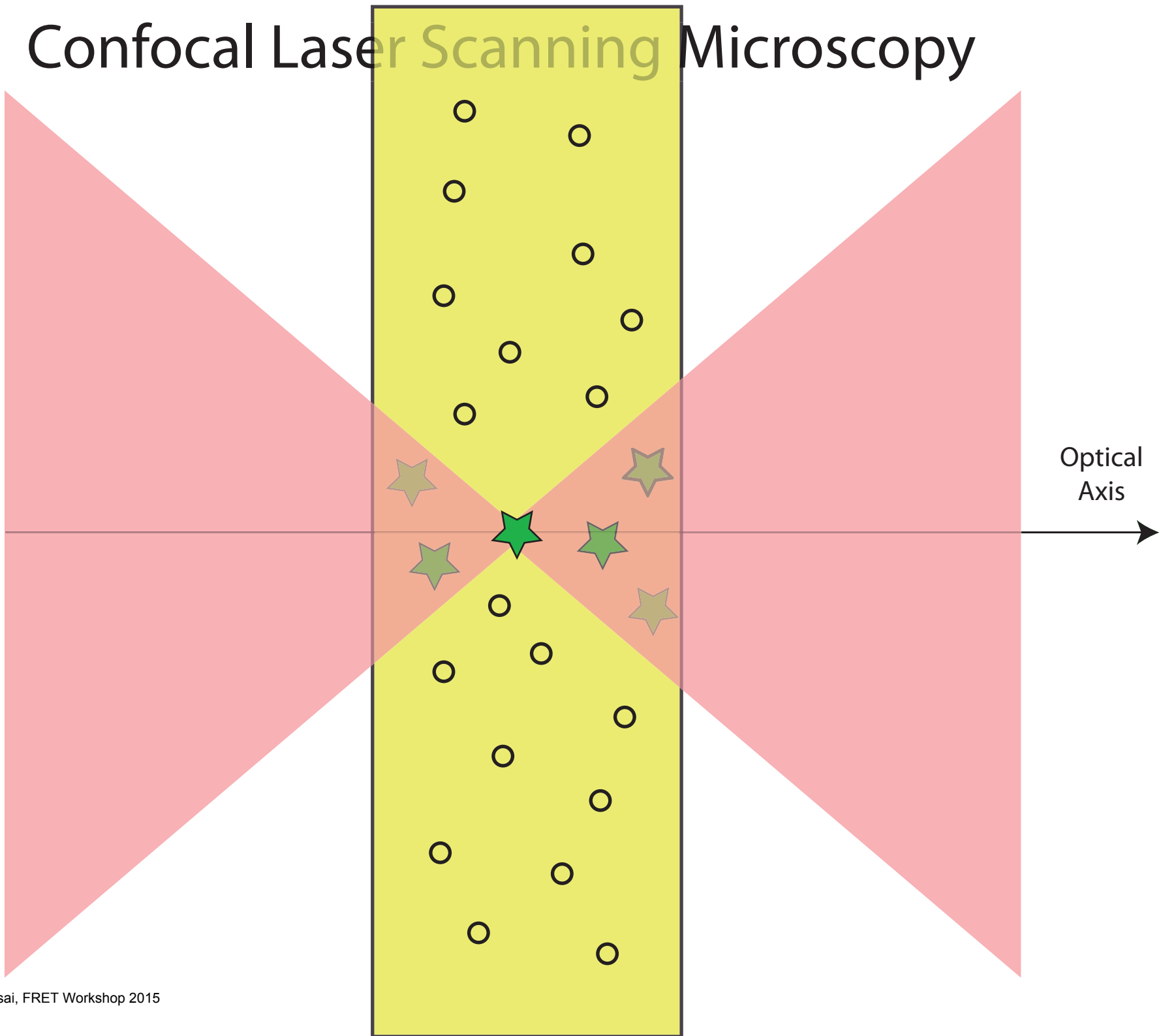


Optical Axis

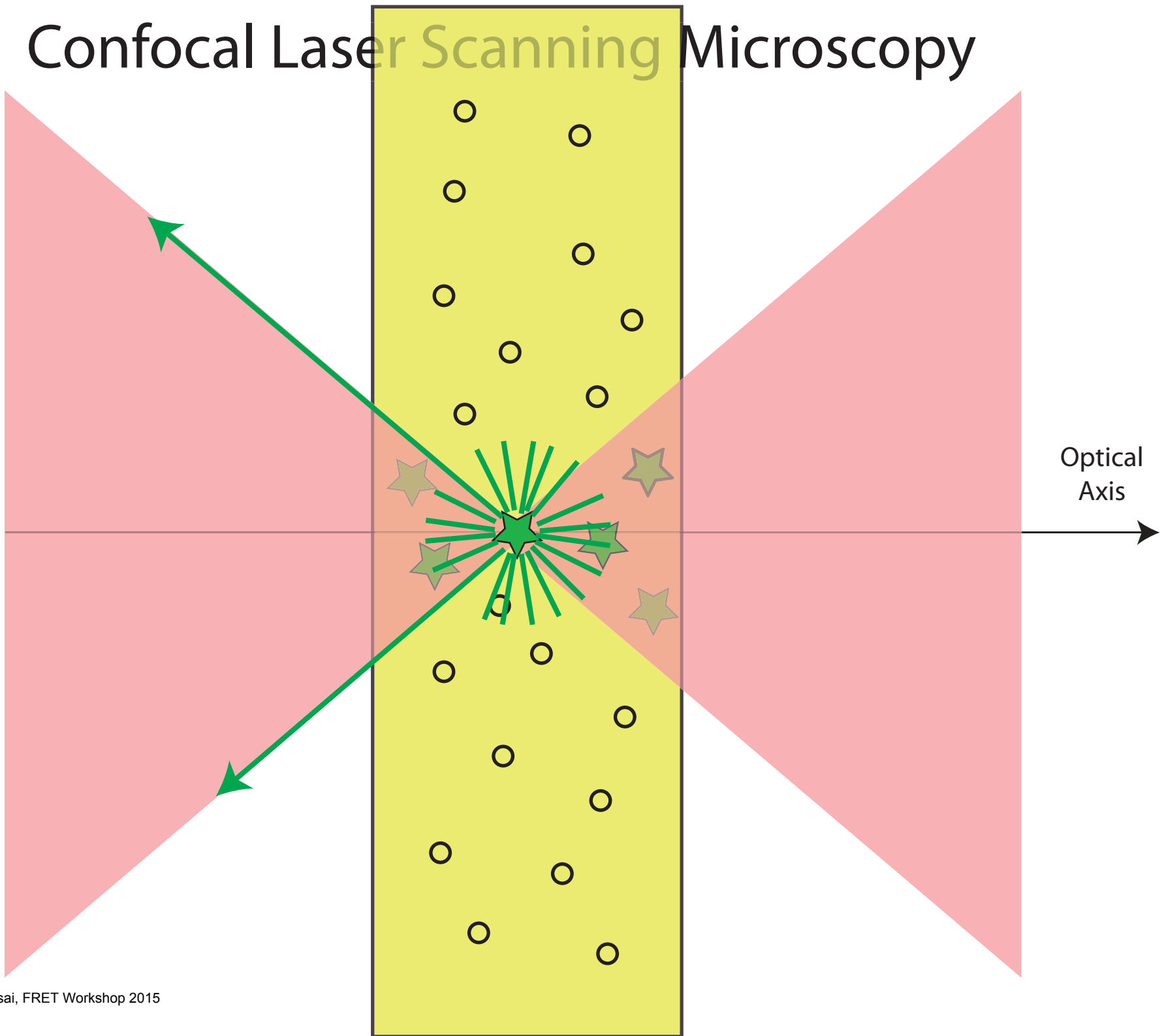
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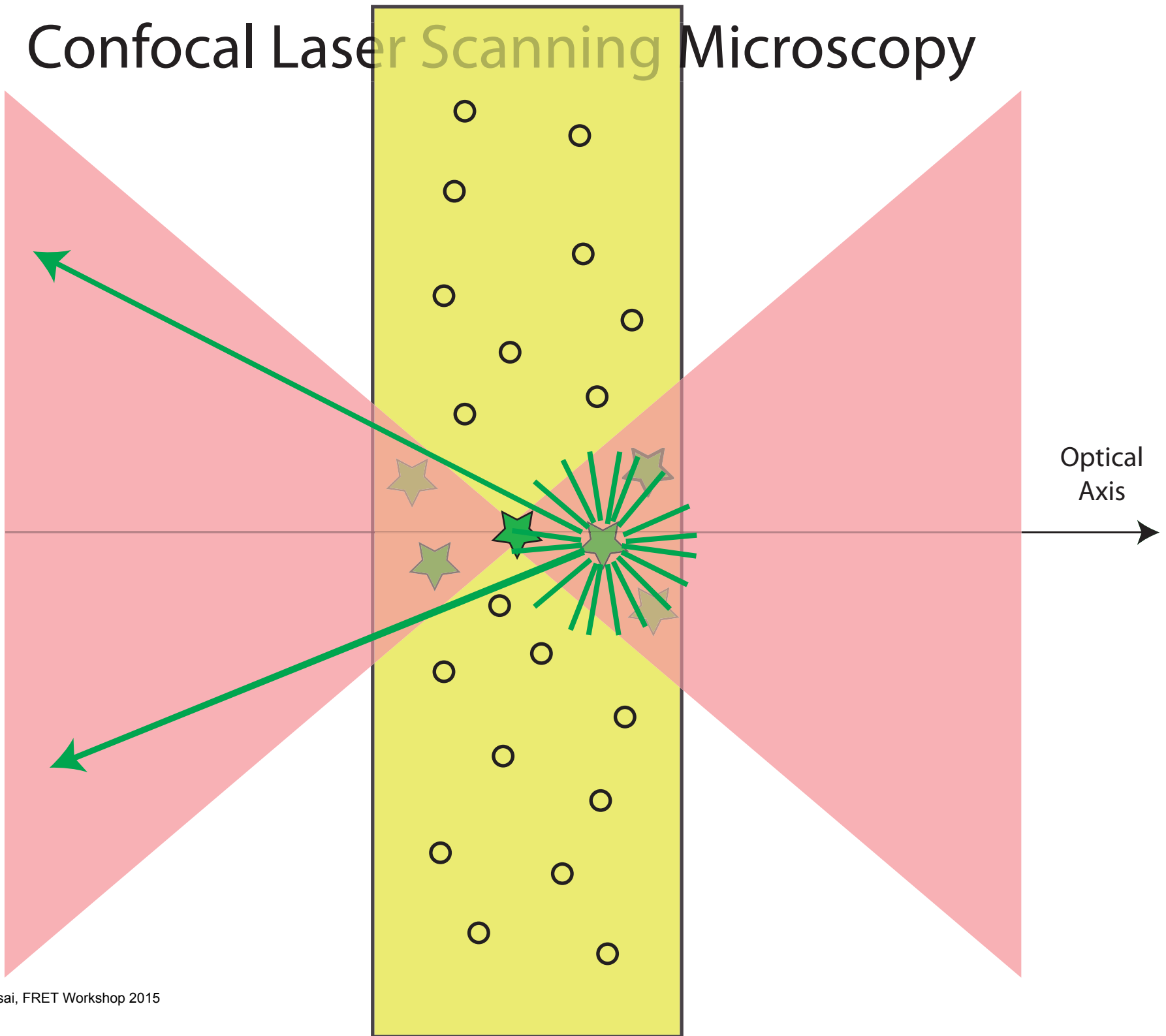
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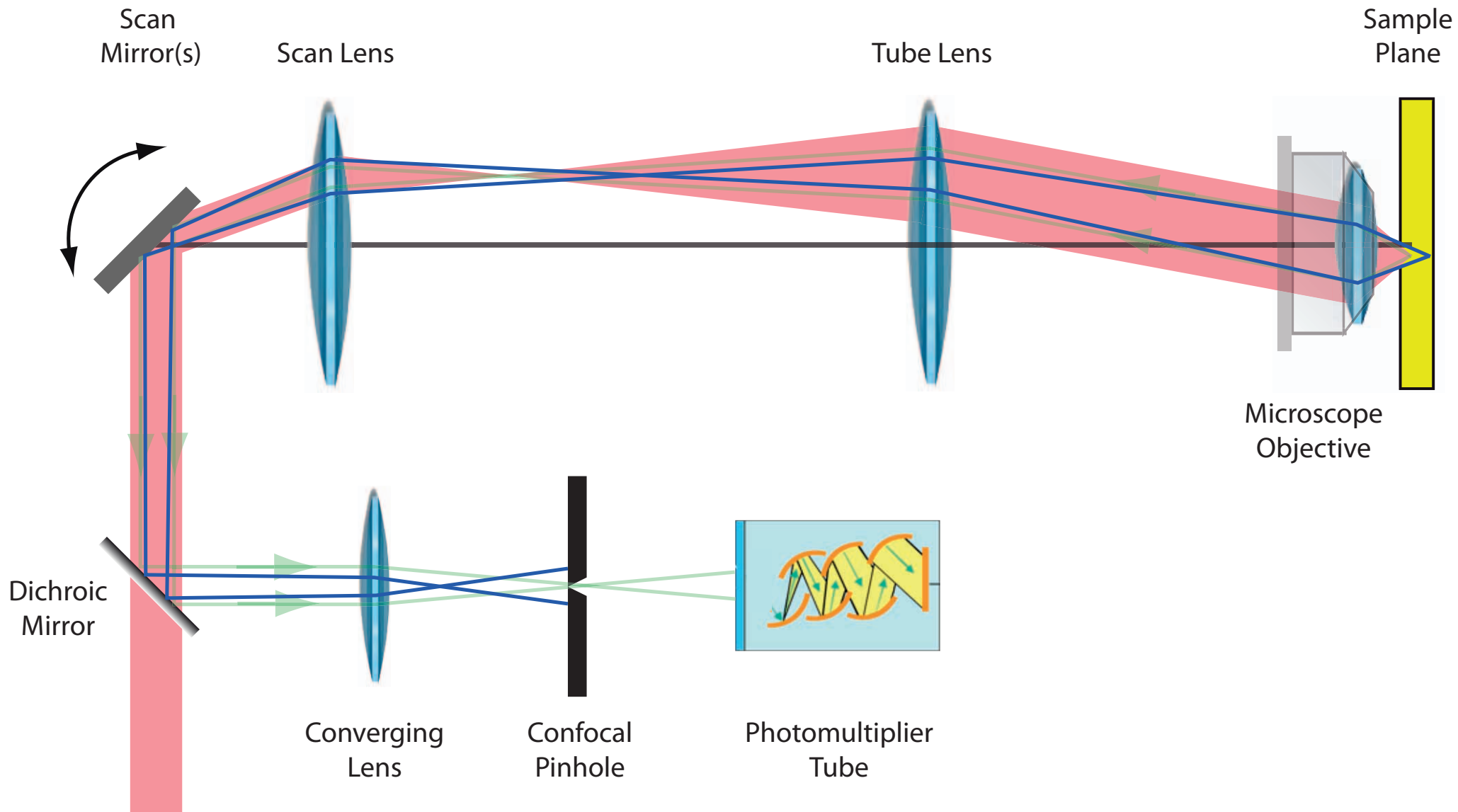
# Confocal Laser Scanning Microscopy



# Confocal Laser Scanning Microscopy



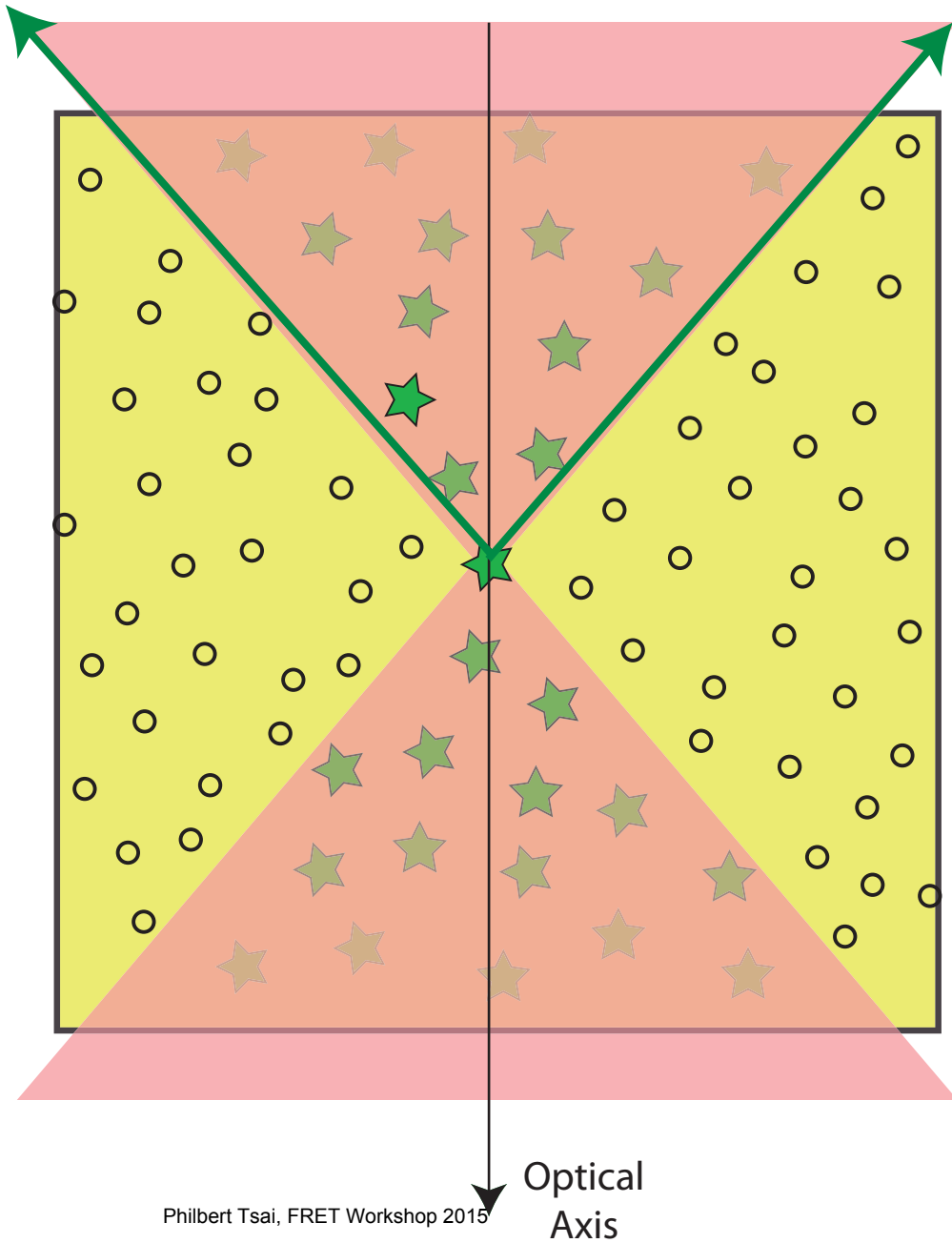
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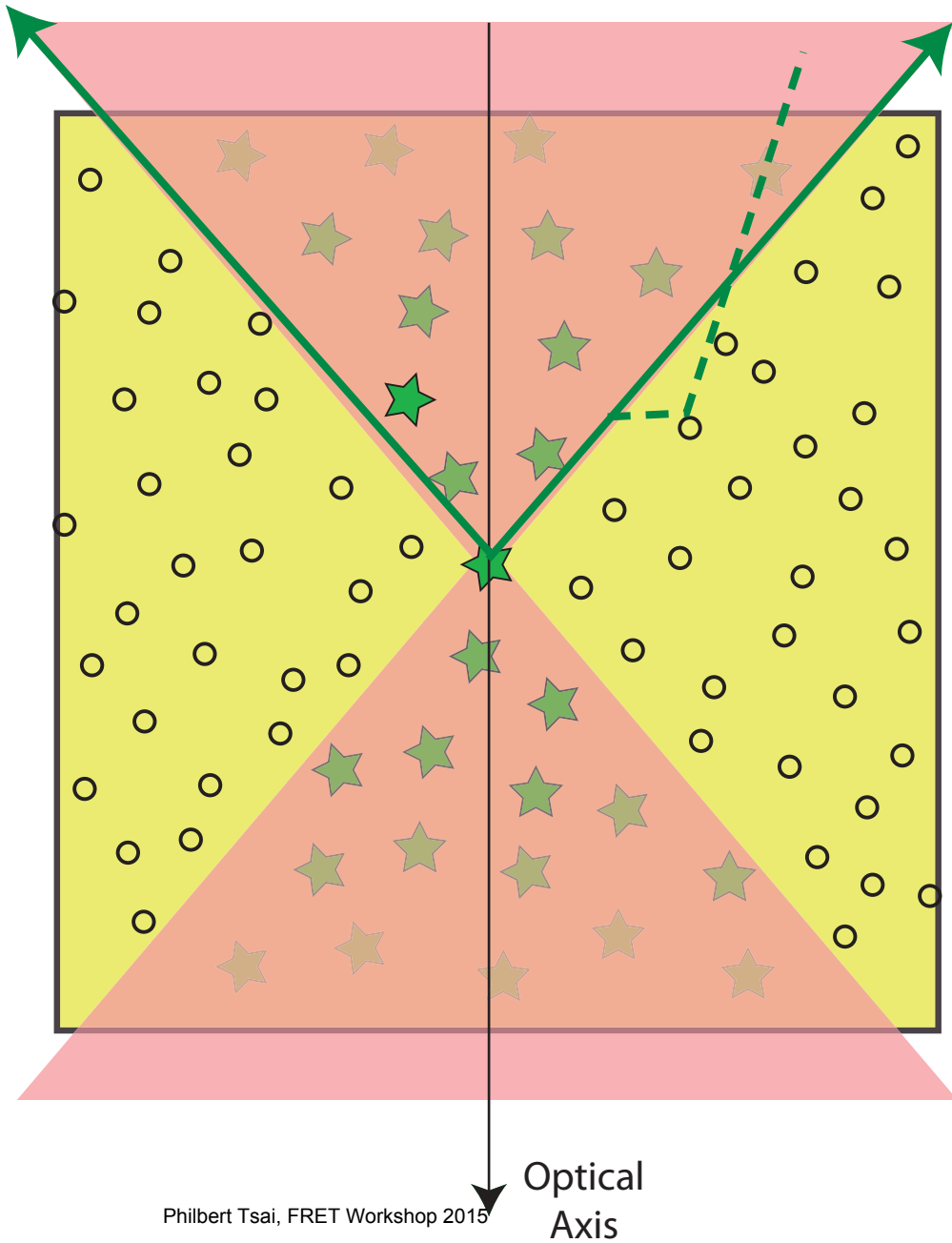




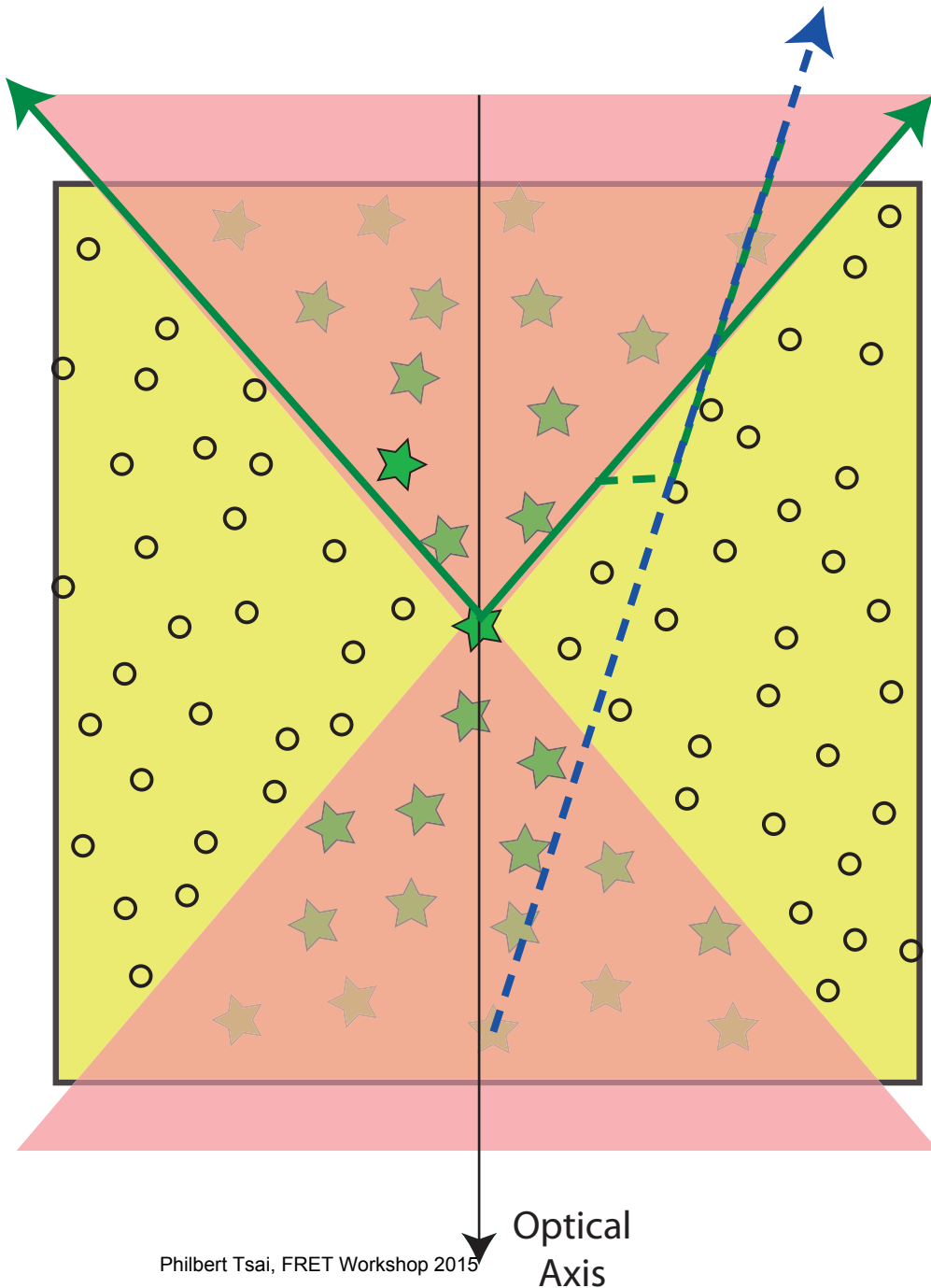
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# Confocal Laser Scanning Microscopy



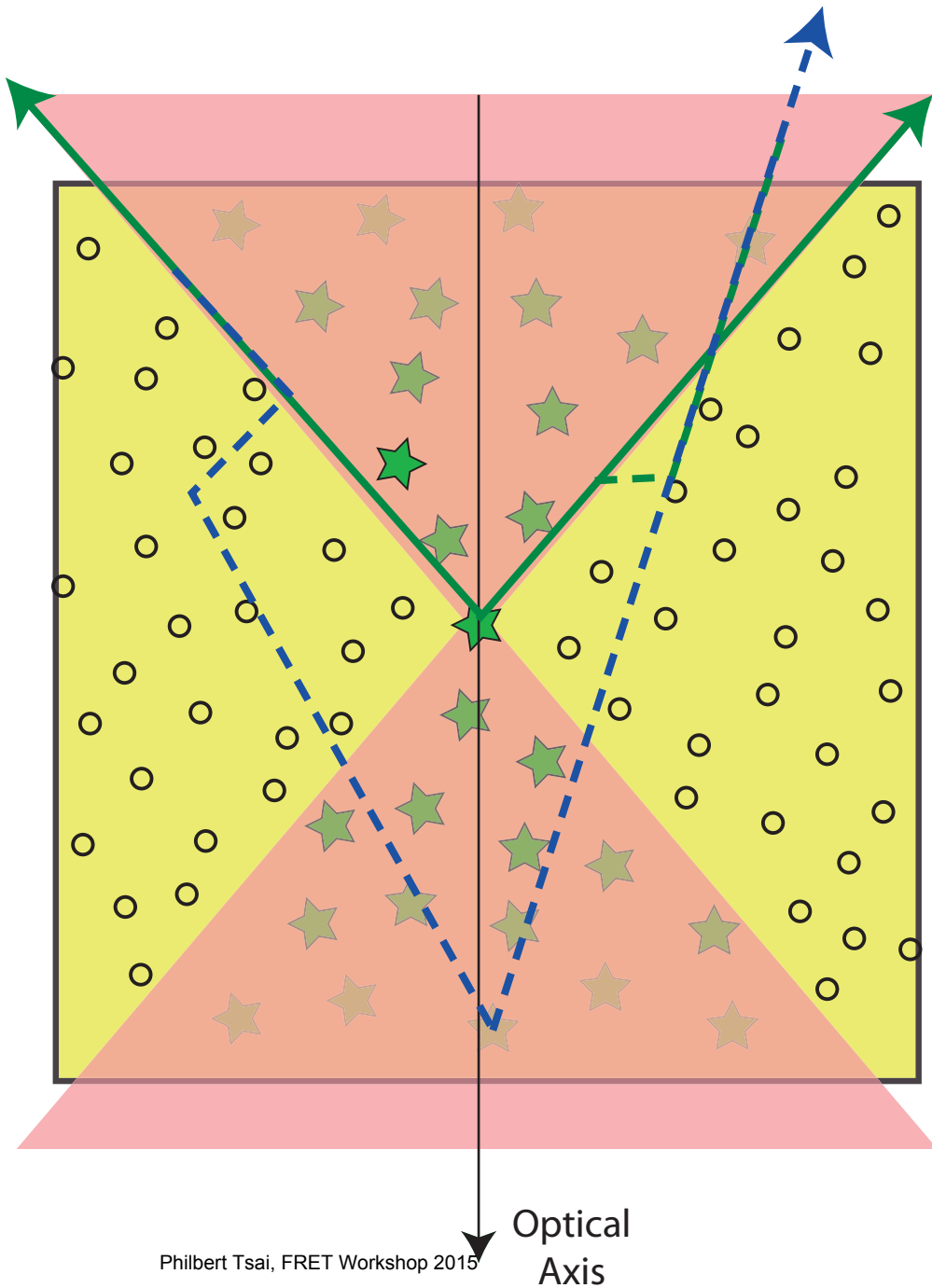
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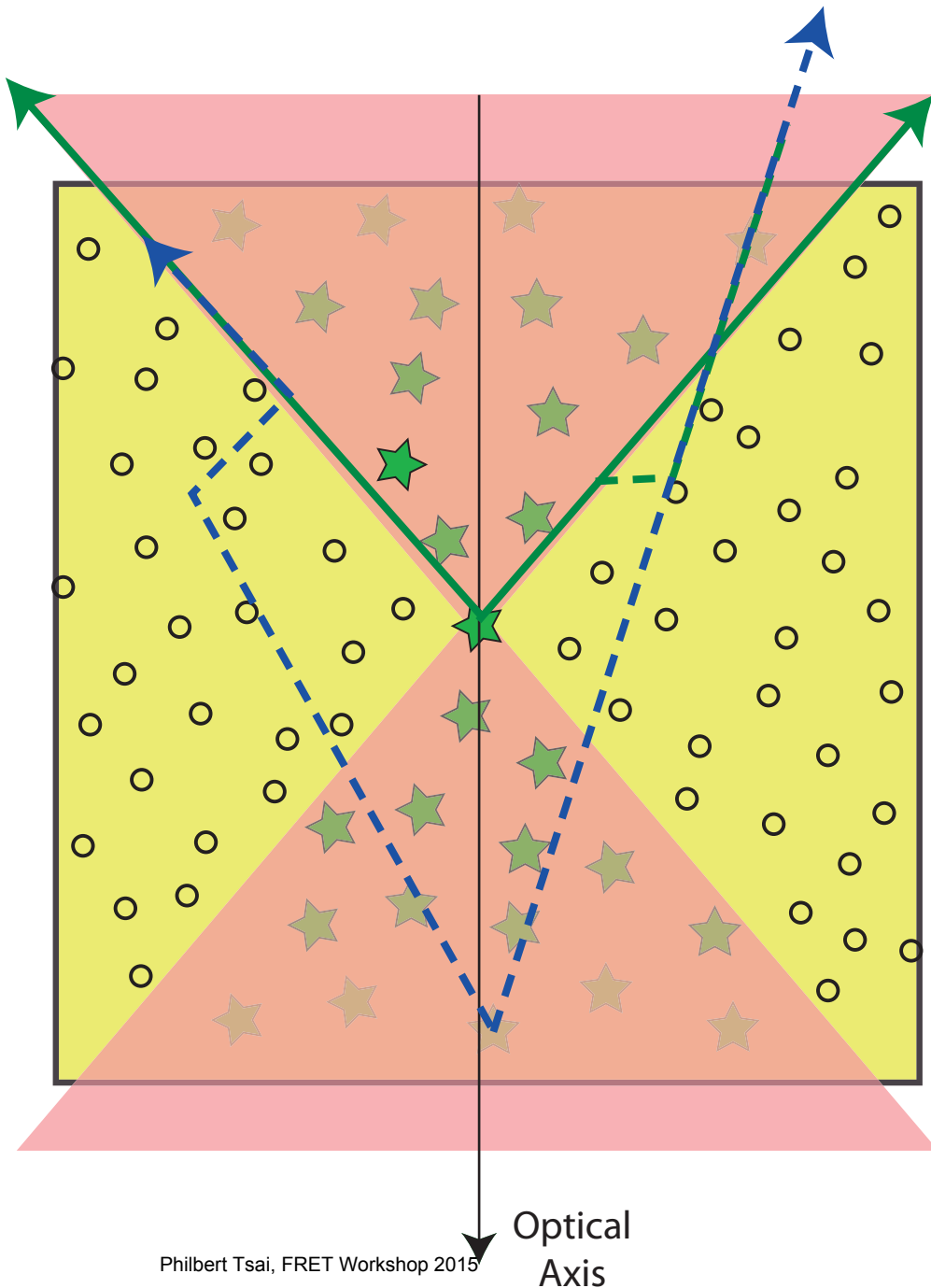
**In-focus fluorescence can scatter into the same path as out-of-focus fluorescence, and be blocked by the confocal pinhole.**

**This decreases the signal reaching the detector.**

# Confocal Laser Scanning Microscopy



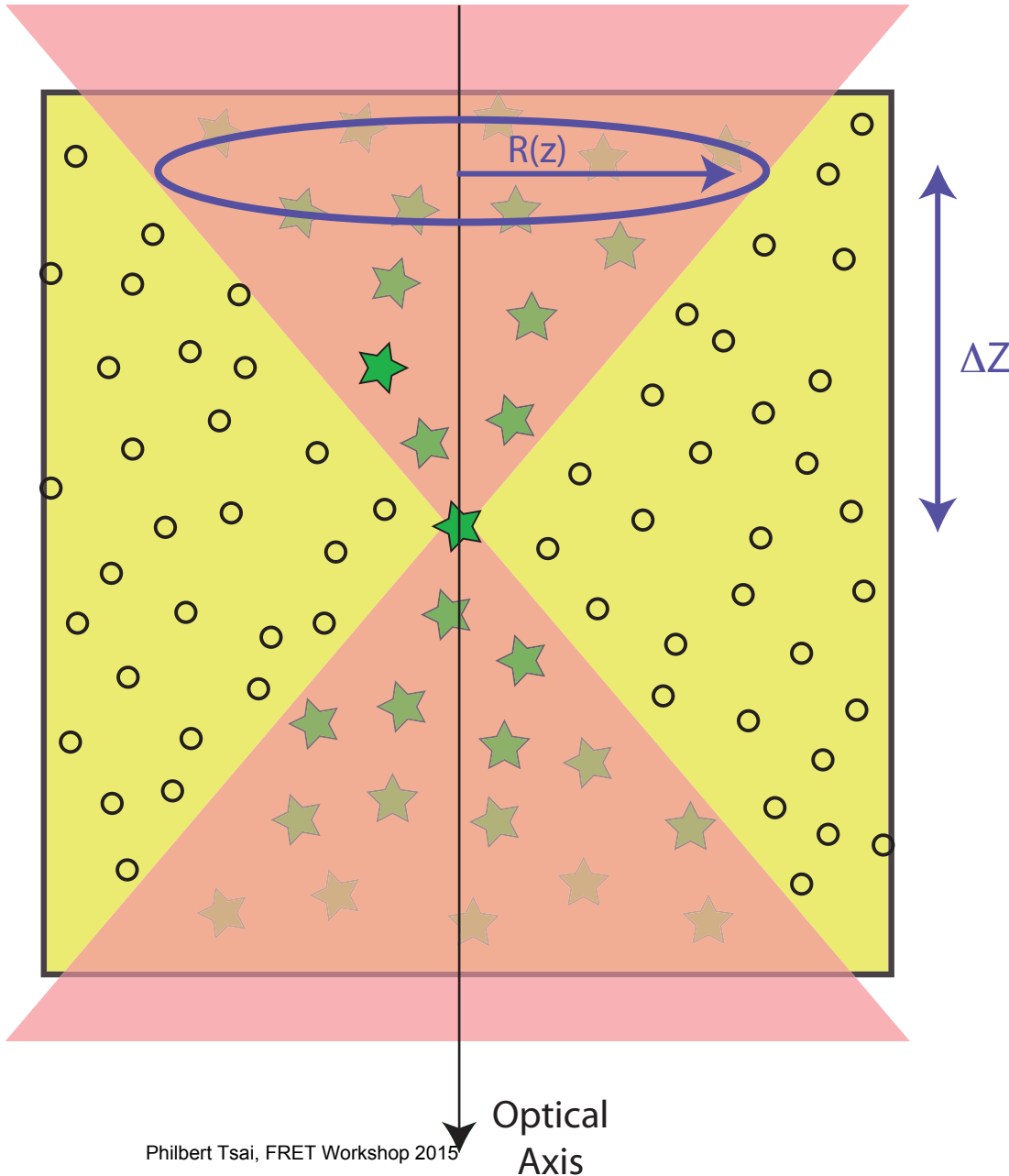
# Confocal Laser Scanning Microscopy



**Out-of-focus fluorescence can scatter into the same path as in-focus fluorescence, and pass through the confocal pinhole.**

**This increased background reduces the signal-to-noise ratio.**

# Two Photon Laser Scanning Microscopy



$R(z)$  = Radius

$A$  = Area

$\Delta Z$  = Distance from Focal Plane

$I$  = Intensity

$P$  = Power

$F_m$  = Fluorescence per Molecule

$\sigma$  = Dye Cross-section

$F_p$  = Fluorescence per Plane

**TWO PHOTON EXCITATION**

$$R(z) \sim \Delta Z$$

$$A \sim R^2 \sim (\Delta Z)^2$$

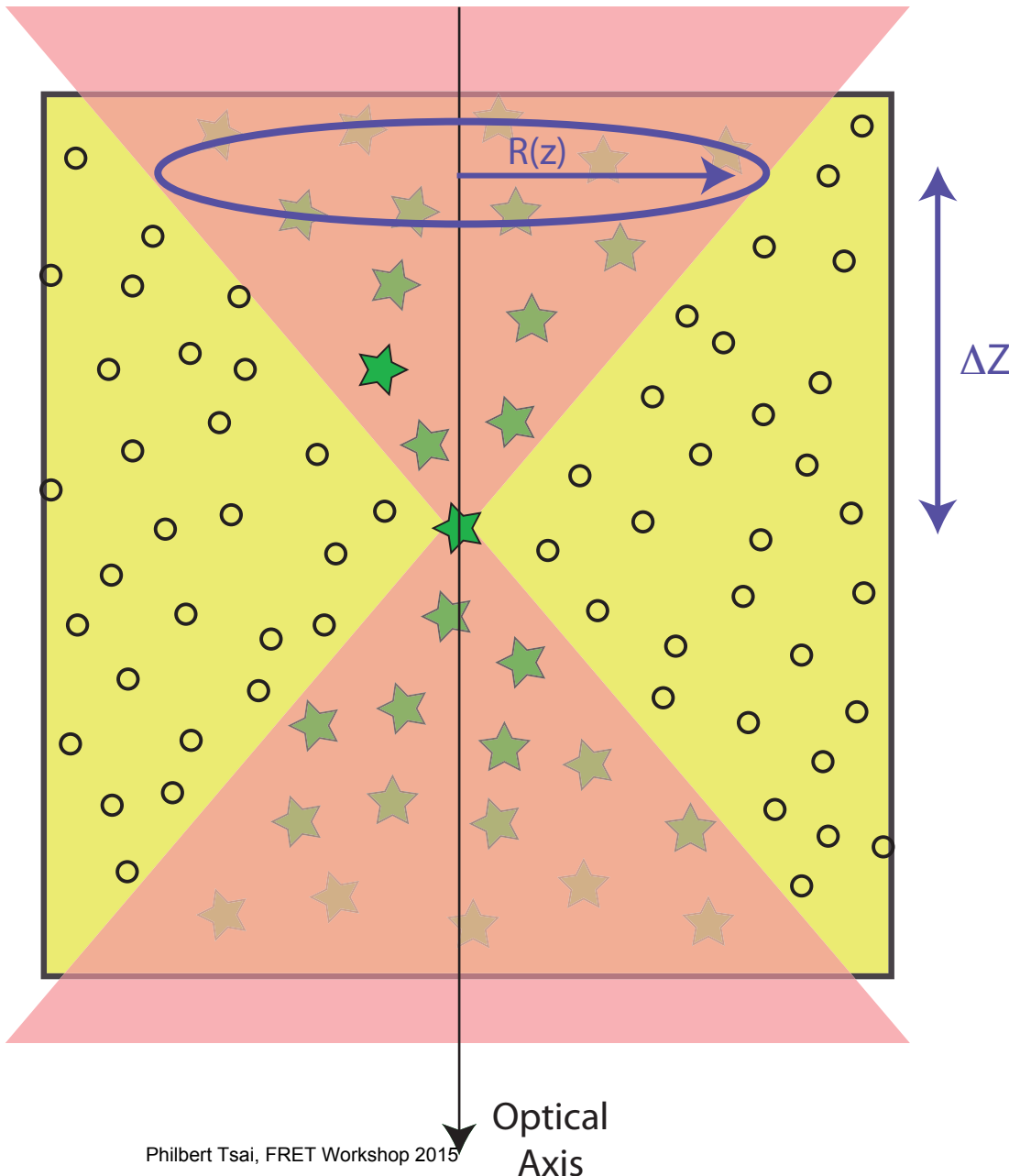
$$I = P / A$$

$$F_m = \sigma * I^2 = \sigma * P^2 / A^2 = \sigma * P^2 / (\Delta Z)^4$$

$$F_p = F_m * A = \sigma * P^2 / A \sim \sigma * P^2 / (\Delta Z)^2$$

**For two photon excitation, the fluorescence per plane falls quadratically with distance from the focal plane!**

# Confocal Laser Scanning Microscopy



$R(z)$  = Radius

$A$  = Area

$\Delta Z$  = Distance from Focal Plane

$I$  = Intensity

$P$  = Power

$F_m$  = Fluorescence per Molecule

$\sigma$  = Dye Cross-section

$F_p$  = Fluorescence per Plane

**SINGLE PHOTON EXCITATION**

$$R(z) \sim \Delta Z$$

$$A \sim R^2 \sim (\Delta Z)^2$$

$$I = P / A$$

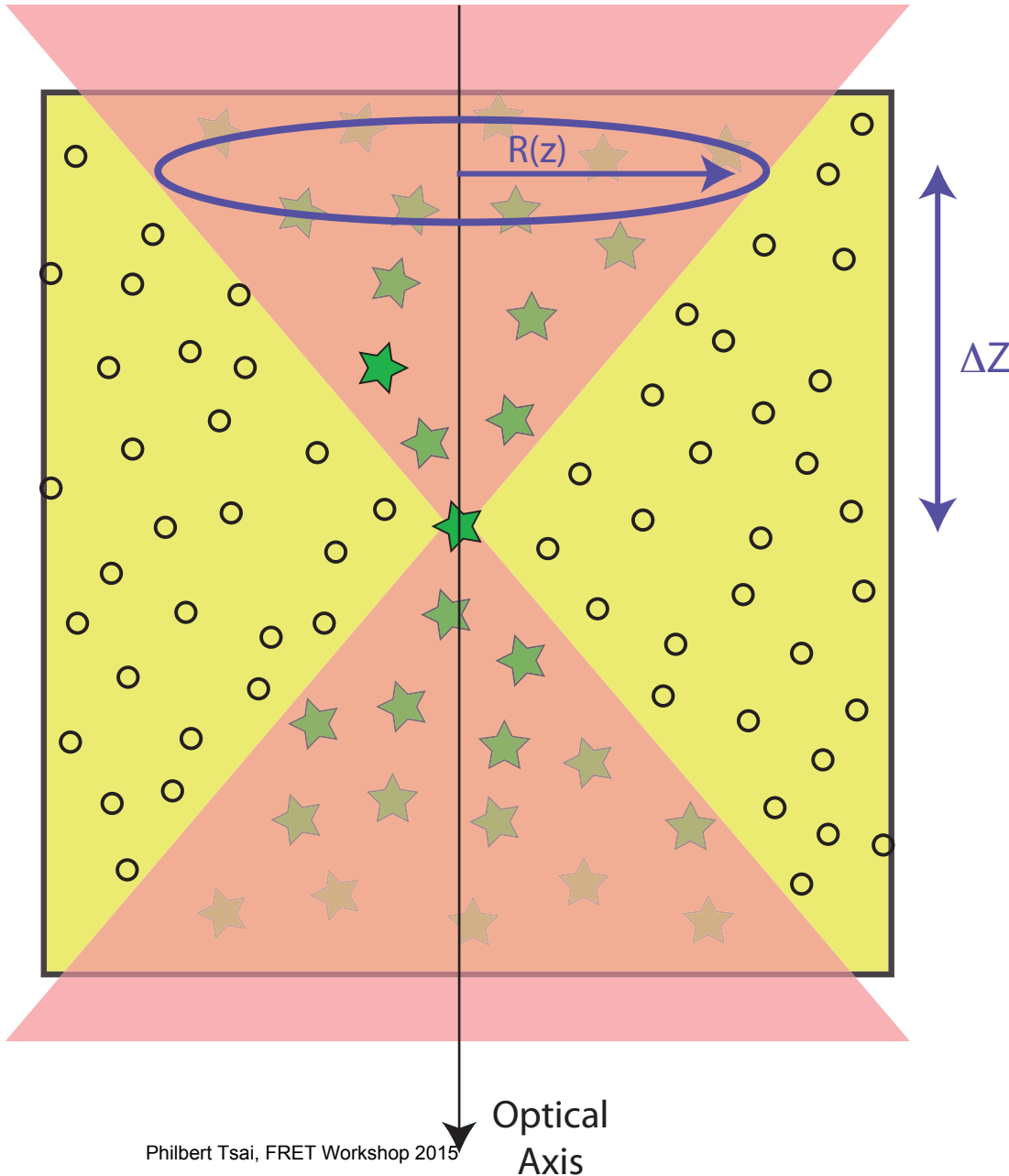
$$F_m = \sigma * I = \sigma * P / A = \sigma * P / (\Delta Z)^2$$

$$F_p = F_m * A = \sigma * P$$

**For single photon excitation, the fluorescence per plane is independent of distance from the focal plane !**



# Two Photon Laser Scanning Microscopy



$R(z)$  = Radius

$A$  = Area

$\Delta Z$  = Distance from Focal Plane

$I$  = Intensity

$P$  = Power

$F_m$  = Fluorescence per Molecule

$\sigma$  = Dye Cross-section

$F_p$  = Fluorescence per Plane

**TWO PHOTON EXCITATION**

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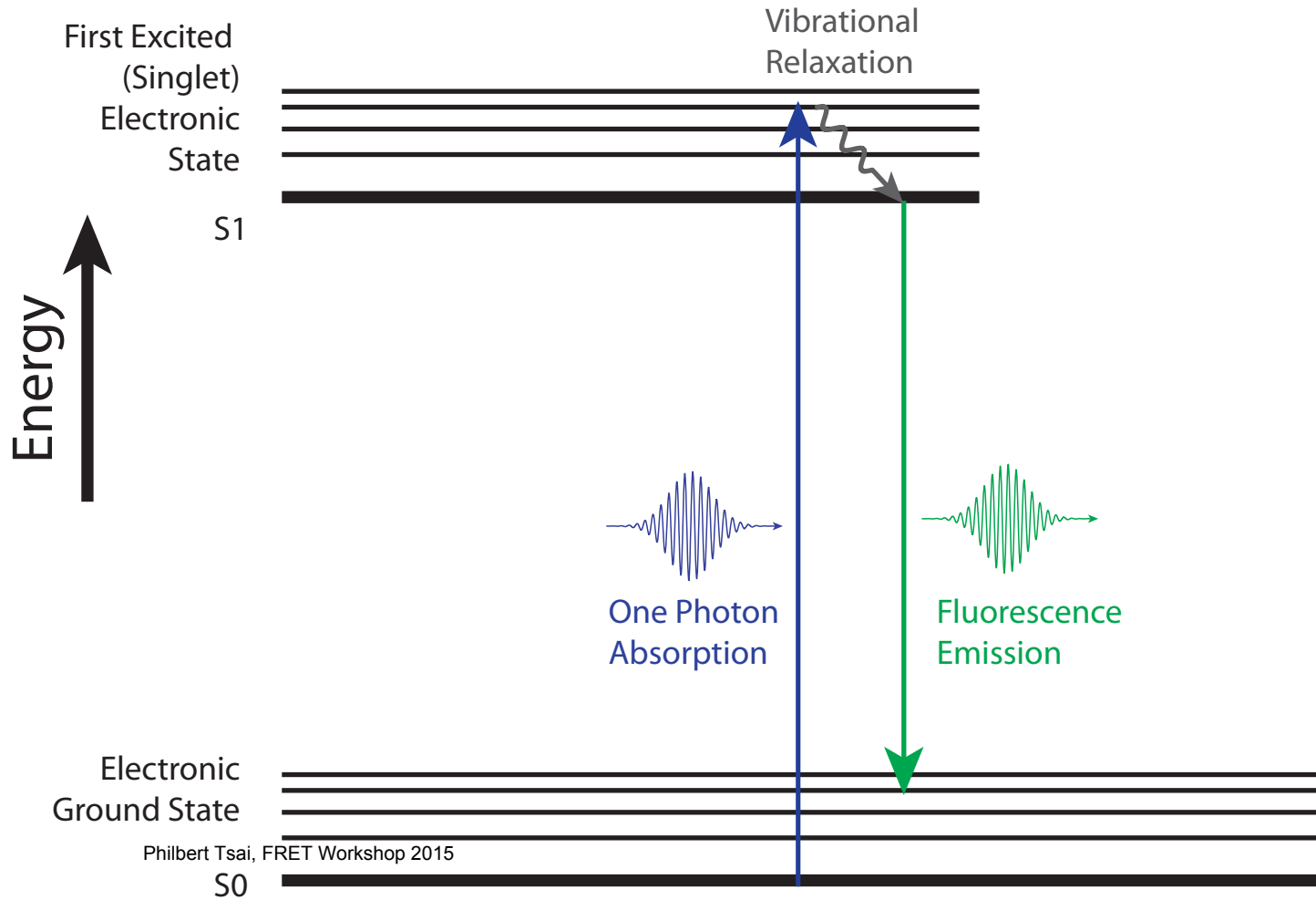
$$I = P / A$$

$$F_m = \sigma * I^2 = \sigma * P^2 / A^2 = \sigma * P^2 / (\Delta Z)^4$$

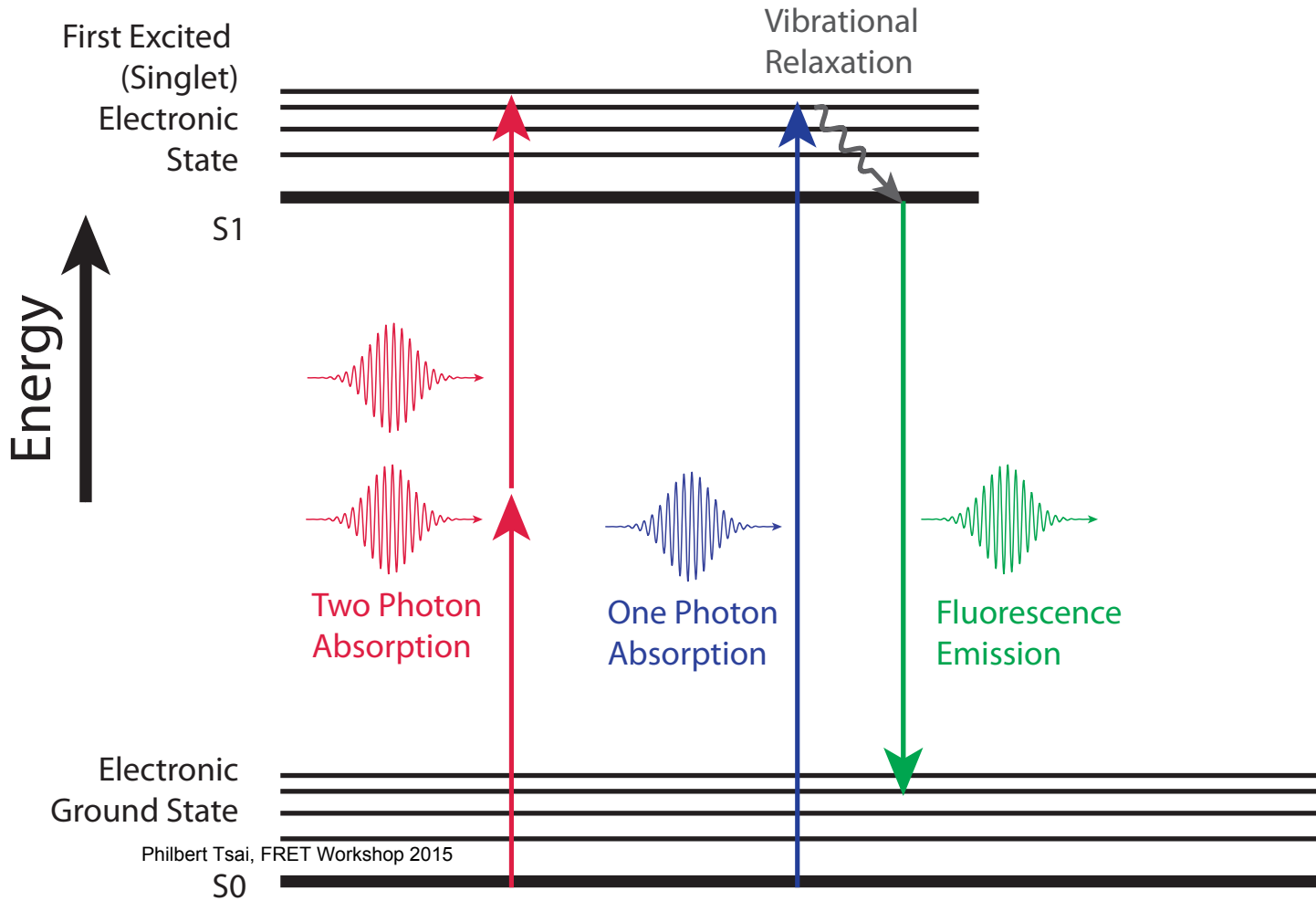
$$F_p = F_m * A = \sigma * P^2 / A \sim \sigma * P^2 / (\Delta Z)^2$$

**For two photon excitation, the fluorescence per plane falls quadratically with distance from the focal plane !**

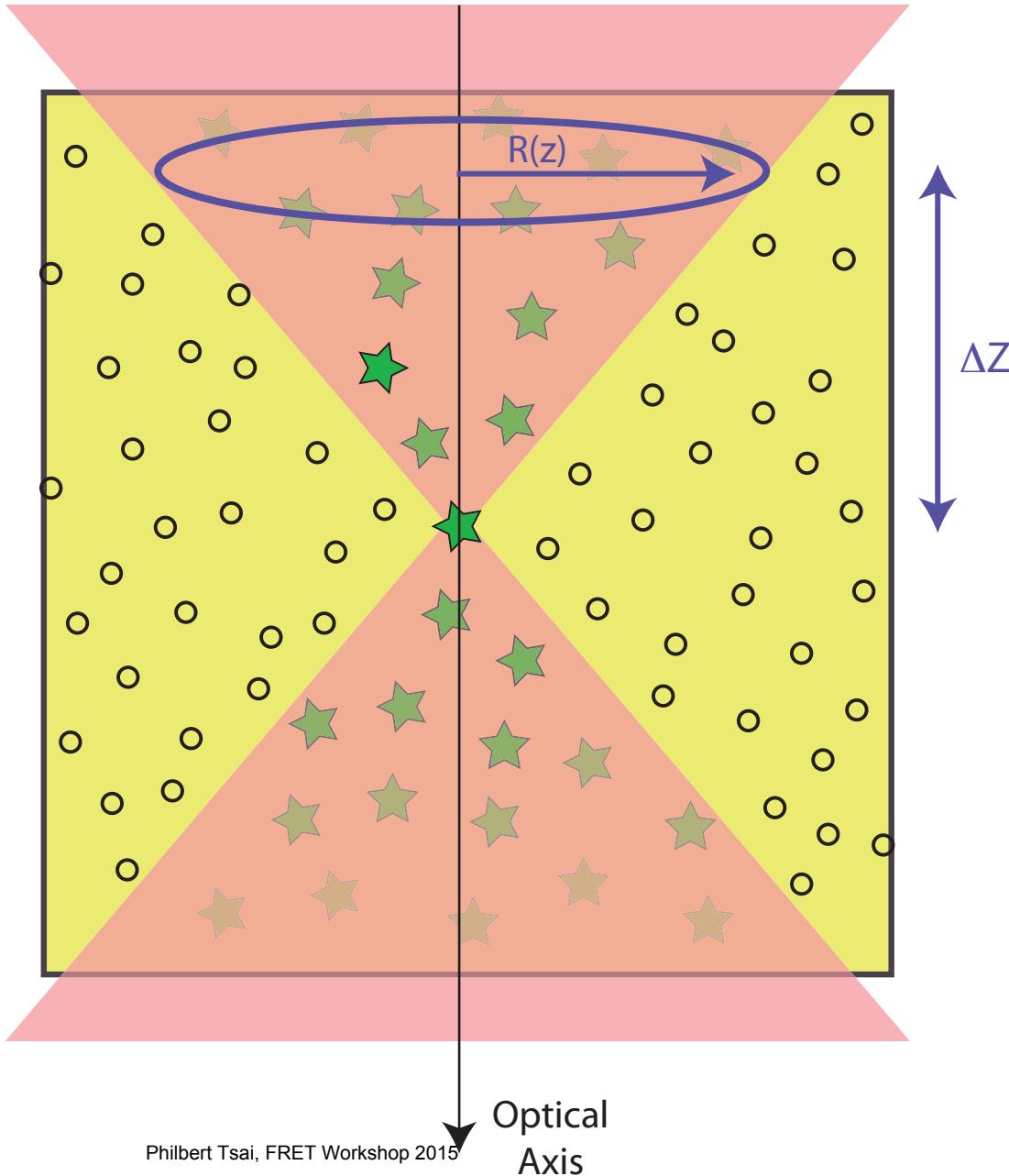
# Jablonski Energy Diagram



# Jablonski Energy Diagram



# Two Photon Laser Scanning Microscopy



$R(z)$  = Radius

$A$  = Area

$\Delta Z$  = Distance from Focal Plane

$I$  = Intensity

$P$  = Power

$F_m$  = Fluorescence per Molecule

$\sigma$  = Dye Cross-section

$F_p$  = Fluorescence per Plane

**TWO PHOTON EXCITATION**

$$R(z) \sim \Delta Z$$

$$A \sim R^2 \sim (\Delta Z)^2$$

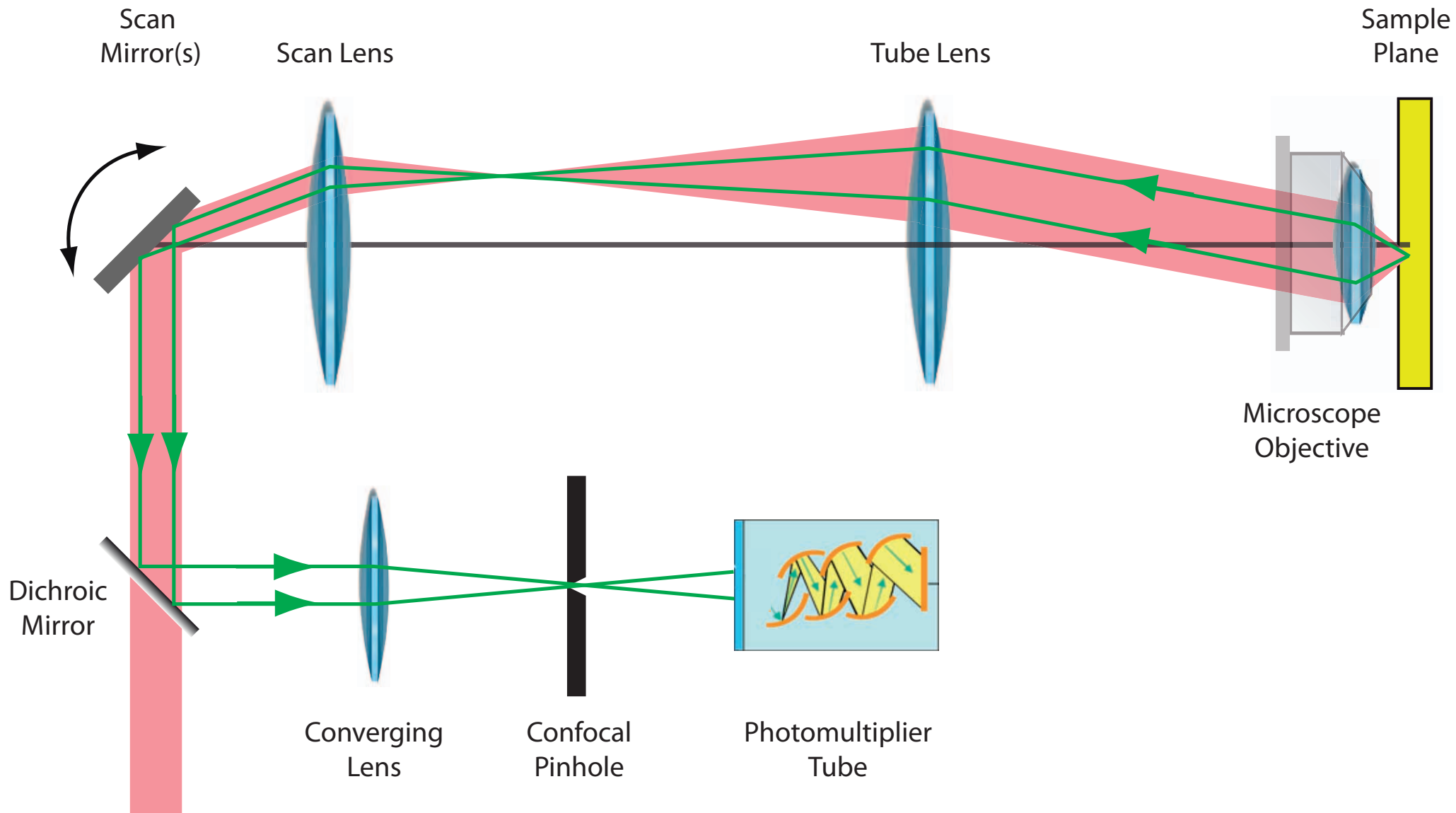
$$I = P / A$$

$$F_m = \sigma * I^2 = \sigma * P^2 / A^2 = \sigma * P^2 / (\Delta Z)^4$$

$$F_p = F_m * A = \sigma * P^2 / A \sim \sigma * P^2 / (\Delta Z)^2$$

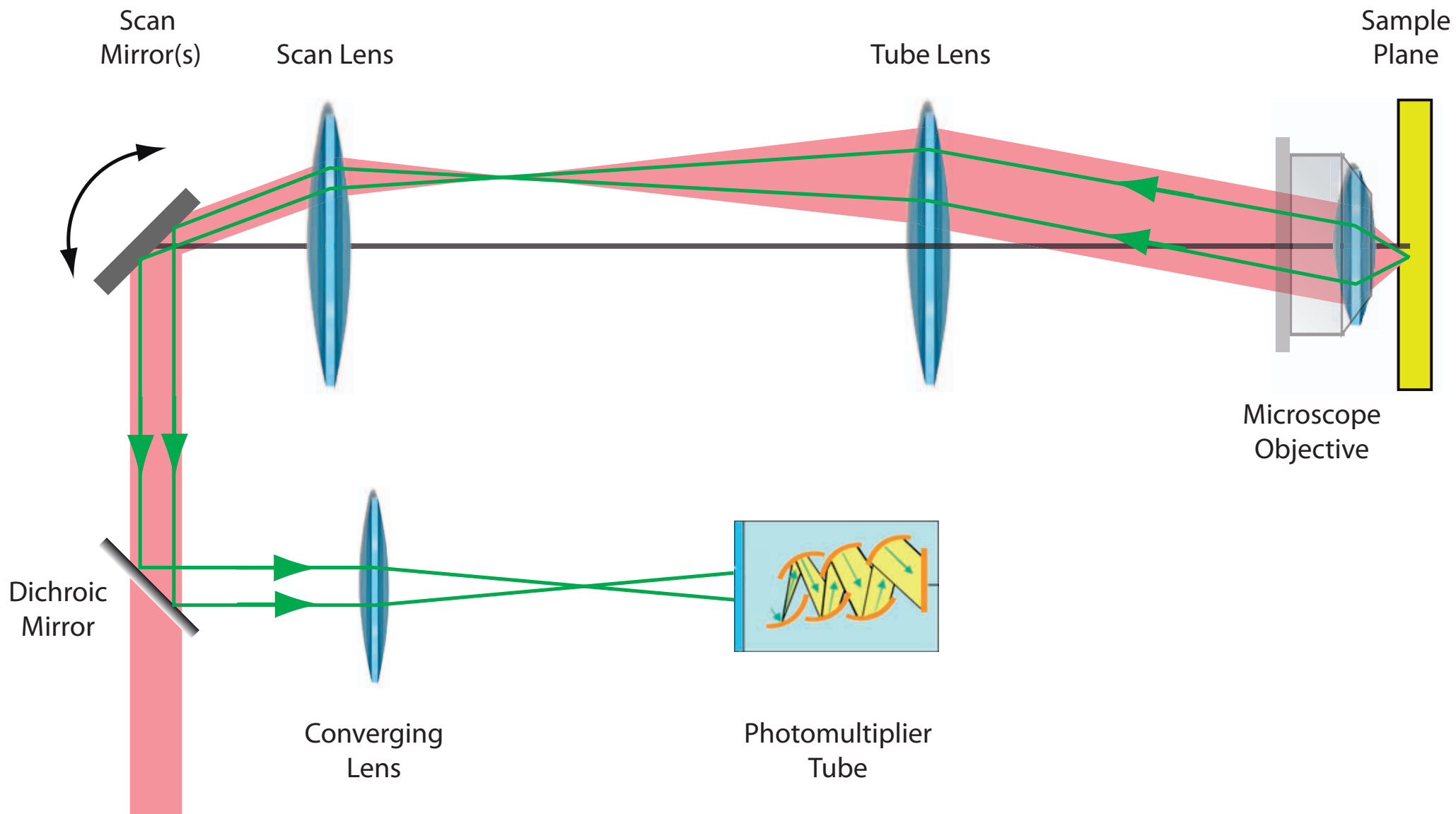
**For two photon excitation, the fluorescence per plane falls quadratically with distance from the focal plane !**

# Confocal Laser Scanning Microscopy



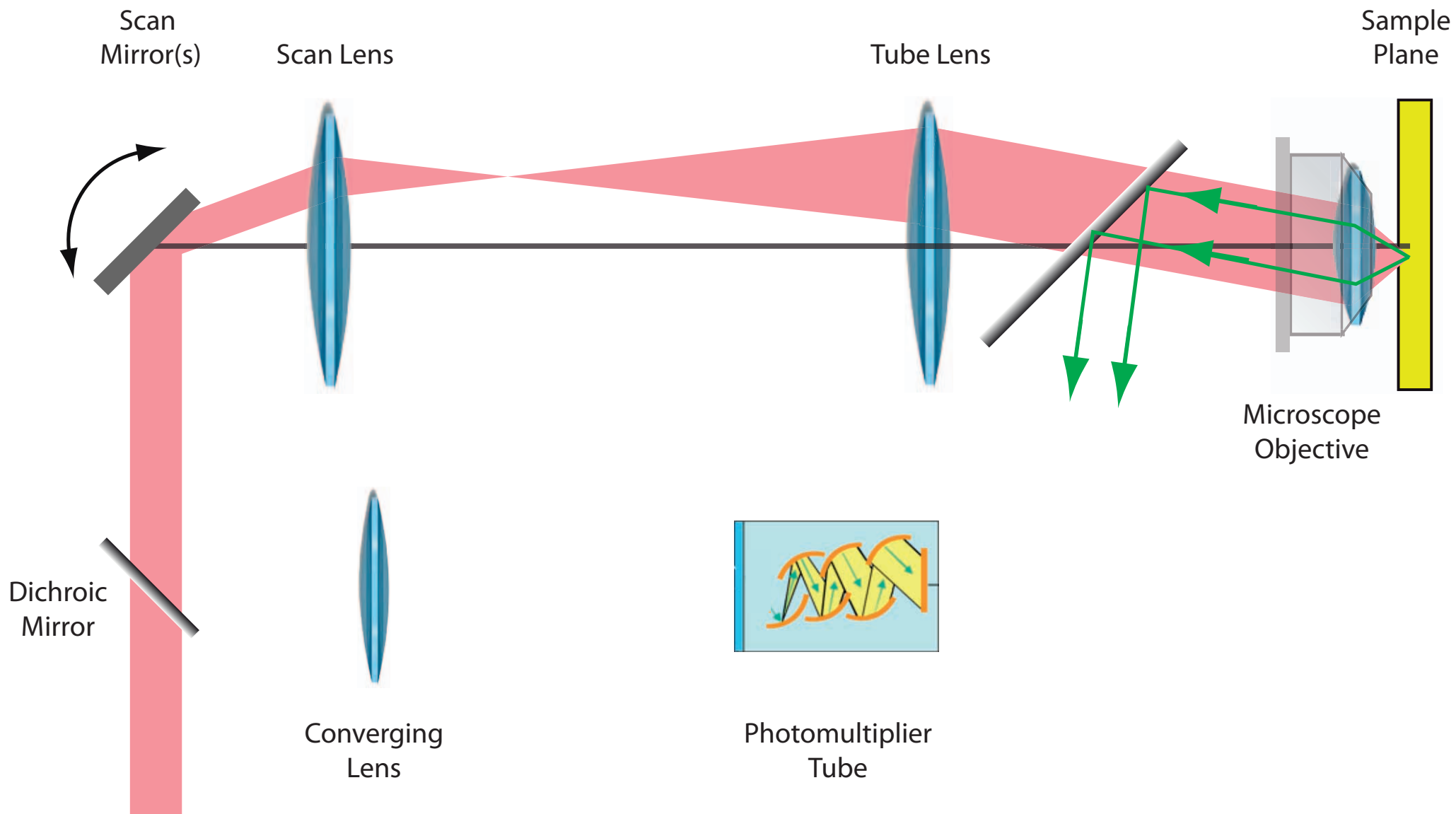
# ~~Confocal~~ Laser Scanning Microscopy

## Two Photon



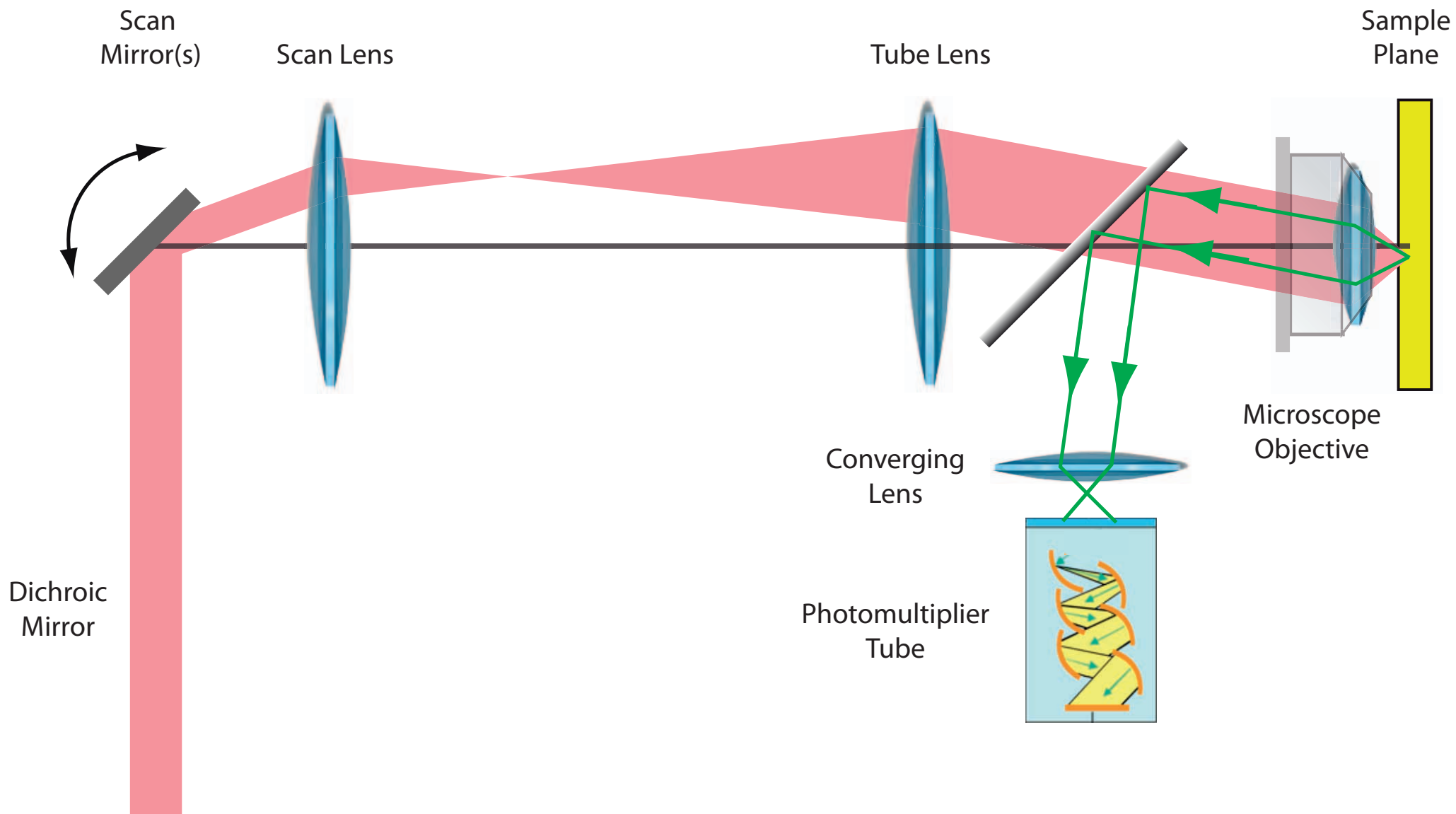
# ~~Confocal~~ Laser Scanning Microscopy

## Two Photon



# ~~Confocal~~ Laser Scanning Microscopy

## Two Photon

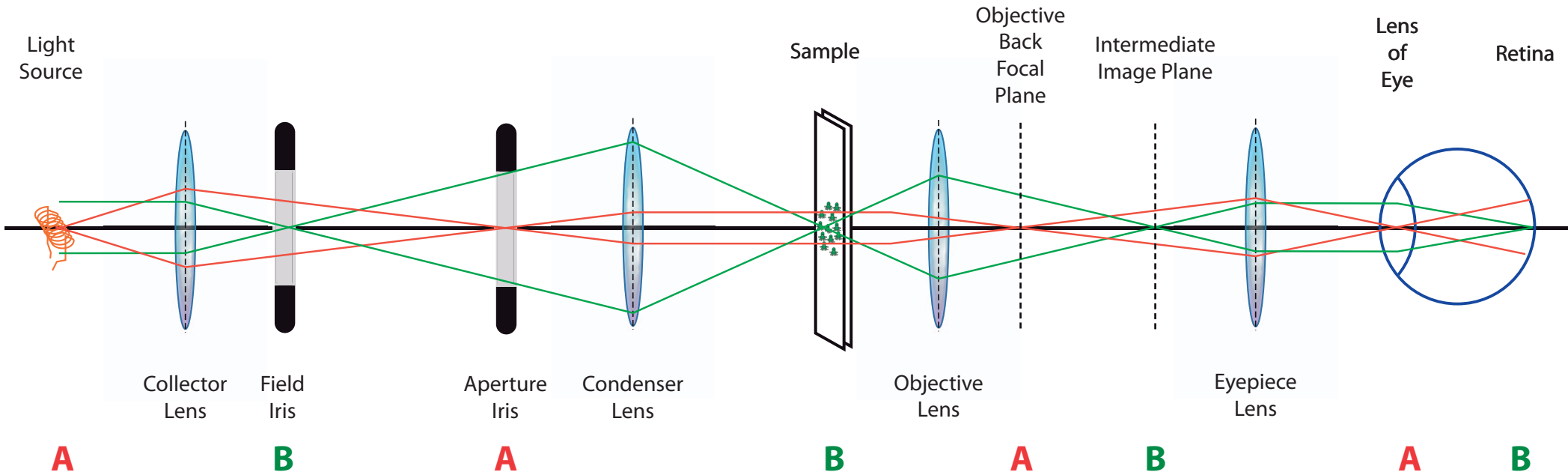






# Kohler Illumination

## Dual Light Paths



### Illumination Conjugate Planes

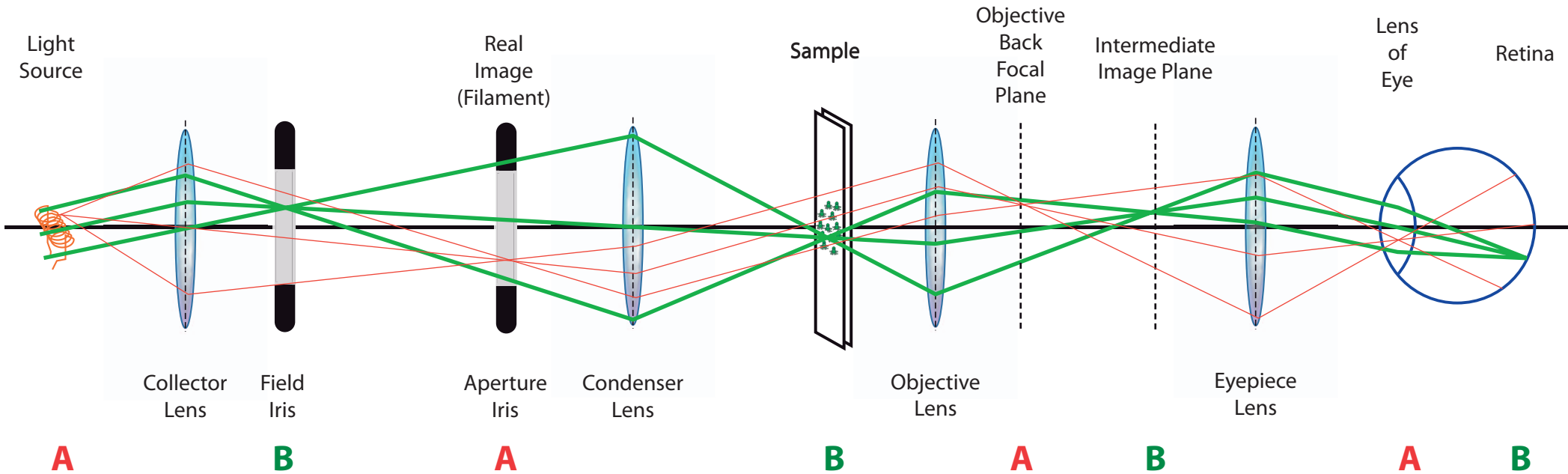
Light Source  
Aperture Iris  
Back focal plane of objective  
Front lens of eye

### Sample Image Conjugate Planes

Field Iris  
Sample plane  
Intermediate image plane  
Retina

# Kohler Illumination

How do we best illuminate the sample?



## Illumination Conjugate Planes

- Light Source
- Aperture Iris
- Back focal plane of objective
- Front lens of eye

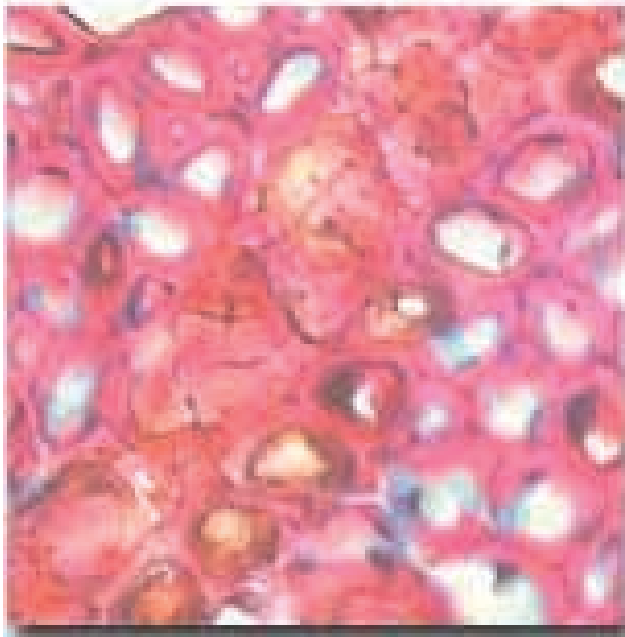
## Sample Image Conjugate Planes

- Field Iris
- Sample plane
- Intermediate image plane
- Retina

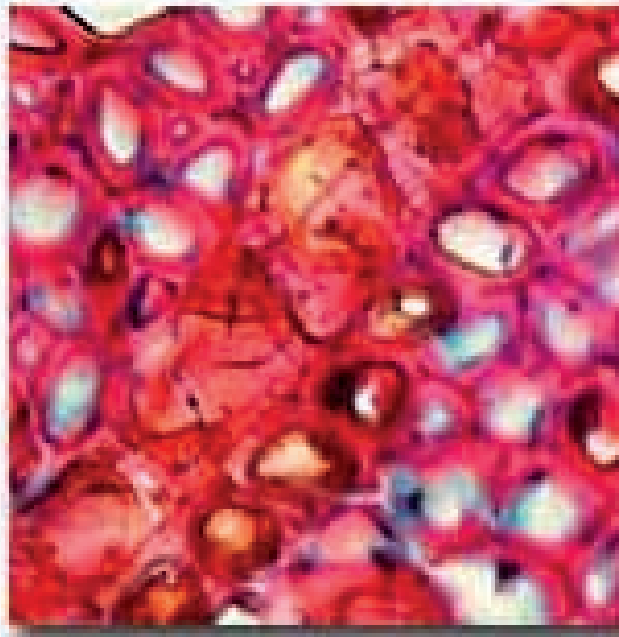
# Kohler Illumination

## Effect of Aperture Diaphragm on Contrast and Resolution

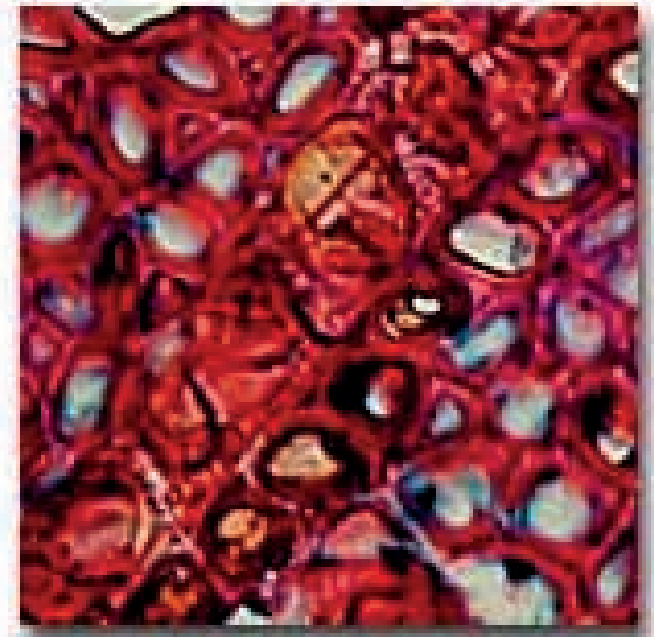
Photomicrograph of Plum Tree Stem infected with Black Knot Fungush



Objective NA = 0.75  
Condenser NA = 0.90



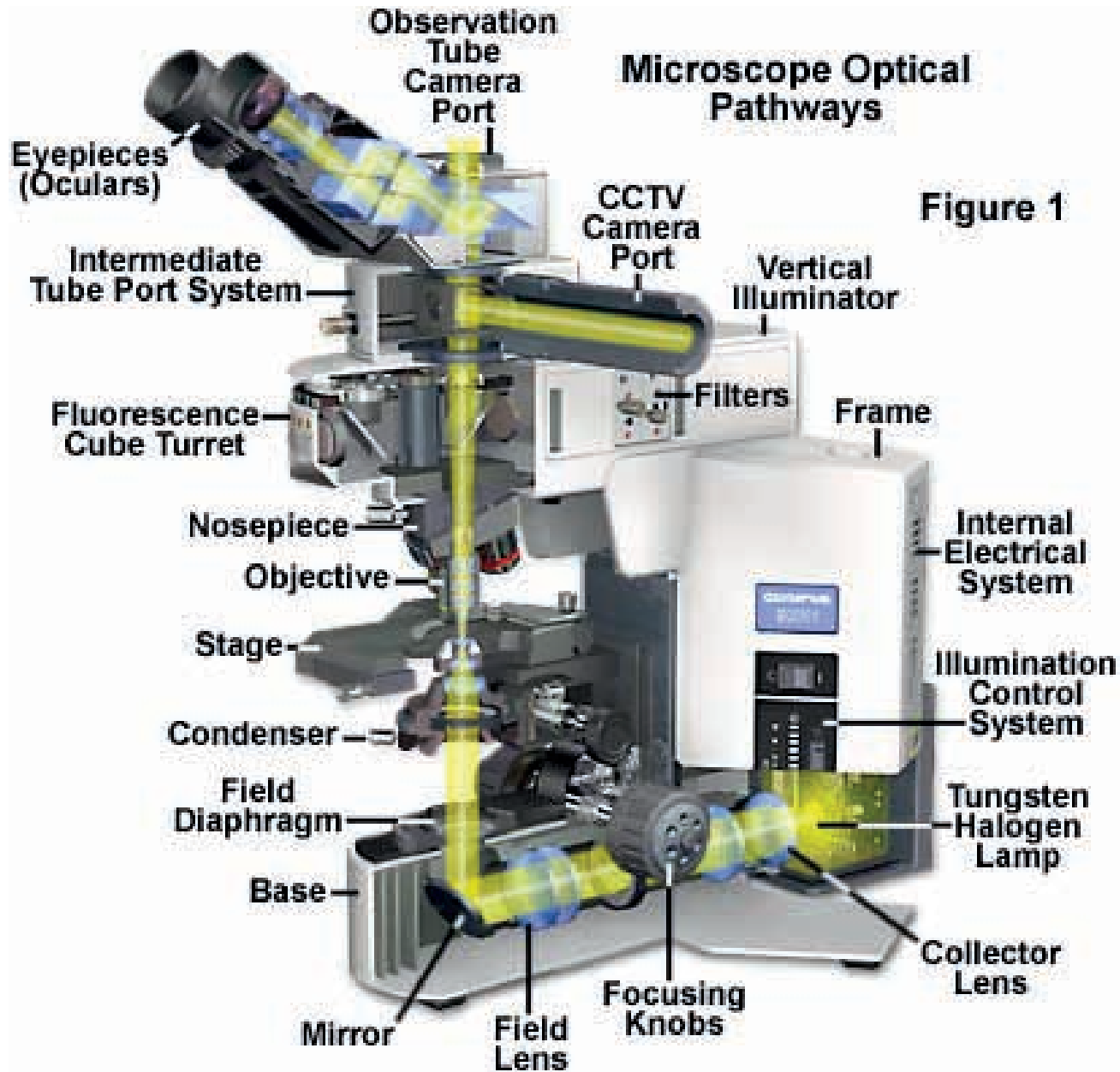
Objective NA = 0.75  
Condenser NA = 0.54



Objective NA = 0.75  
Condenser NA = 0.18

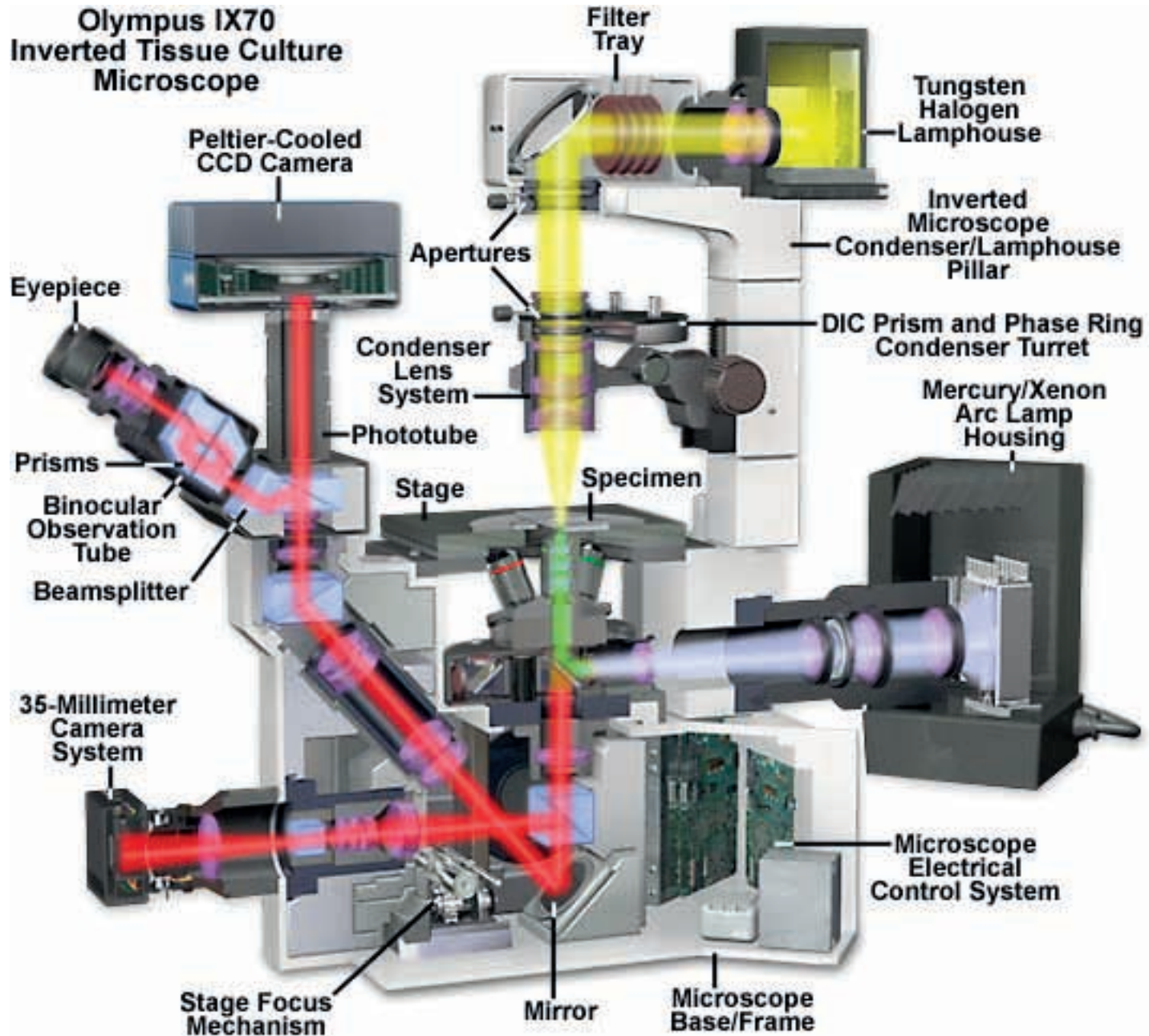
# Kohler Illumination

Light Pathways in an upright microscope

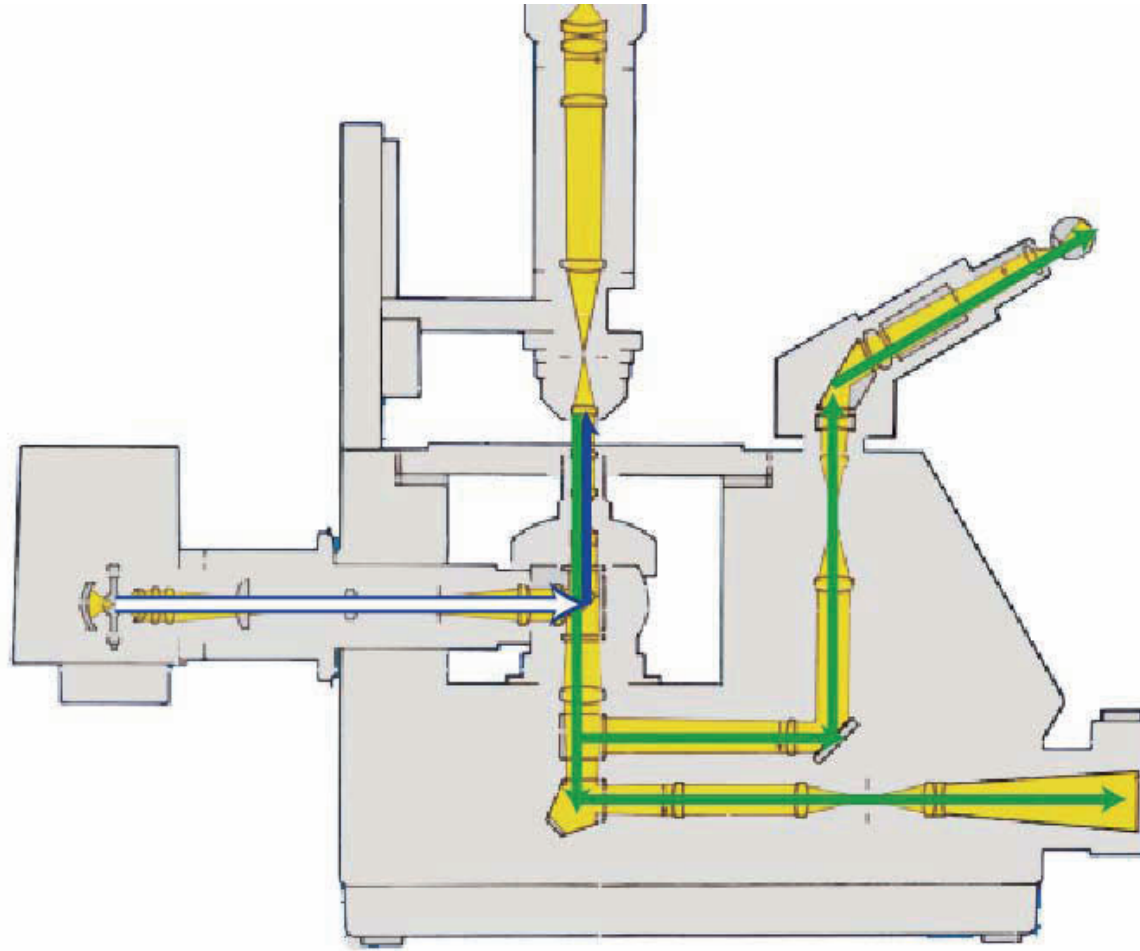


# Kohler Illumination

Light Pathways in an inverted microscope



# Optical schematic of an inverted epifluorescence microscope



Philbert S. Tsai, July 28, 2010





# Periodic Table of the Elements

1	IA H																0 He	
2	Li	IIA Be											IIIA B	IVA C	VA N	VIA O	VIIA F	Ne
3	Na	Mg	IIIB	IVB	VB	VIB	VIIA	VII			IB	IIB	Al	Si	P	S	Cl	Ar
4	K	Ca	Sc	Ti	V	Cr	Mn	Fe	Co	Ni	Cu	Zn	Ga	Ge	As	Se	Br	Kr
5	Rb	Sr	Y	Zr	Nb	Mo	Tc	Ru	Rh	Pd	Ag	Cd	In	Sn	Sb	Te	I	Xe
6	Cs	Ba	*La	Hf	Ta	W	Re	Os	Ir	Pt	Au	Hg	Tl	Pb	Bi	Po	At	Rn
7	Fr	Ra	+Ac	Rf	Ha	Sg	Ns	Hs	Mt	110	111	112	113					

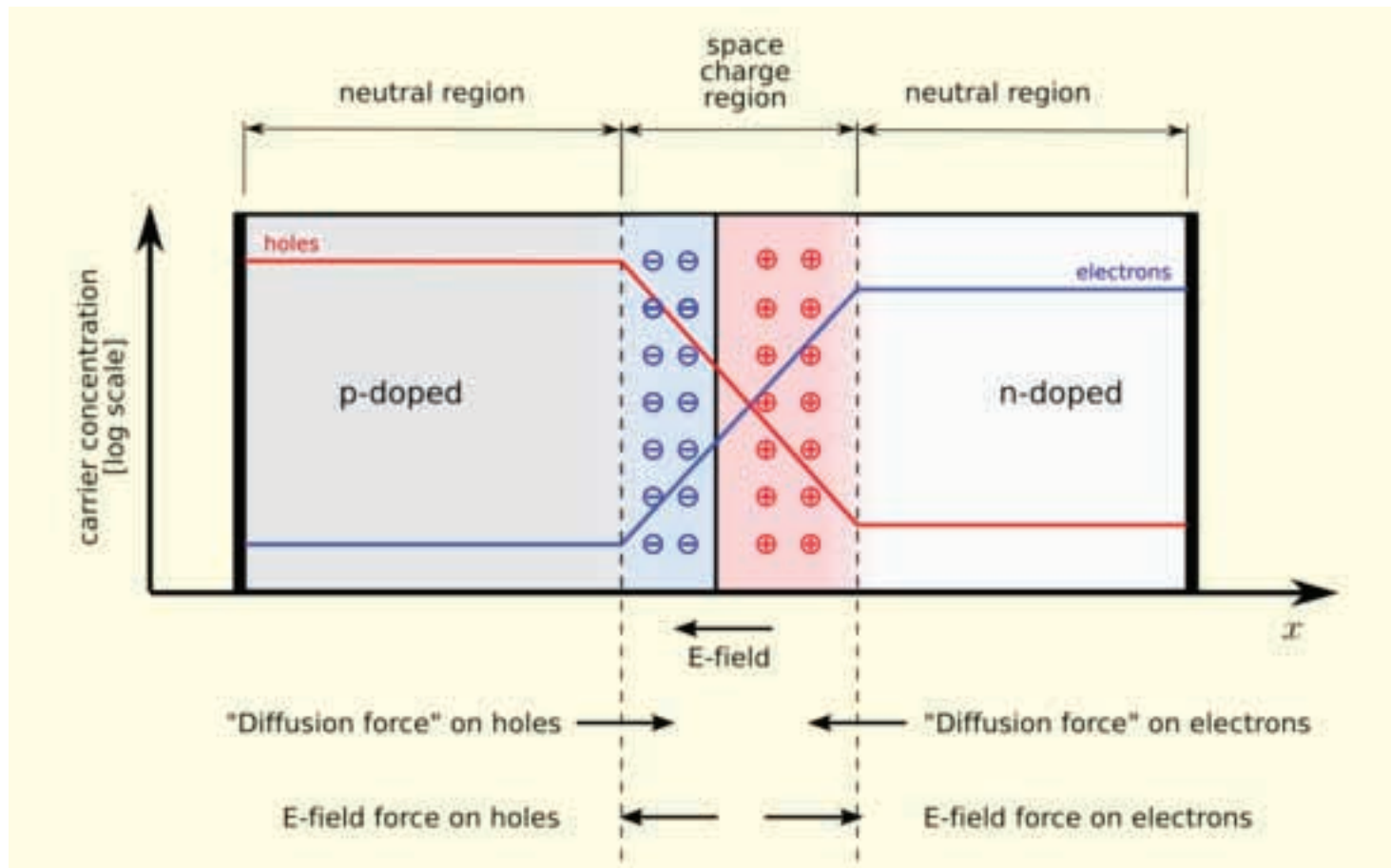
+ Lanthanide Series

58	59	60	61	62	63	64	65	66	67	68	69	70	71
Ce	Pr	Nd	Pm	Sm	Eu	Gd	Tb	Dy	Ho	Er	Tm	Yb	Lu

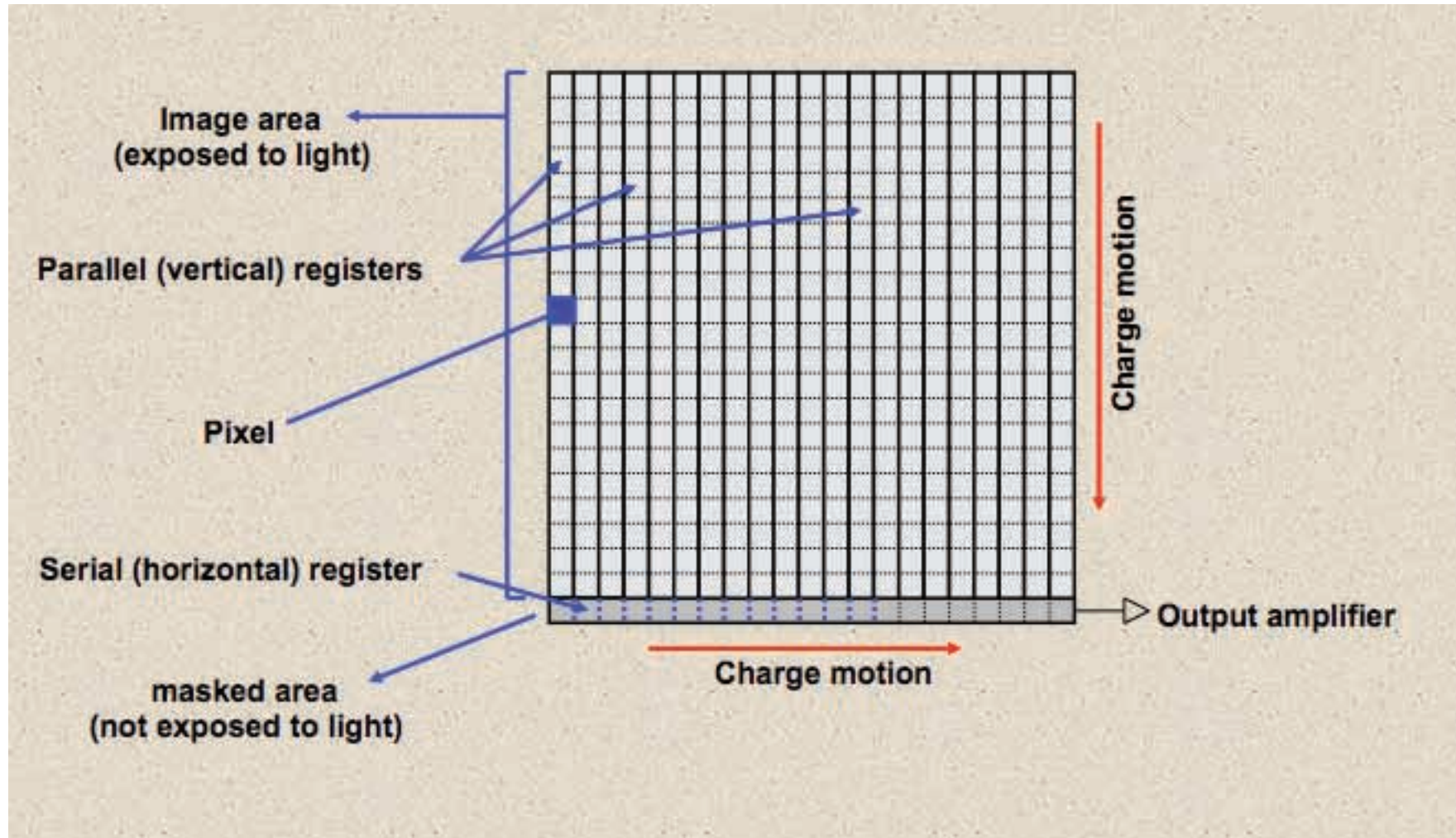
+ Actinide Series

90	91	92	93	94	95	96	97	98	99	100	101	102	103
Th	Pa	U	Np	Pu	Am	Cm	Bk	Cf	Es	Fm	Md	No	Lr

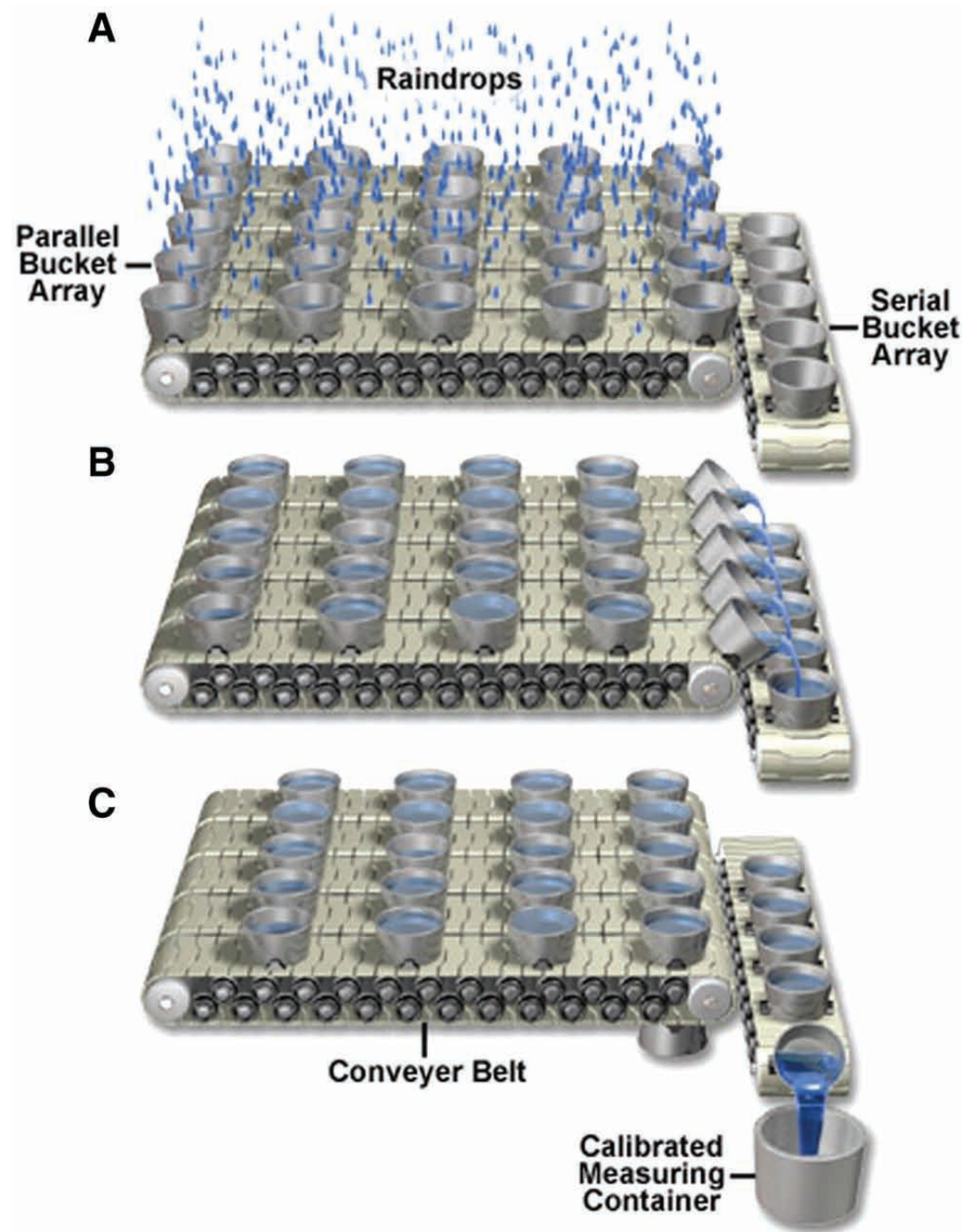
# PN Semiconductor Junction



# CCD Chip Layout



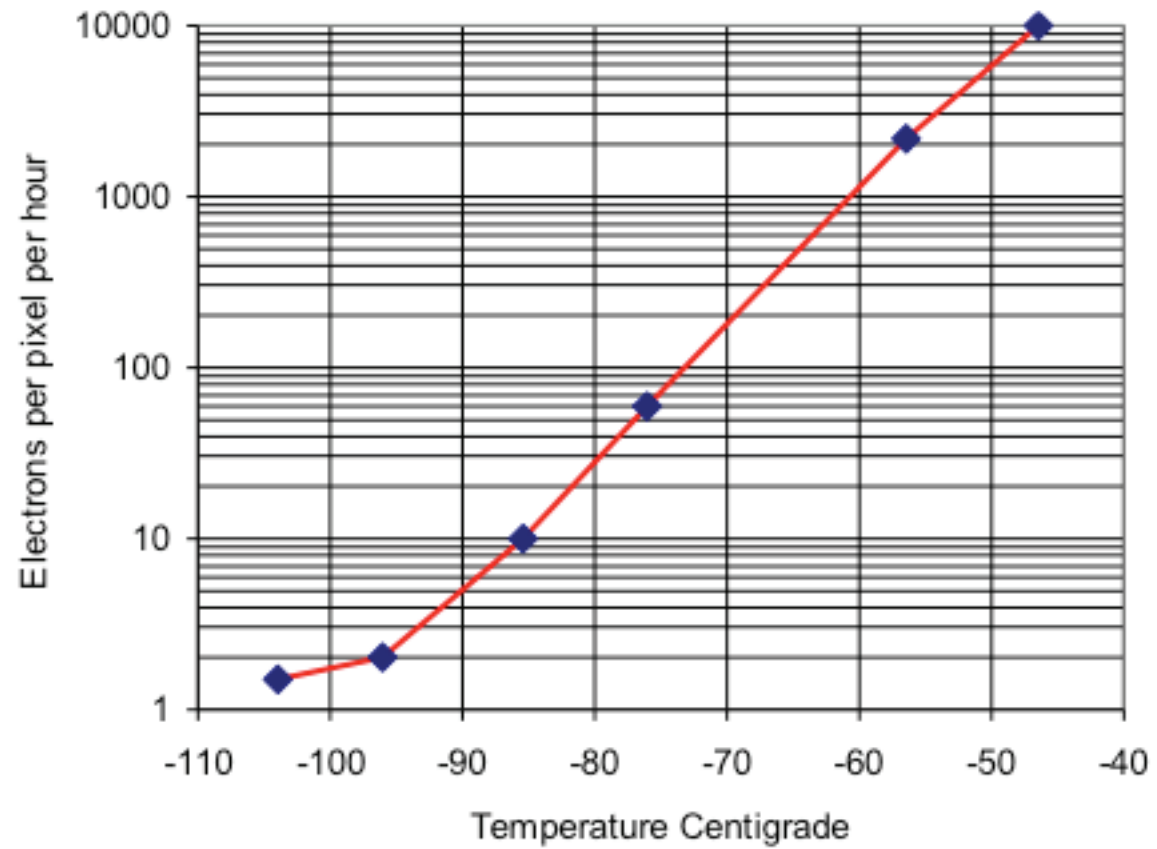
# Charge Coupled Device (CCD) Charge Transfer



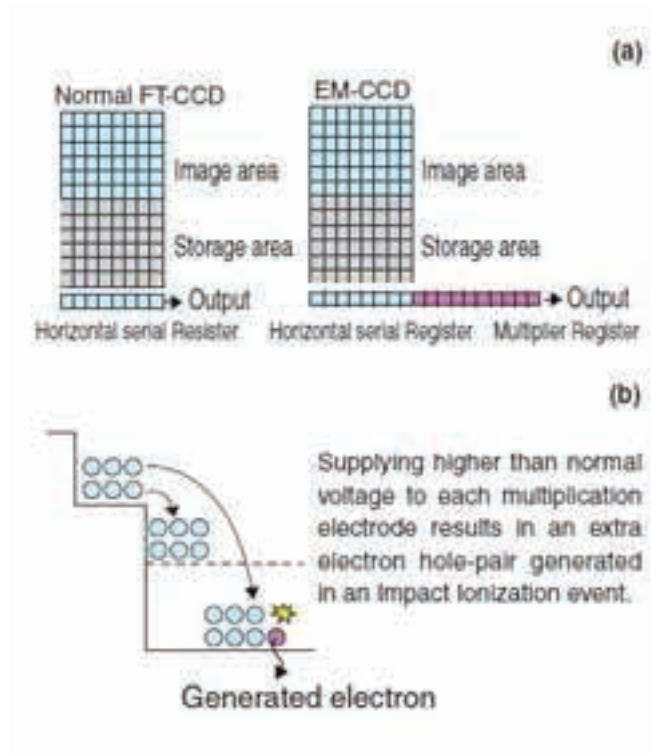
# CCD Performance Categories

- Charge generation
  - Quantum Efficiency (QE), Dark Current
- Charge collection
  - full well capacity, pixels size, pixel uniformity, defects, diffusion (Modulation Transfer Function, MTF)
- Charge transfer
  - Charge transfer efficiency (CTE), defects
- Charge detection
  - Readout Noise (RON), linearity

# Temperature Sensitive of CCDs (Dark Current)

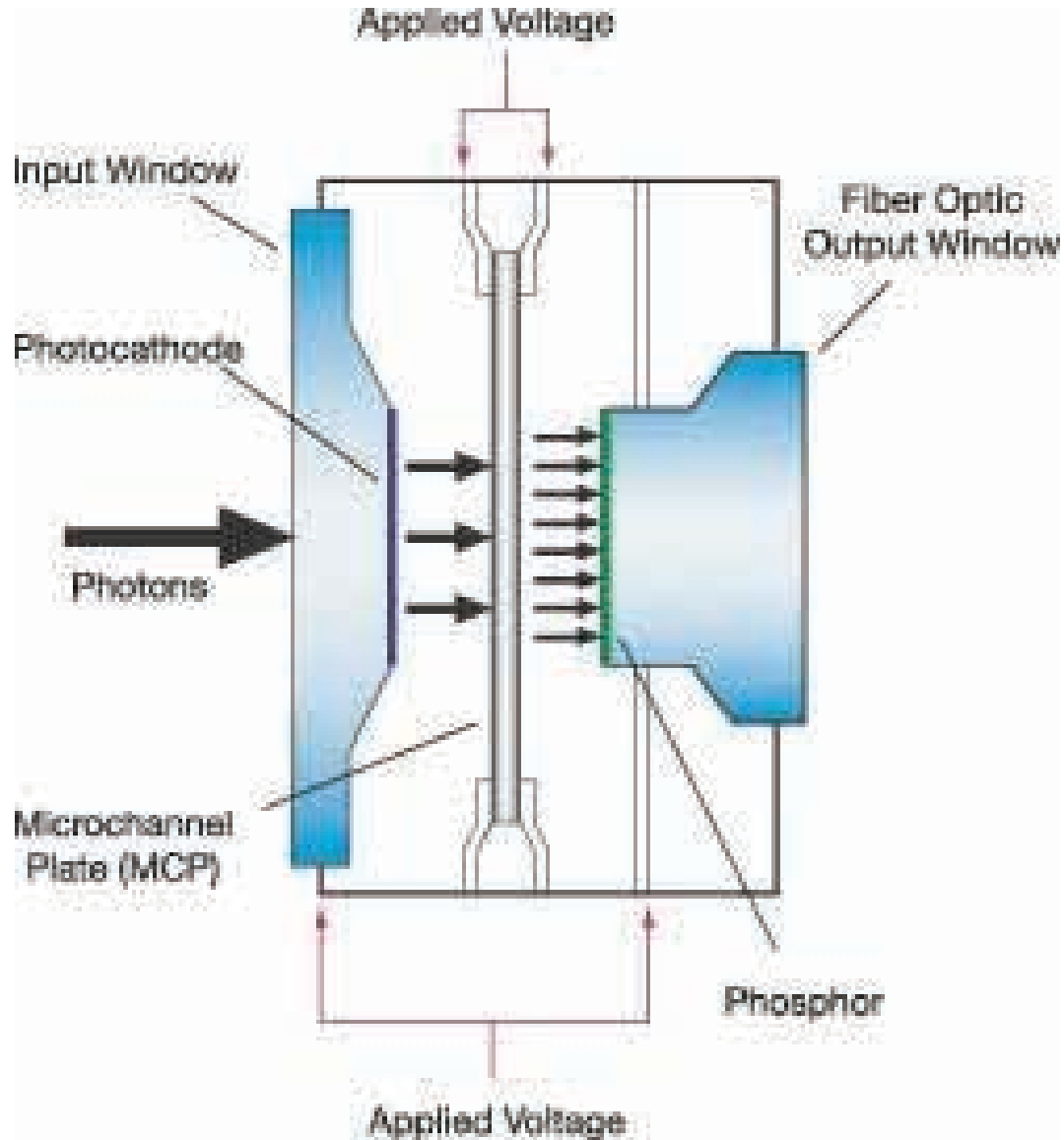


# Electron Multiplied Charge Coupled Device (EMCCD)



Per Transfer Gain  $\sim 1.02$   
but over 500 transfer  
Total Gain is  $> 1000x$

# Intensified Charge Coupled Device (ICCD)

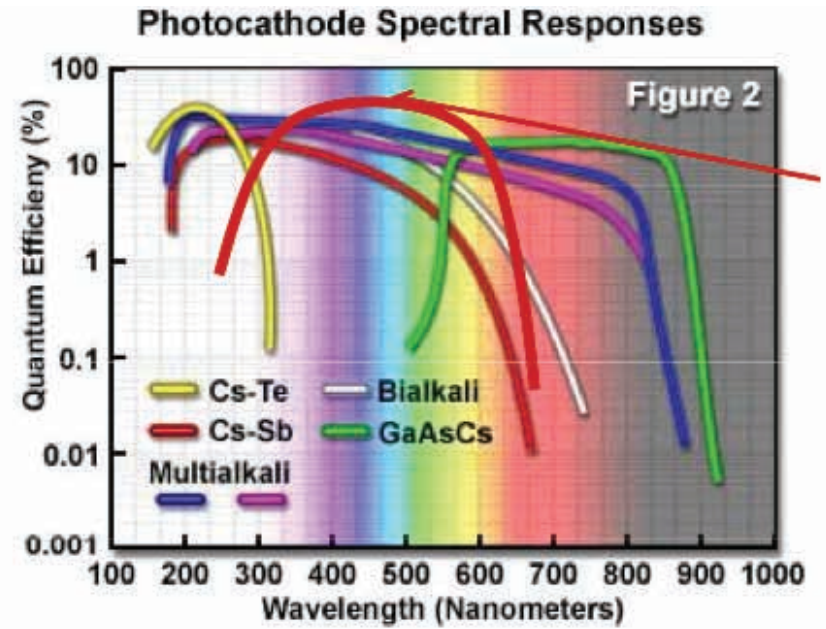
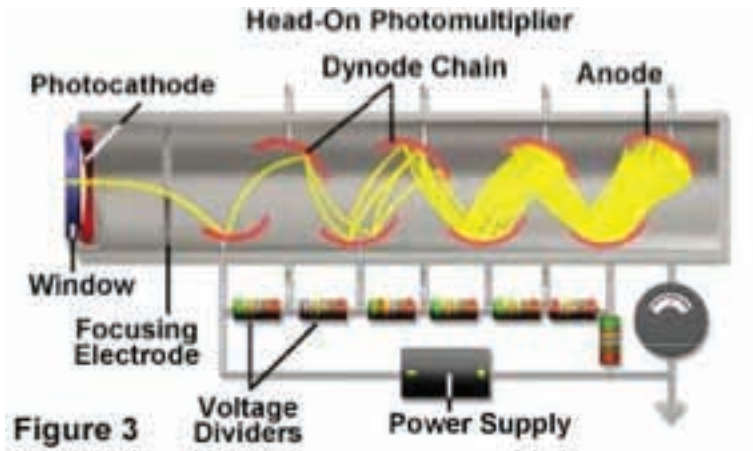




# Charge Coupled Device (CCD) Technologies

Detector Type	Advantages	Disadvantages
<b>EMCCD</b>	<p>Single Photon Sensitive</p> <p>High and broad QE</p> <p>Good resolution - Pixel limited</p> <p>Good dynamic range possible</p> <p>Fast or slow readout</p> <p>Flexible - Operate as EMCCD or CCD (<i>gain can be turned off</i>). Conventional CCD amplifier on some sensors</p> <p>No photocathode!</p> <p>Relatively affordable (broad range of pricing, largely sensor dependent)</p>	<p>No nano or picosecond gating (<i>microsecond gating available on some recent interline EMCCD sensors</i>)</p> <p>Multiplication noise (<i>effectively increases shot noise by x1.41</i>)</p>
<b>CCD</b>	<p>High and broad QE</p> <p>Good resolution – pixel limited</p> <p>Good dynamic range possible</p> <p>No multiplication noise</p> <p>No photocathode!</p> <p>Greater choice of sensor formats available</p>	<p>Read noise limited - not single photon sensitive</p> <p>Limited readout speed due to read noise restraints</p>
<b>ICCD</b>	<p>Single Photon Sensitive</p> <p>Nano and Picosecond time-resolved gating possible</p> <p>Fast or slow readout</p> <p>NIR photocathode options</p>	<p>QE restricted by photocathode (&lt;50% max)</p> <p>Poor dynamic range – need to operate at high gains</p> <p>Cross-talk between channels of MCP – increased point spread function</p> <p>Higher multiplication noise</p> <p>Artefacts, e.g. halo, chickenwire</p> <p>Inflexible – no 'CCD mode'</p> <p>Expensive</p> <p>Damage susceptible – longevity issues</p>

# Photo Multiplier Tube (PMT)



# Photo Multiplier Tube (PMT)

## Side-On New Compact Type Photomultiplier Tubes

Type No.	Remarks	Spectral Response		Photo-cathode Material <sup>(A)</sup>	Window Material <sup>(B)</sup>	Outline No. <sup>(C)</sup>	Dynode Structure <sup>(D)</sup> No. of Stages	Socket Socket Assembly	Maximum Ratings <sup>(F)</sup>		Cathode Sensitivity Luminous	
		Range (nm)	Peak Wave-length (nm)						Anode to Cathode Voltage (Vdc)	Average Anode Current (mA) <sup>(G)</sup>	Min. ( $\mu$ A/lm)	Typ. ( $\mu$ A/lm)
R6350	For UV to visible range, general purpose.	185 to 650	340	Sb-Cs	U	1	CC/9	E678-11U/ <sup>(E)</sup>	1250	0.01	20	40
R6351	Synthetic silica window type of R6350	160 to 650	340	Sb-Cs	Q	2	CC/9	E678-11U/ <sup>(E)</sup>	1250	0.01	20	40
R6352	High sensitivity variant of R6350	185 to 750	420	BA	U	1	CC/9	E678-11U/ <sup>(E)</sup>	1250	0.01	80	120
R6353	Low dark current bialkali photocathode	185 to 680	400	LBA	U	1	CC/9	E678-11U/ <sup>(E)</sup>	1250	0.01	30	70
R6354	For UV range	160 to 320	230	Cs-Te	Q	2	CC/9	E678-11U/ <sup>(E)</sup>	1250	0.01	—	—
R6355	For UV to near IR range, general purpose	185 to 850	530	MA	U	1	CC/9	E678-11U/ <sup>(E)</sup>	1250	0.01	80	150
R6356	High sensitivity variant of R6355	185 to 900	600	MA	U	1	CC/9	E678-11U/ <sup>(E)</sup>	1250	0.01	140	250
R6357 *	High sensitivity variant of R6356, Meshless type	185 to 900	450	MA	U	1	CC/9	E678-11U/ <sup>(E)</sup>	1250	0.01	350	500
R6358	Low dark current variant of R6356	185 to 830	530	LMA	U	1	CC/9	E678-11U/ <sup>(E)</sup>	1250	0.01	140	200

# Photo Multiplier Tube (PMT)

Cathode Sensitivity			Anode to Cathode Supply Voltage (Vdc)	Anode Characteristics								Notes	Type No.
Blue (5-58) Typ. ( $\mu$ A/lm-b)	Red/White Ratio Typ.	Radiant Typ. (mA/W)		Anode Sensitivity			Current Amplification Typ.	Anode Dark Current (After 30 min.)		Time Response			
				Luminous		Radiant Typ. (nm)		Typ.	Max.	Rise Time Typ. (ns)	Electron Transit Time Typ. (ns)		
				Min. (A/lm)	Typ. (A/lm)								
5	—	48	1000	50	300	$3.6 \times 10^5$	$7.5 \times 10^6$	0.5	5	1.4	15	Photon counting type: R6350P: 10cps Typ.	R6350
5	—	48	1000	50	300	$3.6 \times 10^5$	$7.5 \times 10^6$	0.5	5	1.4	15		R6351
10	—	90	1000	100	700	$5.2 \times 10^5$	$5.8 \times 10^6$	1	10	1.4	15		R6352
6.5	—	65	1000	100	400	$3.7 \times 10^5$	$5.7 \times 10^6$	0.1	2	1.4	15	Photon counting type: R6353P: 10cps Typ.	R6353
—	—	62 <sup>a</sup>	1000	—	—	$1.8 \times 10^5$ <sup>a</sup>	$3 \times 10^6$	0.5	5	1.4	15		R6354
6	0.15	45	1000	100	600	$1.8 \times 10^5$	$4 \times 10^6$	1	10	1.4	15		R6355
7	0.3	60	1000	400	2500	$6 \times 10^5$	$1 \times 10^7$	1	10	1.4	15		R6356
13	0.4	105	1000	1000	2000	$4.2 \times 10^5$	$4 \times 10^6$	2	10	1.4	15		R6357 *
7.5	0.15	70	1000	300	700	$2.5 \times 10^5$	$3.5 \times 10^6$	0.1	1	1.4	15	Photon counting type: R6358P: 20cps Typ.	R6358

# GaAsP PMTs

## Metal package PMT with Cooler Photon Counting Head H7421 Series



Heatsink with fan (A7423) sold separately

The H7421 series are photon counting head devices containing a metal package photomultiplier tube having a GaAsP/GaAs photocathode and a thermoelectric cooler. The thermoelectric cooler reduces thermal noise generated from the photocathode which also offers a high quantum efficiency, allowing measurement to be made with a good S/N ratio even at very low light levels.

The H7421-40 has high sensitivity on wavelength from 300 nm to 720 nm. The H7421-50 is sensitive over a wide spectral range from 380 nm to 890 nm. The photomultiplier tube is maintained at a constant temperature by monitoring the output from a thermistor installed near the photomultiplier tube and regulating the current to the thermoelectric cooler.

### Product Variations

Type No.	Spectral Response	Features
H7421-40	300 nm to 720 nm	GaAsP photocathode, QE 40 % at peak wavelength
H7421-50	380 nm to 890 nm	GaAs photocathode, QE 12 % at peak wavelength

### Specifications

Parameter	H7421-40	H7421-50	Unit
Input Voltage	+4.5 to +5.5		V
Max. Input Voltage for Main Unit	+6		V
Max. Input Current for Main Unit	50		mA
Max. Input Voltage for Thermoelectric Cooler	2.6		V
Max. Input Current for Thermoelectric Cooler	2.2		A
Effective Area	ø5		mm
Peak Sensitivity Wavelength	580	800	nm
Count Sensitivity	$7.8 \times 10^5$	$3.9 \times 10^5$	$s^{-1} \cdot pW^{-1}$
Count Linearity *1	$1.5 \times 10^9$	$1.5 \times 10^5$	$s^{-1}$
Dark Count *2 *3	Typ.	100	$s^{-1}$
	Max.	300	
Pulse-pair Resolution	70		ns
Output Pulse Width	30		ns
Output Pulse Height *4	Typ.	3.6	V
	Min.	3.0	
Recommended Load Resistance	50		$\Omega$
Signal Output Logic	Positive logic		—
Operating Ambient Temperature	+5 to +35		$^{\circ}C$
Storage Temperature	-20 to +50		$^{\circ}C$
Weight	340		g

\*1: Random pulse, at 10 % count loss

\*2: PMT setting temperature 0  $^{\circ}C$ , used with C8137, M9011 and A7432

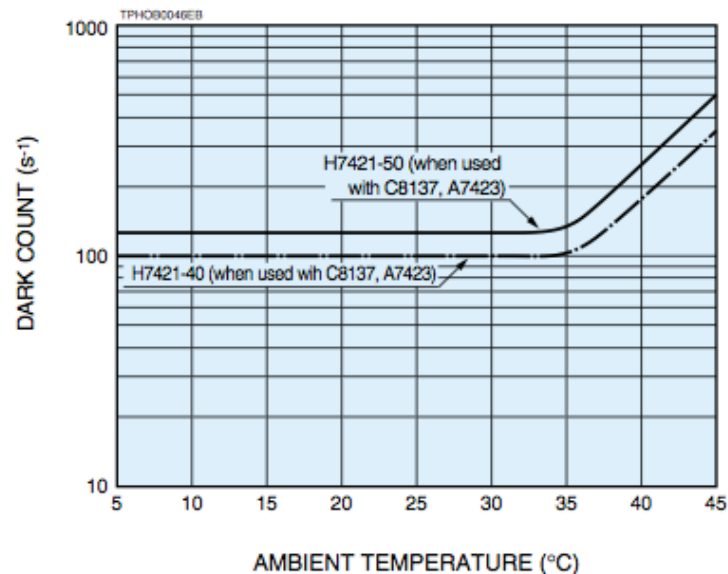
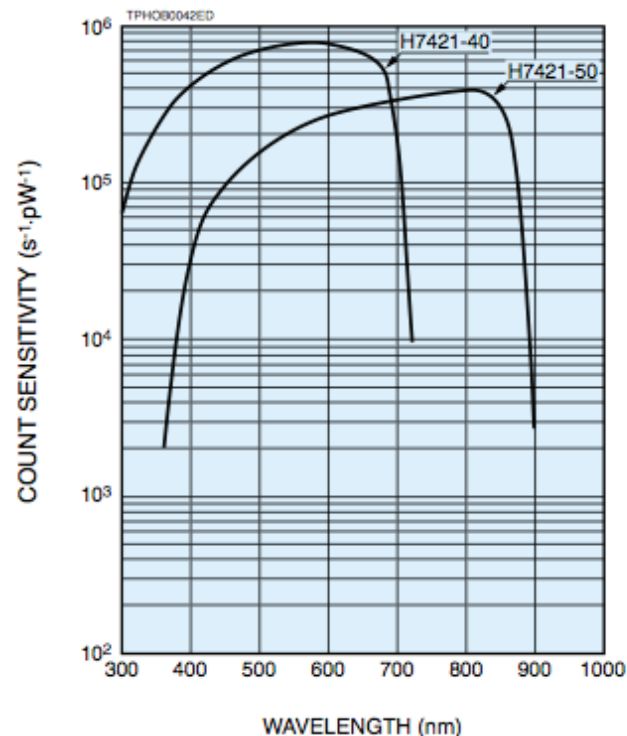
\*3: After 30 minute storage in darkness

\*4: With input voltage +5 V, Load resistance 50  $\Omega$  and Coaxial cable RG-174/U (450 mm)

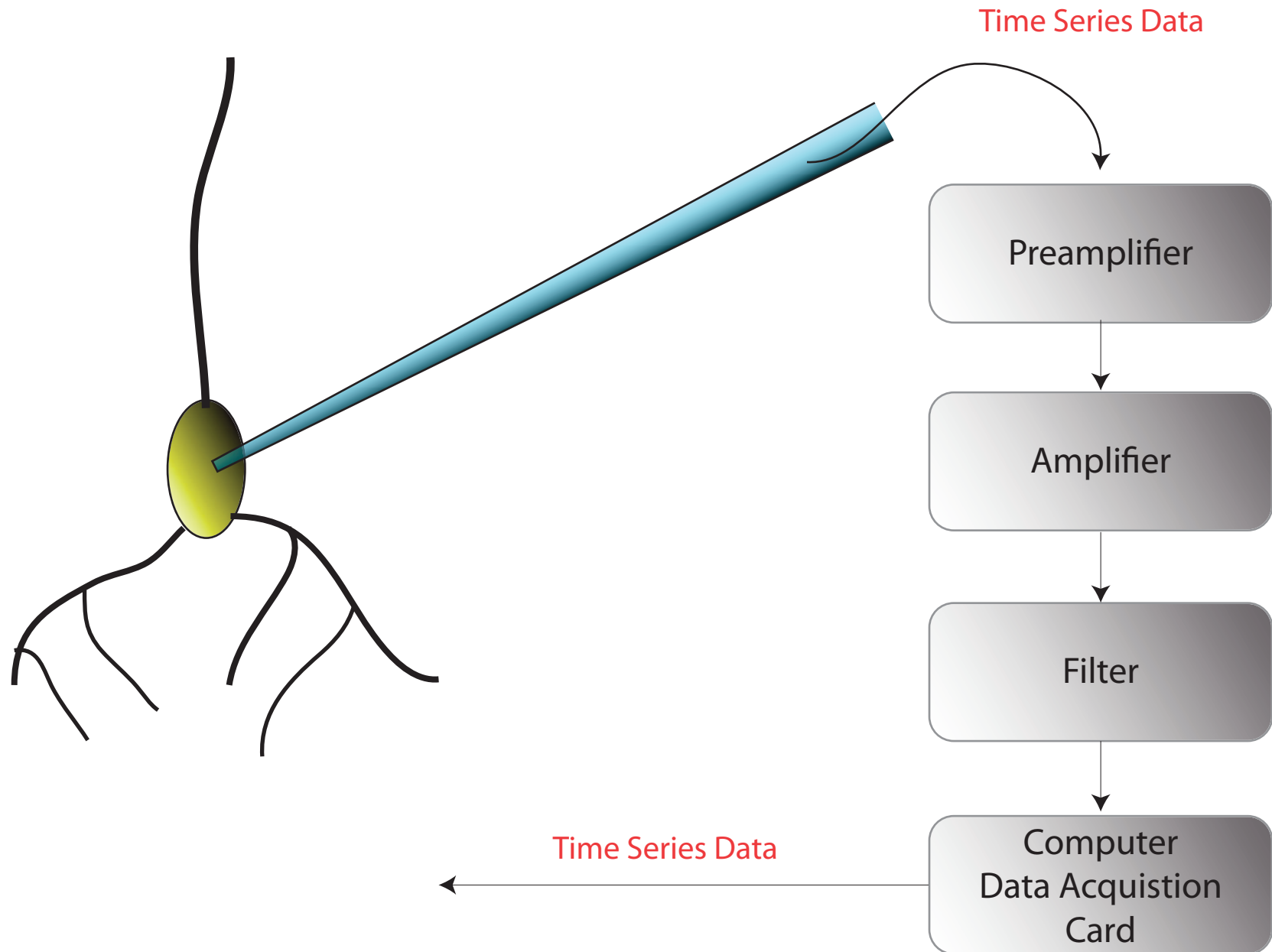
### Cooling Specifications

Parameter	H7421-40/H7421-50	Unit
Cooling Method	Thermoelectric cooling	—
Max. Cooling Temperature ( $\Delta T$ ) *5	35	$^{\circ}C$
Cooling Time	Approx. 5	min

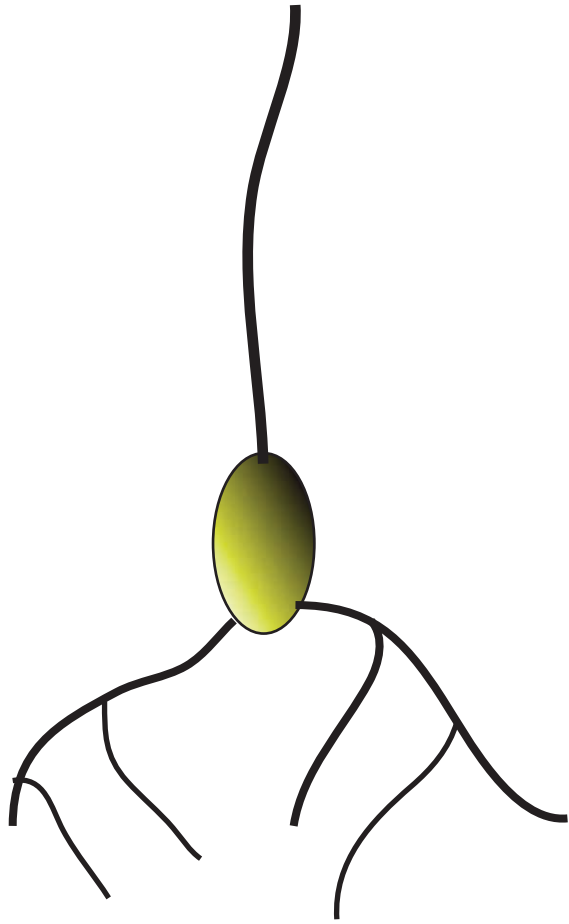
\*5: Input current to thermoelectric cooler = 2.0 A



# Data Acquisition

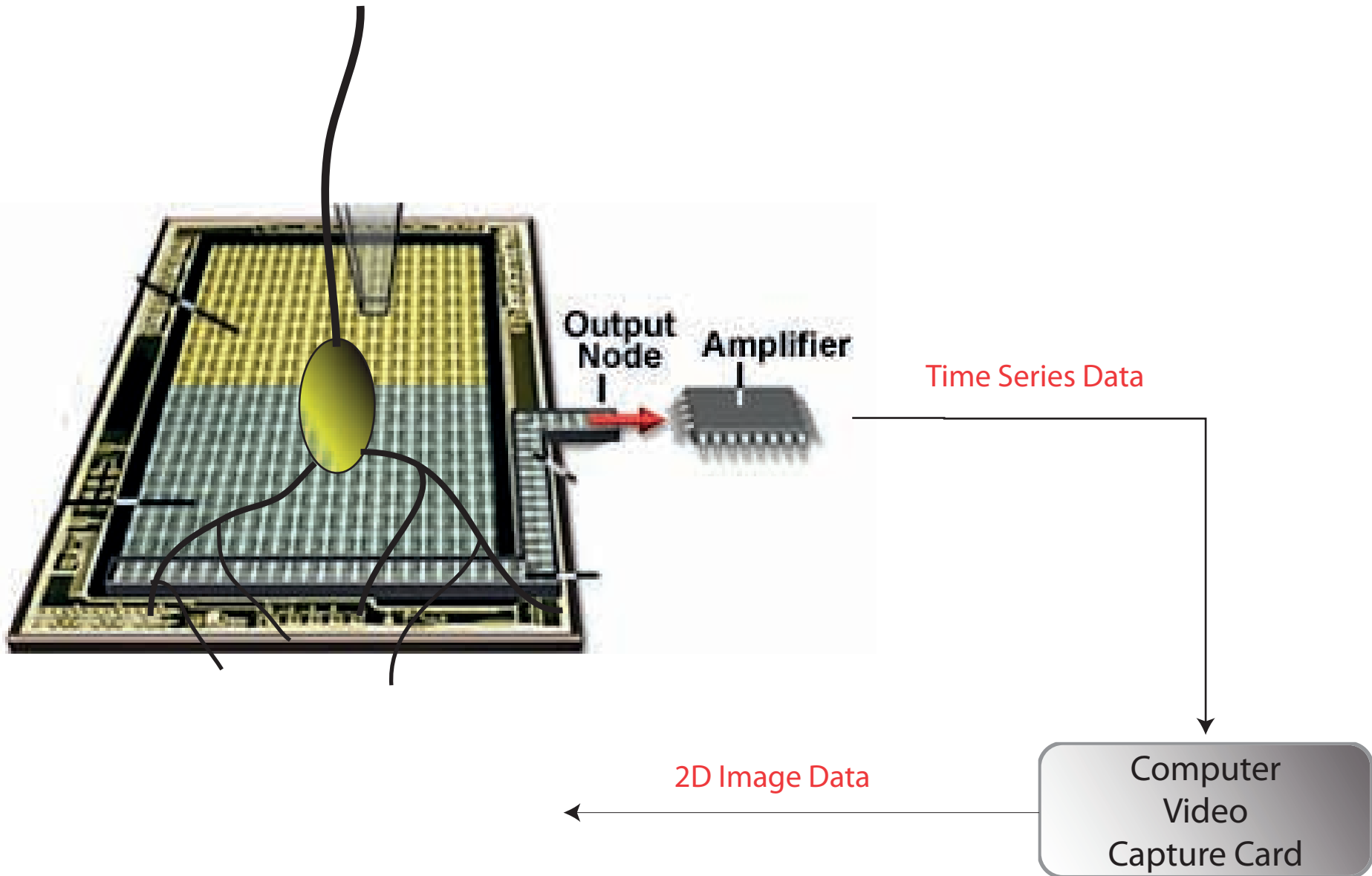


# Data Acquisition



# Data Acquisition

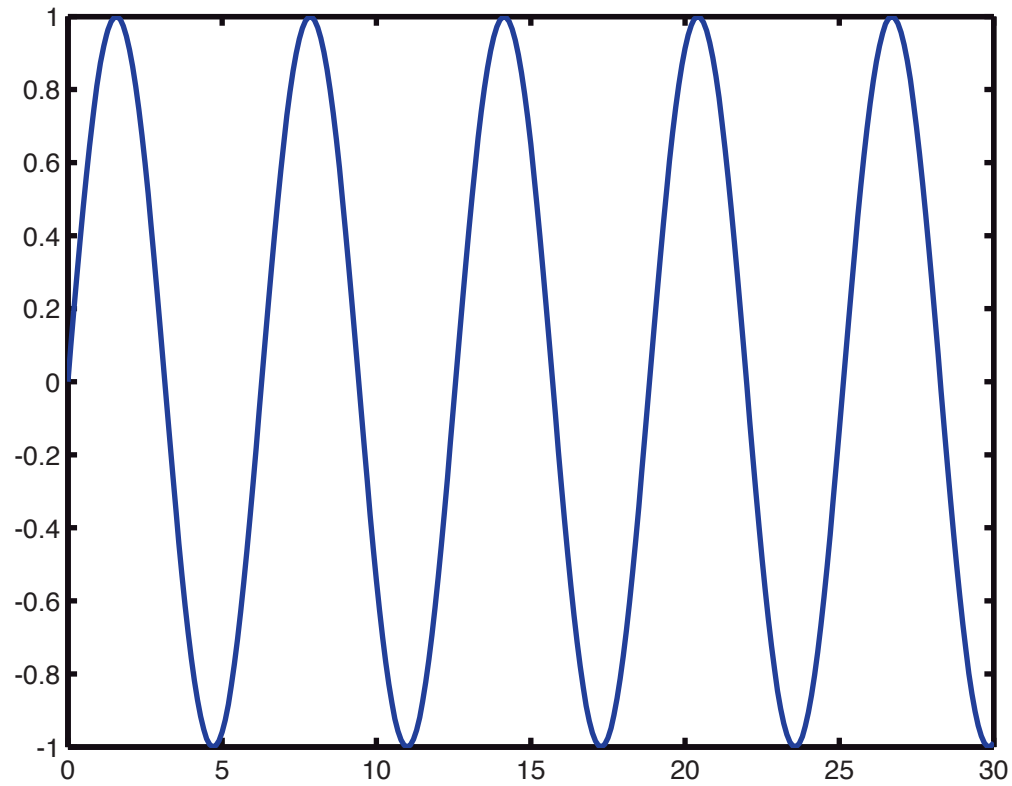
CCD Camera Imaging





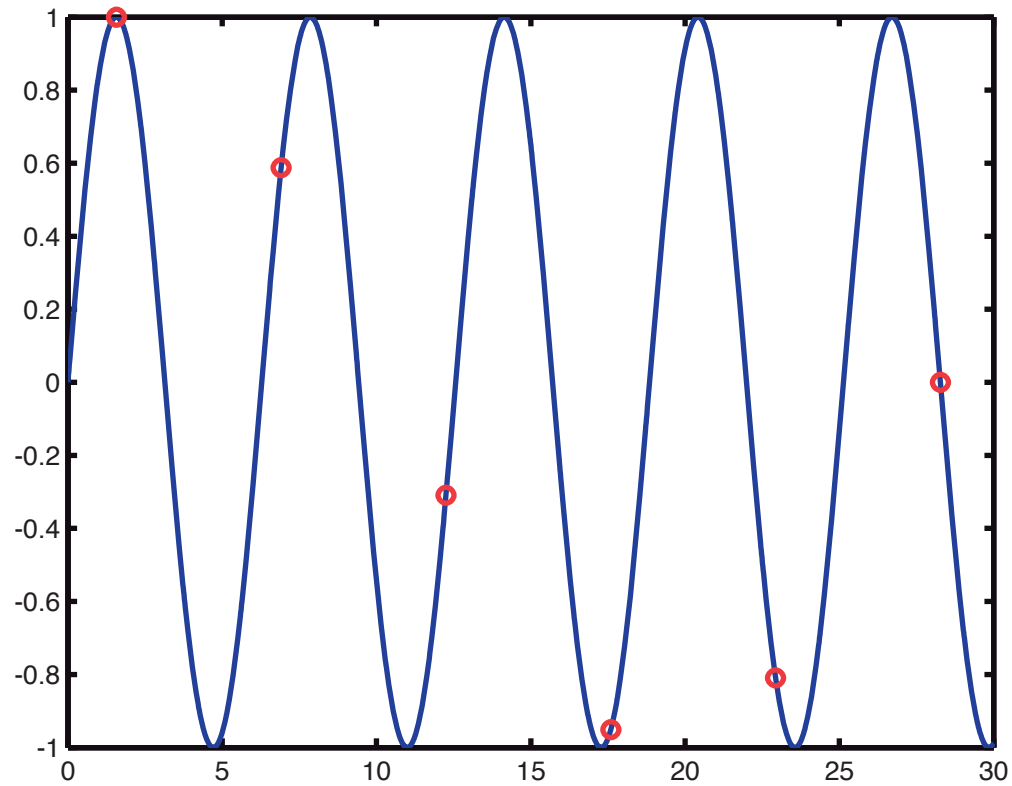
# Nyquist Sampling Theorem

How often should you collect data?



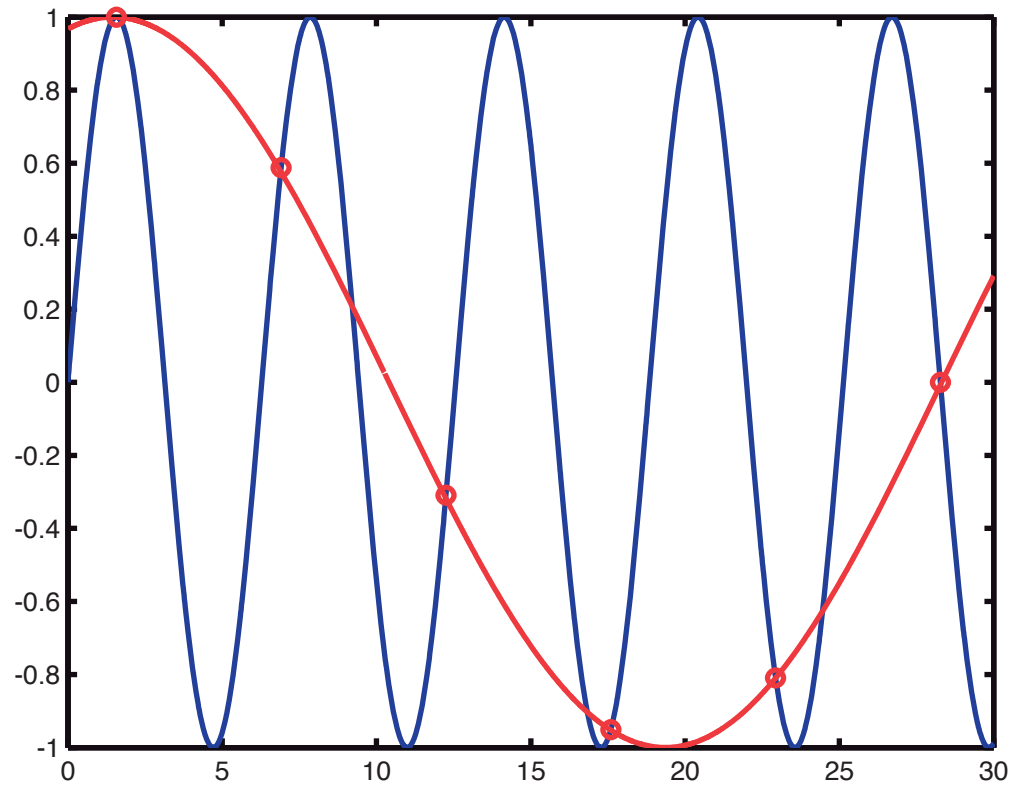
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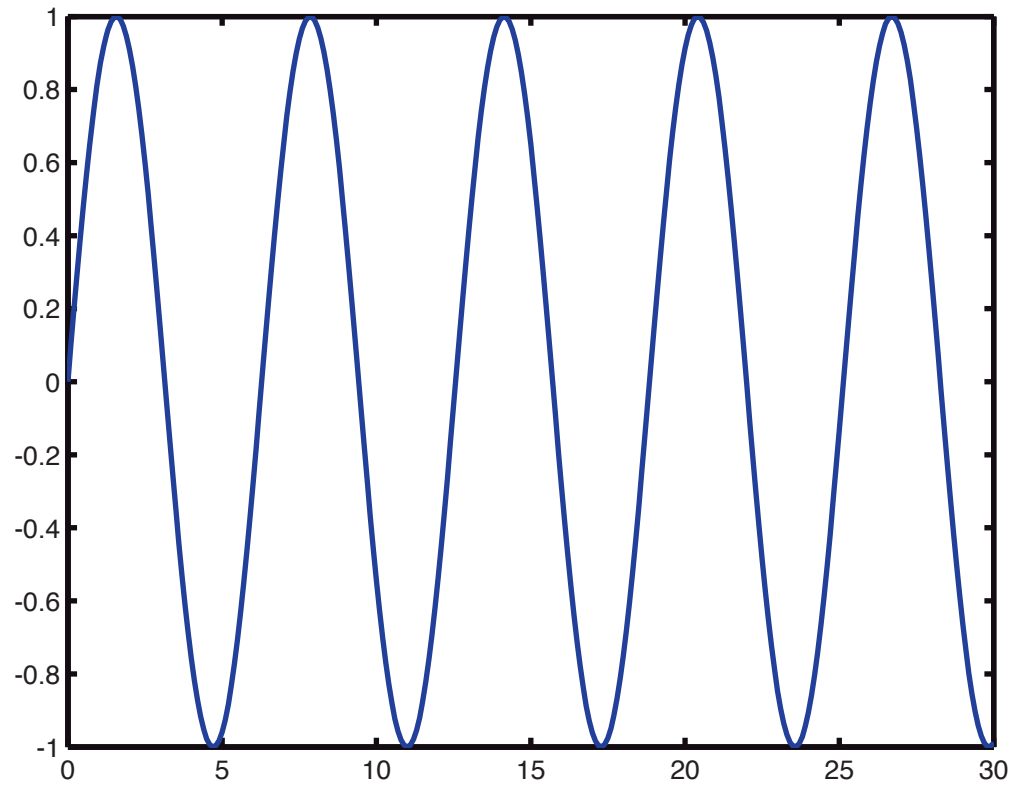
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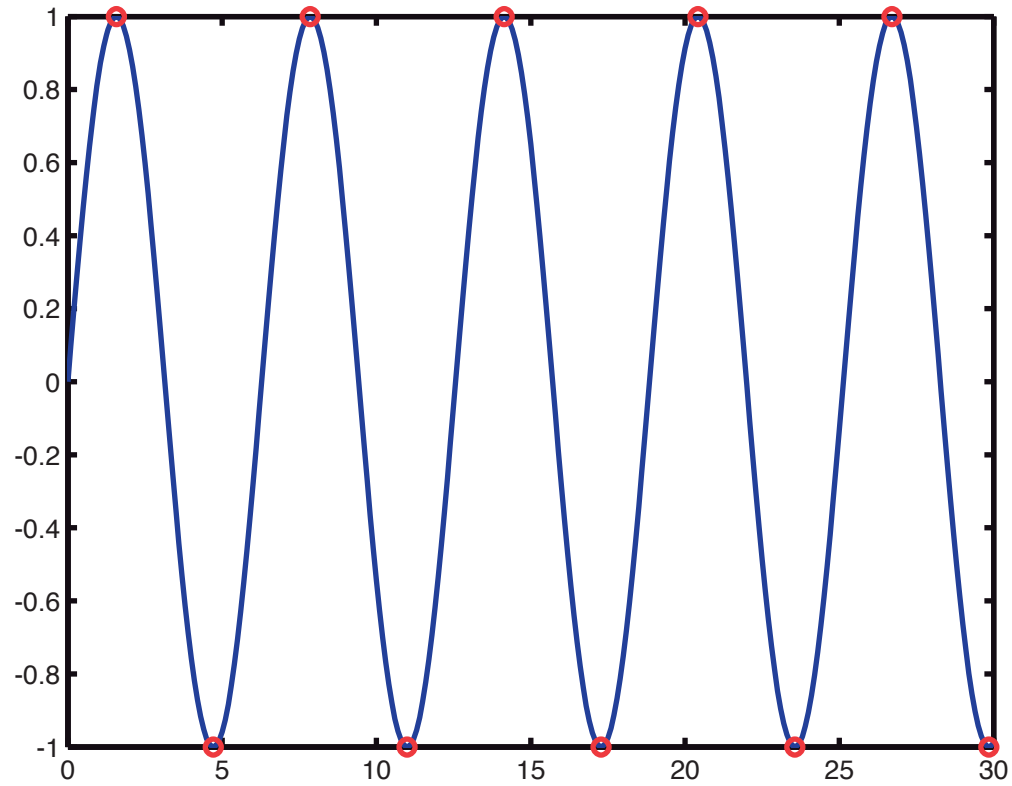
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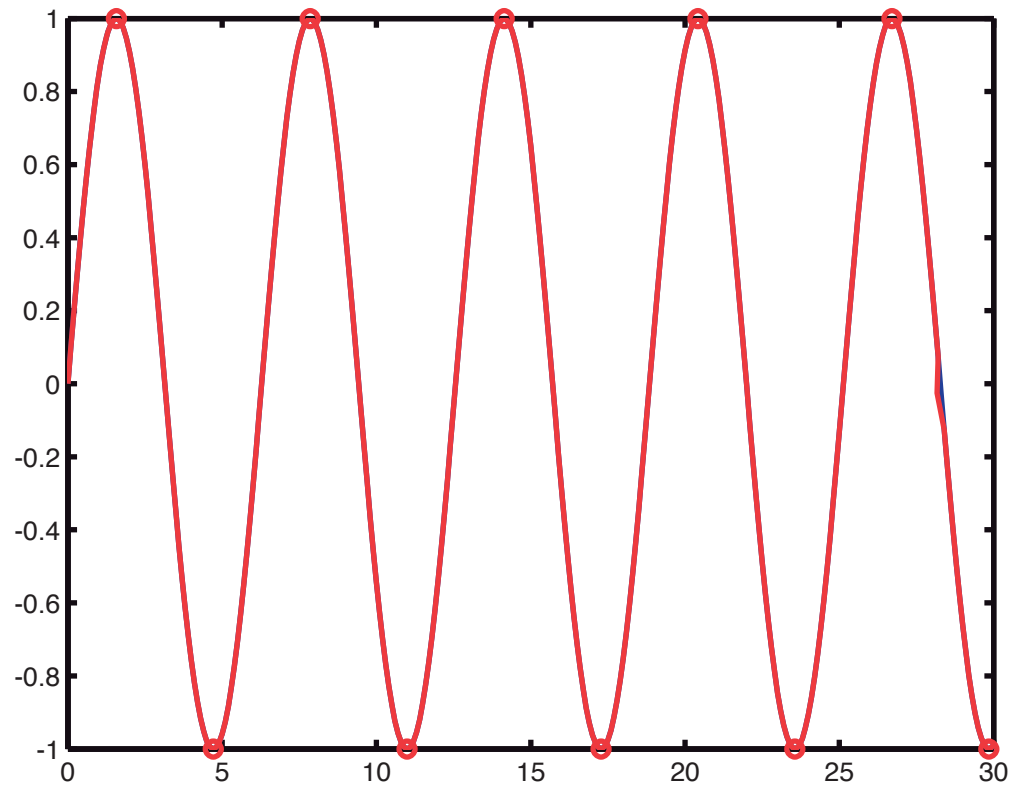
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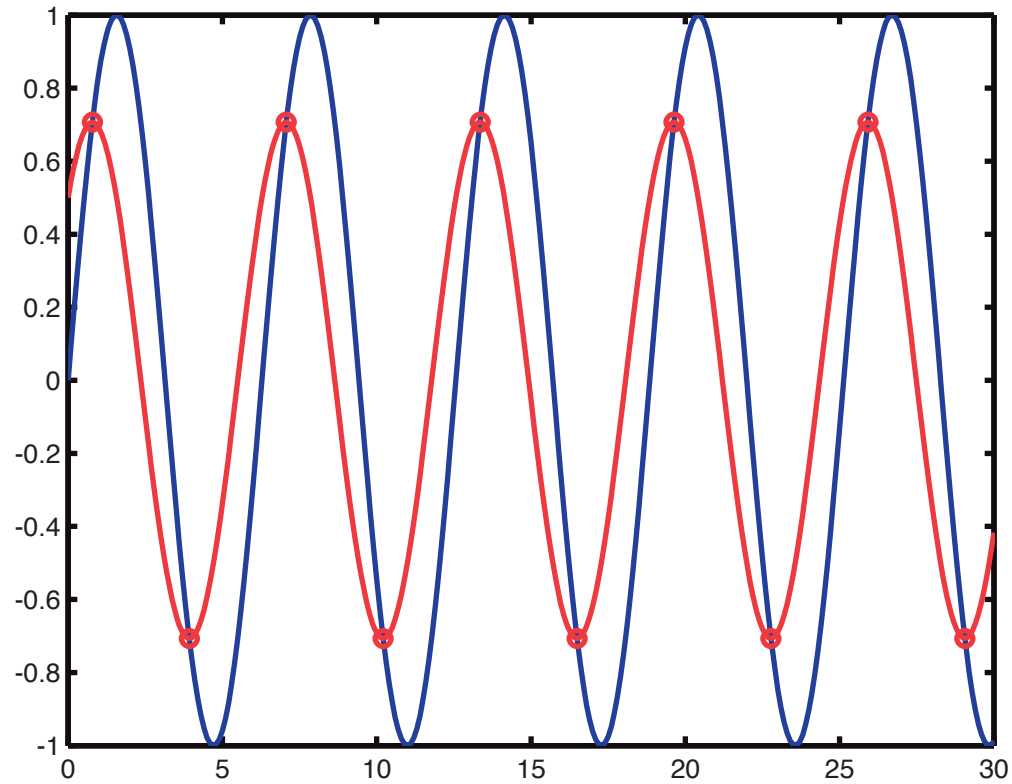
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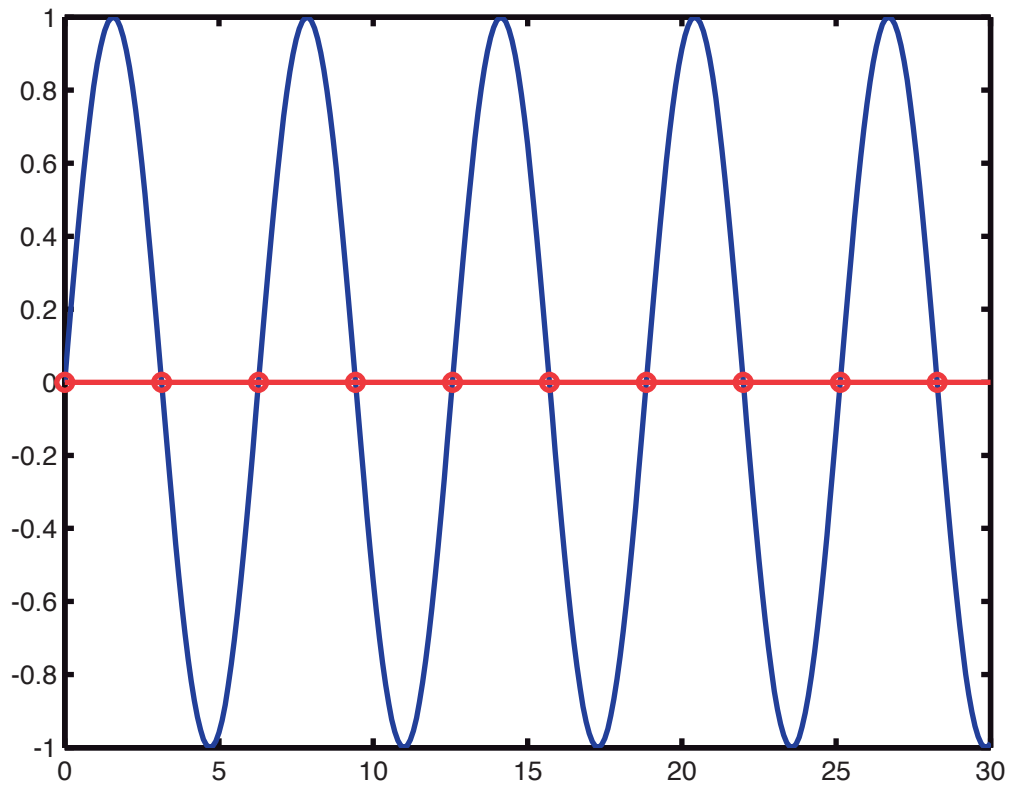
# Nyquist Sampling Theorem

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# Nyquist Sampling Theorem

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# Nature of Light

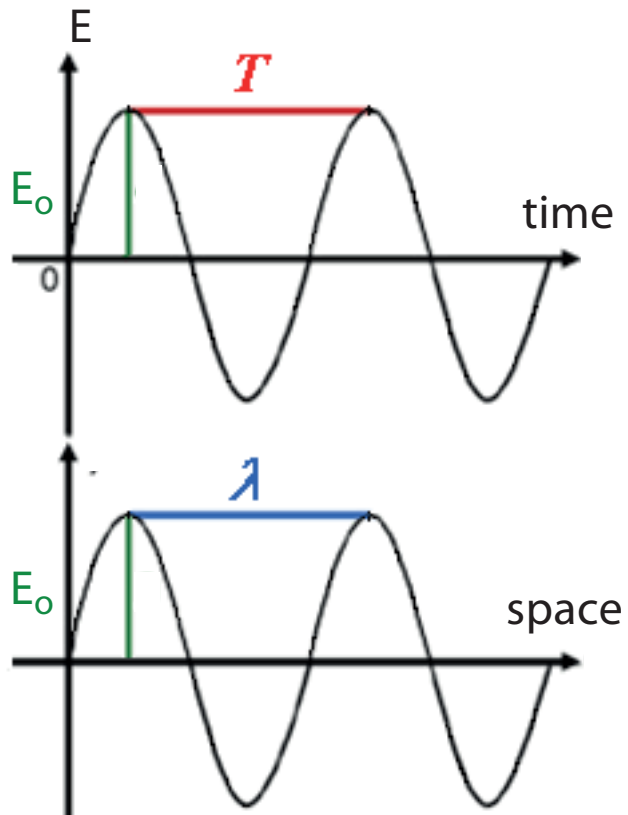
Light can be described as a traveling electromagnetic wave

$$E(\mathbf{r}, t) = E_0 \sin(\mathbf{k} \cdot \mathbf{x} - \omega \cdot t + \phi)$$

$$\omega = 2\pi \cdot f \quad \text{angular frequency}$$

$$f = 1 / T \quad \text{frequency}$$

$$k = 2\pi / \lambda \quad \text{wave number}$$



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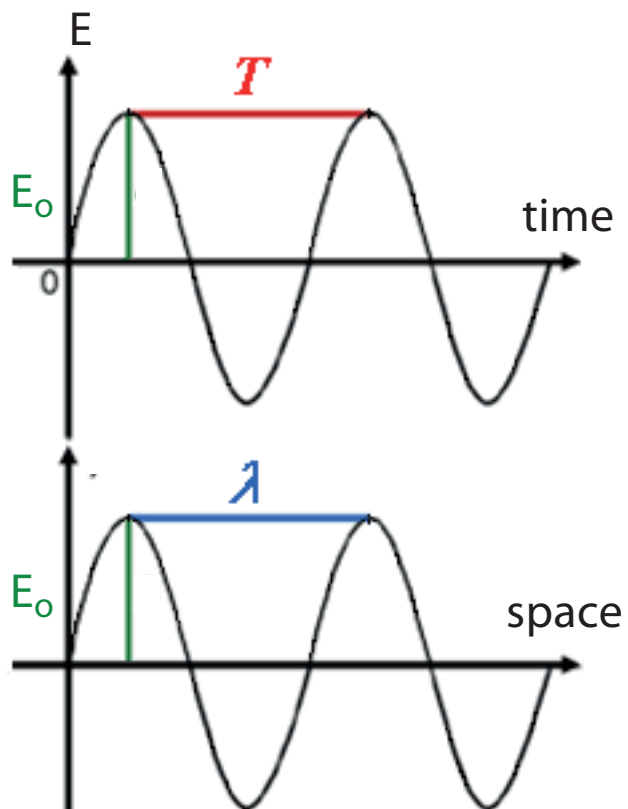
which is a solution to the wave equation:

$$\frac{\partial^2 E}{\partial x^2} = \frac{1}{c^2} \frac{\partial^2 E}{\partial t^2}$$

$c$  = speed of light in vacuum

$$c = f \cdot \lambda = \omega / k$$

$$I = \text{Intensity} = (c \cdot \epsilon_0 \cdot n / 2) \cdot |E|^2$$



# Nature of Light

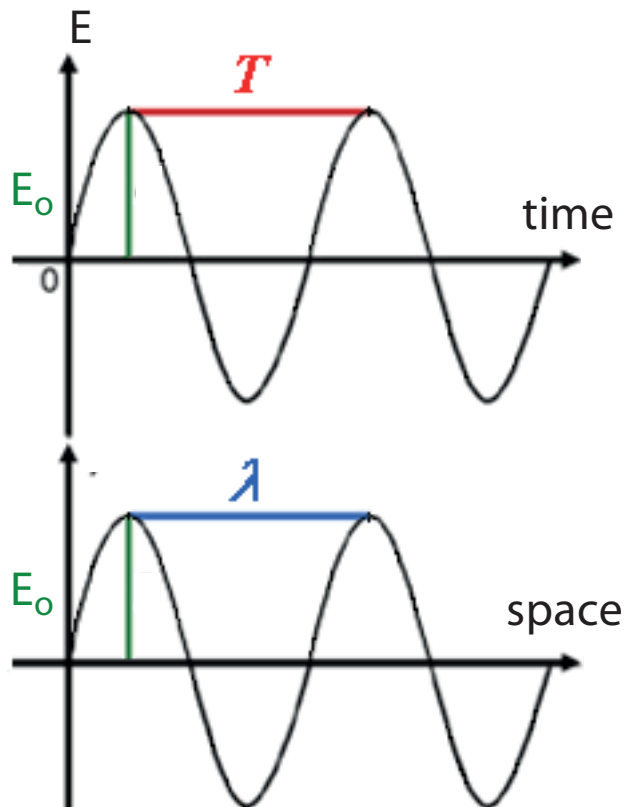
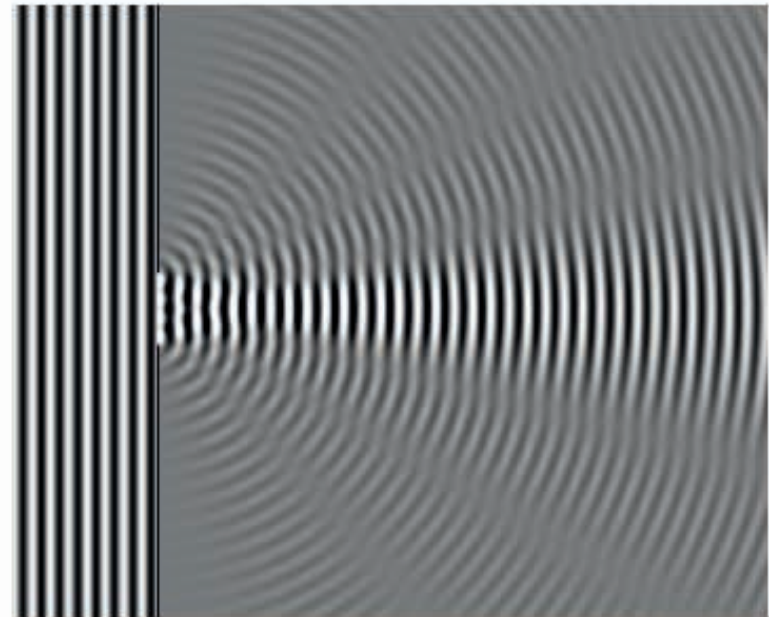
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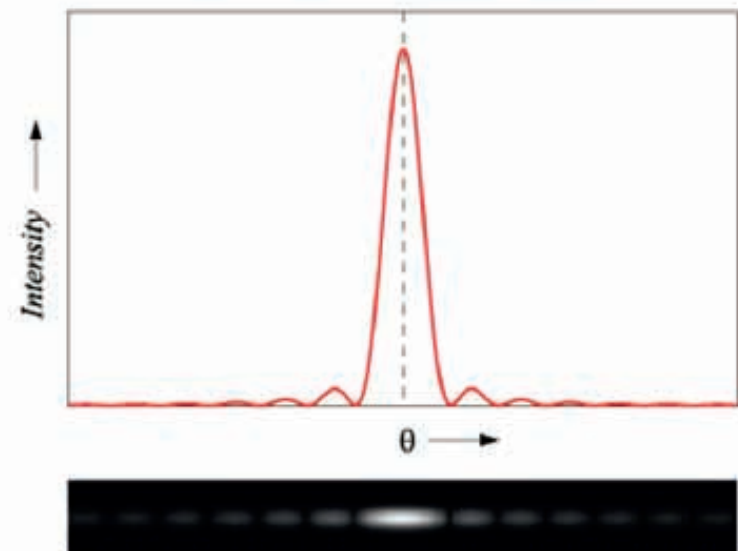
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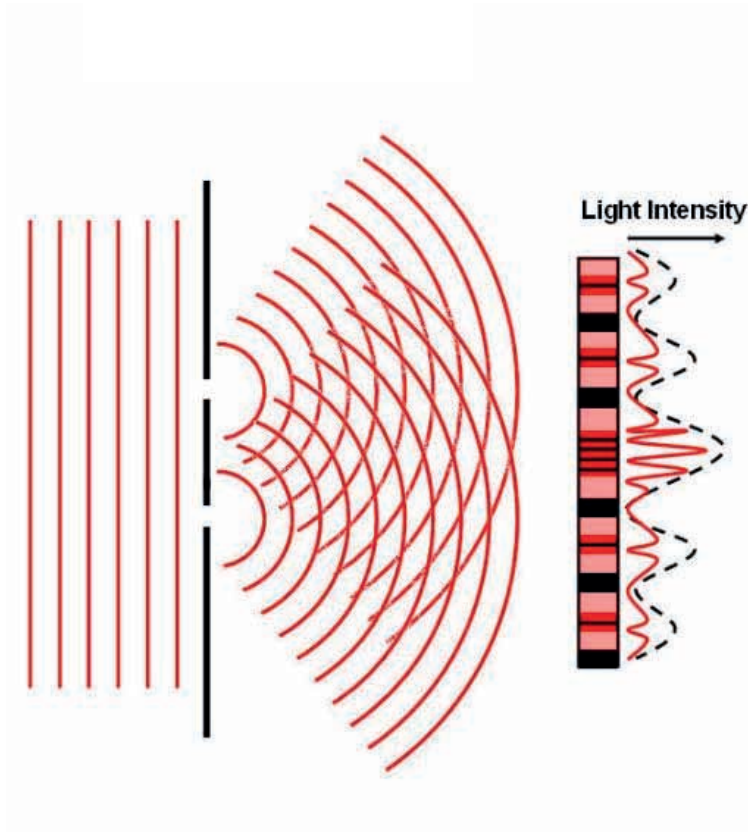


*Single-slit diffraction pattern*

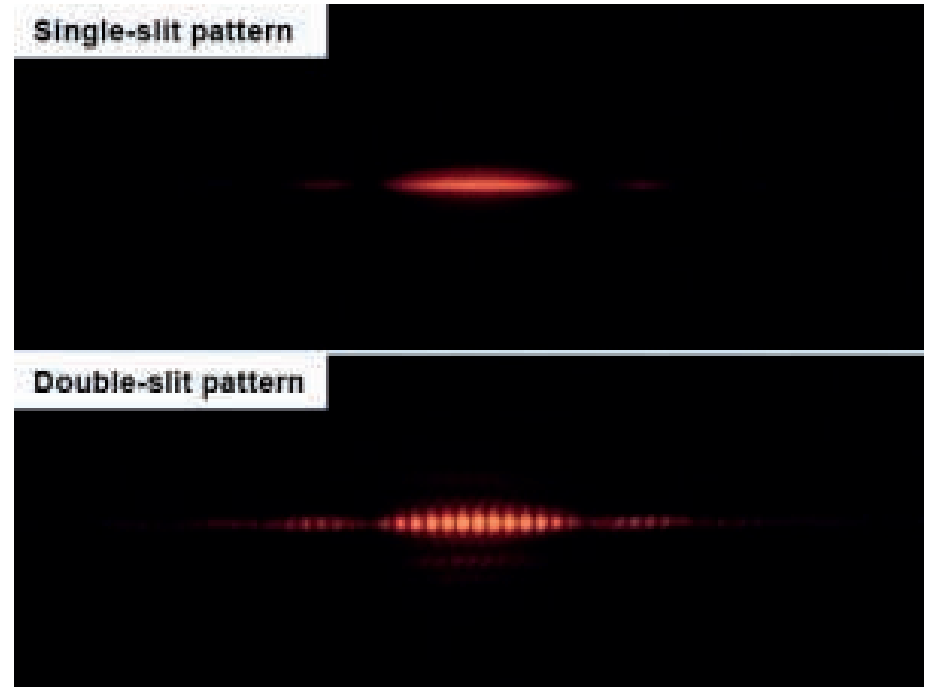


# Nature of Light

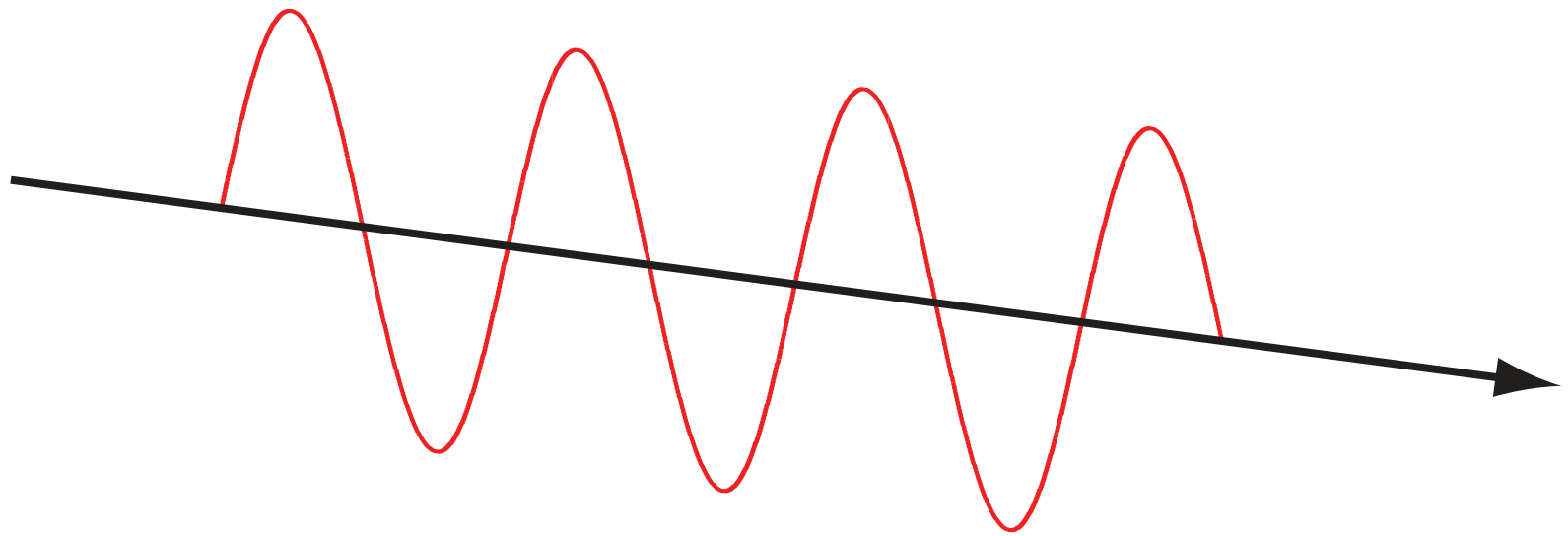
Light can be described as an traveling electromagnetic wave



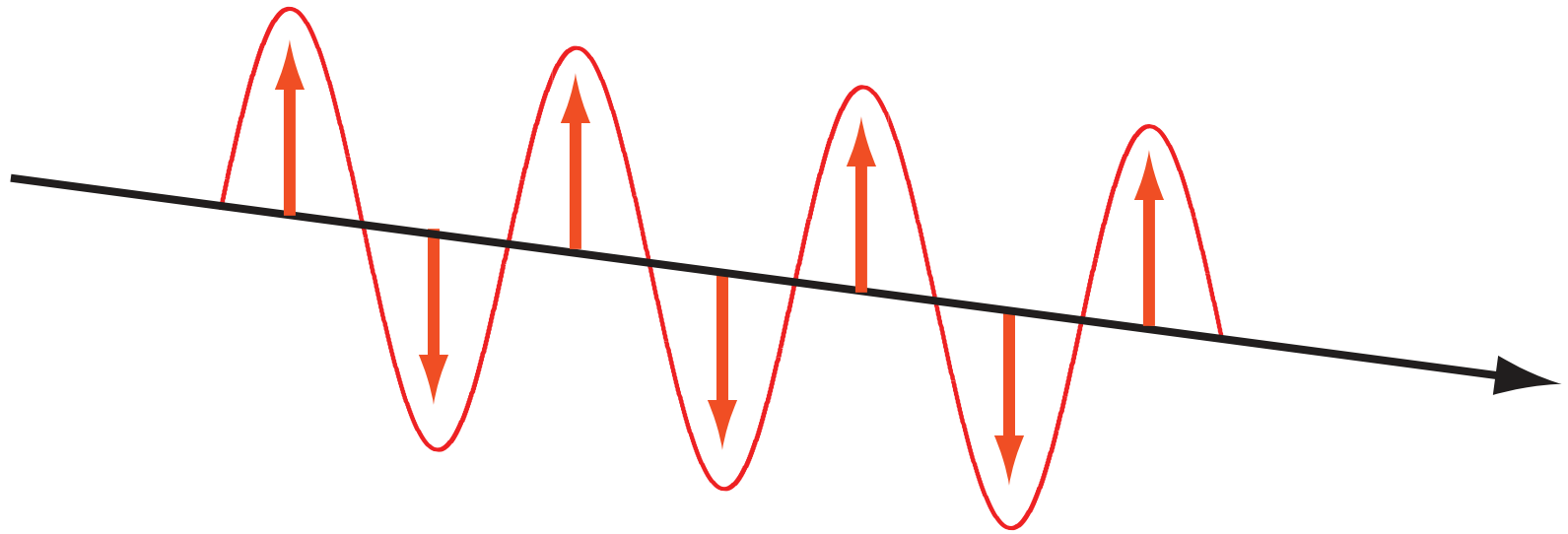
Double Slit  
Diffraction Experiment



# Linearly Polarized Light

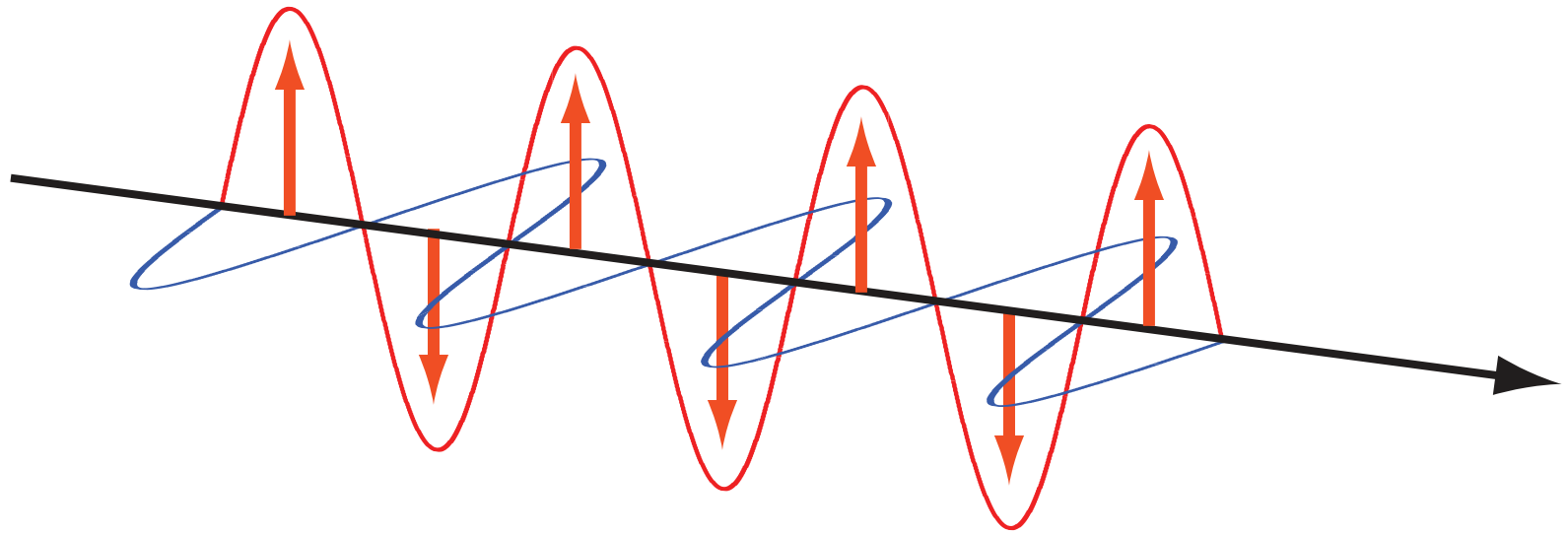


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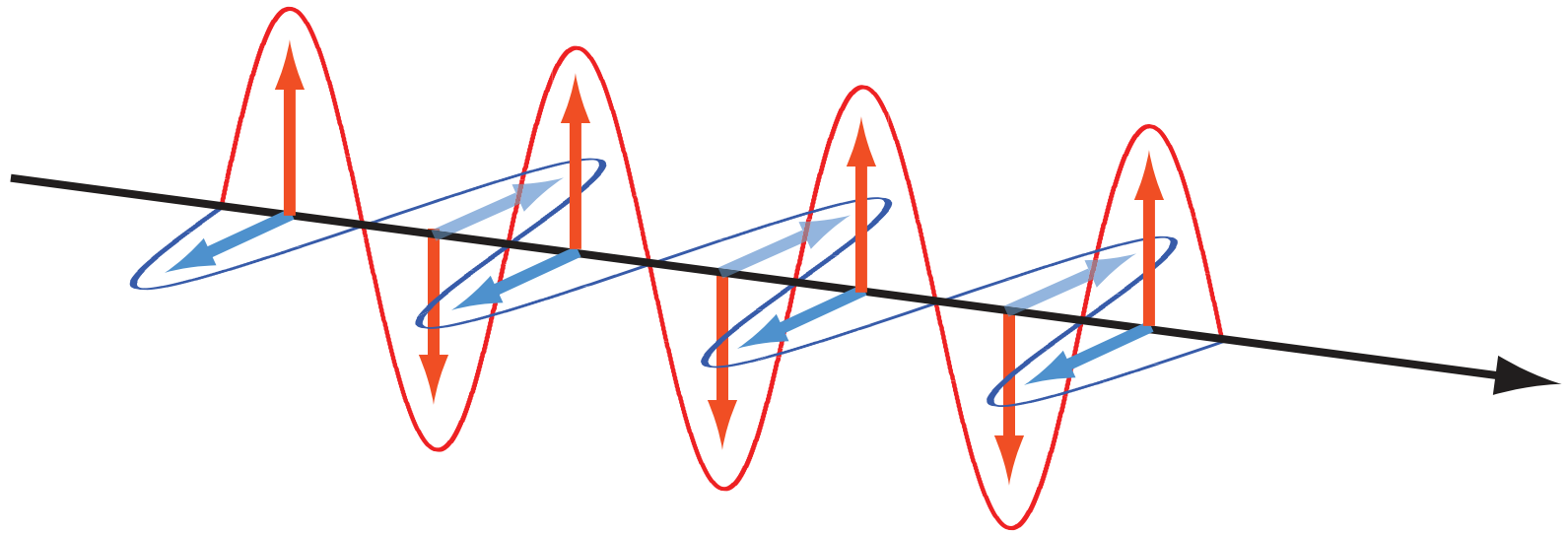




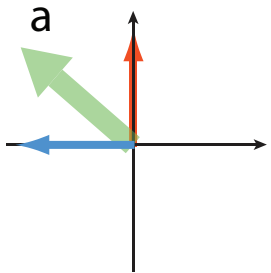
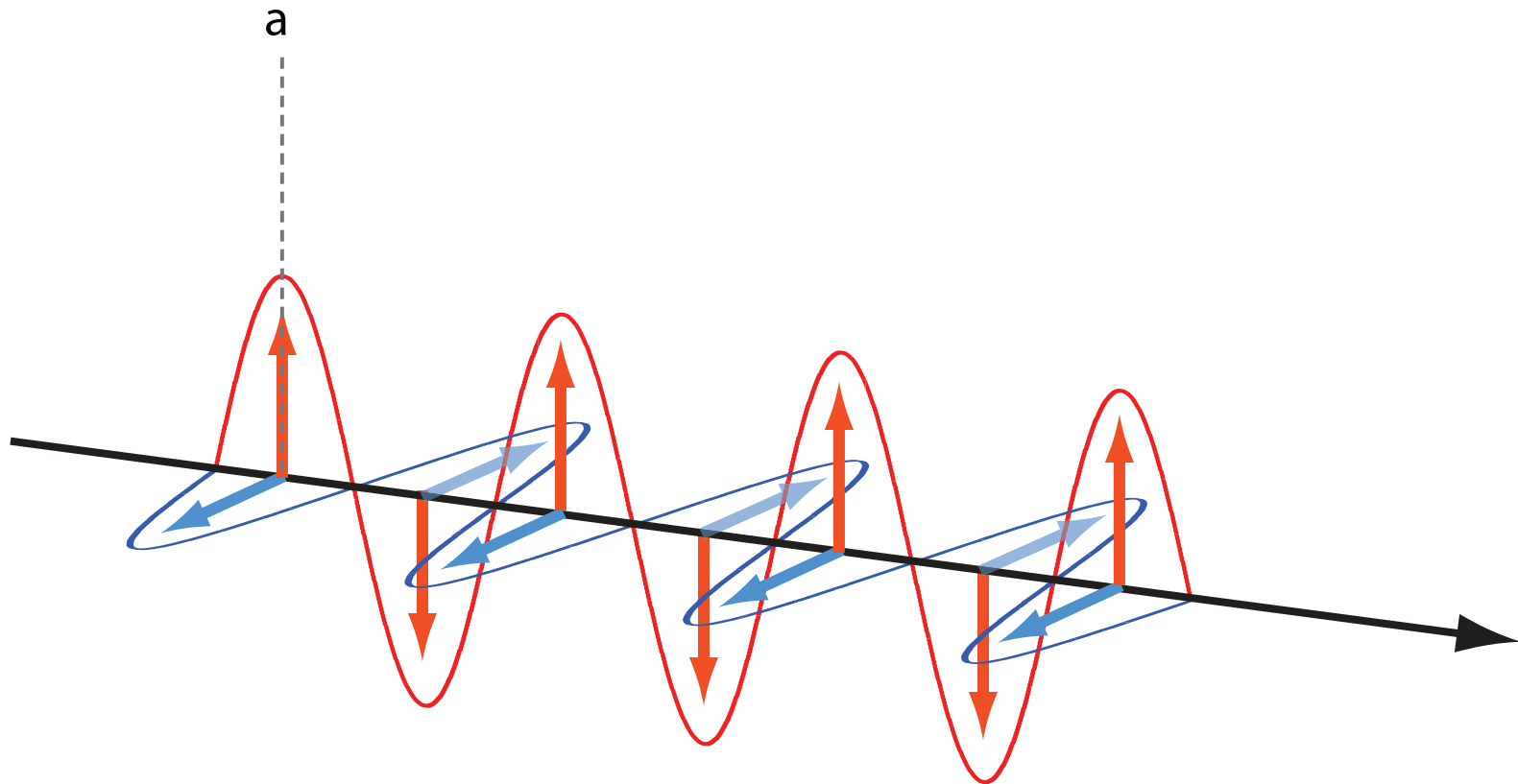
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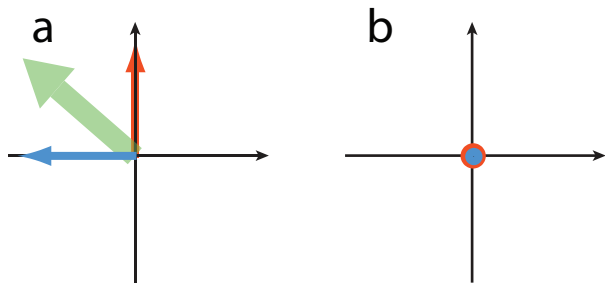
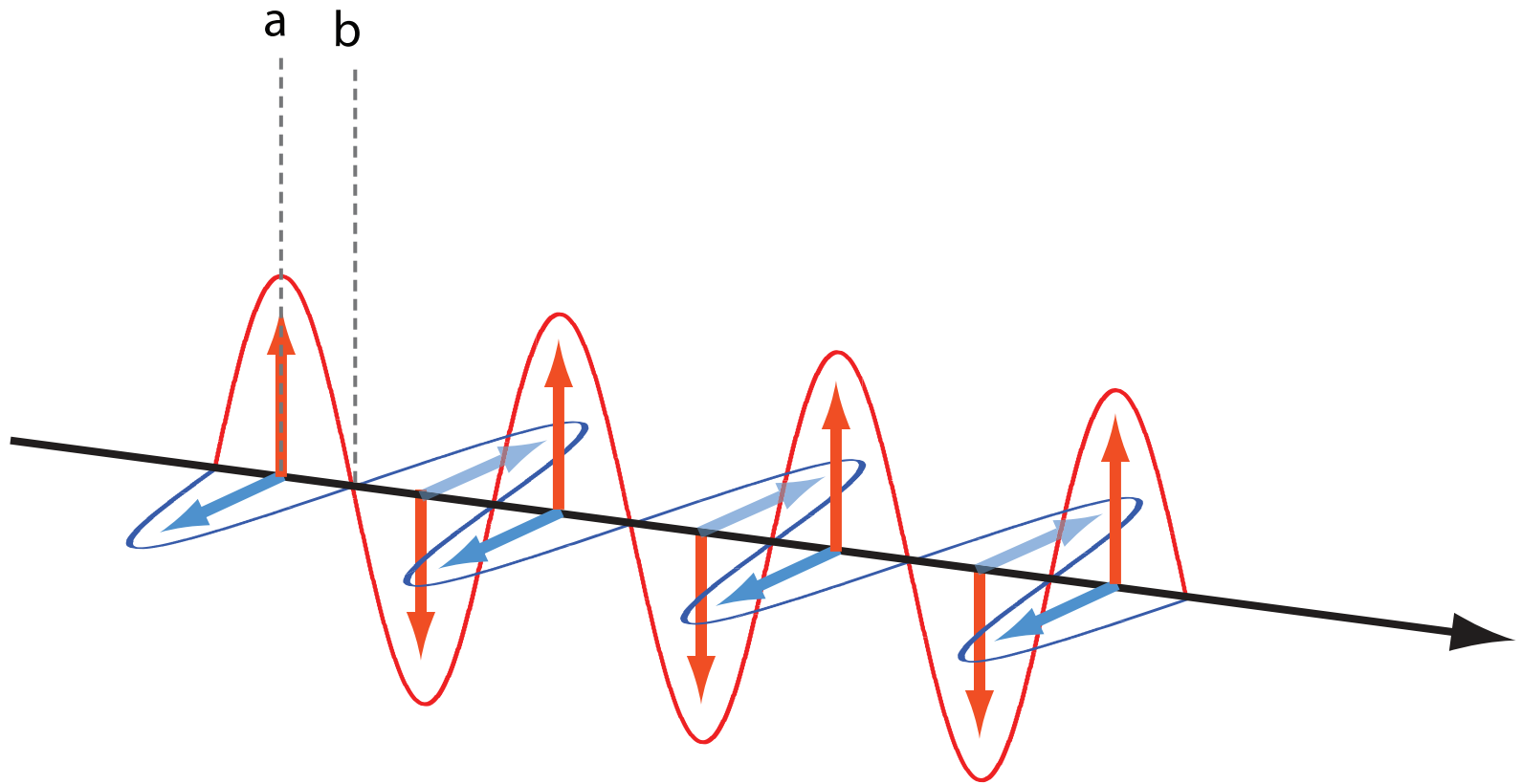
# Linearly Polarized Light



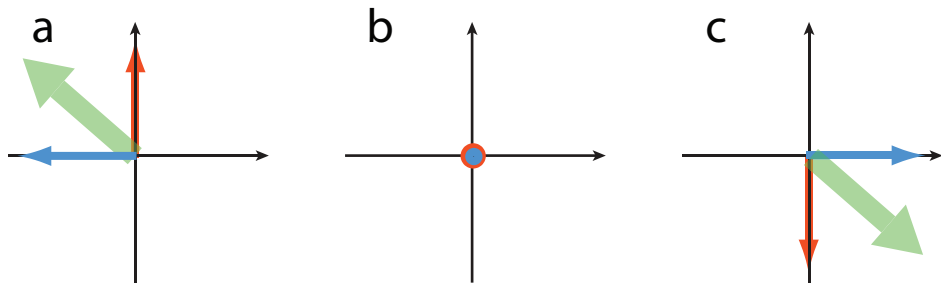
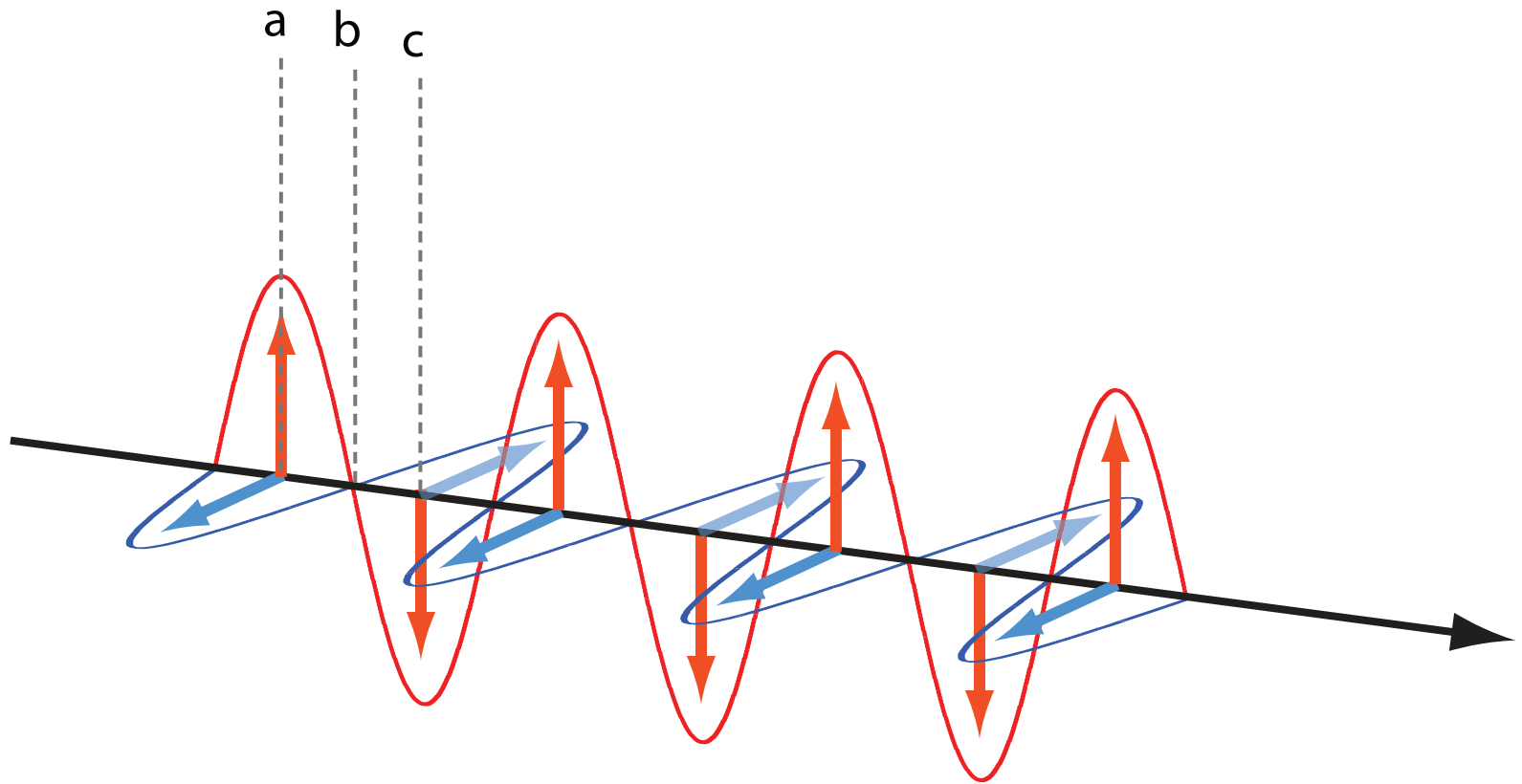
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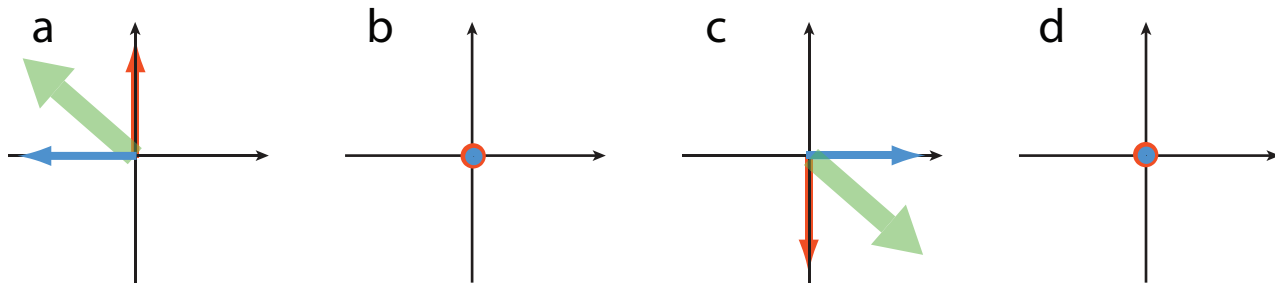
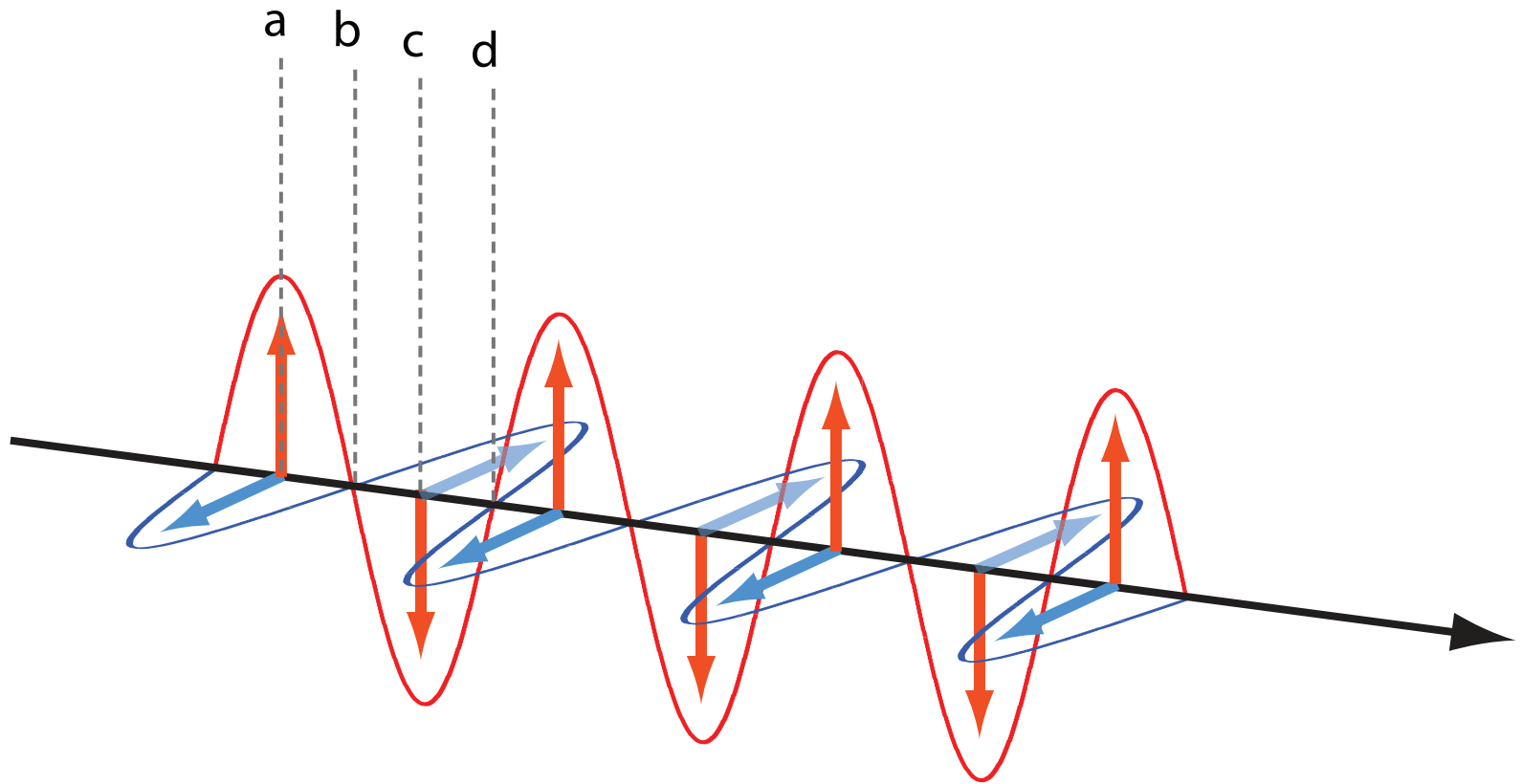
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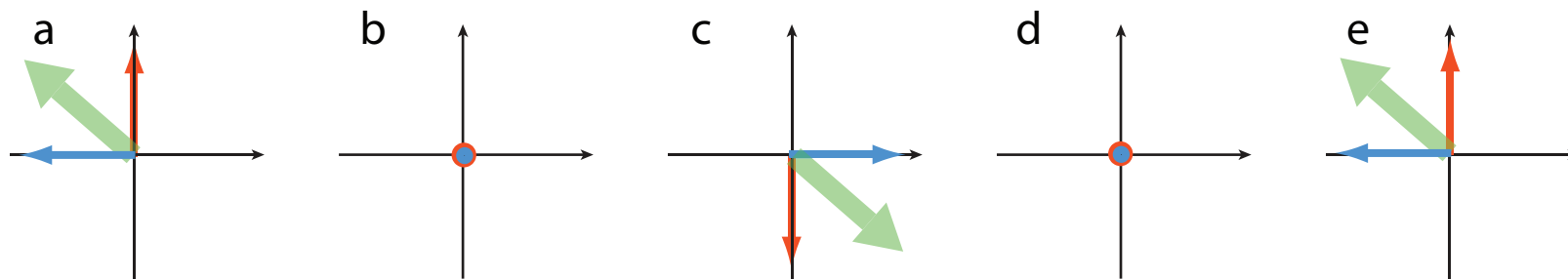
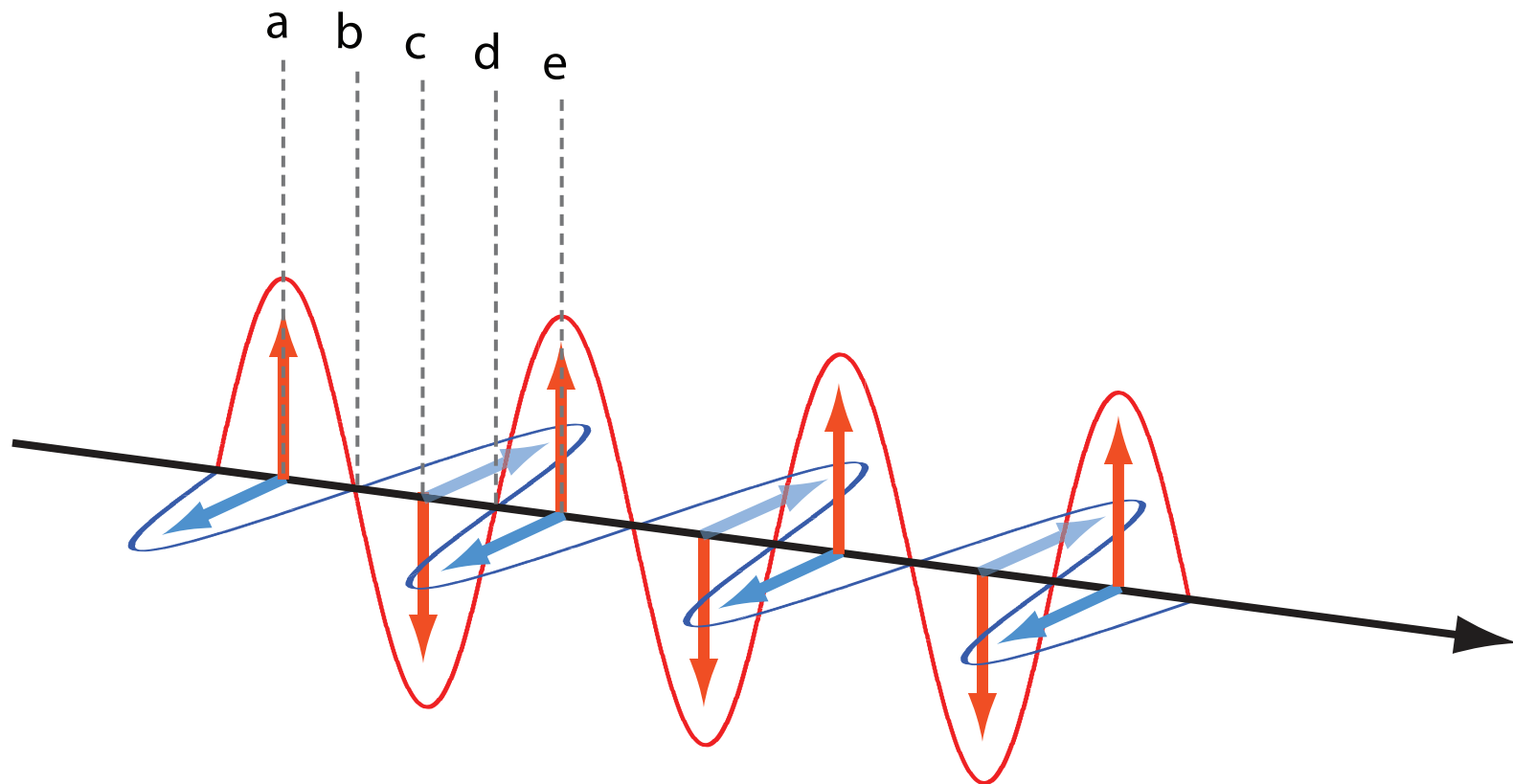
# Linearly Polarized Light



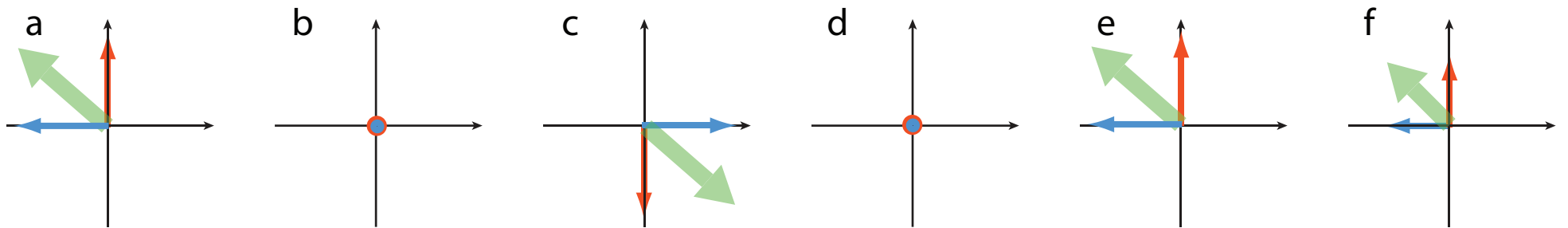
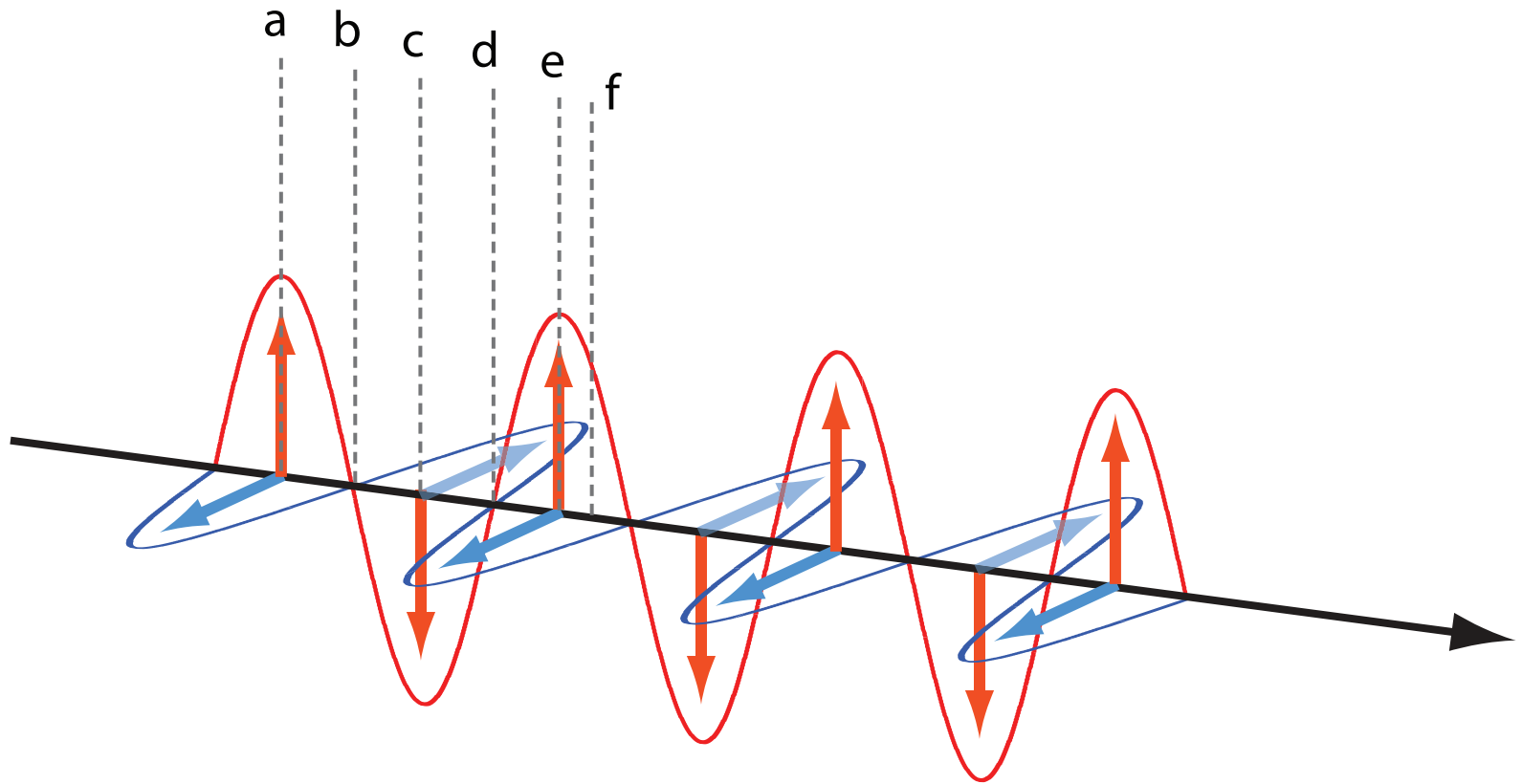
# Linearly Polarized Light



# Linearly Polarized Light

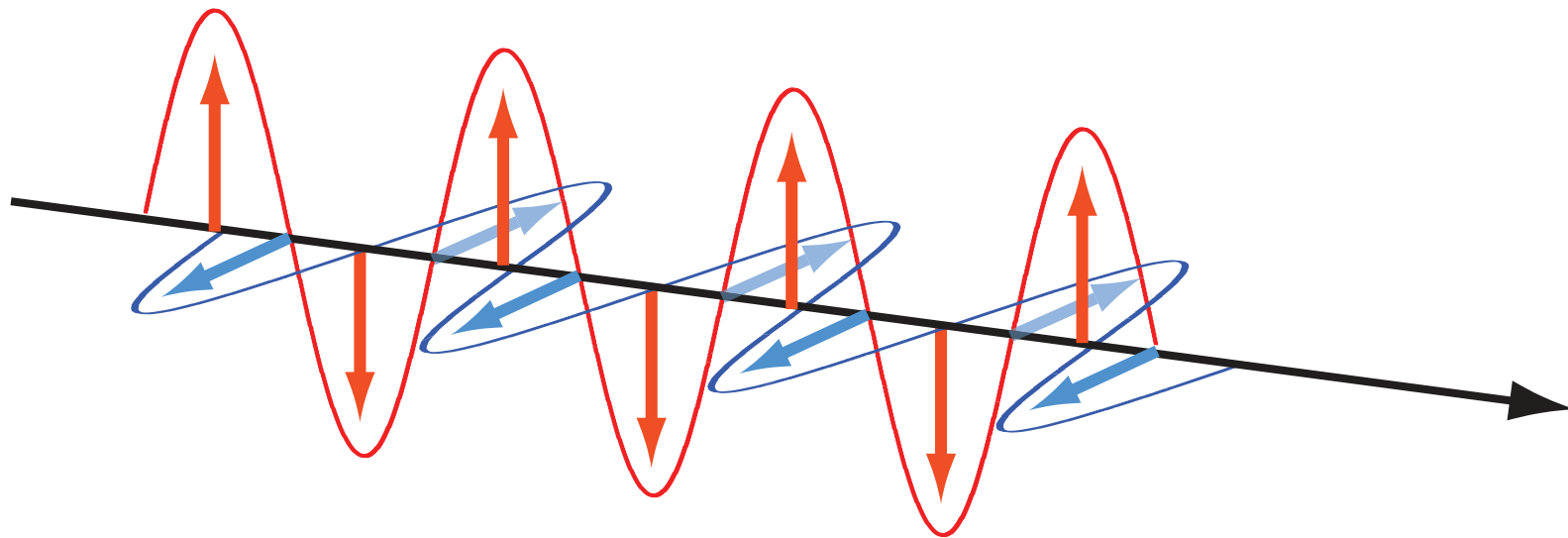


# Linearly Polarized Light

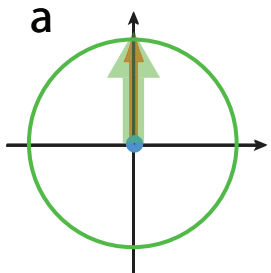
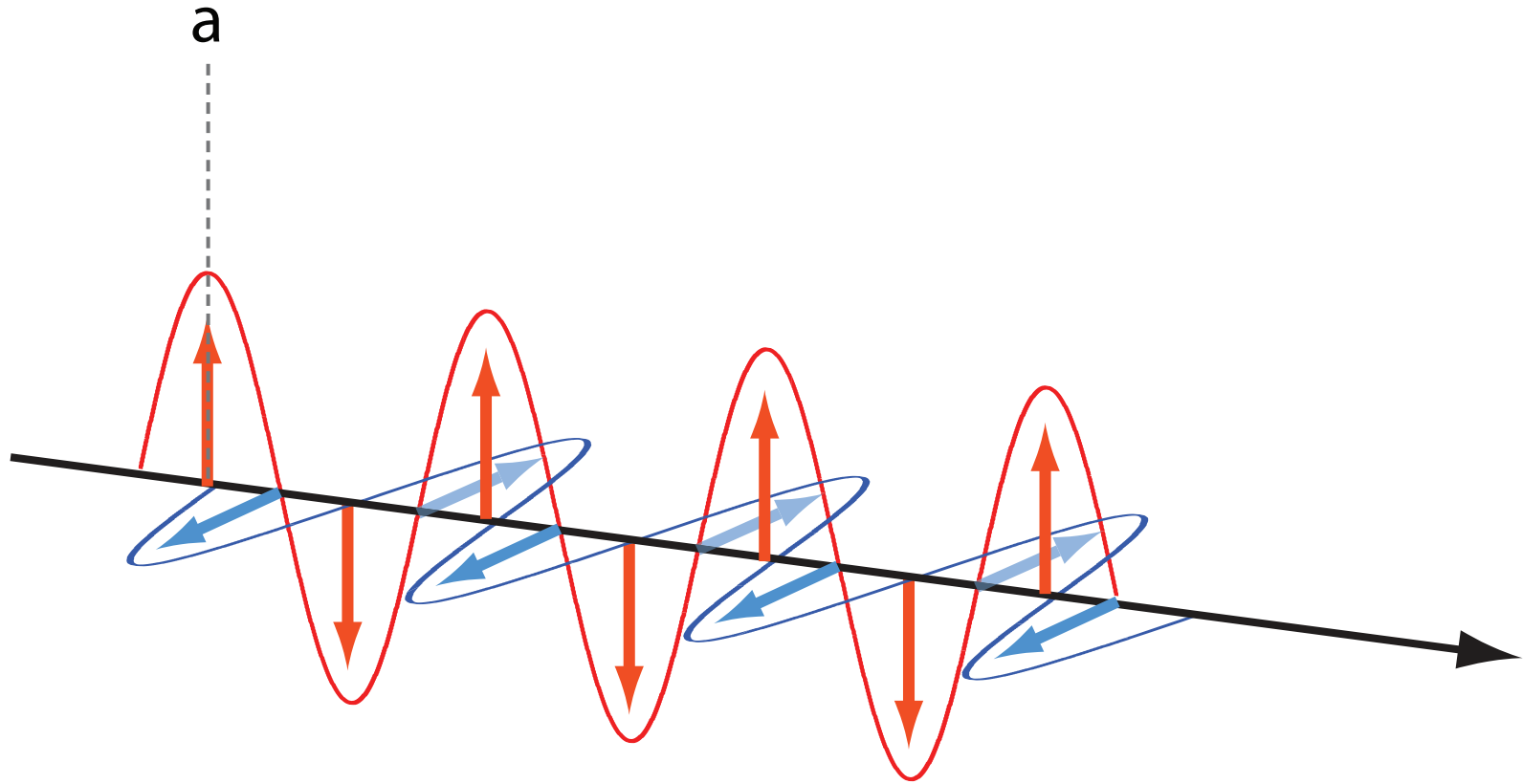




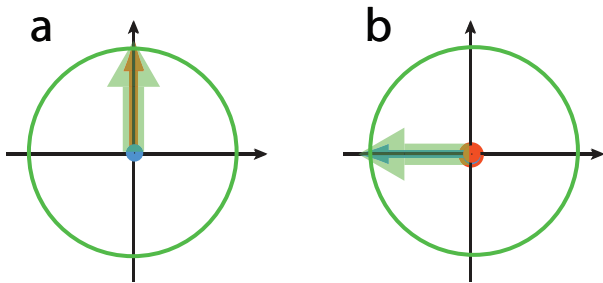
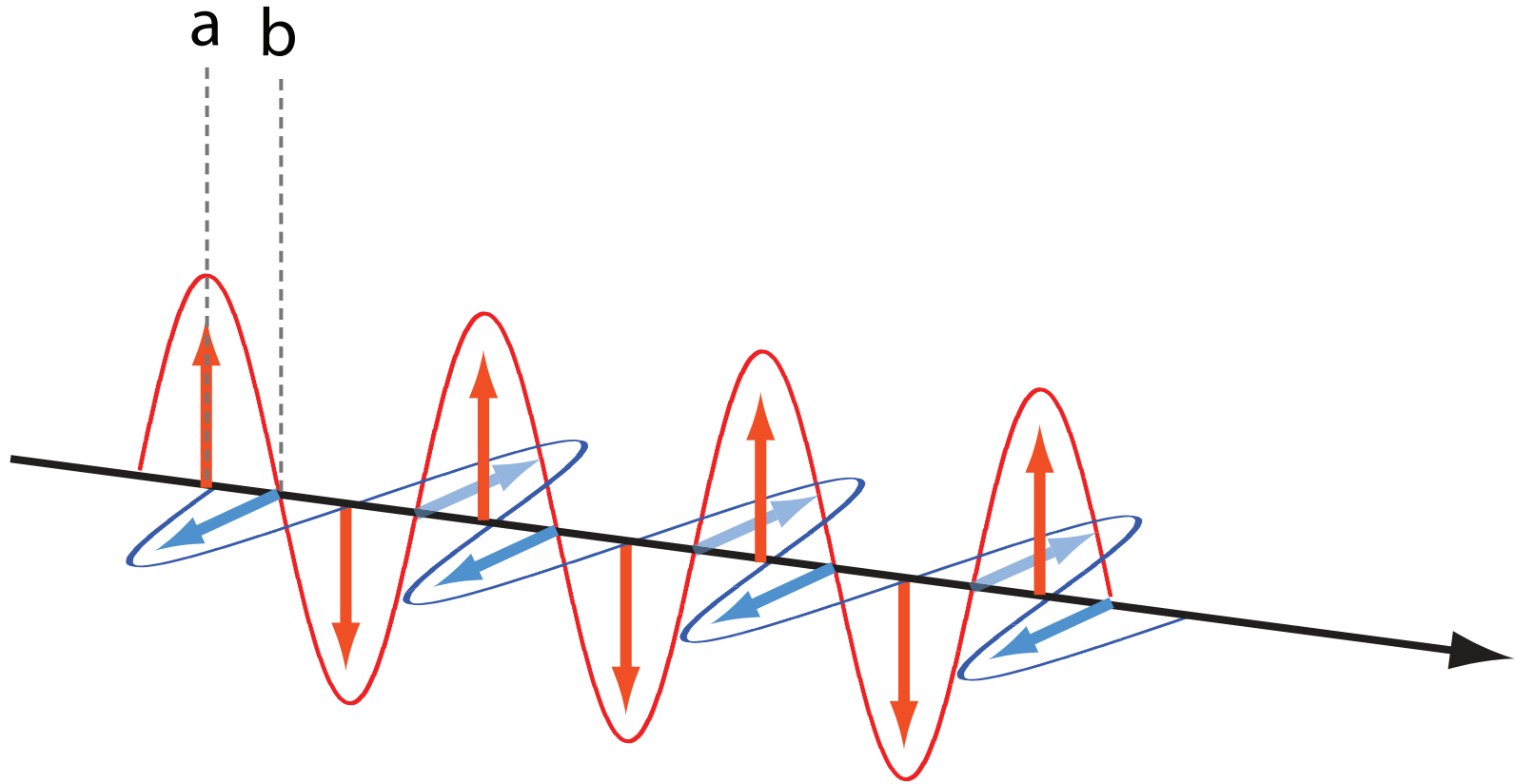
# Circularly Polarized Light



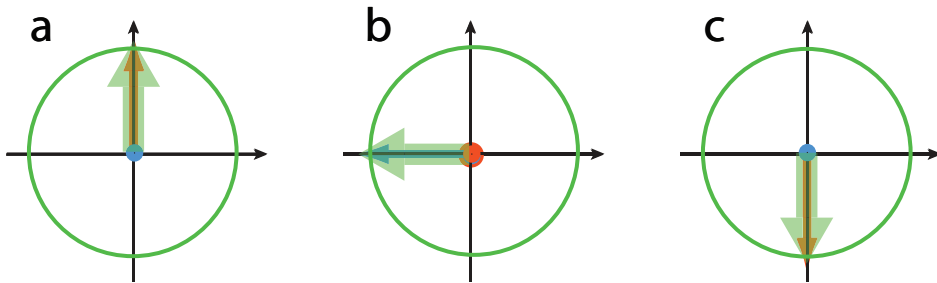
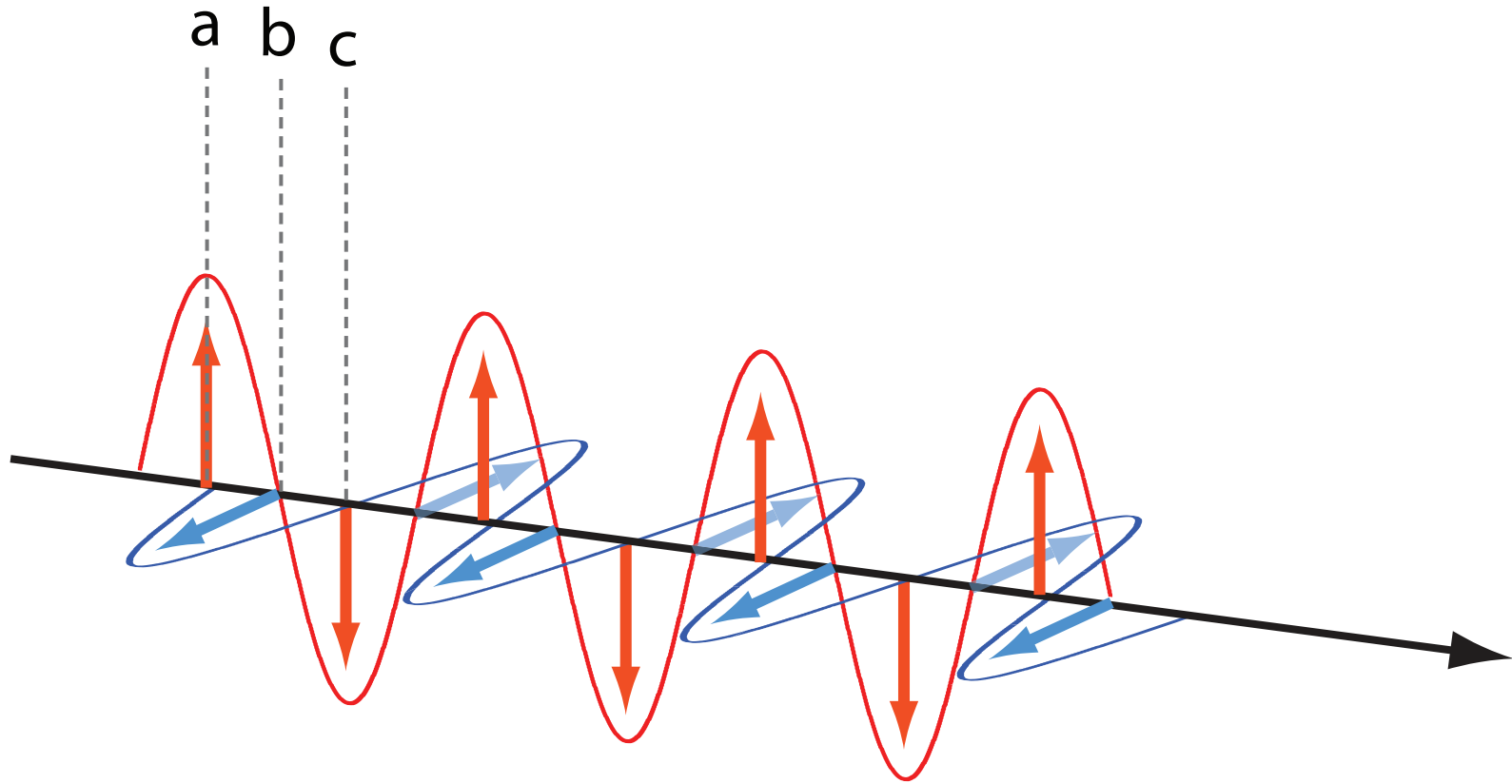
# Circularly Polarized Light



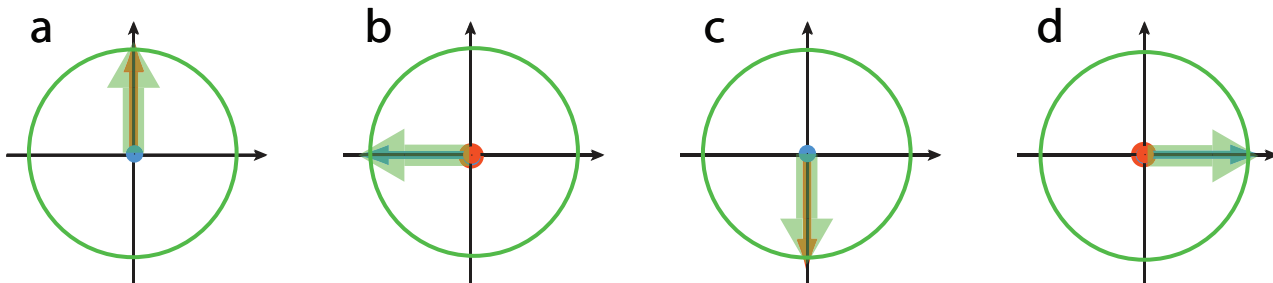
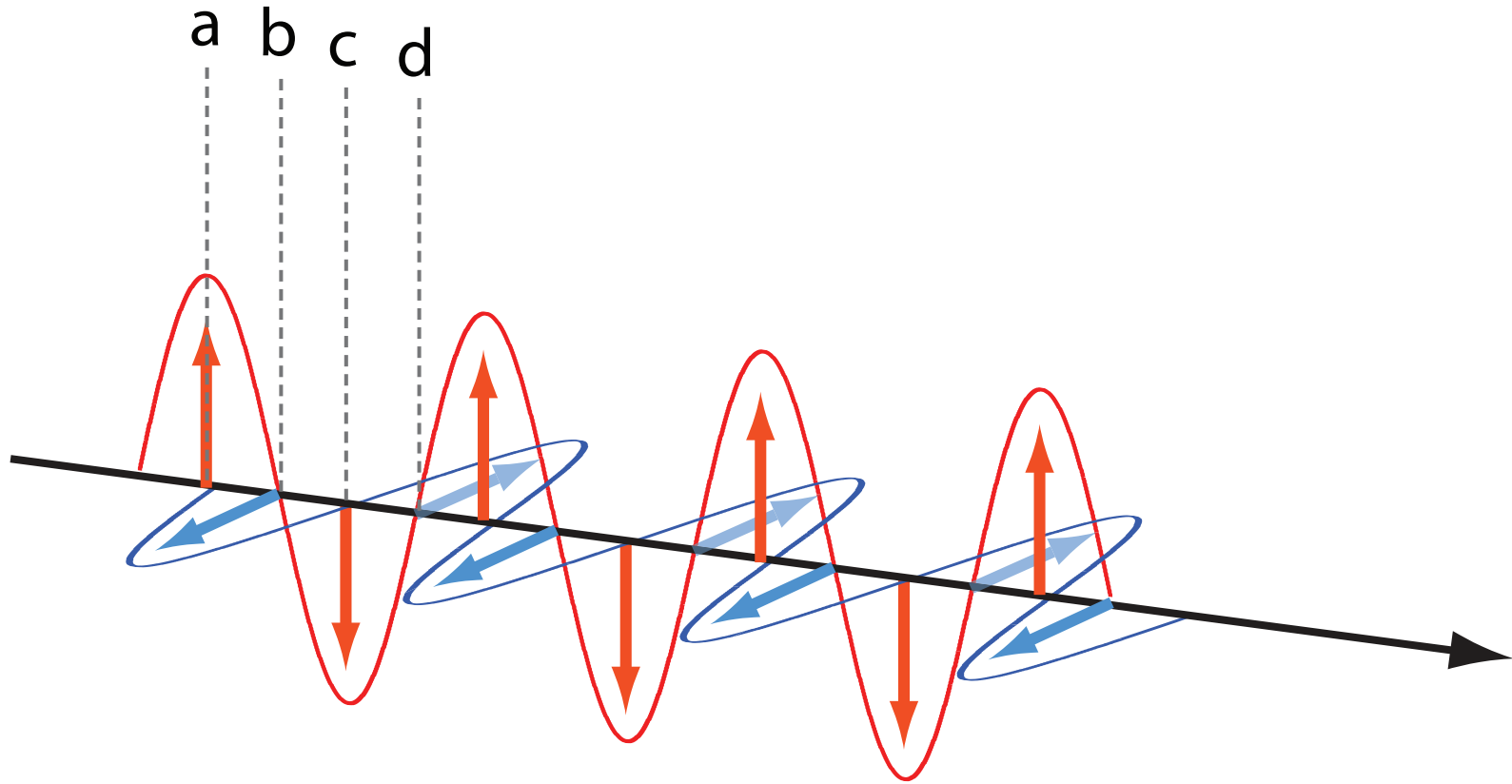
# Circularly Polarized Light



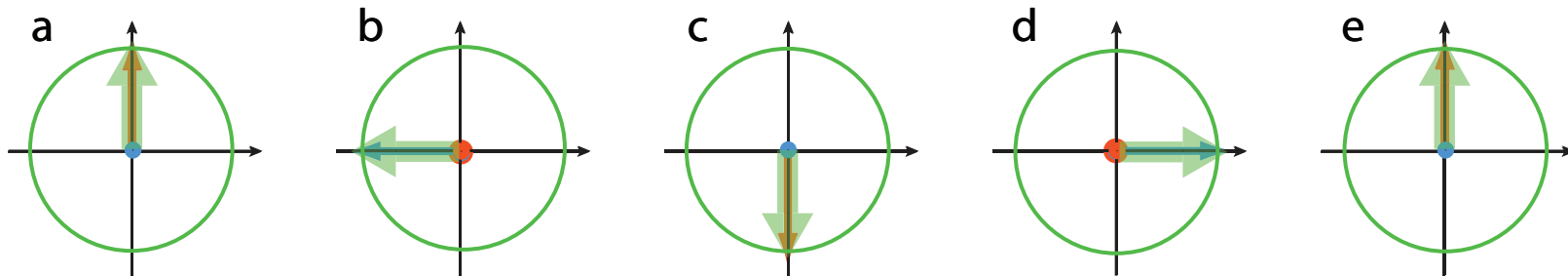
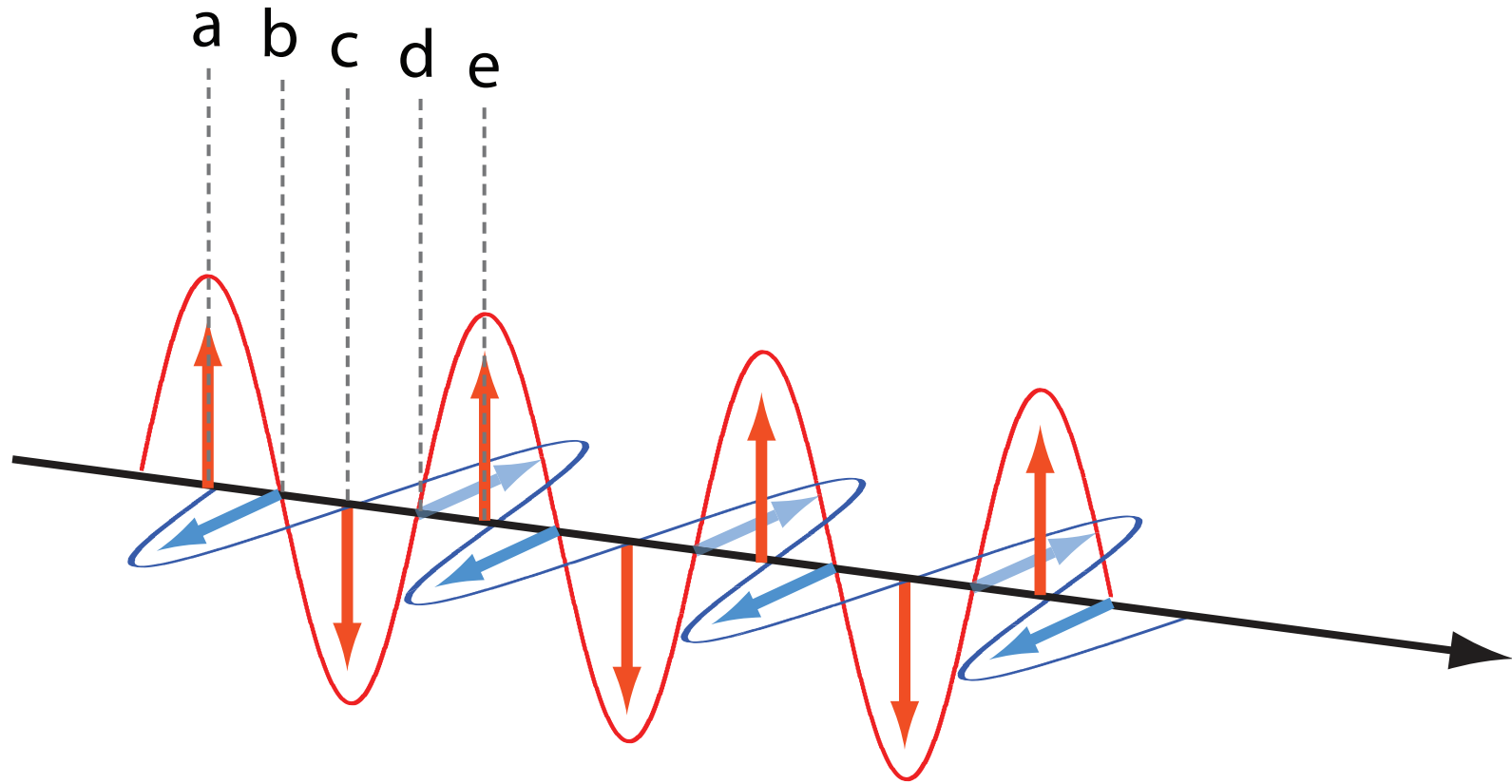
# Circularly Polarized Light



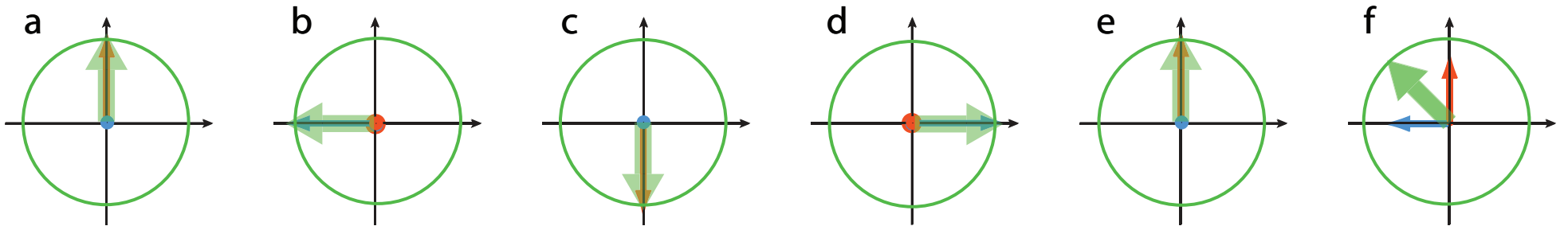
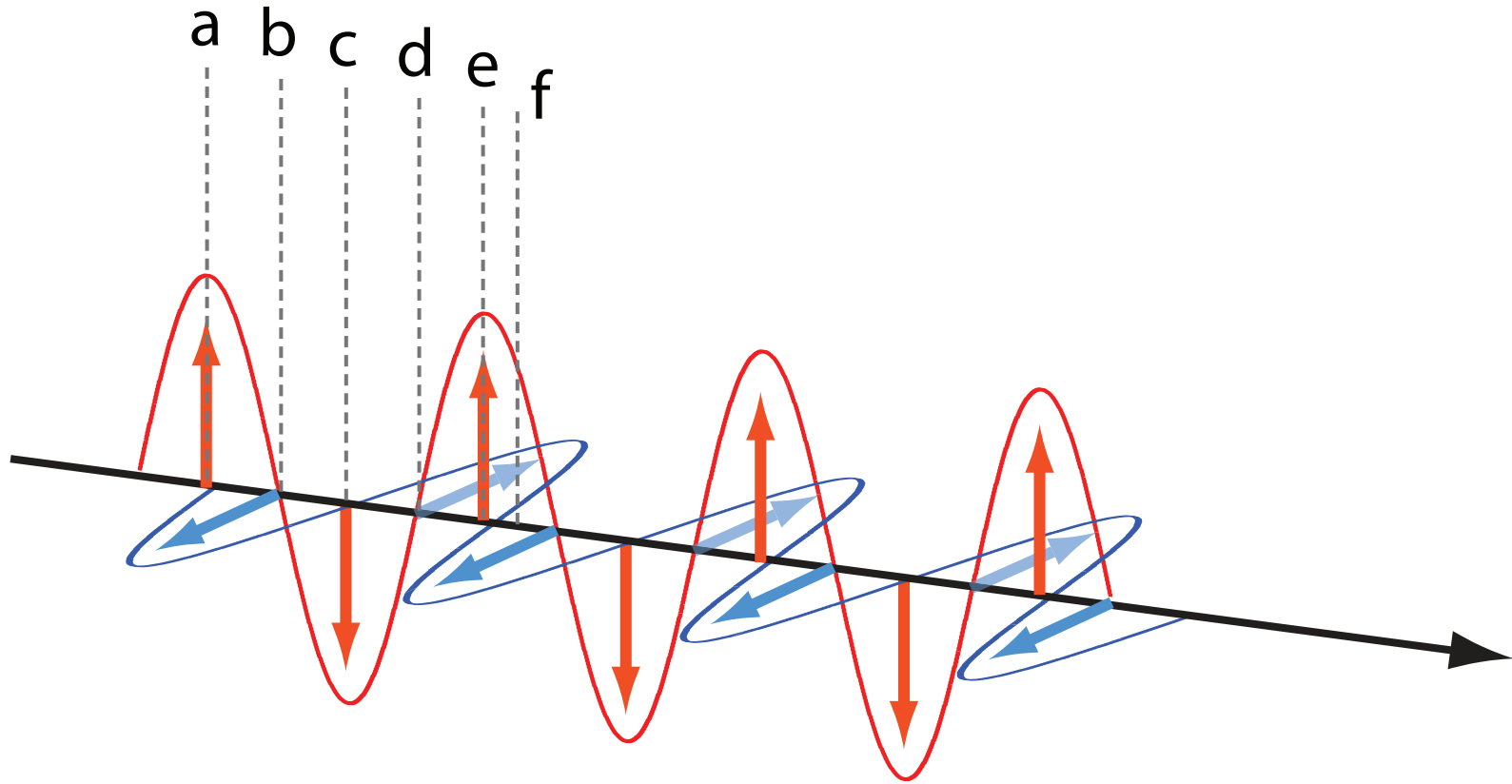
# Circularly Polarized Light



# Circularly Polarized Light

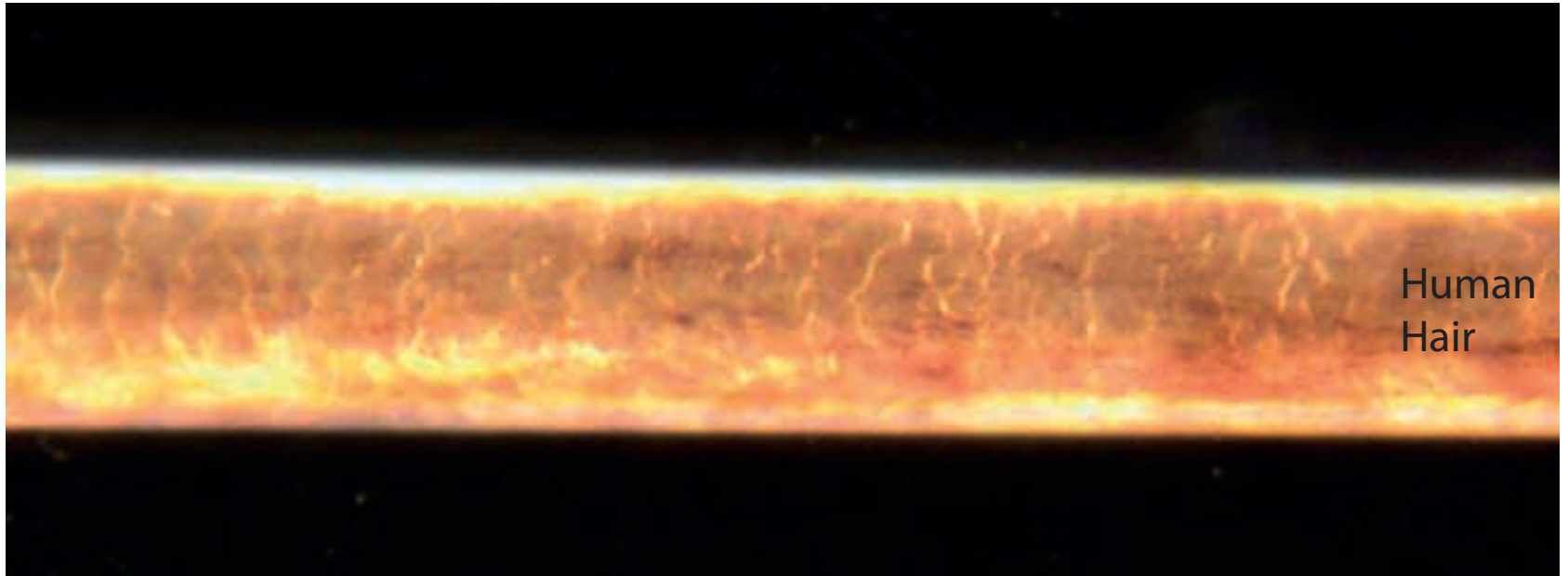


# Circularly Polarized Light

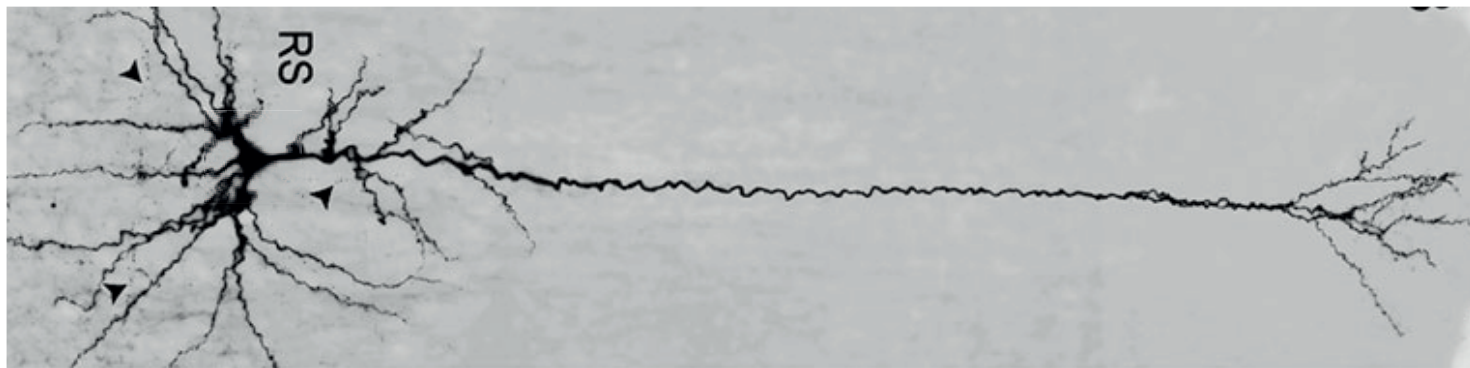


# Sense of Scale

100  $\mu\text{m}$



20  $\mu\text{m}$

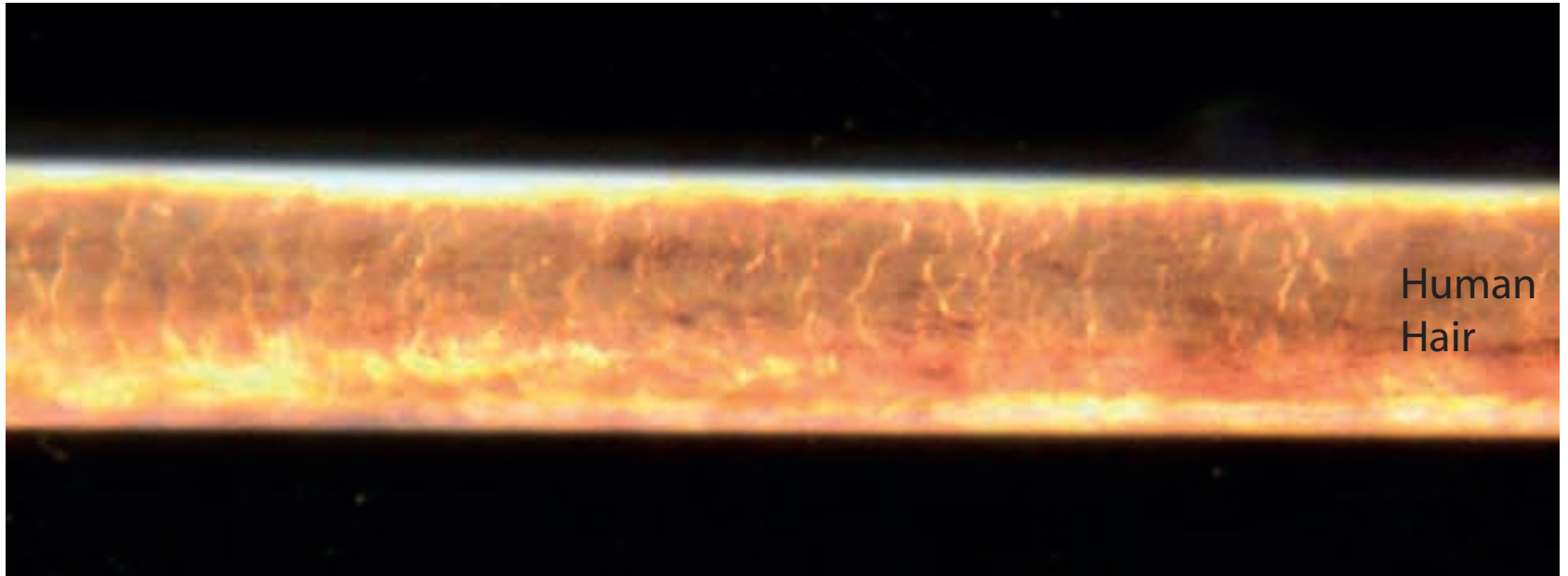


7  $\mu\text{m}$  ■ ● Red Blood Cell

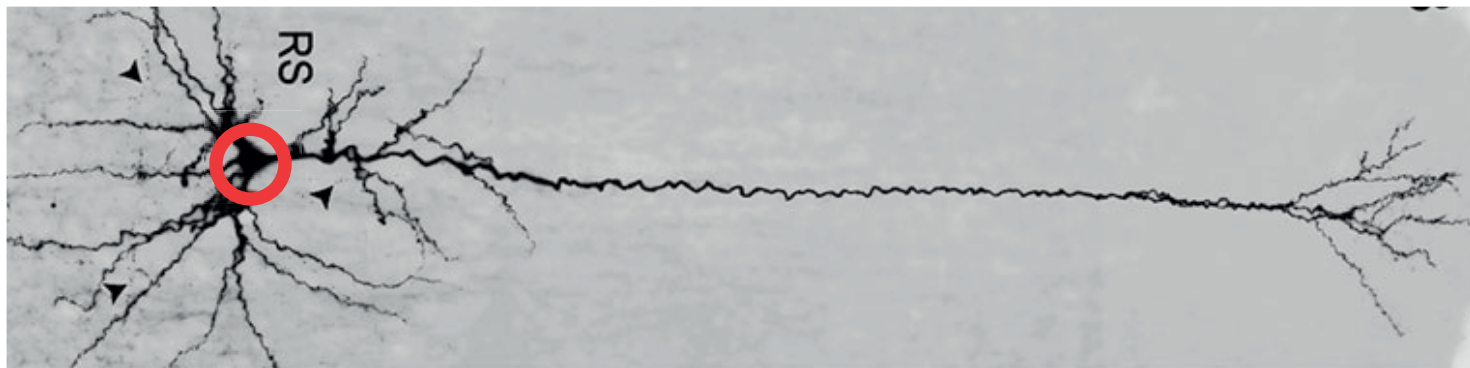


# Sense of Scale

100  $\mu\text{m}$



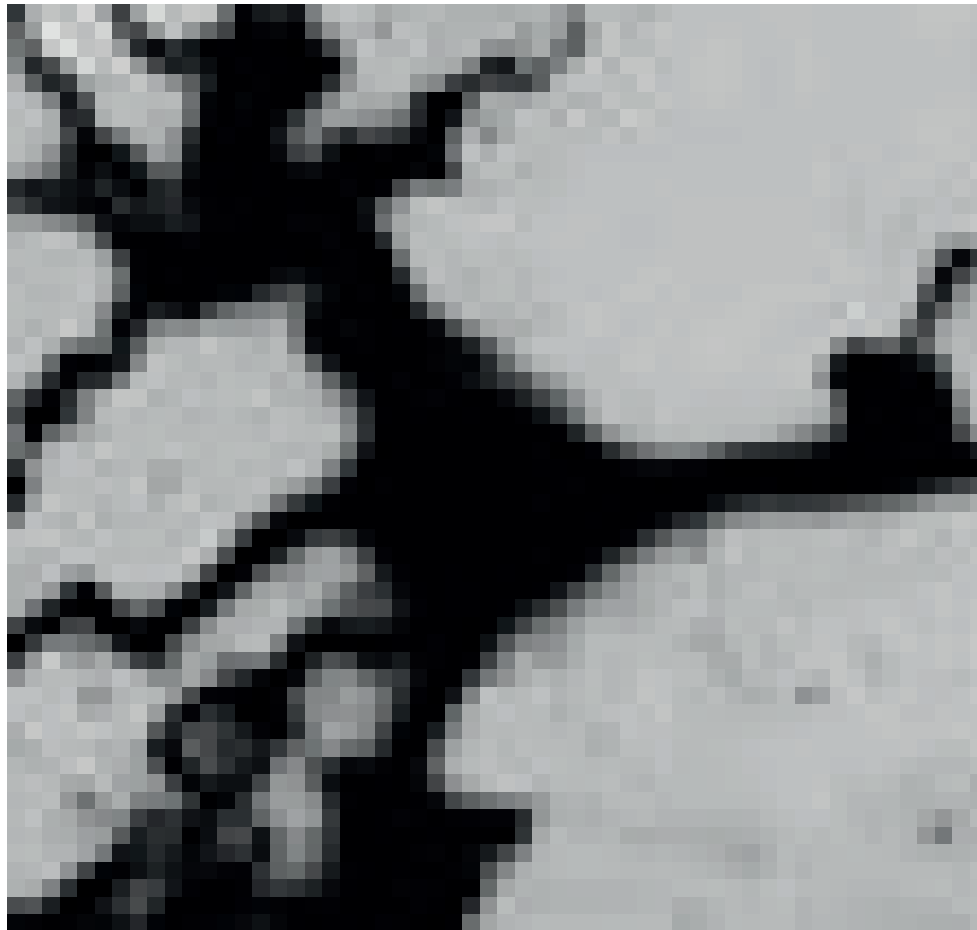
20  $\mu\text{m}$



7  $\mu\text{m}$  ■ ● Red Blood Cell

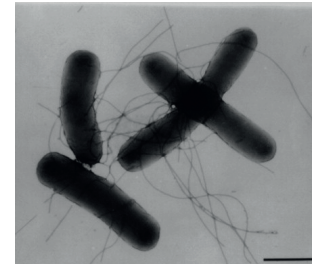
# Sense of Scale

Pyramidal Neuron Cell Body ( $\sim 10 \mu\text{m}$ )

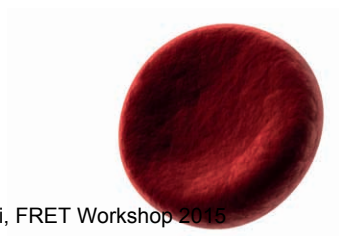
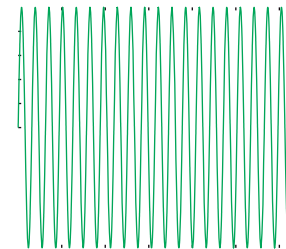


$20 \mu\text{m}$

Bacterium ( $1 \times 5 \mu\text{m}$ )



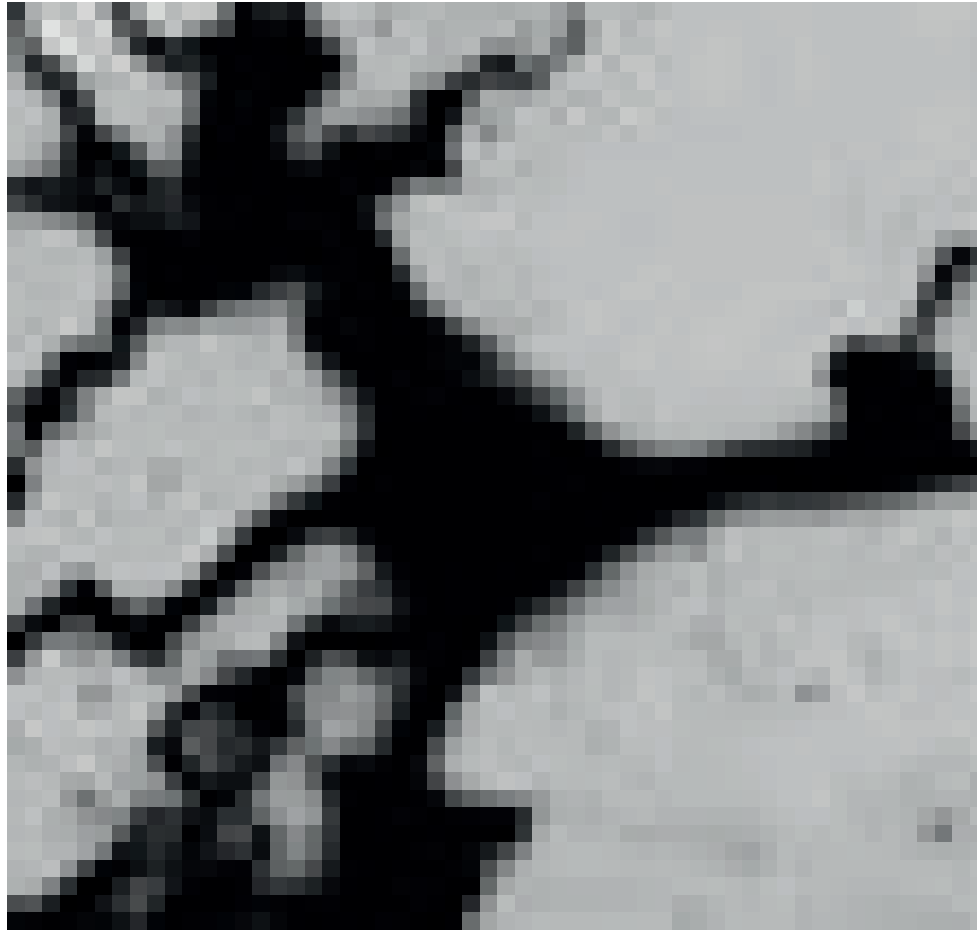
20 cycles of green light  
( $\lambda = 0.5 \mu\text{m}$ )



Red Blood Cell ( $7 \mu\text{m}$ )

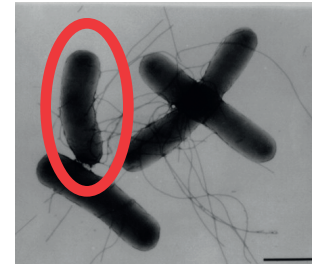
# Sense of Scale

Pyramidal Neuron Cell Body ( $\sim 10 \mu\text{m}$ )

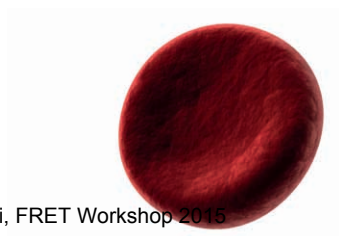
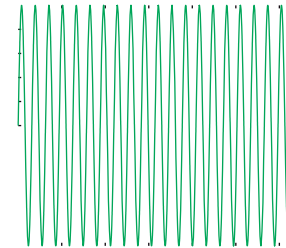


$20 \mu\text{m}$

Bacterium ( $1 \times 5 \mu\text{m}$ )

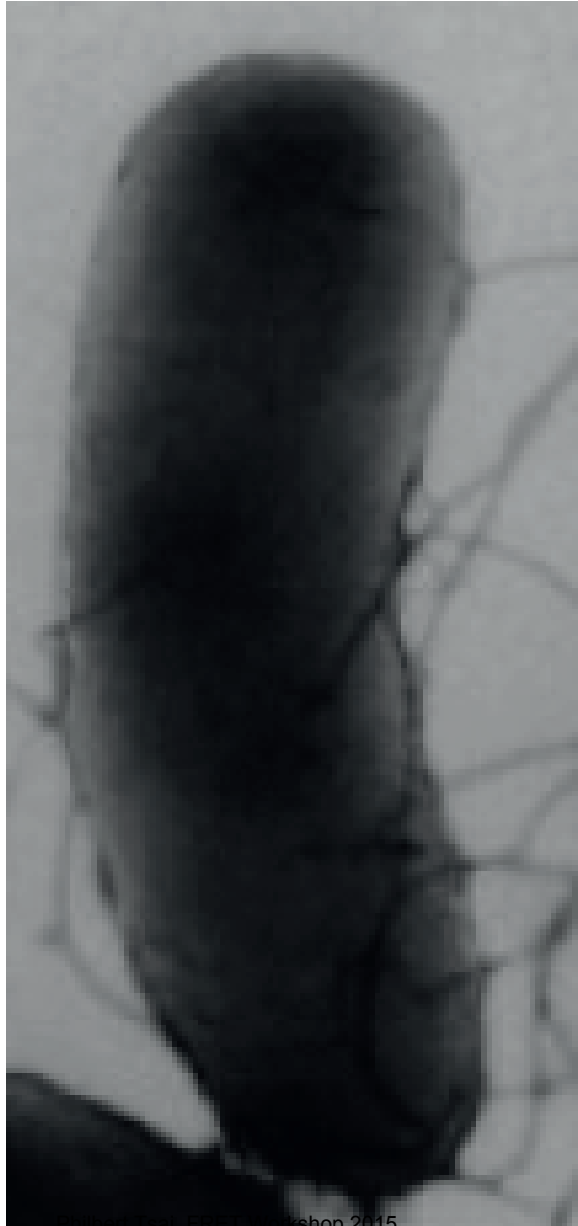


20 cycles of green light  
( $\lambda = 0.5 \mu\text{m}$ )

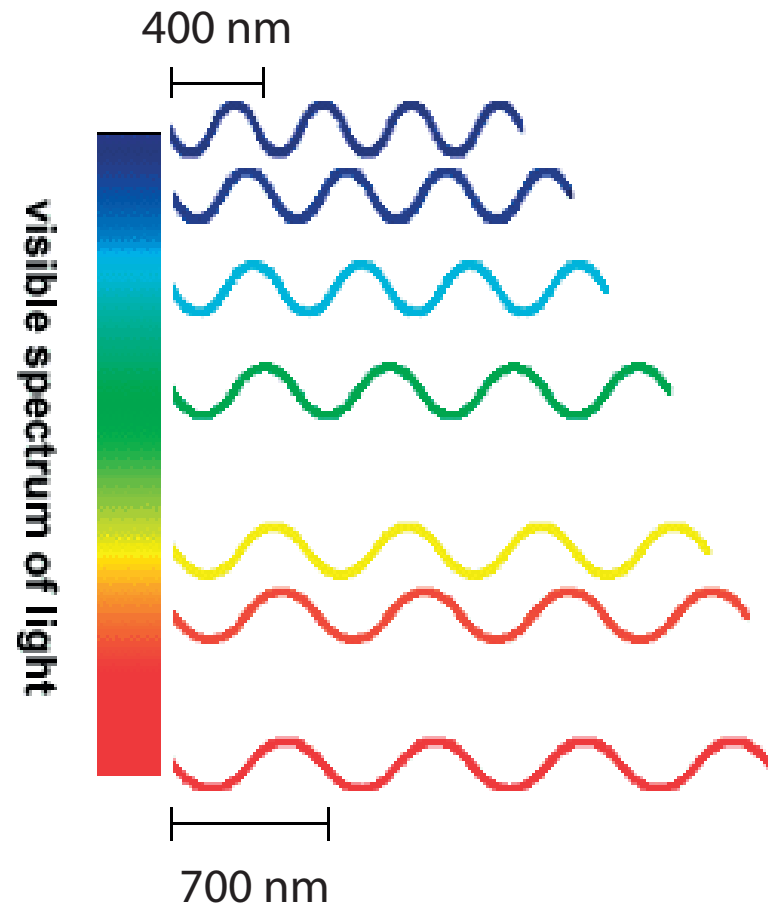


Red Blood Cell ( $7 \mu\text{m}$ )

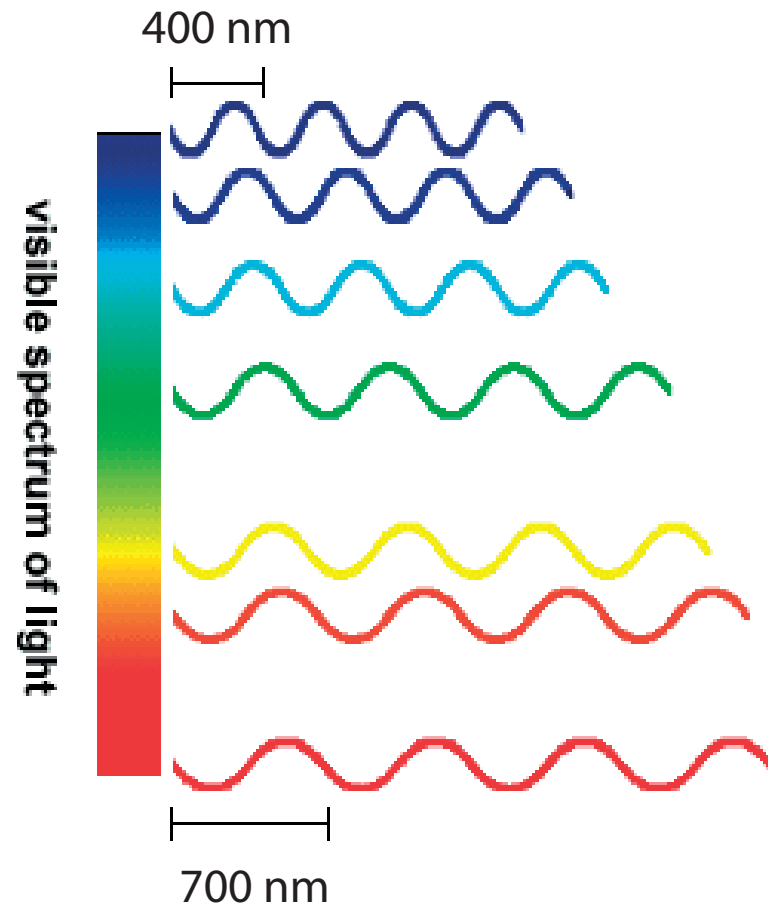
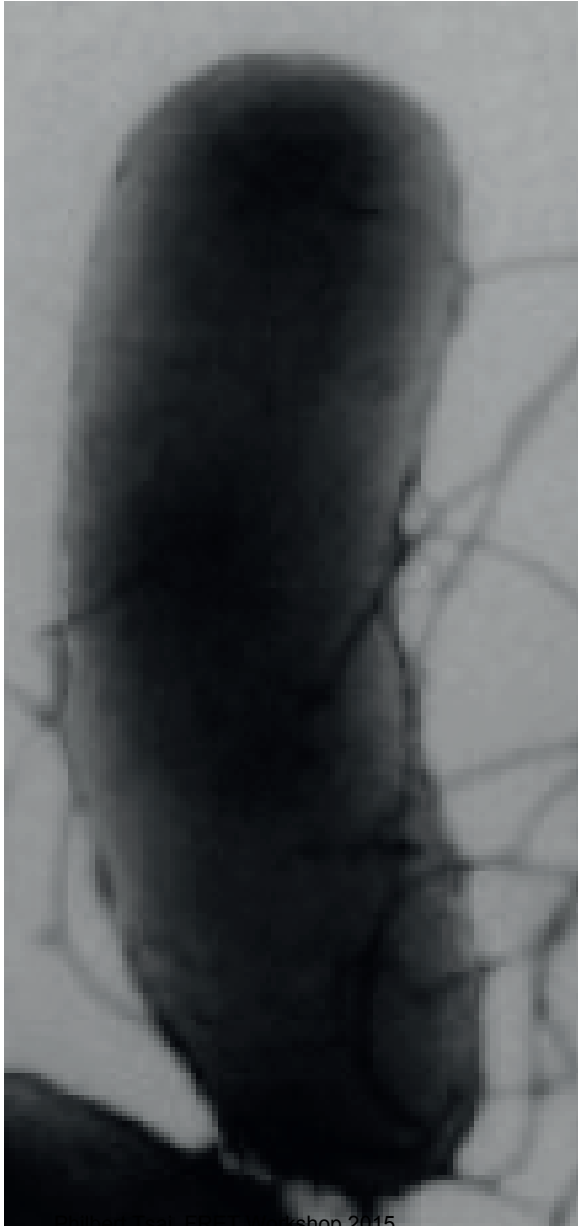
# Sense of Scale



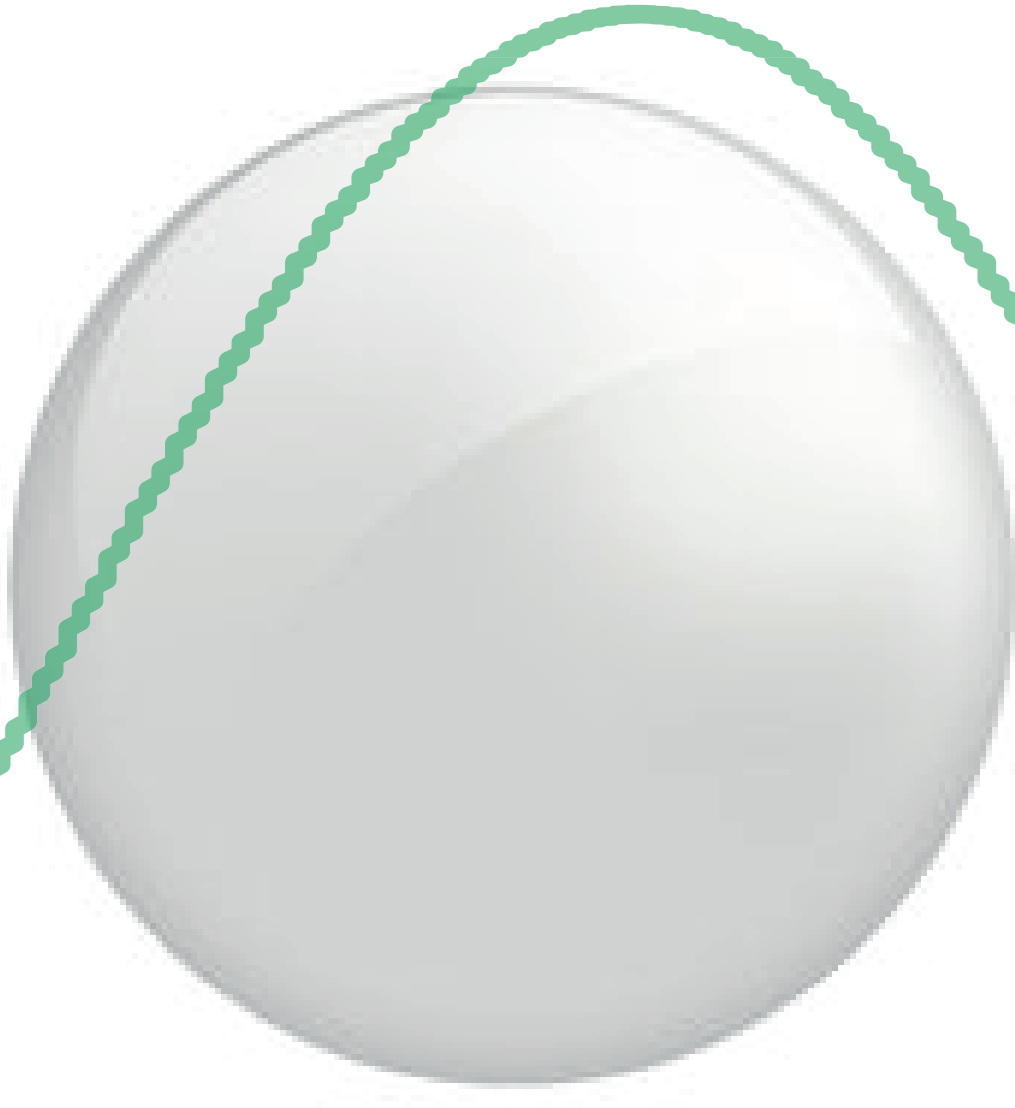
● 200 nm bead



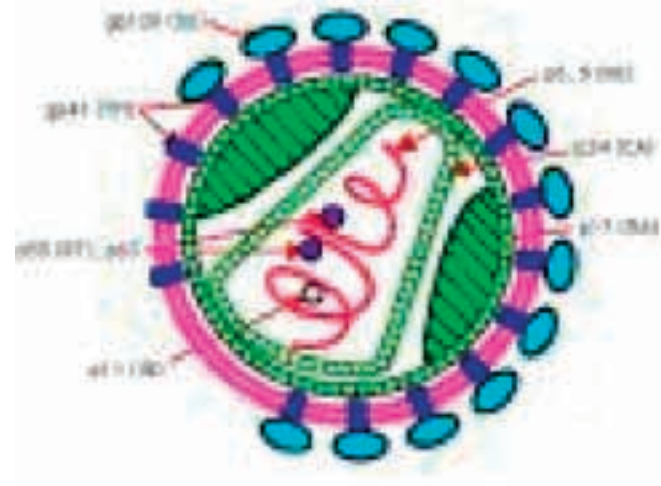
# Sense of Scale



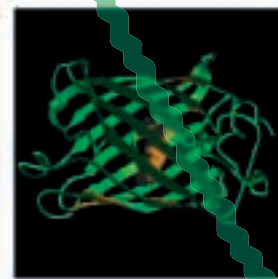
# Sense of Scale



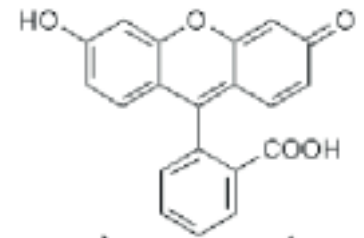
200 nm bead



75 nm Virus Particle



4 nm  
Green Fluorescent  
Protein



2 nm  
Fluorescein  
Molecule

# Modern Microscope Components

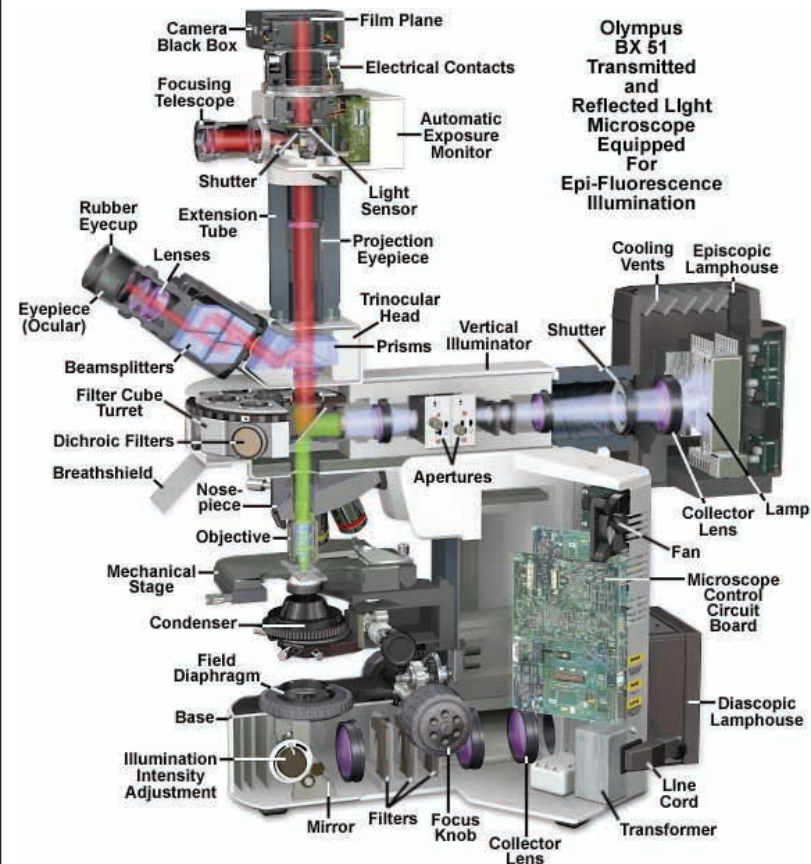


Image from Molecular Expressions webpage

# Modern Microscope Components

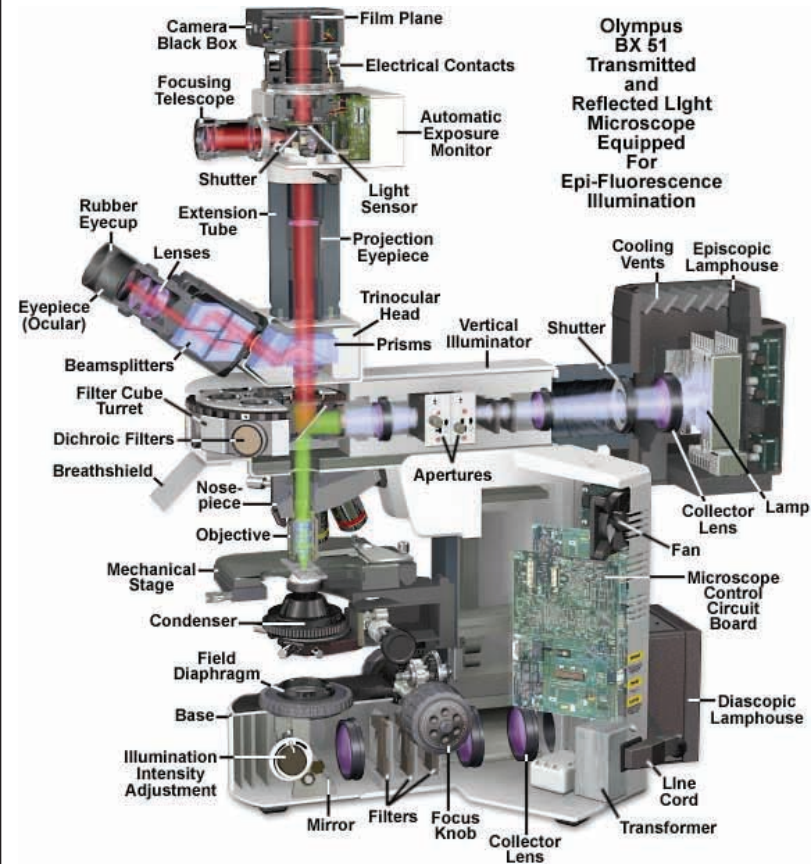


Image from Molecular Expressions webpage

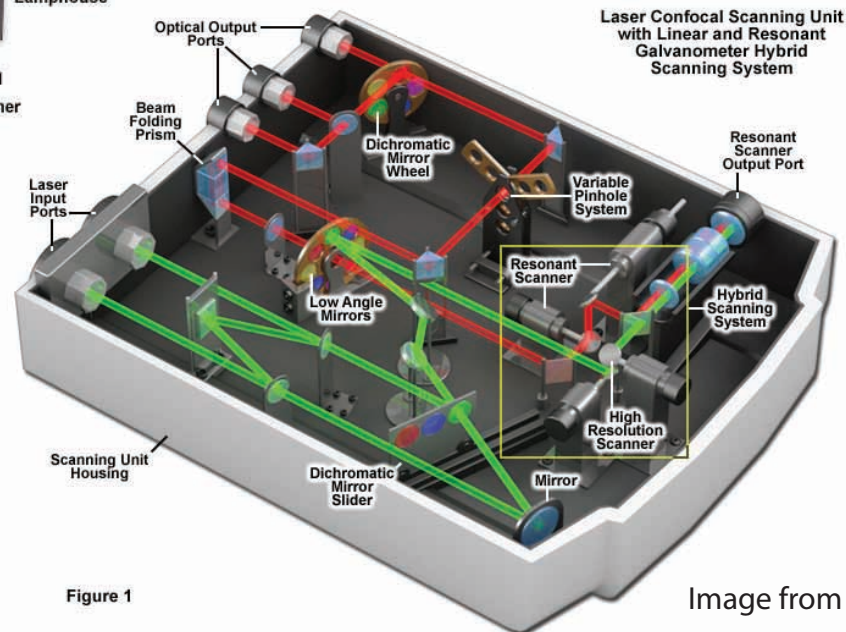


Image from MicroscopyU webpage

Figure 1



# Modern Microscope Components

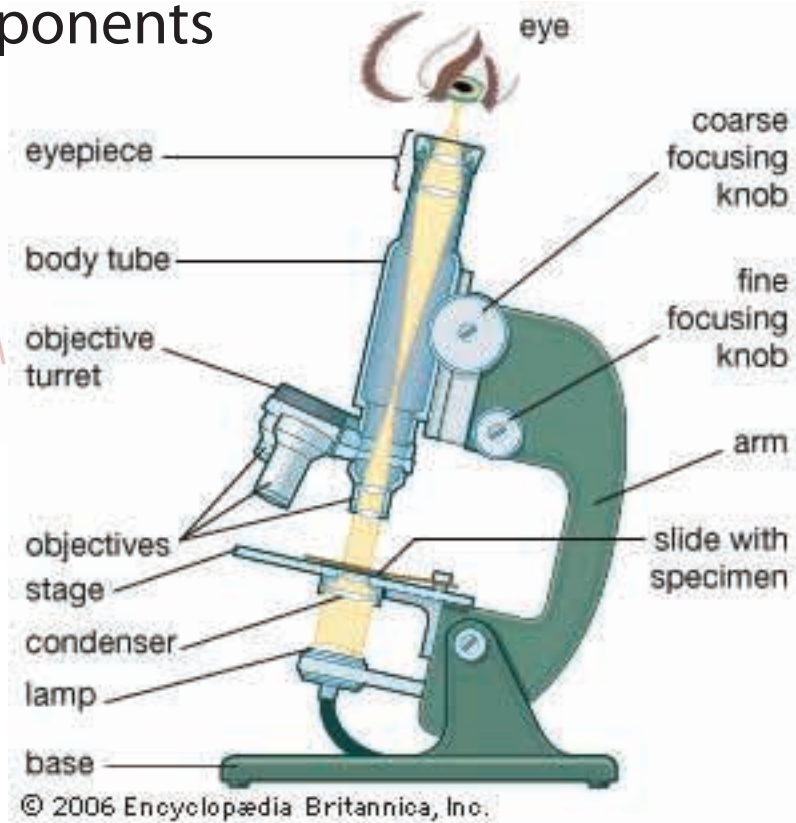
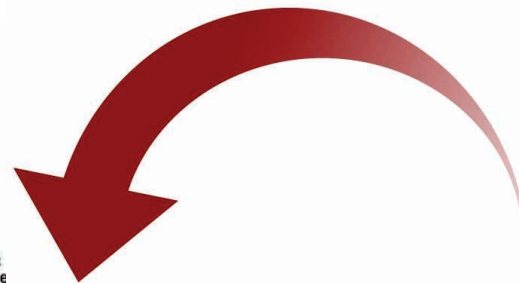
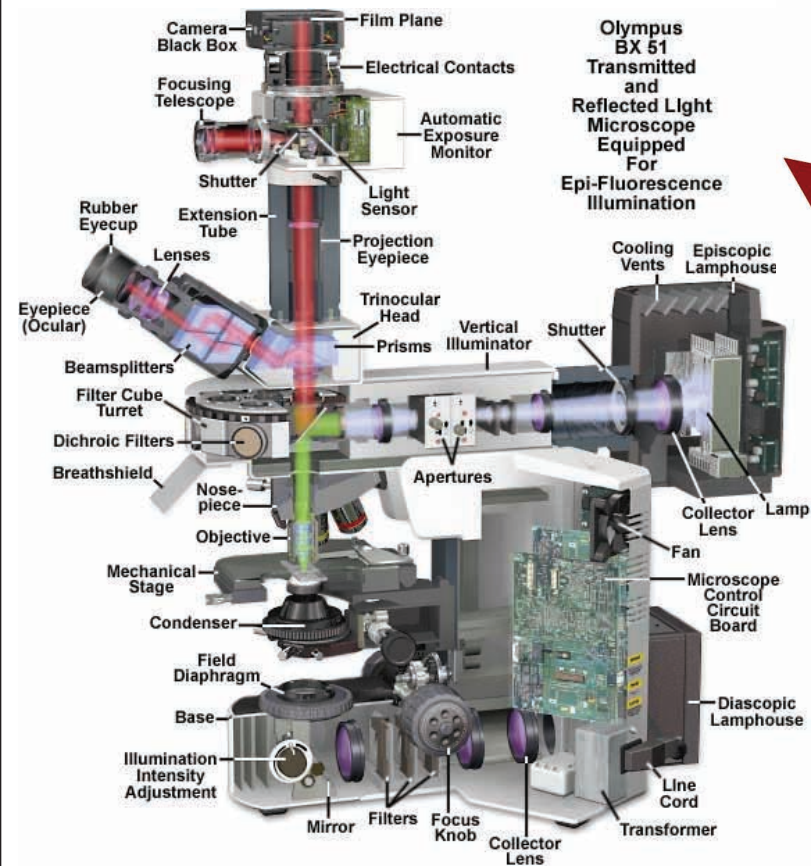


Image from Molecular Expressions webpage

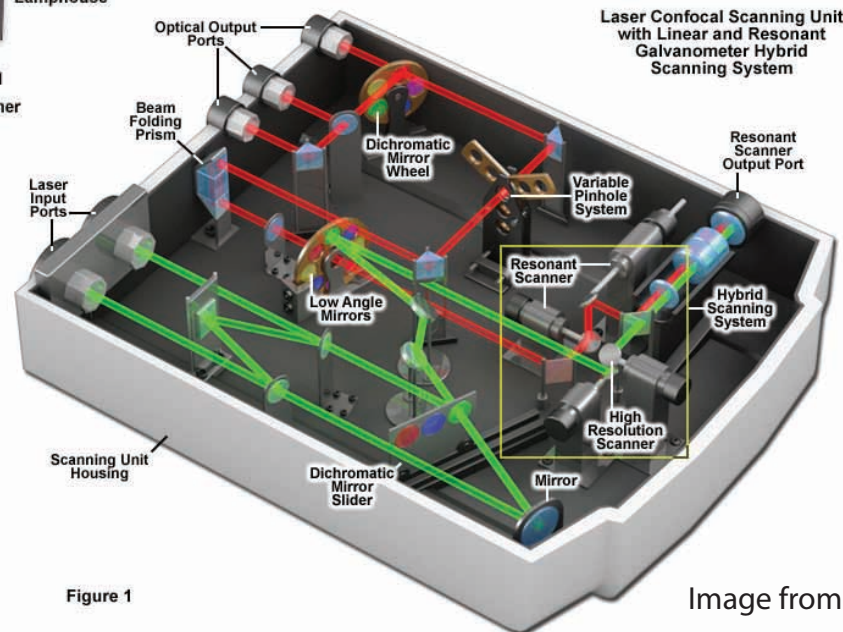
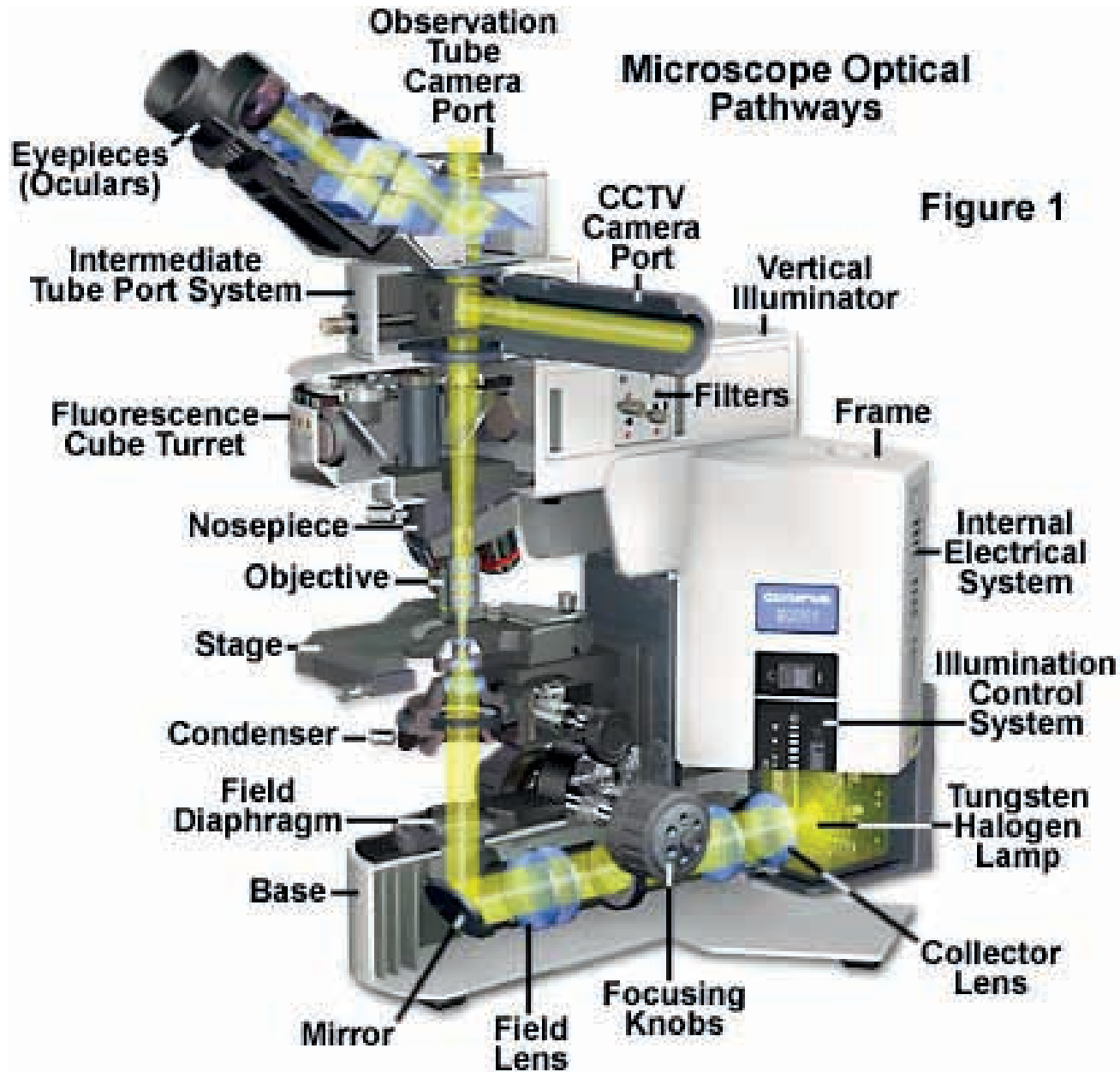


Figure 1

Image from MicroscopyU webpage

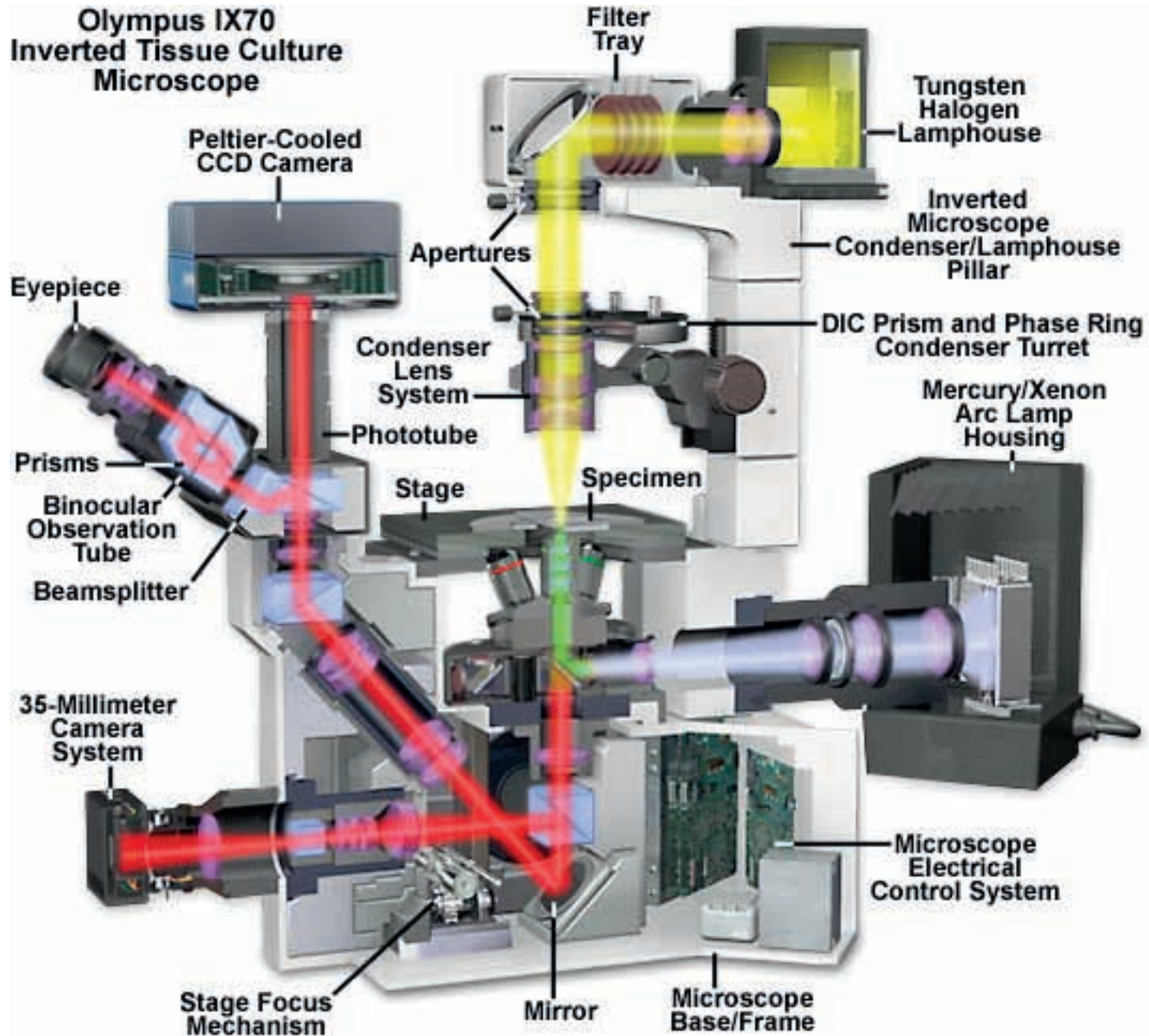
# Kohler Illumination

Light Pathways in an upright microscope



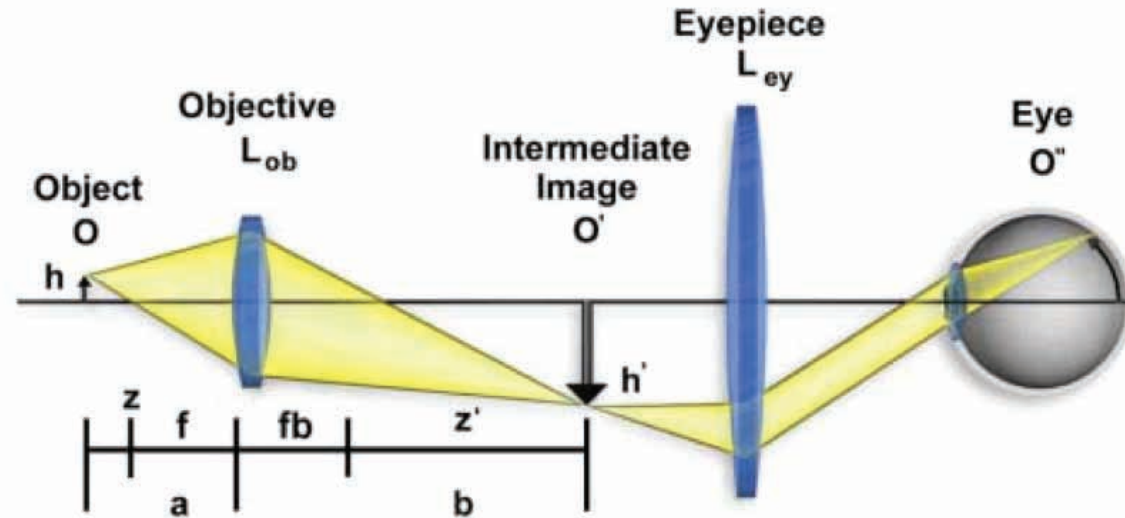
# Kohler Illumination

Light Pathways in an inverted microscope

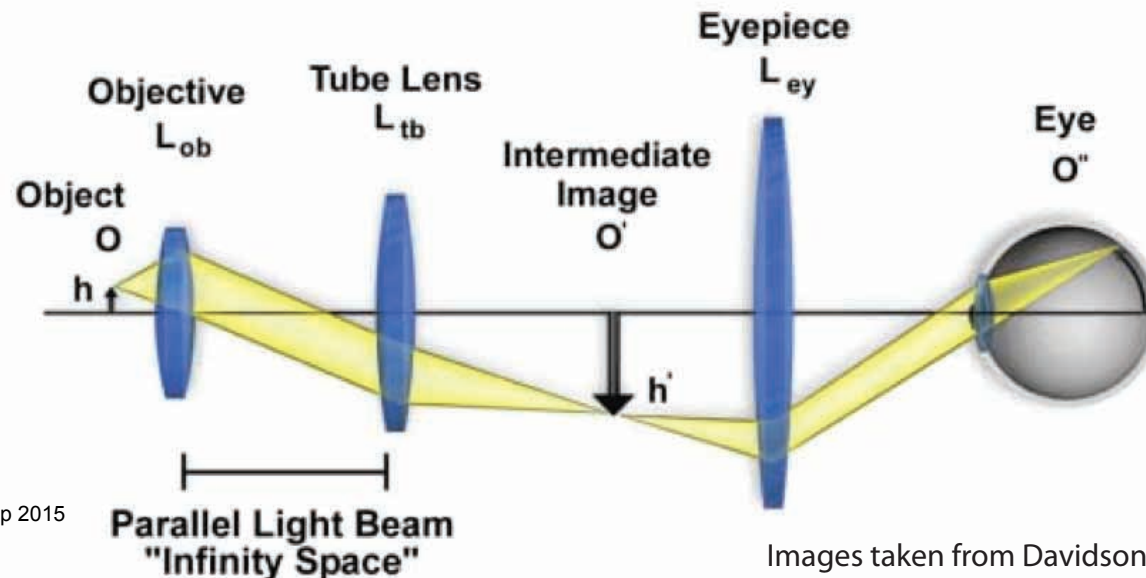


# Infinity-Conjugate vs. Finite-Conjugate Microscopes

## Finite-Tube Length Microscope Ray Paths



## Infinity-Corrected Microscope Ray Paths



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